REVIEW

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Magnetic two-dimensional nanocomposites for multimodal antitumor therapy: a recent review

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Magnetic two-dimensional nanocomposites (M2D NCs) that synergistically combine magnetic nanomedicine and 2D nanomaterials have emerged in multimodal antitumor therapy, attracting great interest in materials science and biomedical engineering. This review provides a summary of the recent advances of M2D NCs and their multimodal antitumor applications. We first introduce the design and fabrication of M2D NCs, followed by discussing new types of M2D NCs that have been recently reported. Then, a detailed analysis and discussions about the different types of M2D NCs are presented based on the structural categories of 2D NMs, including 2D graphene, transition metal dichalcogenides (TMDs), transition metal carbides/nitrides/carbonitrides (MXenes), black phosphorus (BP), layered double hydroxides (LDHs), metal organic frameworks (MOFs), covalent organic frameworks (COFs) and other 2D nanomaterials. In particular, we focus on the synthesis strategies, magnetic or optical responsive performance, and the versatile antitumor applications, which include magnetic hyperthermia therapy (MHT), photothermal therapy (PTT), photodynamic therapy (PDT), drug delivery, immunotherapy and multimodal imaging. We conclude the review by proposing future developments with an emphasis on the mass production and biodegradation mechanism of the M2D NCs. This work is expected to provide a comprehensive overview to researchers and engineers who are interested in such a research field and promote the clinical translation of M2D NCs in practical applications.

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Bo Chen

1. Introduction

Tumor treatment has attracted increasing attention in the field of biomedical research due to the complicated and refractory nature of malignant tumors. Conventional approaches, such as chemotherapy and radiotherapy, have struggled to overcome tumor tolerance and metastasis while causing detrimental effects on normal tissues or organs during the therapeutic process.[1] Recently, emerging antitumor technologies, including magnetic hyperthermia therapy (MHT), photothermal therapy (PTT), photodynamic therapy (PDT), drug delivery and multi-modal imaging have attracted great attention.[2,3] However, most of the therapeutic modalities alone appear to be insufficient in adequately addressing the problems, *e.g.*, tumor tolerance, metastasis and off-target effects.[4,5] Multimodal antitumor approaches that combine different therapeutic modalities are regarded as promising strategies for tumor treatment. A desired multimodal therapeutic agent should deliver precise targeting to tumors, prominent inhibition of tumor growth and metastasis, accurate imaging localization, excellent biocompatibility and minimal adverse effects.[6] The burgeoning nanomaterials have led to recent advances in multimodal antitumor nanoagents.[6,7] Theranostic nanoagents with unique properties, including good physiological stability, tailored degradation metabolism routes and optical/thermal/magnetic stimulus-responsive behaviors, have significantly boosted the development of multimodal antitumor therapy.[8]

Two-dimensional nanomaterials (2D NMs) with a unique planar nanostructure exhibit promising characteristics such as high specific surface area, tailored surface and interface properties and tunable band gap.[9] Its 2D nanostructure has rich active sites and can enhance specific physicochemical activities for desired interaction with biosystems, thus holding promise in the antitumor field.[10–12] In recent years, a variety of 2D NMs including graphene oxide (GO), transition metal dichalcogenides (TMDs),[13] 2D transition metal carbides/nitrides/carbonitrides (MXenes),[14] phosphorene (BPNS),[15] layered double hydroxides (LDHs),[9] 2D metal–organic frameworks (MOFs)[16] and 2D covalent-organic frameworks (COFs),[17] have been explored in tumor diagnostics and therapy. For example, BPNS shows remarkable fluorescence and near-infrared (NIR) imaging capabilities and 2D MoS_2 has been employed in two-photon fluorescence (TFP) bioimaging in tumor diagnosis,[18] while MXenes have demonstrated excellent contrast in X-ray computed tomography (CT) imaging.[19] As for tumor treatment, multimodal antitumor therapy comprising PTT and PDT is realized based on 2D NMs-induced cell apoptosis or necrosis.[20,21] BPNSs have been developed as a theranostic system, incorporating doxorubicin (DOX) for chemotherapy and cyanine for NIR imaging, while functionalizing with folic acid to achieve targeted delivery.[22] 2D $MoSe_2$ exhibits multimodal PTT and PDT outcomes, which are significantly higher compared to Au nanoparticles (NPs).[23] Therefore, increasing attention is being paid to 2D NMs for their promising multimodal antitumor therapy.

Magnetic nanomaterials (MNMs) encompass nanoscale dopants or alloys of magnetic metals such as Fe, Co, Ni, Mn, Gd, magnetic metal oxides, and transition metal ferrites.[24] Due to their high magnetic behavior and good biocompatibility, MNMs have been investigated for various biomedical applications,[25] which include magnetic resonance imaging (MRI),[26] magneto hyperthermia therapy (MHT),[27,28] stem cell labeling/tracking, immunotherapies under magnetic guidance, chemodynamic therapy (CDT) and magneto-responsive drug delivery.[29,30] Iron-based magnetic NPs have been granted clinical approval for use in MRI and iron supplements.[31] In our previous work, a magnetic hydrogel complex was designed and fabricated by loading DOX into an iron-based nanodrug of Ferumoxytol, followed by encapsulation in chitosan, and exhibited pH- and temperature-dependent drug release behavior.[32]

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Chunxian Guo

Moreover, MNMs have been found to show exotic intrinsic enzyme-like activities, promoting numerous novel paradigms for tumor therapy.[33–36] For instance, the pyrite nanozyme proposed by Yan *et al.*, exhibits ultrahigh peroxidase (POD)-like and glutathione oxidase-like activities, constituting a self-cascade platform capable of generating abundant •OH and depleting glutathione, and demonstrating more than 3000-fold increase of POD catalytic efficiency than that of natural horseradish peroxidase (HRP).[33] Nevertheless, although they show magnetic and enzyme-like activities, plain MNMs are not suitable for multimodal antitumor therapy because of their relatively low surface area, poor optical and thermal responsive behaviors. Recent efforts have been focused on the design of MNMs-based nanocomposites for improved multimodal anti-tumor performance.

Very recently, magnetic 2D nanocomposites (M2D NCs) that synergistically combine 2D NMs and MNMs have attracted extensive attention because of their promising multi-modal antitumor applications. They have shown unique physicochemical properties, including optical, magnetic, catalytic, and other intriguing characteristics.[37] For example, a magnetic BPNS/MnO_2 nanocomposite was designed as an intelligent self-propelled theranostic platform, showcasing specific tumor-targeting properties, simultaneous pH/redox-responsive MRI performance, and also pH dependent drug release behavior.[38] A magnetic reduced graphene oxide (RGO)-iron oxide (IO) nanocomposite was developed as a T_2-MRI guided PTT therapy platform.[39] Recent advances have been achieved for the design and fabrication of M2D NCs and their multi-modal antitumor applications. Increasingly more researchers and engineers are beginning to get involved in such a research field. However, there still lacks a timely and comprehensive review about this research field.

In this review, we present an overview of the recent advances in M2D NCs and their nanoagents for multimodal antitumor implementation (Fig. 1). Advantages of the synergistic combination of 2D NMs and MNMs into M2D NCs are firstly introduced. Then, we present the design and material fabrication of M2D NCs, including MNMs assembled on 2D NMs, 2D NMs assembled on MNMs, and *in situ* synthesis. Next, we summarize and discuss the multimodal antitumor applications of M2D NCs that are mainly based on 2D graphene and its derivatives, transition metal dichalcogenides (TMDs), transition metal carbides/nitrides/carbonitrides (MXenes), black phosphorus (BPs),

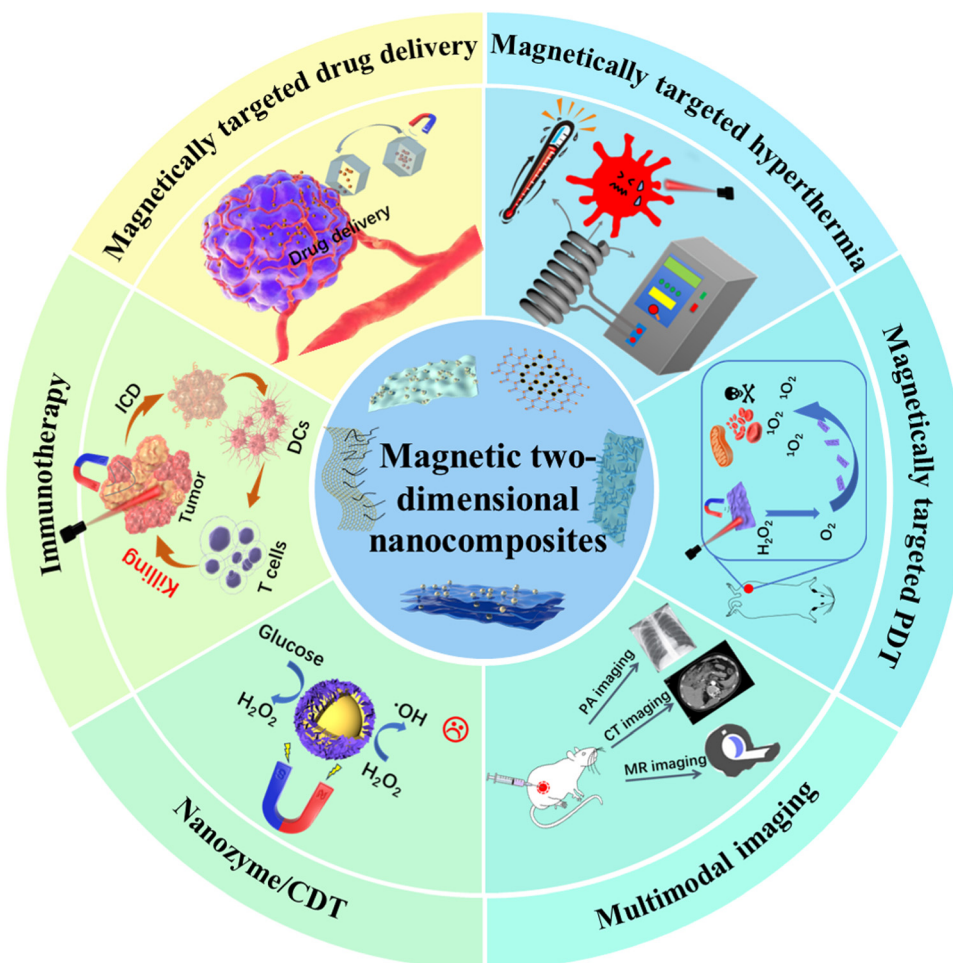Fig. 1 Schematic illustration of the recent advances of magnetic 2D nanocomposites (M2D NCs) and their multimodal tumor therapy and diagnosis.

1406 | *J. Mater. Chem. B*, 2024, **12**, 1404–1428

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layered double hydroxides (LDHs), metal–organic frameworks (MOFs) and covalent-organic frameworks (COFs). In particular, a detailed analysis is conducted on the multimodal applications, including MHT, PTT, PDT, drug delivery, immunotherapy and multimodal imaging. This review concludes by proposing the future development of such a research field with emphasis on the challenges and clinical prospect, including the material customization, exploration of structure-performance relationships, scaling up of the material fabrication, meeting medicinal demand, and elucidating the biodegradation mechanism.

