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Light-triggered nitric oxide (NO) release from photoresponsive polymersomes for corneal wound healing†

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Polymersomes have been extensively used in the delivery of both small and macromolecular payloads. However, the controlled delivery of gaseous therapeutics (e.g., nitric oxide, NO) remains a grand challenge due to its difficulty in loading of gaseous payloads into polymersomes without premature leakage. Herein, NO-releasing vesicles could be fabricated via the self-assembly of NO-releasing amphiphiles, which were synthesized by the direct polymerization of photoresponsive NO monomers (abbreviated as oNBN, pNBN, and BN). These monomers were rationally designed through the integration of the photoresponsive behavior of *N*-nitrosoamine moieties and the self-immolative chemistry of 4-aminobenzyl alcohol derivatives, which outperformed conventional NO donors such as diazeniumdiolates (NONOates) and *S*-nitrosothiols (SNOs) in terms of ease of preparation, stability of storage, and controllability of NO release. The unique design made it possible to selectively release NO by a light stimulus and to regulate the NO release rates. Importantly, the photo-mediated NO release could be manipulated in living cells and showed promising applications in the treatment of corneal wounds. In addition to delivering NO, the current design enabled the synergistic delivery of NO and other therapeutic payloads by taking advantage of NO release-mediated traceless crosslinking of the vesicles.

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Introduction

Polymersomes (also known as polymeric vesicles) with morphological similarities to cellular membranes and viral capsids have been widely used in artificial cells, drug carriers, imaging agents, and so on, which are characterized by their unique nanostructures containing hydrophilic lumens enclosed with a hydrophobic bilayer membrane.^{1–6} The analogs of polymersomes, liposomes, have been clinically used (e.g., Doxil®) with the capability to optimize the biodistributions and attenuate the side effects of doxorubicin (DOX). Therefore, there is mounting interest in developing polymersome-based

nanotherapeutic agents. In comparison with liposomes, polymersomes exhibited excellent stability yet insufficient permeability, which inhibited the release of encapsulated payloads. To resolve this problem, a plethora of methods such as the design of stimuli-responsive polymersomes,^{7–9} the introduction of channel proteins within bilayers,¹⁰ and post-modification of bilayer membranes¹¹ have been proposed to regulate the permeability of polymersomes.

Nitric oxide (NO), a diatom radical, has been recognized as an important gaseous transmitter in cardiovascular, immune, central nervous systems, and so on.^{12,13} Recently, the therapeutic potential of NO in the treatment of cancers, inflammations, and wounds has attracted much attention.^{14,15} Moreover, polymeric NO donors displayed increased half-lives, optimized biodistributions, and increased therapeutic outcomes.^{16–19} Although both hydrophilic and hydrophobic payloads could be successfully delivered by polymeric vesicles, the delivery of gaseous therapeutics (e.g., NO) using vesicular carriers remains elusive due to the difficulty in loading of gaseous NO into vesicles. To address this problem, NO donors were encapsulated into vesicular assemblies to develop NO-releasing vesicles. For example, a NO-releasing donor, diethylenetriamine diazeniumdiolate (DETA NONOate), and an anticancer drug, irinotecan (CPT-11), were loaded into the aqueous lumen of poly(D,L-lactic-co-glycolic acid) (PLGA) capsules and synergistic

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release of NO and CPT-11 could be achieved. However, premature NO release was observed due to the poor stability of NONOates even at physiological pH.²⁰ Fortunately, the labile NONOates could be selectively caged by diverse protecting groups to minimize spontaneous hydrolysis of NONOates.^{21,22} In this regard, hybrid vesicles loaded with β -galactosidase (β -Gal) were fabricated and the extra addition of the β -galactosylpyrrolidinyldiazoniumdiolate (β -Gal-NONOate) donor into the hybrid vesicles led to enzyme-catalyzed NO release.²³ However, the biomedical applications of this NO-releasing vesicle may be limited by the different *in vivo* distributions of the NO donors and the enzyme-loaded vesicles. Despite some achievements, NO-releasing vesicles were routinely fabricated by loading small molecule-based NO donors into either the hydrophilic (e.g., interior or exterior aqueous medium) or the hydrophobic (e.g., bilayer membrane) domains of vesicular assemblies. However, polymersomes that can directly release NO without the extra loading of small molecule NO donors have not been achieved, which were expected to overcome the drawbacks of previously developed NO-releasing vesicles such as low NO loading contents, premature NO leakage, and uncontrolled bio-distributions of NO donors and catalysts.