2. Advantages of the combination of 2D NMs and MNMs into M2D NCs

2.1 Advantages and challenges of 2D NMs in antitumor treatment

Despite the successful fabrication of various 2D NMs through diverse approaches and their extensive application in the field of antitumor theranostics, there are still numerous obstacles that hinder their further applications, primarily including interior stability in physiological environments, poor hydrophilicity, non-negligible biotoxicity, off-target manipulation issues, insufficient photoconversion efficacy and others. From a thermodynamic perspective, the 2D structure faces challenges in maintaining a persistent stable state due to its high surface energy resulting from a significant proportion of exposed unsaturated atoms. Thus, it is not suitable for long-term utilization *in vivo*.[40] Secondly, the majority of 2D NMs exhibit a tendency to aggregation in physiological media, potentially causing damage to normal tissues or organs.[41] Additionally, the release of heavy metal ions from the 2D NMs during decomposition *in vivo* may exceed the tolerance levels of human body, and result in detrimental irreversible impacts on healthy regions. Herein, BPNS is used as an example to discuss the advantages and disadvantages of 2D NMs' metabolic stability. On the one hand, BPNS rapidly decomposes after *in vivo* administration, and is eventually transformed into phosphates or phosphonates that can be reabsorbed and reused by the body.[42] This non-toxic metabolic pathway reduces concerns about potential long-term risks. On the other hand, the short metabolic cycle in the physiological environment severely limits its effectiveness on tumor treatment. Upon exposure to air and water, BPNS rapidly collapses, resulting in a significant reduction of the antitumor outcomes. Thirdly, phototherapy alone by virtue of 2D NMs is generally insufficient for complete tumor eradication. Unfortunately, the current PTT regimen is plagued by challenges such as non-uniform heat distribution and suboptimal hyperthermia outcomes, which significantly impede its clinical translation expansion, particularly for deep-seated metastatic tumors.[43,44] As for PDT, the majority of 2D photosensitizers encounter shortcomings involving high dark toxicity, short blood circulation time, hypoxia microenvironment, and other factors, which ultimately lead to unsatisfactory outcomes.[45] Furthermore, it has been demonstrated that single

PDT or PTT alone is inadequate for complete tumor eradication.[43] Based on the aforementioned analysis, there is an urgent need for the development of novel 2D nanocomposites with a multifaceted therapeutic approach to overcome these challenges and significantly enhance tumor treatment efficacy.

2.2 Advantages and challenges of plain MNMs in antitumor applications

Akin to 2D NMs, the clinical implementation of MNMs is hindered by their inadequate treatment regimes, despite the establishment of various MNM types. It should be noted that several challenges remain unresolved, such as the poor delivery efficiency and uncertainties regarding the balance between the dosage security and therapeutic/diagnostic performance.[85,86] For instance, ferritin-modified MNMs have shown promise as an anticancer nano-vector, but further understanding is needed regarding their impact on inflammation, apoptotic body formation, reactive oxygen species (ROS) production and chromosome aggregation.[87] Moreover, improving the colloidal stability and preventing the carrier media aggregation or precipitation in plasma and tissues are crucial for reducing the acute and long-term toxicity.[88,89] Moreover, it has been observed that exposure to ACMF activates the heat-tolerance pathway in melanoma cells treated with MNMs, indicating that the rapid establishment of thermotolerance alone is insufficient for effective tumor ablation.[90] Overall, in order to address the aforementioned critical clinical issues, it is imperative to explore innovative MNMs that exhibit enhanced safety profiles and multifaceted antitumor capabilities. This necessitates expanding the composition and structure of MNMs, with a focus on pioneering breakthroughs in clinical practice.

2.3 Synergetic M2D NCs for multimodal tumor therapy

As summarized in Table 1, it can be clearly observed that advanced magnetic 2D nanocomposites (M2D NCs) present a promising approach to integrate their respective advantages and tackle critical challenges faced by both materials. In fact, the practical implementation of the M2D NCs strategy has demonstrated its efficacy in achieving optimal tumor therapy and imaging Firstly, it is noteworthy that both 2D NMs and MNMs possess flexible surface activities, which enable the convenient construction of diverse nanocomposite structures for specific antitumor scenarios. Well-ordered magnetic nanocomposites prolong degradation and metabolism, ensuring durable stability *in vivo* to maximize their therapeutic effects. Secondly, the integration of individual phototherapy, magnetotherapy and related imaging properties into one platform through the establishment of M2D NCs significantly enhances the convenience and versatility in practice compared to mono materials. It is expected that neither single 2D NMs nor single MNMs can match the optical/magneto responsiveness of M2D NCs based on current studies. Moreover, by employing various modification measures and coupling groups, M2D NCs can serve as stimuli-responsive drug carriers. A variety of

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J. Mater. Chem. B, 2024, **12**, 1404–1428 | **1407**

Table 1 Summary of the advantages of M2D NCs compared to single therapy of 2D NMs in tumor treatment

2D NMs	M2D NCs	Advantages of M2D NCs
GO	GO-IONP-PEG-DOX[46]	Magnetically targeted DOX delivery, localized PTT guided by magnetic field
GO	FeMn-GO[47]	Efficient pH-responsive drug releasing performance and redox-triggered T_1-weighted MRI
GQD	GQD-MMSNs-DOX[48]	pH-responsive DOX delivery and significant synergistic MHT and PTT
GQD	HMNS/SiO$_2$/GQD[49]	Magneto-mechanical and PTT synergetic therapy
GQD	MnFe$_2$O$_4$@SiO$_2$@GQDs/DAU[50]	pH-responsive DAU delivery and fluorescence resonance energy transfer (FRET) system-enhanced apoptosis
GO	MnO$_2$@Pd@PPy/GO[51]	Strong PTT performance, pH-responsive enzymatic and enhanced MRI performance
GQD	Cur/GQDs-Fe$_3$O$_4$-FA[52]	pH-responsive Cur delivery and magnetic targeting delivery
WS$_2$	WS$_2$-IO@MS-PEG-DOX[53]	Triple modal fluorescence, MR and X-ray CT imaging guided PTT
WS$_2$	WS$_2$:Gd^{3+}-PEG[54]	Strong NIR absorbance and X-ray attenuation ability enables contrasts in PA imaging and CT
MoS$_2$	MoS$_2$/Fe$_3$O$_4$[55]	Magnetic targeted PTT, dual-modal probe for T_2-weighted MR and PAT imaging
MoS$_2$	MoS$_2$-IO-PEG[56]	Triple modal PET, PAT, and MRI guided PTT
MoS$_2$	Mo@Fe-ICG/Pt[57]	Enhanced antitumor efficacy of combined PTT, PDT, and chemotherapy triggered by a single 808 nm NIR laser
Ti$_3$C$_2$	MnOx/Ti$_3$C$_2$[58]	Unique tumor microenvironment-responsive T_1-weighted MRI and PTT performance
Ta$_4$C$_3$	MnOx/Ta$_4$C$_3$[59]	TME-responsive T_1-weighted MRI and enhanced PTT
Ti$_3$C$_2$	Ti$_3$C$_2$-IONP-MXene[60]	Enhanced PTT combined with efficient T$_2$-MRI
Ta$_4$C$_3$	Ta$_4$C$_3$-IONP-SPs[61]	Superior PTT effect combined with dual modal CT imaging and T$_2$-MRI
Ti$_3$C$_2$	Ti$_3$C$_2$-Fe$_3$O$_4$@SiO$_2$-FA[62]	pH-dependent drug release and controlled magnetic therapy
Ti$_3$C$_2$	FTC[63]	Superior PTT performance and enhanced MRI
BPNSs	BPs@Au@Fe$_3$O$_4$[64]	Strong tumor inhibition efficacy, MRI-monitored visualized synergistic PDT and PTT
BPNSs	R^e-MnO$_2$-F^{f}BP[65]	MR/FL dual-modal imaging, continuous local O$_2$ supply to overcome hypoxia for enhanced PDT
BPNSs	BPN/MnO$_2$/DOX[38]	pH and redox-responsive MRI, synergistically enhanced PTT, PDT, and chemotherapy
BPNSs	MUCNPs@BPNS-Ce6[66]	Activated PTT and PDT under a single irradiation light of 808 nm
BPNSs	BPNS-Arg-GOx@MnO$_2$ (BAGM)[67]	Reinforced synergistic PTT/starvation therapy/NO gas therapy triggered by the cascade reaction
BPNSs	RGD-BPNS@SMFN[15]	Target-deliverable PTT–PDT self-synergetic therapy, temperature-dependent catalase (CAT)-like behavior
BPQDs	BPQDs@DOX@ss-Fe$_3$O$_4$@C-EGFR NPs[68]	pH/NIR/GSH-responsive DOX delivery combined with augmented PTT effect
MgAl-LDH	LDH-Gd/Au[69]	pH-responsive DOX delivery, dual modal CT and T_1-MR imaging performance
MgAl-LDH	Mn-LDH[70]	Targeted MR imaging
MgAl-LDH	MnFe-LDH-MTX[71]	Strong magnetic responsibility and pH-responsive MTX delivery
MnAl-LDH	Mn-LDH-siRNA[72]	Effective anticancer drug/gene delivery and T$_1$-MRI for theranostics
CaAl-LDH	LDHs/Fe$_3$O$_4$@dextran/DOX[73]	pH-responsive DOX delivery and magnetic controlled drug release
MgAl-LDH	FA-BSA/Fe$_3$O$_4$@LDH/5-Fu[74]	Efficient magnetic responsiveness, pH-responsive 5-Fu delivery
ZIF-8	Fe$_3$O$_4$/ZIF-8-Au$_{25}$[75]	Magnetically targeted PDT/PTT triggered by single 808 nm laser
Mn-MOF	Mn$_3$O$_4$-PEG@C&A[76]	Glutathione consumption and O$_2$ supply by CAT-like activity of Mn$_3$O$_4$ for enhancing PDT efficacy
Co-Fc MOF	Co-Fc@GOx[77]	Cascade enzymatic/Fenton catalytic, versatile and effective drug delivery
ZIF-8	Fe@ZIF-8@GOx[78]	Magnetic enhanced cellular uptake and cascade enzymatic/Fenton catalytic ROS generation
COF	Fe$_3$O$_4$@COF-DhaTph[79]	Significant PTT and PDT effect, triple-modal MRI/PAI/NIRI
COF	COF-Au–MnO$_2$-HA[80]	Highly efficient cascade reactions and T_1-weighted MRI
COF	Fe$_3$O$_4$@COF-BSA-FA[81]	Highly efficient targeted drug delivery with excellent PTT and magnetic performance
BNNs	Pd@OH-BNNSs/DOX[82]	pH/GSH/NIR-responsive delivery and synergetic CDT and PTT
FePSe$_3$	FePSe$_3$@APP@CCM[83]	Multifunctional synergetic combination of MRI and PAI, PTT and immunotherapy
g-C$_3$N$_4$	C$_3$N$_4$-Fe-TPP NF/MB[84]	Superior PDT performance and effective T_1-weighted MRI

hydrophobic chemotherapeutic drugs, including camptothecin (CPT),[39,91] DOX,[92–94] 1,3-bis(2-chloroethyl)-1-nitrosourea (BCNU) ellagic acid[95] and β-lapachone[96] have been successfully conjugated covalently or non-covalently adsorbed onto of M2D NCs with considerable capacity. These conjugates exhibit well-controlled release behavior in response to external stimuli, such as laser and magnetic field.[97] Rational surface modification can further enhance the targeting ability and stability of M2D NCs, while simultaneously mitigating their side effects. This approach aligns well with clinical demands. Lastly, a rational and comprehensive nanocomposite may give rise to more extraordinary biological machinery that directly impacts the therapeutic and imaging performance. Notably, innovative therapeutic modalities such as cascade-augmented nanozymes and self-advanced intelligent nanoreactors have been established in advanced M2D NCs.[98–101] Collectively, it is evident that the construction of M2D NCs significantly leverages the inherent properties of both materials to address challenging issues, and shows great potential as a tumoricidal therapy option that has garnered significant interest, boosting research on novel theranostic modalities.