On the other hand, we recently proposed a new strategy to concomitantly regulate the stability and permeability of polymersomes using traceless cross-linking chemistry.^{24–26} In this context, highly reactive primary amines could be *in situ* generated within the initially hydrophobic bilayer membranes under specific stimuli through the self-immolative degradation of carbamate linkages. These amine moieties further underwent inter/intrachain amidation reactions, synchronically permeabilizing and cross-linking bilayer membranes. As a result, the synergistic release of payloads from both the aqueous lumens and bilayer membranes could be obtained without the disintegration of vesicles. We surmised that if the traceless crosslinking process could be activated by the triggered NO release, the co-release of NO and other payloads could be possibly achieved. To this end, it is of crucial importance to develop stimuli-responsive NO donors that could be coupled with self-immolative chemistry. We hypothesized that light irradiation could be a potential trigger because of the spatio-temporal precision of the light stimulus. Moreover, light irradiation has been previously employed to regulate the NO release from photoresponsive NO donors.^{27–32} For example, *N*-nitrosoaniline-based NO releasers have been designed and photo-triggered NO release could be achieved by the homolysis of N–NO bonds.^{33–38} The resulting aniliny radicals can be reduced *in situ* to form the corresponding aniline derivatives.^{33,39–41} Note that aniline derivatives (e.g., 4-aminobenzyl alcohol) have been extensively used to fabricate self-immolative linkers.^{42–44} Therefore, if the amine group of 4-aminobenzyl alcohol (ABA) could be caged by NO with the formation of photoresponsive *N*-nitrosoamine residues, the photo-triggered cleavage of the N–NO bond could likely give rise to the reformation of an intact ABA intermediate and the activation of traceless cross-linking reactions.

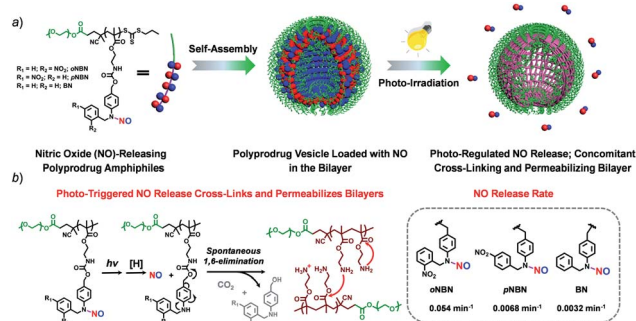
In this work, we synthesized three kinds of *N*-nitrosoaniline-based NO donors (abbreviated as *o*NBN, *p*NBN, and BN) by

nitrosation of 4-aminobenzyl alcohol-based precursors. Unlike conventional NONOate- and SNO-based donors with poor thermo-stabilities, these NO donors can be directly polymerized into amphiphilic block copolymers *via* reversible addition–fragmentation chain transfer (RAFT) polymerization. The resulting amphiphiles self-assembled into diverse nanostructures (e.g., vesicles) with NO loading contents of $\sim 2 \mu\text{mol mg}^{-1}$. Importantly, the NO release rates could be drastically tuned and the photo-triggered NO release could spontaneously activate the traceless cross-linking reactions, cross-linking and permeabilizing the bilayer membranes (Scheme 1), which can be further used to modulate the release of encapsulated payloads.

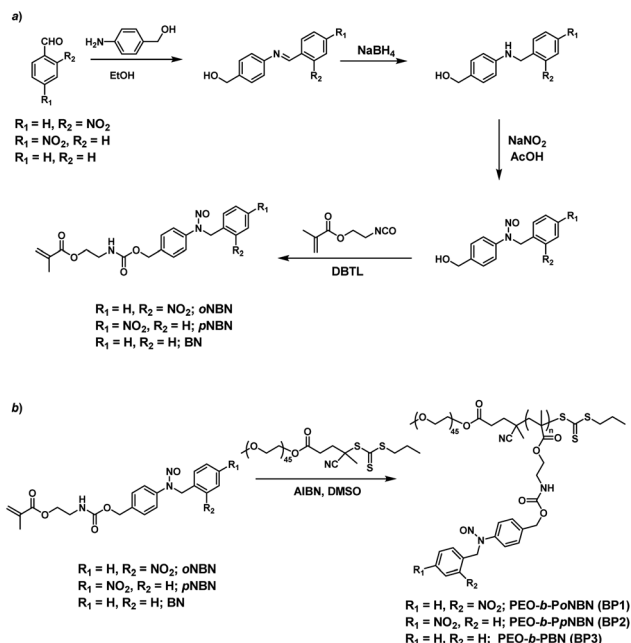
Results and discussion

Synthesis and characterization of NO prodrug monomers

We proposed a facile route to synthesize NO-releasing monomers. First, Schiff bases were formed through equivalent mixing of the corresponding benzaldehydes and 4-aminobenzyl alcohol in ethanol, and the resultant Schiff bases can be readily separated by filtration and no further purification procedures were applied. The Schiff bases were subsequently reduced with sodium borohydride (NaBH_4) and the generated aniline derivatives were treated with sodium nitrite (NaNO_2) and glacial acetic acid at room temperature, giving rise to the corresponding nitrosated precursors. Finally, the hydroxyl groups were functionalized with 2-isocyanatoethyl methacrylate to afford the targeted monomers (*o*NBN, *p*NBN, and BN; Scheme 2a). Notably, the entire synthesis processes were implemented at room temperature and no harsh reaction conditions and tedious separation protocols were involved. In sharp contrast, the preparation of conventional NO donors (e.g., NONOates and SNOs) suffered from either tough reaction conditions (e.g., high pressure) or tedious purification procedures.¹² The chemical structures of the intermediates and the named monomers were unequivocally identified by nuclear magnetic resonance (NMR)



Scheme 1 (a) Schematic illustration of the formation of vesicles assembled from NO-releasing amphiphiles. The resulting vesicles encompass photoresponsive *N*-nitrosoamine moieties within the bilayer membranes shielded by hydrophilic PEO coronas. (b) Under light irradiation, the cleavage of N–NO bonds induces the 1,6-elimination reaction with the release of primary amine groups that further undergo inter/intrachain amidation reactions, concomitantly cross-linking and permeabilizing the bilayers.



Scheme 2 Synthetic routes of (a) NO-releasing monomers, *o*NBN, *p*NBN, and BN and (b) amphiphilic diblock copolymers (BP1–BP3) through RAFT polymerization.

spectroscopy, electrospray ionization mass spectroscopy (ESI-MS), and high-performance liquid chromatography (HPLC) (Fig. S1–S8†).

With *o*NBN, *p*NBN, and BN monomers in hand, we first verified the thermo-stabilities of the three monomers. To avoid thermo-induced polymerization of the monomers, the hydroxyl-terminated precursors were evaluated. Upon heating the three monomers at 70 °C (a typical reaction temperature for RAFT polymerization) for up to 24 h, we did not observe any changes in the HPLC elution profiles (Fig. S9†), suggesting excellent thermo-stabilities of the synthesized monomers; however, NONOate- and SNO-based NO donors have low thermo-stability and have to be stored at low temperature.¹² Next, we verified whether the three monomers could release NO under light irradiation. Upon irradiating the three monomers with a handheld UV lamp (365 nm, ~4 mW cm⁻²; the irradiation intensity remained constant in all the experiments unless otherwise noted), progressive changes in the UV-vis absorbance spectra were observed for all the monomers. This result suggested that all three monomers were responsive to light irradiation (Fig. S10†). The evolution of absorbance intensities at 251 nm (for *o*NBN), 258 nm (for *p*NBN), and 254 nm (for BN) could be fitted by the first-order kinetics ($R^2 > 0.97$); the apparent photolysis rate constants (k_{obs}) were calculated to be ~0.1 min⁻¹, 0.013 min⁻¹, and 0.0023 min⁻¹, respectively. The k_{obs} of two control samples, *N*-(2-cyanobenzyl)-*N*-(4-(hydroxymethyl)phenyl)nitrous amide with an electron-withdrawing group and *N*-(4-(hydroxymethyl)phenyl)-*N*-(2-methoxybenzyl) nitrous amide with an electron-donating group, was determined to be 0.0017 min⁻¹ and 0.0016 min⁻¹, respectively (Fig. S11†), which were quite similar to that of the BN monomer

(0.0023 min⁻¹) without any substituent group (Fig. S10e and f†). These results likely ruled out the effect of the substituent groups on modulation of the NO release rates and suggested that the photoresponsive nature of *o*-nitrobenzyl amine played a crucial role in the faster NO release behavior. In addition, we also measured the NO release rate of a previously reported *N*-nitrosoamine-based NO donor, *N,N'*-di-secbutyl-*N,N'*-dinitroso-1,4-phenylenediamine (BNN6), and found that the photolysis process of BNN6 exhibited an apparent rate constant of 0.005 min⁻¹ (Fig. S12†), twenty times slower than that of the *o*NBN donor.³⁵ Note that bis-*N,N*-nitroso-*p*-phenylenediamine (BNN) derivatives have been recognized as high performance caged NO donors³⁴ and have been used in biological systems.^{35,45} Thus, our design by the introduction of photoresponsive *o*-nitrobenzyl moieties adjacent to the *N*-nitrosoamine moieties provided a feasible way to sensitize *N*-nitrosoamine-based NO donors, which may reduce light irradiation exposure when used in biological systems.