1408 | J. Mater. Chem. B, 2024, 12, 1404–1428

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3. Design and material fabrication of multifunctional M2D NCs

As illustrated in Fig. 2, a variety of M2D NCs have been developed in recent years for antitumor applications. Material fabrication strategies for the 2D NMs can be categorized into top-down and bottom-up routes, which mainly involve hydrothermal/solvothermal methods,[102,103] chemical vapor deposition (CVD),[104,105] liquid phase exfoliation,[106,107] mechanical stripping,[108,109] and electrospinning methods.[110,111] Meanwhile, commonly employed methods for the synthesis of MNMs include co-precipitation, microemulsion and thermal decomposition.[110,112,113] Both 2D NMs and MNMs synthesized in their original forms offer fascinating modification flexibility, enabling convenient tailoring of the multitudinous M2D NCs structure.[114,115] To date, numerous strategies have been developed for the construction of advanced M2D NCs,[41,101,116] which can be broadly categorized into two approaches, namely, post-synthetic surface modification and in situ growth of one on the other.[91,112] The former involves assembly of the two materials, while the latter typically results in a more stable structure through in situ growth. Hereinafter, we classify various composite structures based on the aforementioned pathways as post-synthetic modification type, including MNM@2D NM composites and 2D NM@MNM composites, and in situ synthesis method.

3.1 Synthesis of MNMs on the 2D NMs composite (MNMs@2D NMs)

In this approach, pre-synthesized 2D NMs serve as a robust scaffold, offering abundant binding sites for the growth or modification of MNMs (Fig. 3A). Generally, 2D NMs are initially prepared through either bottom-up or top-down processes, and subsequently functionalized with MNMs via covalent or non-covalent linkages. Covalent bonding is commonly achieved through radical reactions, cycloaddition reactions, or by introducing oxygen-containing functional groups. Non-covalent modifications are typically achieved through hydrophobic and van der Waals forces, electrostatic interactions, hydrogen bonding, and π–π stacking interactions.[112] For instance, Akshaya et al. reported a facile one-pot hydrothermal synthesis method for preparing polymer-stabilized IONP-graphene drug carriers.[117] Ma et al. synthesized a functionalized graphene oxide (GO)–iron oxide nanocomposite by anchoring paramagnetic iron oxide nanoparticles (IONP) and chemotherapeutic drug DOX onto the surface of graphene, then wrapping it with polyethylene glycol (PEG).[46] The as-obtained GO-IONP-PEG-DOX serves as a multifunctional cancer treatment platform that combines magnetic targeting drug delivery, chemotherapy, and MHT. Shadie et al. synthesized a GO/Co nanocomposite by using GO as the carrier material and assembling cobalt NPs with a size of around 15 nm on the surface of GO.[118] This approach is well-suited for loading MNMs of small size onto 2D NMs with a substantial surface area, representing a form of surface passivation strategy. The presence of abundant magnetic particles covering the 2D NMs mitigates rapid decomposition. Furthermore, this method facilitates the anchoring of other molecules or functional materials, thereby extending its applicability.

3.2 Synthesis of 2D NMs on the MNMs composite (2D NMs@MNMs)

In this approach, pre-synthesized MNMs serve as the scaffold for loading or bonding with 2D NMs (Fig. 3B). It is important to note that these MNMs must be functionalized with capping agents or active groups before 2D NMs can grow or anchor onto their surface through covalent linkage, hydrogen bonding, electrostatic interactions, π–π stacking, and other physicochemical mechanisms.[112] Yao et al. fabricated a novel magnetic nanocarrier based on graphene oxide (GO) through the following steps: magnetic mesoporous $Fe_3O_4@SiO_2$ NPs were first prepared via solvothermal method and encapsulated with DOX in the silica shell, followed by grafting of amino-functionalized graphene quantum dots (GQDs) onto the outermost layer of the $Fe_3O_4@SiO_2$ NPs to form the nanocomposite (Fig. 3A).[48] Analogously, Zhang et al. developed pH/NIR/GSH-responsive BPQD-$Fe_3O_4@C$ nanocarriers through disulfide cross-linking (ss-$Fe_3O_4@C$ NCs) using black phosphorus quantum dots (BPQDs) as a capping agent in a one-step method, similar to the aforementioned technology. This approach allows for easy manipulation to obtain M2D NCs.[68] This approach is suitable for loading small-sized 2D NMs, such as QDs and NPs, onto MNMs with a larger diameter. As MNMs occupy the core of the nanocomposite, this material consistently exhibits superior
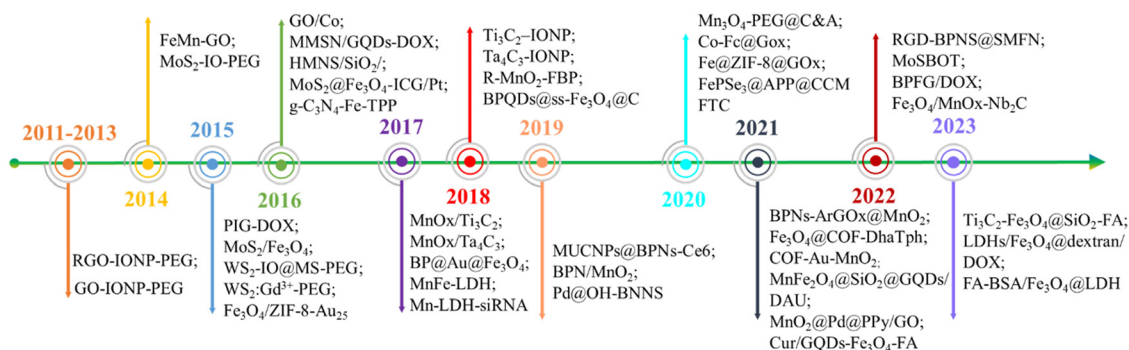

Fig. 2 A brief timeline of the development of M2D NCs in the applications of antitumor field.

Timeline entries:

2011-2013
- RGO-IONP-PEG;
- GO-IONP-PEG

2014
- FeMn-GO;
- MoS₂-IO-PEG

2015

2016
- PIG-DOX;
- MoS₂/Fe₃O₄;
- WS₂-IO@MS-PEG;
- WS₂:Gd³⁺-PEG;
- Fe₃O₄/ZIF-8-Au₂₅

- GO/Co;
- MMSN/GQDs-DOX;
- HMNS/SiO₂/;
- MoS₂@Fe₃O₄-ICG/Pt;
- g-C₃N₄-Fe-TPP

2017

2018
- MnOx/Ti₃C₂;
- MnOx/Ta₄C₃;
- BP@Au@Fe₃O₄;
- MnFe-LDH;
- Mn-LDH-siRNA

- Ti₃C₂–IONP;
- Ta₄C₃–IONP;
- R-MnO₂-FBP;
- BPQDs@ss-Fe₃O₄@C

2019
- MUCNPs@BPNs-Ce6;
- BPN/MnO₂;
- Pd@OH-BNNS

- Mn₃O₄-PEG@C&A;
- Co-Fc@Gox;
- Fe@ZIF-8@GOx;
- FePSe₃@APP@CCM
- FTC

2020

2021

2022
- BPNs-ArGOx@MnO₂;
- Fe₃O₄@COF-DhaTph;
- COF-Au-MnO₂;
- MnFe₂O₄@SiO₂@GQDs/DAU;
- MnO₂@Pd@PPy/GO;
- Cur/GQDs-Fe₃O₄-FA

- RGD-BPNS@SMFN;
- MoSBOT;
- BPFG/DOX;
- Fe₃O₄/MnOx-Nb₂C

2023
- Ti₃C₂-Fe₃O₄@SiO₂-FA;
- LDHs/Fe₃O₄@dextran/DOX;
- FA-BSA/Fe₃O₄@LDH

Fig. 3 Schematic illustration of the synthesis strategies for advanced multifunctional M2D NCs. (A) Synthesis of 2D NMs on the MNMs composite (2D NMs@MNMs). (B) Synthesis of 2D NMs on the MNMs composite (2D NMs@MNMs). (C) ① *In situ* synthesis of MNMs on 2D NMs; ② *In situ* synthesis of 2D NMs on MNMs.

magnetic performance compared to alternative structures. Additionally, the small 2D NMs are shielded from rapid degradation by anchoring onto MNMs.

3.3 Synthesis of *in situ* growth of one on the other

In addition to the aforementioned composite structure type and synthetic pathways, it is also plausible that *in situ* synthesis of MNMs (Fig. 3C1) or 2D NMs (Fig. 3C2) onto the other one forms a nanohybrid. Liu *et al.* achieved the *in situ* growth of superparamagnetic Fe_3O_4 NPs on the surface of Ta_4C_3 by redox reaction, followed by coating with soybean phospholipids (SP) to prepare Ta_4C_3-IONP-SPs nanocomposites that exhibited superior performance in PTT therapy and NIR imaging.[61] $MnFe_2O_4$-MOFs nanocomposites were synthesized *via in situ* growth of MOFs on the surface of $MnFe_2O_4$ NPs. Initially, $MnFe_2O_4$ NPs were prepared through the thermal decomposition of metal acetyl acetone precursors, and subsequently modified with polyvinylpyrrolidone (PVP). Subsequently, PVP-modified $MnFe_2O_4$ was utilized as the supporting material to selectively adsorb Zr^{4+} ions and tetranuclear (4-carboxyphenyl) porphyrin (TCPP), facilitating the growth of MOFs on its surface and resulting in the formation of a well-defined nanocomposite structure (Fig. 3B).[119] This strategy affords a diverse composite structure for M2D NCs, unconstrained by the intrinsic structure of single MNMs or 2D NMs. Through well-designed chemical reactions, these materials demonstrate a more controllable synthesis, a more stable composition, and a more ordered structure. The myriad structures enhance the versatility of M2D NCs, significantly amplifying their effectiveness and broadening their range of applications.

4. M2D NCs and their multimodal antitumor applications

After the meticulous design and construction, advanced M2D NCs not only exhibit enhanced optical/magnetic performance compared to their individual components, but also demonstrate synergistic effects that lead to unexpected biological responses or exotic behaviors in the tumor microenvironment (TME), thus opening up new avenues for antitumor nanotechnologies. In this section, we systematically elucidate different types of M2D NCs used for tumoricidal purposes based on their structure categories of 2D NMs (Table 2), incorporating our innovative ideas in devising fabrication processes and therapeutic/imaging modalities, as well as highlighting their remarkable antitumor advantages.

4.1 Magnetic 2D graphene nanocomposites and their multimodal antitumor applications

Due to their inherent distinctive physical and chemical properties, graphene and its derivatives, as the most popular two-dimensional sp^2 carbon NMs, have been extensively utilized in biosensing, bioimaging, drug/gene delivery and various types of cancer therapies.[47] Graphene oxide (GO) has been more frequently employed than graphene in constructing nanocomposites due to its better stability in physiological environments. When a magnetic component is elaborately introduced into GO-based materials, the resulting magnetic nanocomposites acquire additional magnetic responsive properties that extend antitumor applications, such as magnetic field-enhanced

Table 2 Summary of representative advanced M2D NCs for tumor therapy and imaging based on the components of 2D NMs

2D NMs type	M2D NCs	Type of tumor	Therapeutic modalities	Imaging modalities	Stimulus source
GO	GO-IONP-PEG-DOX[46]	4T1 tumor	PTT/magnetically targeted drug delivery	MRI	Static magnetic field/808 nm laser
	FeMn-GO[47]	MCF-7/ADR/MDA-MB-231 tumor	MHT/chemotherapy	MRI	Alternating magnetic field/pH
	RGO-IONP-PEG[39]	4T1 tumor	PTT	MRI/PAT	808 nm laser
	GQD-MMSNs-DOX[48]	4T1 tumor	PTT/MHT/chemotherapy	—	Alternating magnetic field/808 nm laser
	HMNS/SiO2/GQD[49]	Eca-109 tumor	PTT/PDT/magneto-mechanical/chemotherapy	—	Alternating magnetic field/808 nm laser
	MnFe2O4@SiO2@GQDs/DAU[50]	MCF-7/HEK-293 tumor	DAU delivery	—	Static magnetic field/pH
	MnO2@Pd@PPy/GO[51]	MCF-7 tumor	PTT/CDT	MRI	808 nm laser
	Cur/GQDs-Fe3O4-FA[52]	MCF-7/MDA-MB-231 tumor	Cur delivery	—	pH
TMDs	WS2-IO@MS-PEG-DOX[53]	4T1 tumor	PTT/DOX delivery	MRI/CT/PAT	808 nm laser/pH
	WS2_Gd3+-PEG[54]	4T1 tumor	PTT/radiotherapy	PAT/CT/MRI	X-ray RT/808 nm laser
	MoS2/Fe3O4[55]	HeLa and HepG2 tumor	PTT/magnetically Targeted photothermal therapy	MRI/PAT	Static magnetic field/808 nm laser
	MoS2-IO-PEG[56]	4T1 tumor	PTT	PET/PAT/MRI	808 nm laser
	Mo@Fe-ICG/Pt[57]	HeLa tumor	PTT/PDT/chemotherapy	MRI/IR/PAT	808 nm laser
MXenes	MnOx/Ti3C2[58]	4T1 tumor	PTT	MRI/PAI	808 nm laser/pH
	MnOx/Ta4C3[59]	4T1 tumor	PTT	MRI/CT/PAI	X-ray/808 nm laser
	Ti3C2-IONP-MXene[60]	4T1 tumor	PTT	MRI	X-ray/808 nm laser
	Ta4C3-IONP-SPs[61]	4T1 tumor	PTT	MRI/CT	X-ray/808 nm laser
	Ti3C2-Fe3O4@SiO2-FA[62]	HeLa tumor	Cisplatin delivery and chemotherapy	—	Static magnetic field/pH
	FTC[63]	MKN45 tumor	PTT/CDT	MRI	808 nm laser
BPNSs	BPs@Au@Fe3O4[64]	U14 tumor	PTT/PDT	MRI	Static magnetic field/650 nm laser/pH
	Re-MnO2-FfBP[65]	HeLa tumor	PDT	MRI/FI	660 nm laser/pH
	BPN/MnO2/DOX[38]	HeLa tumor	PDT/PTT/chemotherapy	MRI/IR	660 nm laser/808 nm laser
	MUCNPs@BPNS-Ce6[66]	HeLa tumor	PTT/PDT	MRI/FI	808 nm laser
	BPNS-Arg-GOx@MnO2 (BAGM)[67]	MCF-7 tumor	PTT/starvation therapy/NO gas therapy	MRI/US	660 nm laser/808 nm laser
	RGD-BPNS@SMFN[15]	HeLa tumor	PTT/PDT	—	Static magnetic field/808 nm laser
	BPQDs@DOX@ss-Fe3O4@C-EGFR NPs[68]	HeLa/C6/A549/MCF-7 tumor	Chemotherapy/PTT	MRI/FI	808 nm laser/pH
LDHs	LDH-Gd/Au[69]	L929 and HeLa tumor	Dox delivery and chemotherapy	CT/MRI	pH
	Mn-LDH[70]	B16F10 tumor	dsDNA-cy5 delivery	MRI	pH
	MnFe-LDH-MTX[71]	HeLa and HepG2 tumor	MTX delivery and chemotherapy	MRI	pH
	Mn-LDH-siRNA[72]	Neuro-2a tumor	siRNA delivery	MRI	pH
	Fe3O4@LDH-MTX[128]	MCF-7 and HepG2 tumor	MTX delivery and chemotherapy	—	pH
	LDHs/Fe3O4@dextran/DOX[73]	—	DOX delivery	—	pH
	FA-BSA/Fe3O4@LDH/5-Fu[74]	HepG2 tumor	5-Fu delivery	—	pH
2D MOFs	Fe3O4/ZIF-8-Au[25]	HeLa tumor	Magnetically targeted photodynamic/PTT	MRI	Static magnetic field/808 nm laser
	Mn3O4-PEG@C&A[76]	4T1 tumor	Nucleus-targeted PDT enhanced by CAT and GSH consumption properties	—	660 nm laser
2D COFs	Co-Fc@GOx[77]	4T1 tumor	Cascade enzymatic/Fenton catalytic ROS	—	pH
	Fe@ZIF-8@GOx[78]	HeLa tumor	Magnetically triggered enhanced uptake	—	Static magnetic field
	Fe3O4@COF-DhaTph[79]	MCF-7 tumor	PDT/PTT	MR/PAI/IR	660 nm laser
	COF-Au-MnO2-HA[80]	BALB/C tumor	PDT/catalytic cascade reaction	—	650 nm laser
	Fe3O4@COF-BSA-FA[81]	HeLa tumor	PTT/chemotherapy	—	Static magnetic field/808 nm laser
	Pd@OH-BNNSs/DOX[82]	MCF-7 tumor	PTT/chemotherapy	—	808 nm laser/pH
Other 2D NMs	FePSe3@APP@CCM[83]	CT26 tumor	Immune therapy/PTT	MRI/PAI/IR	Static magnetic field/808 nm laser
	C3N4-Fe-TPP NF/MB[84]	HeLa tumor	PDT	MRI	650 nm laser

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J. Mater. Chem. B, 2024, **12**, 1404–1428 | **1411**

tumor targeting and imaging, or magnetothermally triggered drug release.

As the representative MNMs, IONP was initially employed as a building block for constructing M2D graphene CNs. For instance, the GO-IONP-PEG-DOX complex mentioned above was employed as an MRI-guided PTT/chemotherapy antitumor nanoplatform.[46] Another GO-based MNMs, denoted as a GO-Fe_3O_4 nanocomposite, was prepared *via* chemical precipitation method by doping superparamagnetic Fe_3O_4 into GO.[93] The resulting MNMs exhibited favorable superparamagnetic properties with a saturation magnetization (M_s) of 47.56 emu g^{-1}, and could reach 92.8 °C after only 500 s exposure to an alternating current magnetic field (ACMF), demonstrating their enhanced magnetothermal properties that benefit solid tumor eradication. Elham *et al.* devised a magnetically-targeted multifunctional nanocarrier denoted as Cur/GQDs-Fe_3O_4-FA. Fe^{2+} and Fe^{3+} were chemically co-precipitated onto GQDs for producing a magnetic nanocomposite, then curcumin (Cur) and conjugating folic acid (FA) were loaded to obtain the cancer-targeting agent (Fig. 4A1).[52] This nanoagent exhibits superparamagnetic behavior (M_s = 60.6 emu g^{-1}), and can be guided to the malignancy site by an applied magnetic field and FA without endangering healthy tissues (Fig. 4A2). It was found that 33% of the total curcumin was released after 150 h (Fig. 4A3), then the cell viability of MCF-7 cells treated with Cur/GQDs-Fe_3O_4 and Cur/GQDs-Fe_3O_4-FA is 31% and 25%, respectively (Fig. 4A4). Similarly, Tao *et al.* fabricated a nano-drug carrier MGO-MDP-FA with 30.18 emu g^{-1} by covering the surface of Fe_3O_4-modified graphene oxide (MGO) with folic acid-grafted maltodextrin polymers (MDP-FA) (Fig. 4B1 and B2).[120] DOX showed a maximum loading capacity of 657.9 mg g^{-1} and 39.68 wt% *via* π–π, hydrogen bond and hydrophobic interactions (Fig. 4B3). This nanoagnet showed excellent chemo-photothermal synergistic tumor inhibition *in vitro* (tumor cell killing rate reached 80%) (Fig. 4B4).

In addition to IONP, other MNMs are sequentially incorporated into the graphene- based nanocomposite. Chen *et al.* fabricated a FeMn-GO composite using a dual redox strategy that involved the *in situ* synthesis of superparamagnetic Fe_3O_4 and paramagnetic MnO_x onto exfoliated GO nanosheets.[47] By virtue of its exceptional magnetic properties, high drug loading capacity, and disintegration behavior in a mildly acidic environment, the resulting FeMn-GO exhibits remarkable stimulus-responsive therapeutic and imaging capabilities. These include pH-responsive MRI and drug release, redox-responsive MRI, as well as magnetic-responsive MRI-guided hyperthermia. More importantly, this platform effectively inhibits tumor metastasis and dramatically reverses the multidrug resistance. Zahra *et al.* developed a pH-sensitive nanoplatform utilizing a fluorescence resonance energy transfer (FRET) system, $MnFe_2O_4$@SiO_2@ graphene quantum dots with a saturation magnetization of 28.02 emu g^{-1} (Fig. 4C1–C3). MTT assay results indicate that the nanoplatform induces cell apoptosis by inhibiting the growth of more than 95% of the MCF-7 cells (Fig. 4C4).[50]

4.2 Magnetic 2D transition metal dichalcogenides (TMDs) nanocomposites and their multimodal antitumor applications

2D TMDs are a prominent class of graphene analogues that have garnered significant interest due to their diverse composition, consisting of monolayers of MX_2 where M is a transition metal and X is a chalcogen element such as S, Se, or Te.[101] TMDs can exist in the form of either triangular or octahedral prisms. Examples of representative TMDs include MoS_2, WS_2 and $MoSe_2$, which can be prepared by various methods such as mechanical exfoliation, lithium-ion intercalation, liquid exfoliation, and meteorological precipitation.[96] The utilization of MoS_2 nanosheets as an effective PTT agent for tumor ablation was firstly reported by Chou *et al.*[49] Since then, numerous TMDs-based MNMs have also been fabricated for diverse antitumor applications.