To confirm the NO release under light irradiation, a spin trapping agent, 2-phenyl-4,4,5,5-tetramethylimidazoline-1-oxyl-3-oxide (PTIO), was used to *in situ* capture the generated NO radical with the formation of 2-phenyl-4,4,5,5-tetramethylimidazoline-1-oxyl (PTI).⁴⁶ This transition can be easily monitored by electron paramagnetic resonance (EPR) spectroscopy. In the absence of NO-releasing monomers, there were no EPR signal changes after UV light irradiation, suggesting the inert nature of PTIO under light irradiation (Fig. 1a). Moreover, direct mixing of the monomers and PTIO did not change the EPR signals of PTIO either, indicative of no premature NO leakage. However, once shining light on the mixtures of PTIO and NO-releasing monomers, the characteristic EPR signals of PTI were observed and typical EPR spectra were recorded after 20 min (Fig. 1b–d). The above result confirmed that the formation of NO under light irradiation, which was ascribed to the homolysis rather than the heterolysis of N–NO bonds in the NO-releasing monomers, in accordance with a previous conclusion that homolytic cleavage of *N*-nitrosoamine was more energetically favorable.⁴⁷ Density functional theory (DFT) calculation revealed that the N–N bond dissociation energy (BDE) of *o*NBN, *p*NBN, and BN was 20.8 kcal mol⁻¹, 22.0 kcal mol⁻¹, and 32.5 kcal mol⁻¹, respectively (Fig. S13†), revealing that the release of NO from the *o*NBN monomer was easier than from the other two monomers, in good agreement with the kinetic data (Fig. S10†).

Besides the EPR technique, the photo-triggered NO release was observed by the remarkable fluorescence turn-on of a previously reported NO-selective fluorescent probe based on pyronine chromophores (Fig. S14†).⁴⁸ The NO yield was ~92% for the *o*NBN monomer using the standard Griess assay (Fig. 1e), representing a relatively high NO yield as compared to that of previously reported *N*-nitrosoamine-based NO donors.³³ We assumed that the high NO yield was likely ascribed to the enhanced photo-reactivity of the *o*NBN monomer that may avoid adverse side reactions. Moreover, the NO release process could be alternately activated and deactivated by switching on/off the incident light (Fig. 1f), making the spatiotemporal regulation of NO release possible.



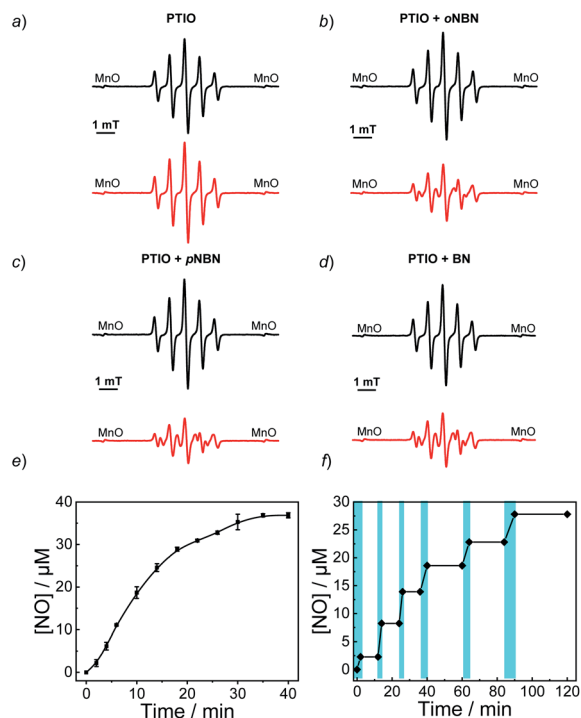


Fig. 1 EPR spectroscopy of aqueous solutions (20 mM PBS buffer containing 20% DMSO, pH 7.4) for (a) PTIO, (b) oNBN with PTIO, (c) pNBN with PTIO, and (d) BN with PTIO before (black lines) and after (red lines) UV 365 nm irradiation (4 mW cm^{-2}) for 20 min. In all cases, the concentrations of PTIO and NO-releasing monomers were $20 \mu\text{M}$. (e and f) NO release profiles of the oNBN monomer ($40 \mu\text{M}$) in an aqueous medium (20 mM PBS buffer containing 5% DMSO) under (e) continuous (mean $\pm$ s.d.; $n = 3$) or (f) intermittent (the cyan areas indicate the light on) UV 365 nm irradiation (4 mW cm^{-2}).

NO-releasing mechanism of the monomers

To unravel the mechanism of photo-induced NO release from the NO-releasing monomers, especially for the oNBN monomer containing both photoresponsive 2-nitrobenzyl amine and *N*-nitrosoamine moieties bonded to the same nitrogen atom, *N*-(2-nitrobenzyl)-*N*-phenylnitrosamine (M1, Fig. S15†) and *N*-benzyl-*N*-phenylnitrosamine control molecules (M3, Fig. S15†) were synthesized. Under identical UV light irradiation (4 mW cm^{-2}), the progressive consumption of M1 and M3 and the simultaneous formation of *N*-(2-nitrobenzyl)aniline (M2) and *N*-benzylaniline (M4) were detected by HPLC, which were identified by comparison with the corresponding authentic samples. Moreover, the reaction rate of M1 was faster than that of M3, in good agreement with the fact that oNBN released NO more quickly than the BN monomer (Fig. S10†). In addition, we found that the M2 intermediate was subjected to a further photolysis reaction with the formation of *o*-nitrosobenzaldehyde (M5) and aniline (M6), which was, however, not observed for M4. Notably, if the cleavage of 2-nitrobenzyl amine moieties proceeded prior to that of *N*-nitrosoamine moieties, nitrogen gas rather than NO would be released.⁴⁹ Although the simultaneous cleavage of *N*-nitrosoamine and 2-nitrobenzyl amine moieties in M1 cannot be completely ruled out, the

primary photolysis process likely followed two steps, namely, the fast cleavage of *N*-nitrosoamine moieties with the release of NO and the relatively slow photo-degradation of 2-nitrobenzyl amine residues, as evidenced by the formation of an M2 intermediate (Fig. S15†). We, therefore, proposed the following reaction mechanism: under light irradiation, *N*-nitrosoamines underwent photolysis and a NO radical was released. The resultant aniliny radical was then reduced to anilines in aqueous solutions.⁴¹ It is worth noting that the formation of aniline derivatives led to spontaneous 1,4- or 1,6-elimination reactions if esters, carbonates, or carbamate linkages were present in the *ortho*- or *para*-positions.⁴⁴

To further elucidate the NO release mechanism of the monomers, a counterpart compound, NB(NO)A, was synthesized (Fig. S16†) and the photolysis process was investigated (Fig. 2a and b). As expected, akin to the M1 donor, the photo-mediated NO release generated an aniliny radical that could be reduced with the formation of a secondary aniline intermediate (*i.e.*, NBA), followed by a spontaneous 1,6-elimination reaction with the release of *N*-(2-nitrobenzyl)-4-aminobenzyl alcohol (A) and 4-nitroaniline (B).⁵⁰ Note the existence of the A intermediate even after the complete consumption of the NB(NO)A donor. This result, once again, confirmed that the photo-degradation of NB(NO)A was composed of a fast NO release process and a relatively slow photolysis process of 2-nitrobenzyl amine derivatives. Indeed, we examined the photolysis process of an authentic A compound and the result revealed an apparent photolysis rate constant of 0.024 min^{-1} (Fig. S17†), whereas the NO release of oNBN had an apparent rate constant of 0.1 min^{-1} (Fig. S8a and b†). The further photolysis of the A compound likely gave rise to the elution peak close to A in Fig. 2b, which was assigned to *o*-nitrosobenzene according to HRMS analysis.⁵¹

Because the oNBN monomer had a comparable chemical structure to the NB(NO)A model compound, the photo-mediated NO release of the oNBN monomer was proposed to