TMD nanosheets exhibit an ultrahigh specific surface area and a large number of active sites, facilitating efficient binding with MNMs. For instance, Yang *et al.* designed a multifunctional nanoplatform WS_2-IO@MS-PEG-DOX by encapsulating abundant IONP and DOX. In addition to possessing a series of inherent fine physical properties, the nanoplatform presents NIR laser-triggered drug release behavior, enabling CT imaging-guided dual PTT/chemotherapy upon laser irradiation (Fig. 5A1–A3).[53] The nanoplatform realized effective tumor ablation, delivered excellent *in vivo* synergistic therapeutic effect of photothermal and chemotherapy under laser stimuli (Fig. 5A4). Additionally, the ultrahigh photoconversion efficiency is highly suitable for the implementation of PDT. Moreover, when doped with MNMs, multimodal tumor bioimaging can be readily achieved through CT, MRI, fluorescence imaging (FI) and photoacoustic imaging (PAI) techniques. Cheng *et al.* developed Gd^{3+}-doped WS_2 nanosheets modified with PEG (WS_2:Gd^{3+}-PEG) for enhanced radiotherapy/PTT guided by PA/CT/MR imaging. WS_2 exhibited strong NIR absorption and X-ray attenuation, enabling it to serve as a contrast for PAI and CT. Additionally, the introduction of Gd^{3+} doping enhanced its MRI properties.[54] Collectively, the trimodal imaging approach demonstrated that WS_2:Gd^{3+}-PEG rapidly accumulates in tumor tissues following intravenous injection (Fig. 5B1 and B2). The nanocomposite realized the inhibition of tumor growth completely under NIR and X-ray irradiation, demonstrating the remarkable advantage of combination therapy in comparison to monotherapy (Fig. 5B3). Yu *et al.* prepared biocompatible PEG-MoS_2/Fe_3O_4 composites (MSIOs) by a simple two-step hydrothermal method, which served as a bimodal T_2-MRI and PAI agent for precise real-time monitoring of PTT.[55] Similarly, Liu *et al.* synthesized Fe_3O_4 NPs with a homogeneous nanoflower shape in sizes ranging from 80–180 nm by hydrothermal method, and then covalently grafted onto polyimide (PEI)-functionalized MoS_2, finally encapsulating into indocyanine green (ICG) molecules and Pt(iv) precursors, resulting in MoS_2@Fe-ICG/Pt nanocomposites (Fig. 5C1).[57] The incorporation of ICG into the composites conferred additional NIR imaging properties, enabling remarkable trimodal NIR/MR/PA imaging-guided PTT, PDT, and chemotherapeutic synergistic treatment triggered by a single 808 nm NIR laser (Fig. 5C2).
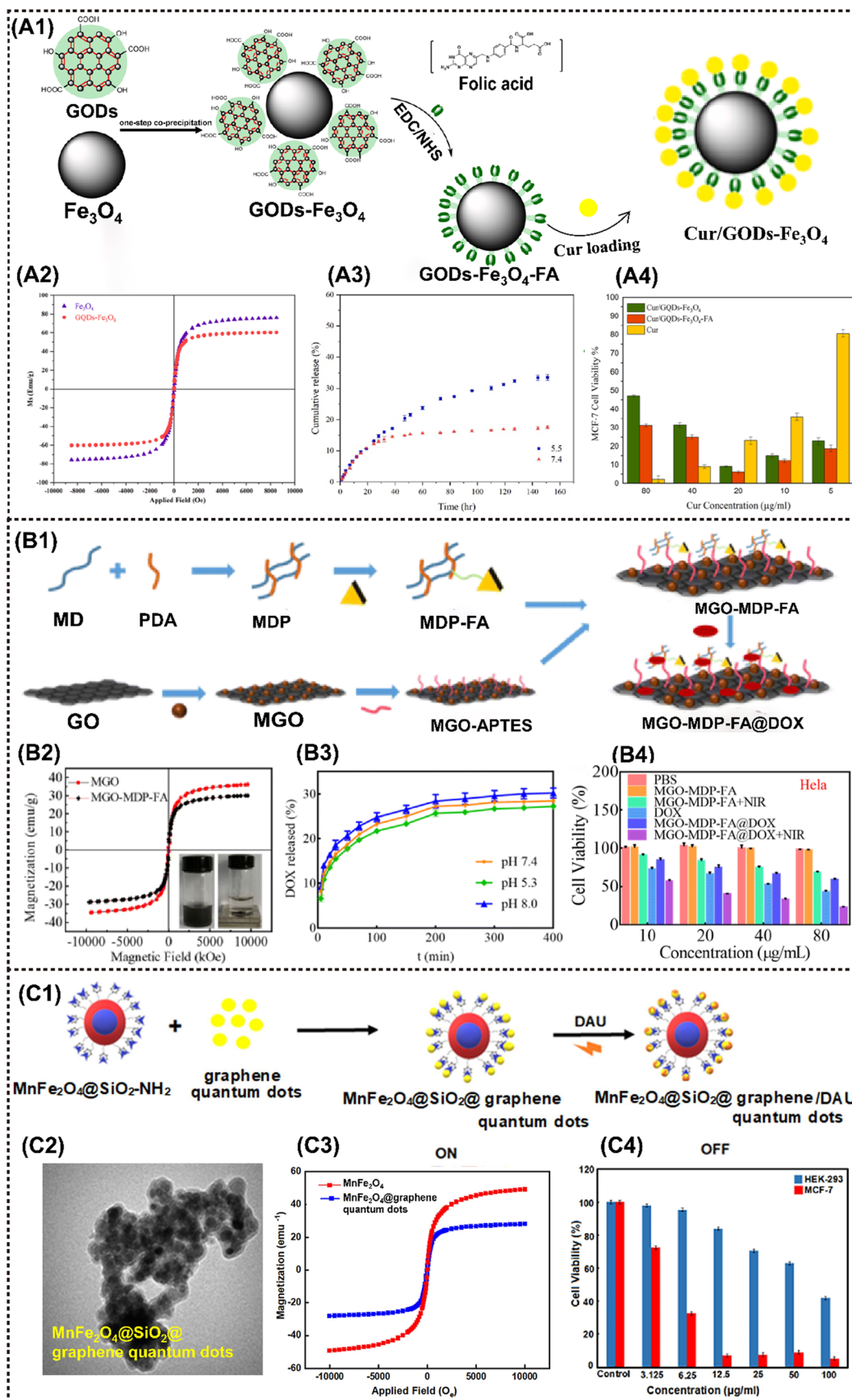
1412 | *J. Mater. Chem. B*, 2024, **12**, 1404–1428

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Fig. 4 Advanced magnetic 2D graphene nanocomposites for cancer therapy and drug delivery. (A1) Schematic diagram of the Cur/GQDs-Fe$_3$O$_4$-FA preparation. (A2) Magnetic hysteresis loop of Fe$_3$O$_4$ and GQDs-Fe$_3$O$_4$. (A3) Cumulative release of curcumin at pH values of 5.5 and 7.4 from Cur/GQDs-Fe$_3$O$_4$-FA. (A4) Cell

viability profiles of Cur, Cur/GQDs-Fe$_3$O$_4$, and Cur/GQDs-Fe$_3$O$_4$-FA after 48 h incubation. Reproduced with permission.[52] Copyright 2023, Elsevier. (B1) The synthetic route of the MGO-MDP-FA nano-drug carrier. (B2) Magnetic hysteresis loop of MGO and MGO-MDP-FA. (B3) The drug releasing rate of DOX from MGO-MDP-FA in PBS with pH 7.4 and 5.3 at 37 °C. (B4) Cell viability of HeLa treated with PBS, MGO-MDP-FA, MGO-MDP-FA + NIR, DOX, MGO-MDP-FA@DOX and MGO-MDP-FA@DOX + NIR. Reproduced with permission.[120] Copyright 2023, RSC Advances. (C1) Schematic diagram of DAU loading on MnFe$_2$O$_4$@SiO$_2$@GQDs. (C2) TEM image of MnFe$_2$O$_4$@SiO$_2$@GQDs. (C3) Magnetic hysteresis loop of MnFe$_2$O$_4$@SiO$_2$@GQDs. (C4) Cell viability for the HEK-293 normal cells and MCF-7 cancer cells in various concentrations of MnFe$_2$O$_4$@SiO$_2$@GQDs/DAU after 48 h incubation. Reproduced with permission.[50] Copyright 2022, Elsevier.

In vitro and *in vivo* results showed that the as-fabricated Mo@Fe-ICG/Pt nanocomposites exhibit good MR/IR/PA trimodal imaging capacity and conspicuous PDT/PTT/chemo-combined effect (Fig. 5C3 and C4).

4.3 Magnetic 2D transition metal carbide/nitride/carbonitride (MXenes) nanocomposites and their multimodal antitumor applications

A significant type of multifunctional 2D NMs, known as MXenes, comprises various transition metal carbides and carbonitrides. MXenes demonstrate enhanced hydrophilicity for *in vivo* application compared to 2D graphene and TMD NMs due to the presence of fluorine, oxygen, or hydroxyl groups and stronger NIR absorption. 2D MXenes such as Ti$_3$C$_2$ and Ta$_4$C$_3$ were first prepared by exfoliating MAX compounds with the general formula $M_{n+1}AX_n$, where M represents a transition metal, A denotes a group 13 or 14 element, X stands for carbon or nitrogen, and n ranges from 1 to 3. The formula for MXenes is represented by $M_{n+1}X_nT_x$, where T denotes the surface termination group (=O, −F, or −OH), and x indicates the number of surface functional groups.[121] Chen *et al.* reported the utilization of Ti$_3$C$_2$ nanosheets with a remarkable photothermal conversion efficiency (PTCE) of 30.6% for efficient tumor thermotherapy and recurrence prevention under laser irradiation, highlighting the immense application potential of MXenes-based nanomaterials *in vivo*.[122]

MXenes are a suitable nanocarrier due to their typical 2D planar topology, which facilitates the loading of MNMs onto the laminar surface.[123] Chen *et al.* successfully constructed MnO$_x$/Ti$_3$C$_2$ nanocomplexes by *in situ* growth of small MnO$_x$ nanosheets on the surface of Ti$_3$C$_2$ MXenes based on their specific surface activity through a facile redox reaction. These nanocomplexes were developed as a multifunctional theranostic platform for MRI/PAI dual-modal imaging-guided PTT. It is noteworthy that the modification of the MnO$_x$ component has enabled the nanocomplex to show T$_1$-MRI performance that is responsive to stimuli of TME, resulting in significant inhibition of tumor growth.[58,124]

A similar strategy was reported in MnO$_x$/Ta$_4$C$_3$ nanocomposites for MRI/CT/PAI guided PTT against cancer. The incorporation of Ta, with its high atomic number, into MnO$_x$/Ta$_4$C$_3$ rendered excellent contrast enhancement for CT imaging. In addition, the integrated MnO$_x$ component demonstrated TME-responsive T$_1$-MRI behavior, while the inherent PAI performance originated from MXenes. Moreover, the nanocomposites achieved a remarkable PTCE of up to 34.9%, leading to complete tumor eradication in mice (Fig. 6A1–A3).[59] Liu *et al.* synthesized a Ti$_3$C$_2$-IONP-MXenes nanohybrid by *in situ* growth

of small superparamagnetic Fe$_3$O$_4$ nanocrystals on the surface of Ti$_3$C$_2$ MXenes, which present high T_2-MR relaxation rates (394.2 mM^{-1} s^{-1}), thus showing great potential for MRI-guided therapy.[65] Subsequently, Ta$_4$C$_3$-IONP-MXenes were fabricated using a similar method, resulting in enhanced CT and MRI performance due to the high X-ray attenuation coefficient and the ordered integration of superparamagnetic IONP. This successively enabled the dual-modal imaging-guided PTT for breast tumor.[61] Furthermore, Wu *et al.* anchored Fe^{2+} ions into the layers of 2D ultrathin TC nanosheets (TC NSs) to synthesize a multifunctional nanoshell of Fe(II)–Ti$_3$C$_2$ (FTC) through interlayer electrostatic adsorption (Fig. 6B1).[63] The coupling of Fe (II) ions enhanced the tumoricidal activity by photothermal and chemodynamic therapy (Fig. 6B2), and achieved MRI (Fig. 6B3). The development of titanium carbide magnetic core–shell nanocarriers (Ti$_3$C$_2$–Fe$_3$O$_4$@SiO$_2$-FA) by Mahdieh *et al.* is particularly noteworthy given that it allows for pH-responsive drug release (Fig. 6C1) and magnetic manipulation (Fig. 6C2).[62] The findings demonstrated that the utilization of magnetism to regulate cisplatin release resulted in enhanced suppression of tumor growth by Ti$_3$C$_2$-Fe$_3$O$_4$@SiO$_2$-FA nanocarriers (Fig. 6C3).

4.4 Magnetic 2D black phosphorus (BPs) nanocomposites and their multimodal antitumor applications

Phosphorene, also known as black phosphorus nanosheets (BPNSs), demonstrated an exceptionally high surface area and volume ratio owing to their puckered honeycomb structure composed of phosphorus atoms. It has been reported that the loading capacity of DOX on the BPNSs' surface can reach up to 950% in weight, surpassing that of other 2D materials systems.[125] Therefore, the abundance of active sites on the BPNS surface is advantageous for anchoring MNMs, resulting in the magneto-responsive nanocomposites.