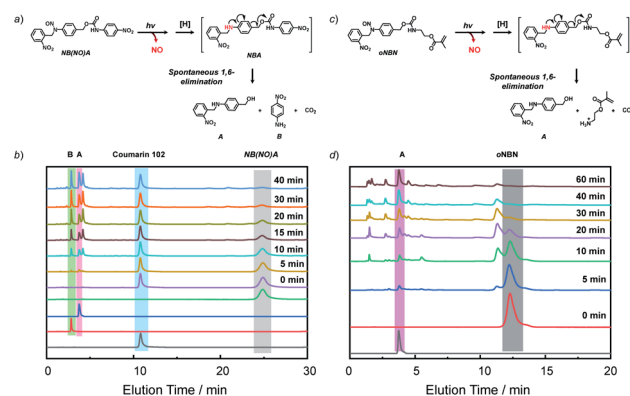


Fig. 2 (a and c) Proposed degradation mechanism of the (a) NB(NO)A model compound and (c) oNBN monomer under light irradiation. (b and d) HPLC profiles recorded at 254 nm for (b) NB(NO)A and (d) oNBN (0.25 mM ; $\text{CH}_3\text{CN}/\text{H}_2\text{O}$, v/v = 1/1 as the eluent) under UV 365 nm irradiation (4 mW cm^{-2}) for varying durations. Coumarin 102 was used as the internal standard in (b).



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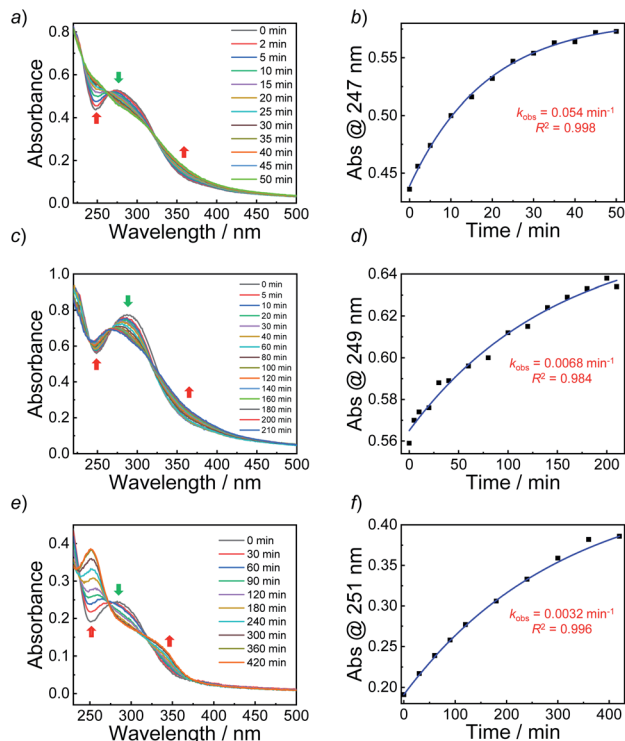


Fig. 4 (a, c and e) Absorbance spectra and (b, d and f) absorbance intensity changes together with a mono-exponential fit of aqueous dispersions (0.1 g L^{-1} , 25°C) of (a and b) BP1 vesicles, (c and d) BP2 vesicles, and (e and f) BP3 micelles under UV 365 nm irradiation (4 mW cm^{-2}).

linking the bilayer membrane through inter/intrachain cross-linking reactions (Scheme 1).^{25,35,53} Because BP1 released NO faster than BP2 and BP3 which could shorten the irradiation period in biological applications, we further investigated the *in vitro* and *in vivo* applications of these NO-releasing materials using BP1 as a representative example.

In vitro and *in vivo* NO release

It is known that NONOate-based NO donors are highly susceptible to acidic pH, while ultrasound could lead to NO release from *N*-nitrosoamine-based BNN6 donors.⁴⁵ In contrast, we found that neither acidic pH nor sonication could trigger the NO release from BP1 vesicles, as evidenced by negligible changes in the fluorescence intensity of the pyronine probe (Fig. S20†). Moreover, BP1 vesicles were relatively stable in the presence of an esterase (0.2 U L^{-1}), fetal bovine serum (FBS), DMEM, and cell lysate, and in a relatively broad pH range (4–8), as evidenced by negligible changes in UV-vis spectra (Fig. S21†). However, photo-mediated NO release could be readily detected using a pyronine probe (Fig. S22†). The generated NO concentration of BP1 vesicles at a concentration of 0.1 g L^{-1} was determined to be $154 \text{ }\mu\text{M}$ (relative to $\sim 82\%$ *N*-nitrosoaniline moieties; Fig. 3d). Moreover, in addition to UV light, we found that visible light (410 nm , 30 mW cm^{-2}) can also activate the NO release process (Fig. S23†). Although there were no significant changes in NO concentrations after irradiation of 365 nm or

410 nm for 30 min , the NO release rates can be tuned by the irradiation wavelengths and intensities. The selective NO release under light irradiation thus made it possible to spatio-temporally control the NO release process, which could be potentially used in localized NO delivery in biological systems. To verify this idea, we monitored the photo-mediated NO release of BP1 vesicles in HeLa cells. Upon incubating BP1 vesicles and a pyronine probe with HeLa cells, we can readily observe red fluorescence of the activated pyronine probe after irradiating the cells with UV light for 20 min , suggesting photo-mediated intracellular NO release. In contrast, the control groups without BP1 vesicles with 20 min irradiation or with BP1 vesicles without irradiation had no detectable red fluorescence under otherwise identical conditions, revealing no spontaneous NO release (Fig. 5).

Given that NO has broad therapeutic functions, we further evaluated the potential use of BP1 vesicles in corneal wound healing by taking advantage of NO in mediating cell proliferation and migration.⁵⁶ A corneal wound model was fabricated by scratching mouse corneas using a surgical blade and the wounded corneas could be stained with fluorescein sodium. We then used the BP1 vesicles as an eye drop for the treatment of the corneal wound. At predetermined time points (every 8 h), an irradiated BP1 dispersion was topically applied to the wounded corneas. Phosphate buffer solution (PBS), non-irradiated BP1 vesicles, and *S*-nitrosoglutathione (GSNO, a commercially available NO donor) were also used for the treatment of the corneal wound. We found that the irradiated BP1-based eye drop with light-controlled NO release gave rise to a faster corneal healing rate than that of PBS and non-irradiated BP1 vesicles. Specifically, after 88 h , the BP1-treated group with light irradiation was completely recovered (Fig. 6). Importantly, we did not observe obvious side effects of the BP1-based eye drop

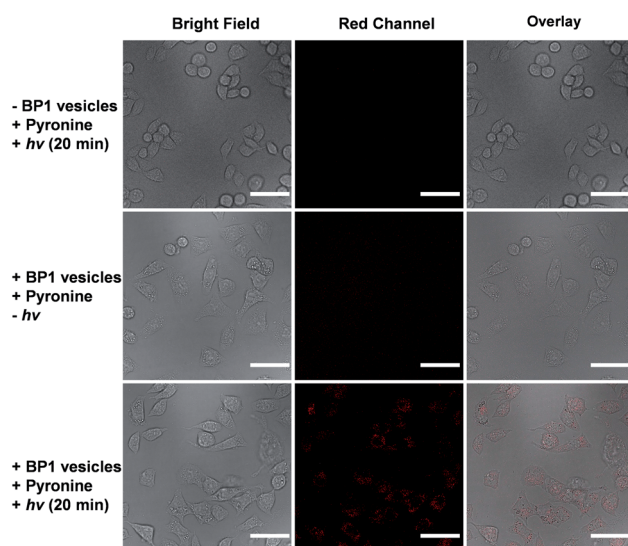


Fig. 5 Confocal laser scanning microscopy (CLSM) images of HeLa cells co-incubated with BP1 vesicles (0.4 g L^{-1}) and a pyronine probe (0.1 mM) without or with irradiation for 20 min . The scale bars are $50 \text{ }\mu\text{m}$.



because the wounded areas were not adversely affected by the non-irradiated **BP1** vesicles, suggesting good biocompatibility of the **BP1** vesicles. Moreover, the irradiated **BP1** vesicles exhibited negligible cytotoxicity as well (Fig. S24d†). Notably, GSNO was known to spontaneously release NO under biological conditions and the GSNO-treated group also exhibited a faster healing performance than the PBS-treated and non-irradiated control group, suggesting that it was the released NO that exerted a positive effect on the corneal wound healing process.

To understand the faster healing processes and explore the potential of the NO-releasable vesicles in the treatment of human corneal wounds, we monitored the migration of human corneal epithelial cells (HCECs) to mimic the corneal healing process using the wound healing assay.⁵⁷ Intriguingly, we observed that the scratch recovery process was highly dependent on the irradiation time (Fig. S24a and b†) and a 10 min irradiation led to a faster healing of the scratch. Quantitative analysis by Griess assay revealed that the nitrite concentrations in the supernatant of cell lysates were positively correlated with the irradiation time. Similarly, a noticeable increase of the nitrite level was observed for cells after GSNO treatment, which confirmed that the light-triggered NO release accounted for the faster wound healing (Fig. S24c†). Notably, there were obvious increases in the cell viability after 20 min irradiation at the tested **BP1** concentrations of 0.05–0.4 g L^{−1}, which became more pronounced upon increasing the incubation time, in agreement with the accelerated wound healing performance