Zhang *et al.* developed a novel theranostics platform based on BPNS, which integrates small Fe$_3$O$_4$@MnO$_2$-doped NaY-F$_4$:Yb/Er/Nd UCNPs (MUCNPs) and chlorin e6 (Ce6) on the ultrathin BPNS to fabricate MUCNPs@BPNS-Ce6. This platform can be used for optical imaging and PDT *in vivo* (Fig. 7A1). The nanoplatform exhibits a high photosensitizing efficiency and saturation magnetization (Fig. 7A2). Initially, PTT was activated by 808 nm laser irradiation, followed by adjustment to 660–670 nm, enabling flexible operation of PDT in both BPNS and Ce6. During the hyperthermia process, Mn^{2+} decomposed from MnO$_2$ and catalyzed excessive intracellular H$_2$O$_2$ in acidic TME to efficiently generate O$_2$ through the Fenton reaction, which was crucial for enhancing PDT. Additionally, the obtained Mn^{2+} provided explicit T$_1$-MRI signal, while Fe$_3$O$_4$ served as the T$_2$-MRI contrast agent and Ce6 acted as a FI probe, collectively

1414 | *J. Mater. Chem. B*, 2024, **12**, 1404–1428

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Fig. 5 Advanced 2D TMDs nanocomposites for cancer therapy and imaging. (A1)–(A3) A procedure showing the fabrication of WS$_2$-IO@MS-PEG/DOX and the application in CT imaging-guided tumor treatment. (A4) The photographs of 4T1 tumors excised from mice at the end of treatments (day 14).

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J. Mater. Chem. B, 2024, **12**, 1404–1428 | **1415**

resulting in the impressive multimodal imaging performance *in vivo* (Fig. 7A3).[66] Photographs of excised tumors verified the safety and enhanced antitumor effect of this nanoplatform (Fig. 7A4).

Liu *et al.* developed a magnetic nanoplatform based on BPNS termed as R^e-MnO$_2$-F^{f}BP. This platform was modified with fluorescein isothiocyanate (FITC)-labelled peptide-functionalized BPNS, and incorporated with rhodamine B (RhB) encapsulated-manganese dioxide (R^e-MnO$_2$). It enables bimodal monitoring of oxygen self-supply and enhanced PTT.[65] The multifunctional R^e-MnO$_2$-F^{f}BP nanoplatform demonstrated striking synergistic effect in delivering continuous local O$_2$ to overcome hypoxia and boost the PDT performance. Simultaneously, the released Mn^{2+} and RhB dye were employed for dual-mode MRI/FI, enabling real-time monitoring of the oxygen self-supply process as a feedback mechanism for therapeutic efficacy. Yang *et al.* prepared a BPs@Au@Fe$_3$O$_4$ nanohybrid for MRI-monitoring PTT and PDT on HeLa tumors in mice. Compared to the three individual materials of BPNSs, BPs@Au and BPs@Fe$_3$O$_4$, the BPs@Au@Fe$_3$O$_4$ nanohybrid demonstrated superior tumor inhibition efficacy *in vivo* when triggered by a 650 nm laser radiation and an external magnetic field. The synergistic antitumor performance can be attributed to the well-ordered hybrid nanostructure, rather than a simple summation of the individual functional components.[64]

The potential of the BPNS-based MNMs has also been investigated as an intelligent nanozyme or nanoreactor system. Our group proposed a biocompatible and targeted delivery PTT–PDT self-synergetic nanoplatform, denoted as RGD-BPNS@SMFN, based on temperature-dependent catalase (CAT)-like behavior for efficient tumor elimination. It was found that the PTT-promoted inherent CAT-like activity within the nanoplatform remodels the tumor hypoxic microenvironment, thereby ameliorating the PDT efficiency and providing a synergetic dual-mode PTT/PDT approach with exceptional performance (Fig. 7B1).[15] It was determined that BPNS@SMFN has the highest saturation magnetization (150.0 emu g^{-1}) (Fig. 7B2). *In vitro* and *in vivo* experiments further indicated the optimal tumor synergetic treatment outcomes compared to the monotherapy of BPNS or SMFN (Fig. 7B3 and B4). Su *et al.* innovatively constructed a novel nanozyme system termed BPNSs-Arg-GOx@MnO$_2$ (BAGM), which served as a multimodal synergistic therapeutic platform. The BAGM nanozyme effectively initiates a cascade reaction by depleting intracellular glucose to generate H$_2$O$_2$, subsequently converting H$_2$O$_2$ into O$_2$ within the acidic microenvironment of cells and thereby facilitating the oxidation of L-Arg to nitric oxide (NO). Thereafter, NO production can activate matrix metalloproteinases to degrade the dense extracellular matrix (ECM) in solid tumors

and convert collagen within the matrix into a more porous state. In turn, this heightened the accumulation of the BAGM nanozyme within the loose ECM and improves the PTT performance.[67] Similarly, Wu *et al.* engineered a modified BPNS by incorporating MnO$_2$ NPs, resulting in the development of an intelligent self-driven theranostic platform with specific tumor targeting capabilities (Fig. 7C1). The BPNS/MnO$_2$ platform displayed simultaneous pH and redox-responsive MRI performance, as well as drug release behavior. In comparison to bare BPNS, the newly developed BPN/MnO$_2$ nanohybrid achieves 37% increase in PTCE and an additional 3.8-fold enhancement in PDT within hypoxic TME. The multiple properties responsive to TME provide intelligent MR and thermal imaging, facilitating precise monitoring of drug delivery to the tumor with nearly 4-fold greater release than that that stimulated by acid alone, thereby further reducing potential chemotherapy side effects on normal tissues (Fig. 7C2).[38]

In addition to BPNS, black phosphorus quantum dots (BPQD) have been employed in the construction of M2D NCs. Zhang *et al.* fabricated a multifunctional nanocomposite BPQDs@DOX@ss-Fe$_3$O$_4$@C-EGFR that is responsive to pH/NIR/glutathione (GSH). Initially, DOX was encapsulated into ss-Fe$_3$O$_4$@C, then conjugated with PEGylation BPQDs. Finally, the nanocomposite was modified with epidermal growth factor receptor (EGFR) on the outer shell. Specifically, the nanocomposite exhibits significant accumulation within the tumor due to its EGFR active targeting and magnetic orientation, which can be effectively monitored through dual MRI/FI. Furthermore, BPQDs@DOX@ss-Fe$_3$O$_4$@C showcased significant tumor suppression *in vivo* due to its pH, NIR, and redox-responsive drug release behavior, surpassing the efficacy of mono-phototherapy or chemotherapy, while maintaining high safety on healthy tissues.[68]

4.5 Magnetic 2D layered double hydroxides (LDHs) nanocomposites and their multimodal antitumor applications

The layer double hydroxides (LDHs), also referred to as hydrotalcite-like compounds, exhibit the general formula of $[M^{2+}_{1-x}M^{3+}_x(OH)_2]^{x+}(A^{m-})_{x/m}\cdot nH_2O$, where M represents metal elements with either divalent or trivalent oxidation states, and A represents interlayer anions.[96] Notably, the majority of LDHs consist of silicate clay-like minerals exhibiting minimal toxicity and high solubility in physiological environment. Consequently, M2D LDHs CNs have been effectively employed in the field of antitumor research through further targeted modifications specific to tumor cells and encapsulation of functional payloads.

Zhao *et al.* developed magnetic Fe$_3$O$_4$@MTX-LDH/Au NPs encapsulating the anticancer agent of methotrexate (MTX) *via* a

1416 | *J. Mater. Chem. B*, 2024, **12**, 1404–1428

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Fig. 6 Advanced magnetic 2D MXenes nanocomposites for cancer therapy and imaging. (A1) Scheme to present the tumor theranostics of the MnO_x/Ta_4C_3-SP composite for MR/CT/PA imaging-guided PTT. (A2) *In vivo* 3D reconstruction CT (left) and contrast (right) images of mice before and after i.v. administration of the MnO_x/Ta_4C_3-SP composite nanosheets for 2 h. (B3) T_1-weighted imaging of 4T1 tumor-bearing mice after i.v. administration of the MnO_x/Ta_4C_3-SP composite nanosheets for prolonged time intervals. Reproduced with permission.[59] Copyright 2017, ACS. (B1) FE-SEM pattern of FTC. (B2) Confocal fluorescence images of live (green) and dead (red) cells after different treatments. (B3) MRI images of MKN45 tumor-bearing Balb/c nude mice at different time points after intratumoral injection. Reproduced with permission.[63] Copyright 2021, Wiley-ACH. (C1) Schematic illustration of the fabrication of Ti_3C_2-Fe_3O_4@SiO_2-FA nanoplatforms and cisplatin targeting for cervical cancer delivery *in vivo* study. (C2) Magnetic hysteresis loop of Ti_3C_2-Fe_3O_4@SiO_2-FA. (C3) Ti_3C_2-Fe_3O_4@SiO_2-FA-cisplatin reduces the tumor size in cervical cancer tumors. Reproduced with permission.[62] Copyright 2023, Wiley-ACH.

coprecipitation-electrostatic interaction strategy.[126] Firstly, MgAl-LDH materials were deposited over the surface of Fe_3O_4 NPs by the coprecipitation method. Secondly, Au NPs were successfully anchored onto the surface of LDH through electrostatic interaction (Fig. 8A1). These particles presented a well-defined core–shell structure, strong magnetization (Fig. 8A2), and a high drug-loading capacity. Cell lethal test of Fe_3O_4@MTX-LDH/Au NPs revealed that the platform exhibited

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J. Mater. Chem. B, 2024, **12**, 1404–1428 | **1417**