(Fig. S25†). Moreover, the irradiated **BP1** vesicles were nontoxic to HCECs as well at a concentration up to 0.4 g L^{−1} (Fig. S26†). Taken together, the photo-triggered NO release exerted a positive effect on the increased cell migration and viability which may synergistically contribute to the faster corneal healing process (Fig. 6).⁵⁸

Finally, **BP1** self-assembled into vesicular assemblies and the photo-triggered NO release resulted in the formation of cross-linked vesicles with enhanced permeability (Scheme 1). We envisioned that the NO-releasing vesicles can be further employed to encapsulate other therapeutic agents, exerting a synergistic therapeutic effect.¹ Subsequently, we used a polarity-sensitive probe, Nile red (NR), as a model drug to mimic the controlled release behavior of encapsulated payloads. The fluorescence of NR-loaded **BP1** vesicles continuously dropped when subjected to light irradiation, indicative of photo-triggered NR release from **BP1** vesicles. However, there were no changes in NR fluorescence without light irradiation; we did not observe remarkable photobleaching of NR fluorophores either (Fig. S27†). This result encouraged us to fabricate a nanovector for synergistic delivery of NO and chemotherapy drugs. Previous results revealed that NO can reverse the multidrug resistance (MDR) effect of cancer cells, improving the therapeutic performance.⁵⁹ After loading doxorubicin into the aqueous lumens of **BP1** vesicles, we found that the DOX release was highly dependent on the irradiation time. Specifically, less than 15% DOX was released without light irradiation but over 70% DOX was released after 10 min light irradiation (Fig. S28†). Thus, the NO-releasable **BP1** vesicles could be employed for synergistic delivery of NO and DOX, which may exhibit better performance in treating cancers.

Conclusions

In conclusion, we have proposed a direct polymerization approach to fabricate polymeric NO donors through the polymerization of *N*-nitrosoamine-based monomers. These monomers exhibited excellent thermo-stability and were compatible with RAFT polymerization conditions, and outperformed widely used NONOate and SNO donors. Moreover, NO release rates could be efficiently modulated. The RAFT polymerization of the NO monomers led to the formation of well-defined NO-releasing amphiphiles. Intracellular NO release could be achieved by taking advantage of the spatiotemporal precision of light stimuli. Preliminary results demonstrated that the light-mediated NO release from the vesicular assemblies could stimulate corneal wound healing. Moreover, the co-release of NO and chemotherapy drugs can be achieved by means of photo-mediated cross-linking and permeabilization of vesicle bilayers. The screening of other photoresponsive moieties capable of shifting the irradiation wavelengths to the near-infrared (NIR) region without compromising the NO release performance is currently underway.

Conflicts of interest

The authors declare no competing financial interest.

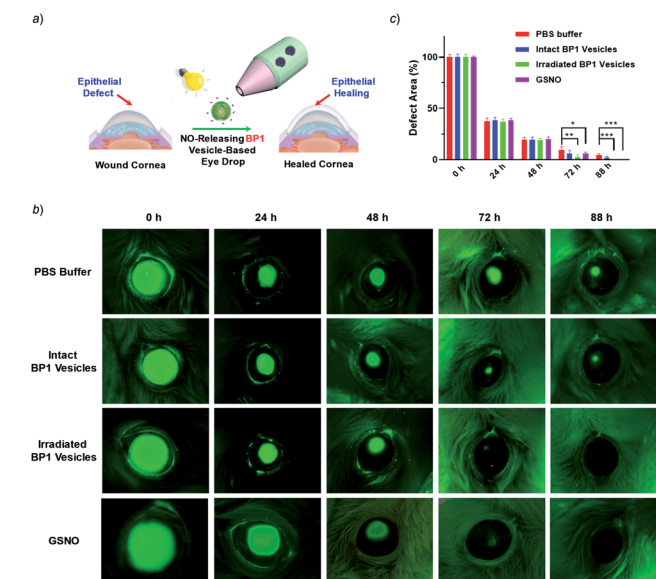


Fig. 6 (a) Schematic illustration of the *in vivo* corneal healing process using NO-releasing **BP1** vesicle-based eye drops. (b) Representative photographs of the wounded corneas treated with PBS buffer, untreated **BP1** vesicles, irradiated **BP1** vesicles, and GSNO, respectively. After each treatment, the corneas were stained with 0.5% sodium fluorescein solution and were imaged by using a Dino-lite hand-held microscope. (c) Quantitative analysis of the wounded areas in (b) using ImageJ software. Values are presented as mean $\pm$ s.d. ($n = 4$). p values were calculated in comparison with the group treated with PBS, ** $p < 0.01$; *** $p < 0.001$.



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