Fig. 7 Advanced magnetic 2D BP nanocomposites for cancer therapy and imaging. (A1) Schematic illustration for the fabrication of MUCNPs@BPNS-Ce6 nanoplatforms. (A2) Magnetic hysteresis loop for MUCNPs and MUCNPs@BPNs-Ce6. (A3) *In vivo* MR images (left) and *in vivo* fluorescence images (right) of the tumor-bearing mice before and after injection with MUCNPs@BPNs-Ce6 for 24 h. (A4) Photographs of excised tumors from mice under different treatment. Reproduced with permission.[66] Copyright 2020, Elsevier. (B1) Schematic illustration for the construction of the RGD-BPNS@SMFN nanoplatform. (B2) The field-dependent magnetic hysteresis loops of the samples. (B3) *In vitro* cell viabilities of HeLa cells after different treatments with nanomaterials as-synthesized. (B4) Tumor volume variation in different treatment groups with time. Reproduced with permission.[15] Copyright 2022, Wiley-ACH. (C1) Schematic presentation of the preparation of multifunctional BPN/MnO$_2$/DOX nanostructures. (C2) *In vivo* MRI of mice bearing HeLa tumors after the intravenous injection of BPN/MnO$_2$/DOX and time-dependent T_1 value changes. (C3) Time-dependent tumor growth of mice with different treatments. Reproduced with permission.[38] Copyright 2019, Elsevier.
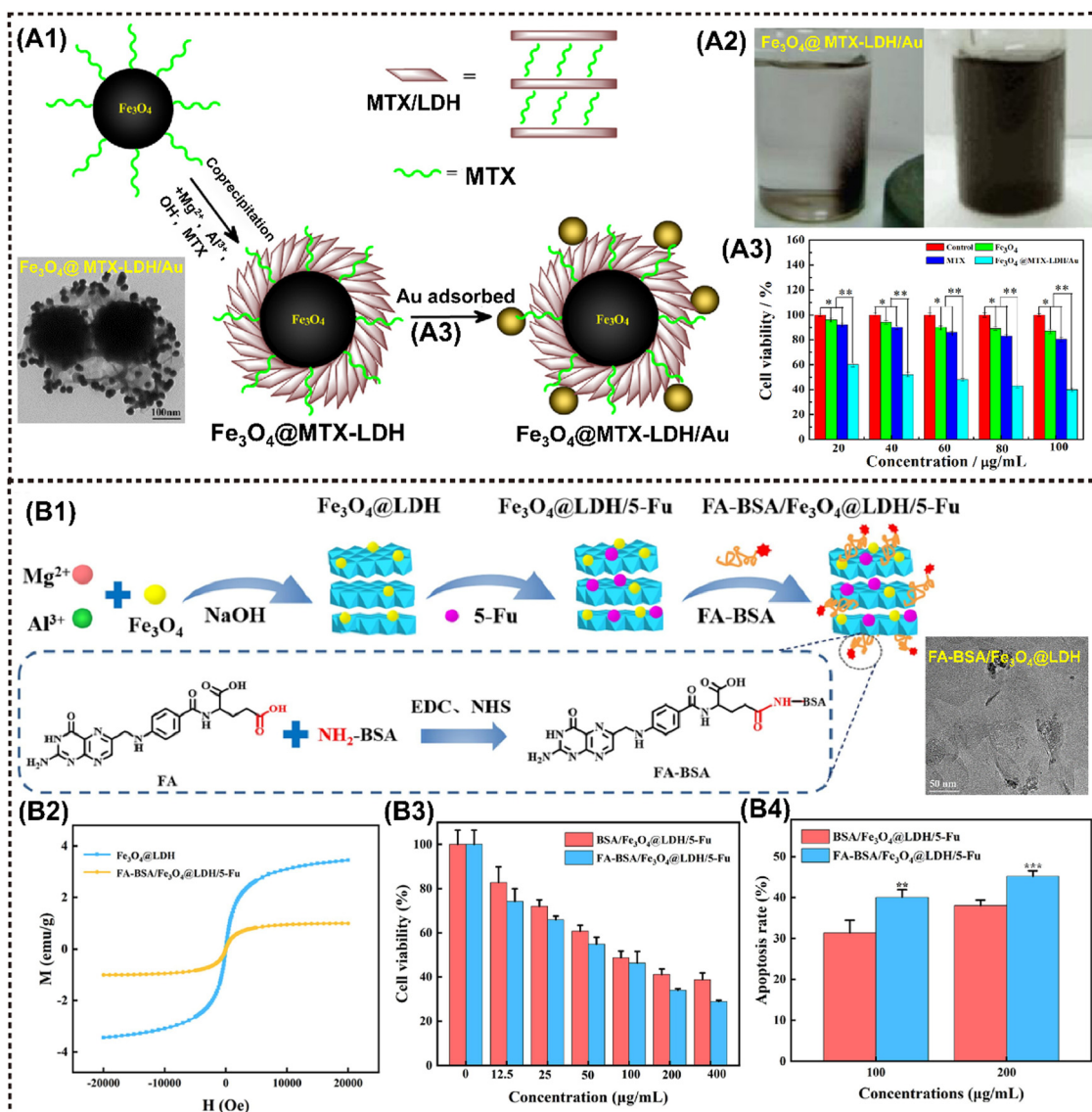
1418 | *J. Mater. Chem. B*, 2024, **12**, 1404–1428

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Fig. 8 Advanced magnetic 2D LDHs nanocomposites for cancer therapy and imaging. (A1) Schematic procedure for the preparation of Fe_3O_4@MTX-LDH/Au NPs. (A2) Photographs of the Fe_3O_4@MTX-LDH/Au NPs in the presence of the external magnet (left), and photographs of the Fe_3O_4@MTX-LDH/Au NPs after ultrasonication when removing the external magnet (right). (A3) Comparison of cell viabilities for MTX, Fe_3O_4 NPs, Fe_3O_4@MTX-LDH/Au NPs at various concentrations after 48 h of incubation. Reproduced with permission.[126] Copyright 2018, Elsevier. (B1) Schematic illustration of the preparation process of FA-BSA/Fe_3O_4@LDH/5-Fu. (B2) Magnetic hysteresis loop of different samples. (B3) Cell viability of HepG2 cells after treatment. (B4) Quantitative analysis results of the apoptosis rate of hepatoma cell microspheres. Reproduced with permission.[74] Copyright 2023, Elsevier.

the lowest cell vitality of only 40% (Fig. 8A3). Interestingly, MnAl-LDH serves as a dual-functional platform for MRI and siRNA delivery *via* cellular metabolism pathway, showing improved biosafety and therapeutic efficacy with r_1 value of 4.47 mM^{-1} s^{-1} that is even higher than that of commercial contrast agent gadolinium complexes (r_1 = 3.4 mM^{-1} s^{-1}).[72] Particularly, the cell-death siRNA (CD-siRNA) delivered by Mn-LDH demonstrated stronger lethal effects on brain cancer cells compared to free CD-siRNA.

Introducing magnetic elements or other inorganic NMs into LDH layers through rich intercalation chemistry provides a facile approach to constructing a magnetic nanohybrid. For instance, Gd^{3+} and Mn^{2+} are paramagnetic metal ions that can

be utilized in MRI.[127] The LDH-Gd/Au nanocomposite was synthesized by incorporating Gd and Au into LDH, which has been recognized as a multifunctional platform for CT/MR bimodal imaging and simultaneous drug delivery. Interestingly, LDH-Gd/Au displayed an improved dose-dependent positive CT contrast enhancement, with significantly stronger brightness compared to commercial Iobitridol. Moreover, a series of metal-doped LDH nanohybrids have been developed for pH-responsive tumor theranostic platforms, inspired by the disintegrating behavior of metals (Fe, Mn, Gd, *etc.*) and hydroxides in acidic TME. Li *et al.* designed pH-sensitive manganese-based double hydroxide (Mn-LDH) nanocomposites, which demonstrated tumor-specific MRI enhancement rather than

normal tissues in mice.[70] Huang *et al.* reported on manganese-iron layered hydroxides (MnFe-LDH), showcasing excellent responsiveness to acidic TME and releasing paramagnetic Mn^{2+} and Fe^{3+} ions for T_1-MRI in tumor regions, as well as delivering chemotherapeutic drugs in a pH-controlled manner.[71] Analogously, Wu *et al.* successfully prepared the nanocomposite Fe_3O_4@LDH-MTX by utilizing LDH as a host for both Fe_3O_4 and the anticancer drug methotrexate (MTX). The resulting material exhibited significant anticancer activity due to its magnetically guided and pH-responsive drug release properties.[128] Similarly, Liu *et al.* proposed a novel FA-BSA/Fe_3O_4@LDH composed of a folic acid-bovine serum albumin conjugate (FA-BSA) conjugated with nano Fe_3O_4 and LDH for the delivery of the anticancer drug 5-Fluorouracil (5-Fu) (Fig. 8B1).[74] FA-BSA/Fe_3O_4@LDH/5-Fu showed pH-responsive release behavior; the releasing rate is significantly higher in pH 5.0 release medium than that in pH 7.4 release medium (Fig. 8B2). *In vitro* results showed that the nanocomposite resulted in the strongest apoptosis outcomes of hepatocellular carcinoma cells (Fig. 8B3 and B4).

4.6 Magnetic 2D MOFs nanocomposites and their multimodal antitumor applications

2D Metal–organic frameworks (MOFs) materials are built by the coordination of metal cations and organic ligands, facilitating their application in various biomedical fields such as biosensing, bioimaging, and disease treatment due to their remarkable functional groups, porous structure, and tunable properties.[96,101] Meanwhile, the efficient biodegradation and rapid renal clearance behavior ensure excellent biosafety within the body. Regarding antitumor applications, MOFs-based NMs generally exhibit superior PDT/PTT/drug delivery behavior and imaging performance, resulting in effective tumor suppression. For instance, Yang *et al.* synthesized Fe_3O_4/ZIF-8-Au_{25} nanocomposites as a cooperative therapeutic system by grafting $Au_{25}(SR)_{18}^-$ clusters and Fe_3O_4 NPs onto MOFs. This multifunctional magnetic core–shell composites exhibited magnetic targeted trimodal PDT/PTT/MHT capabilities that could be monitored using MRI. *In vivo* experiments further confirmed the synergistic inhibitory effect of combined theranostics on tumor, with fewer side effects on normal organs compared to single PDT or PTT treatment.[75]

The application of cascade nanozyme catalysis therapy in M2D MOFs CNs has been extensively investigated. Zeng *et al.* developed a novel cascade nanozyme Mn_3O_4-PEG@C&A using the template of MOFs. The M2D NCs derived from MOFs with intrinsic catalase-like activity engendered the conversion of H_2O_2 into O_2, thereby enhancing PDT efficacy through simultaneous GSH consumption. The Mn_3O_4 NPs were synthesized using MOFs as a substrate, resulting in a larger pore size and surface area compared to native MOFs. The larger pore size and surface area favor the loading of high dose photosensitizer molecules. Following the decoration with the AS1411 aptamer and PEG, the M2D NCs were synthesized, showing phenomenal nucleus-targeted PDT properties. This innovative approach offers a novel strategy for designing a functional nanozyme

that specially target subcellular organelles to enhance the modulation of drug resistance in tumor eradication.[76] A novel nanozyme structure of Fe@ZIF-8@GOx nanorods (NRs) was proposed by Li *et al.*, wherein the NRs were prepared *via* the iron mineralization during the growth of ZIF-8, followed by glucose oxidase (GOx) loading. The NRs can be efficiently internalized into cancer cells under an external magnetic field, thereby initiating a cascade catalysis reaction as follows: at the outset, GOx catalyzes intracellular glucose into H_2O_2, followed by NRs serving as a peroxidase-like nanozyme to produce hydroxyl radicals (•OH) from H_2O_2 under mild acidic condition in lysosomes at physiological temperature. Concurrently, the combination of glucose consumption and continuous generation of toxic ROS achieves severe damage to tumor cells through starvation therapy (Fig. 9A1).[78] Fe@ZIF-8 NPs exhibited a ferrimagnetism with a coercive field of 0.022 T and remnant magnetization of 3.15 A m^2 kg^{-1}. In contrast, ZIF-8 NPs had no magnetism at room temperature (Fig. 9A2). The cytotoxicity test of CCK-8 indicated that using Fe@ZIF-8@GOx+magnet almost eradicated the cancer cells *in vitro* (Fig. 9A3).

In a similar way, Fang *et al.* integrated a nanoscale Co-ferrocene MOFs (Co-Fc NMOF) with high Fenton reaction activity and GOx to construct a cascade enzymatic/Fenton catalytic platform termed as Co-Fc@GOx. In this system, Co-Fc NMOF not only served as a versatile and efficient carrier for GOx, but also showed exceptional Fenton effect, leading to the generation of highly toxic •OH radicals. In TME, GOx delivered by Co-Fc NMOF catalyzes the conversion of endogenous glucose to gluconic acid and H_2O_2. The resulting intracellular acidity and on-site concentration of H_2O_2 favors the Fenton reaction of Co-Fc NMOF, leading to enhanced generation of ROS (Fig. 9B1 and B2). The finding obtained from both *in vitro* and *in vivo* experiments demonstrated that the cascade enzymatic/Fenton catalytic reaction triggered by the Co-Fc@GOx nanozyme exhibits remarkable anticancer properties (Fig. 9B2 and B3).[77]

4.7 Magnetic 2D COFs nanocomposites for multimodal antitumor

COFs are a newly-emerged 2D crystalline material that possess the similar framework structure of MOFs, thereby exhibiting tunable spatial arrangement and orderly accurate assembly pattern.[129] In addition to sharing the common advantages of other 2D NMs, COFs demonstrate intriguing reactive properties and favorable biocompatibility, attributed to their diverse organic structure. The covalent organic unit can be designed and synthesized as a structure sensitive to TME with a controllable degradation period, thereby easily collapsing under TME stimuli, further exerting flexible action on tumor eradication with high biocompatibility. In recent years, M2D COFs CNs have been extensively investigated, increasingly emerging as promising candidates for photo/magneto-active nanoagents in tumor combination therapy.[130–133] Zhao *et al.* proposed a nanocomposite termed Fe_3O_4@COF-BSA-FA for targeted drug delivery, consisting of magnetic Fe_3O_4 as the core and functionalized COFs loading into DOX as the shell, further modified

1420 | *J. Mater. Chem. B*, 2024, **12**, 1404–1428

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Fig. 9 Advanced magnetic 2D MOFs nanocomposites for cancer therapy and imaging. (A1) The fabrication procedure of Fe@ZIF-8@GOx NRs, and its combining PDT and starvation therapy for magnetically enhanced antitumor application. (A2) Magnetic hysteresis loop of ZIF-8 NPs, Fe@ZIF-8 NPs and Fe@ZIF-8@Gox NRs at 300 K. (A3) Relative viability of HeLa cells incubated with different materials. Reproduced with permission.[78] Copyright 2020, Elsevier. (B1) The synergetic therapy via Enzymatic/Fenton effect of Co-Fc@GOx as an antitumor platform. (B2) Cell viabilities of 4T1 tumor cells incubated with Co-Fc NMOF. (B3) Tumor volume variation of mice in the following 14 days. Reproduced with permission.[77] Copyright 2020, Wiley-ACH.

with bull serum albumin (BSA) and folic acid (FA) (Fig. 10A1). The tumor inhibition rate was observed to reach up to 80% (Fig. 10A3). More importantly, the π–π interaction between DOX and COFs provides a fluorescence resonance energy transfer (FRET) system, enabling the monitoring of drug release through changes in both UV absorption and fluorescence intensity.[81]

Cai et al. proposed a nanocomposite denoted as COFs-Au–MnO_2 for implementing the ROS catalysis reaction in TME, where Au NPs were grown on the surface using COFs as a template and then modified with a thin layer of MnO_2 before being coated with biocompatible hyaluronic acid (HA). Under hypoxic conditions in TME, COFs-Au–MnO_2 can react with overexpressed H_2O_2 to produce O_2, enhancing type II PDT. Au NPs can also decompose glucose to promote starvation therapy, while the resulting H_2O_2 benefits oxygen generation. Meanwhile, MnO_2 consumes GSH, thereby elevating the oxidative stress level. The released Mn^{2+} can be utilized for T_1-MRI. In vitro and in vivo experiments demonstrated the strong tumor killing efficiency of this cascade cycle.[80] M2D COFs CNs can also serve as a versatile multimodal imaging agent. Feng et al. proposed the synthesis of Fe_3O_4@COF-DhaTph, a core–shell

structured nanocomposite, through an in situ seed growth method (Fig. 10B1). This nanocomposite enabled dual-modal phototherapy with a single laser irradiation. More importantly, the high relaxation rate and excellent PTCE enable the expedient realization of tri-modal MR/PA/IR imaging-guided treatment (Fig. 10B2 and B3). The combined phototherapy demonstrated the ability to kill cancer cells effectively in vitro, and suppress tumor growth with excellent biocompatibility in vivo (Fig. 10B4 and B5).[79]

4.8 Other magnetic 2D composites for multimodal antitumor

In addition to the aforementioned 2D NMs, numerous other newly emerging 2D NMs have been harnessed for the fabrication of advanced M2D NCs in biomedical applications, including boron nitride nanosheets (BNNSs), g-C_3N_4 nanosheets, 2D $FePSe_3$ nanosheets and so on.[101] 2D BNNSs with high NIR absorption properties are a promising PTT agent. Zhang et al. proposed a facile hydrothermal substitution method for the in situ formation of Pd NPs on the BNNSs surface, resulting in well-dispersed Pd@OH-BNNSs (Fig. 11A1).[82] Both Pd NPs and BNNSs exhibit high PTCE and wide-band NIR absorption. Moreover, the modification of Pd has been demonstrated to

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J. Mater. Chem. B, 2024, 12, 1404–1428 | 1421

Fig. 10 Advanced magnetic 2D COFs nanocomposites for cancer therapy and imaging. (A) Schematic diagram for constructing the Fe$_3$O$_4$@COF-BSA-FA drug delivery system and PTT/chemotherapy synergistic treatment. Reproduced with permission.[81] Copyright 2021, Elsevier. (B) Schematic illustration of Fe$_3$O$_4$@COF-DhaTph as a multifunctional nanosystem for MR/PA/IR imaging-guided combined phototherapy upon single laser excitation. Reproduced with permission.[80] Copyright 2021, ACS.

prolong blood circulation, thereby allowing massive accumulation of MNMs at the targeted tumor site for enhanced PTT. Additionally, Pd@OH-BNNSs displayed heat-triggered drug release behavior, and the synergistic treatment significantly suppressed tumor growth within a mere two weeks (Fig. 11A2 and A3).

Graphitic-phase carbon nitride (g-C$_3$N$_4$)-based MNMs has attracted far-ranging attention due to the high photoluminescence quantum yield, facile fabrication, great biocompatibility, and low toxicity.[134] Ma *et al.* developed a mitochondria-targeting PDT nanoplatform that exhibits excellent O$_2$ catalytic production from H$_2$O$_2$ in cancer cells, utilizing Fe^{III}-doped 2D g-

1422 | *J. Mater. Chem. B*, 2024, **12**, 1404–1428

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Fig. 11 Other magnetic 2D nanocomposites for cancer therapy and imaging. (A1) Schematic presentation for the synthesis of Pd@OH-BNNS/DOX and the PTT/chemotherapy synergistic antitumor mechanism. (A2) Viabilities of MCF-7 cells incubated with various materials. (A3) Tumor volumes of different groups during therapy (left) and tumor tissues (right). Reproduced with permission.[82] Copyright 2019, Elsevier. (B1) Schematic illustration for the preparation of FePSe$_3$@APP@CCM NSs. (B2) T_2-weighted MR images of FePSe$_3$@CCM NSs in the tumor site (left), and the ΔR_2* value in the tumor site after i.v. injection with FePSe$_3$@CCM NSs and FePSe3@CS NSs at different time intervals (right). (B3) Tumor growth curves and (B4) tumor weight plots of tumor-bearing mice from the different treatment groups (1: control; 2: free APP; 3: FePSe$_3$@CCM; 4: FePSe$_3$@CCM plus laser irradiation; 5: FePSe$_3$@APP@CCM; 6: FePSe$_3$@APP@CCM plus laser irradiation). (B5) Photographs of tumor tissues resected from mice after different treatment groups. Reproduced with permission.[83] Copyright 2021, Wiley-ACH.

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J. Mater. Chem. B, 2024, **12**, 1404–1428 | **1423**

C_3N_4 nanoholes. Moreover, this platform confers prominent T_1-MRI capability *in vivo*.[84] A metal phosphorous trichalcogenides (MPX$_3$)-based magnetic nanohybrid has been developed in recent years as an efficient PTT/CDT/MRI anti-cancer theranostic platform. For instance, Fang *et al.* developed a FePSe$_3$-based MNMs (FePSe$_3$@APP@CCM) functionalized with anti-PD-1 peptide (APP), which can serve as the MRI/PAI contrast agent and PTT/immunotherapeutic agent against CT26 cancer cells by targeting immune escape mechanisms (Fig. 11B1).[83] The functionalized 2D FePSe$_3$-based NSs exhibit an efficient tumor targeting ability because of the CCM decoration, and strong APP-related immunotherapy triggered by PTT, which can be monitored by precise MRI (Fig. 11B2). The multimodal imaging guided synergistic therapy significantly prolongs the lifespan of experimental mice (Fig. 11B3–B5).

5. Summary and perspectives

This review presents an overview of the recent advances in M2D NCs and their multimodal antitumor implementation. Advantages of the synergistic combination of 2D NMs and MNMs into M2D NCs are first discussed, followed by an introduction of the design and material fabrication of M2D NCs. Multimodal antitumor applications of M2D NCs, including 2D graphene and its derivatives, TMDs, transition metal carbides/nitrides/carbonitrides, BPs, LDHs, MOFs and COFs, are summarized and discussed. In particular, a detailed analysis is presented on the multimodal applications, including MHT, PTT, PDT, drug delivery, immunotherapy and multimodal imaging. Lastly, this review proposes the future development of such a research field with an emphasis on the scaling up of material fabrication, inherent structure-performance relationship, and elucidating the biodegradation mechanism. Additionally, it offers the capability to remotely modulate the structure disintegration and drug release in response to various external stimuli or TME conditions, holding great potential for achieving a more effective tumor treatment and facilitating the development of intelligent nanomedicine platforms, such as stimuli-responsive theranostic and cascade nanozyme catalytic reaction systems. Undoubtedly, M2D NCs have a great prospect for clinical translation in tumor treatment, while still facing some challenges and limitations that need to be tackled. Here, we make a comprehensive analysis of the challenges and clinical prospects associated with M2D NCs.

5.1 Challenges

The practical antitumor applications of M2D NCs in clinics is still currently encountering some challenges, with the primary concern being their controllable fabrication. The imperative for scalable application hinges on achieving production that is both controllable and repeatable. The attainment of M2D NCs characterized by high performance, uniform shape, customized size, and robust stability necessitates the development of meticulously designed material synthesis conditions. Upon transitioning from laboratory settings to semi-works plants, a re-exploration of the effects of temperature, pressure, reagent addition, gaseous atmosphere, and the selection of elements or functional molecules on the physiochemical properties of M2D NCs becomes paramount. Another challenge pertains to adhering to stringent quality standards in pharmaceutics. Analogous to conventional clinical drugs or materials, it is indispensable to standardize the dosage, administration regimen, contraindications, and precautions associated with the use of M2D NCs as a pharmaceutical agent. Prior to clinical implementation, comprehensive preclinical investigations must be conducted to assess the long-term safety, biodegradability, and potential toxicities linked to M2D NCs, ensuring their adequate safety for *in vivo* use. Potential bio-risks may arise not only from the toxic chemical solvents or reagents employed in the product fabrication, but also from the toxic degradation components or byproducts. The mitigation of these risks necessitates advanced green manufacturing approaches, substantial investment, and long-term tracking investigations. Lastly, the relationship between the structure of M2D NCs and their antitumor outcomes, as well as the biodegradation mechanism, remains unclear, and there is a lack of sophisticated measurements for precise prediction and systematic analysis. Despite significant efforts to comprehend the interaction between M2D NCs and TME, the intricate mutual effects are still unknown, warranting urgent and thorough investigation.

5.2 Opportunities and outlooks

Despite the numerous challenges facing M2D NCs and their early-stage clinical applications in antitumor treatment, notable progress has been made in the development of M2D NCs for multimodal antitumor therapy. Recent advancements in various emerging thoughts and technologies hold promise for addressing these challenges, thereby facilitating further clinical advancements.

The first imperative involves leveraging the advantages of artificial intelligence (AI)-guided material customization. AI, in its capacity, extends beyond merely screening material species and synthesis routes or predicting therapeutic performance. It significantly contributes to enhancing our comprehension of the interactions between M2D NCs and malignancy. This encompasses elucidating the targeting pathway, cellular uptake, intercellular transportation, and cumulative outcomes in tumor regions. For instance, machine learning (ML), as a subset of AI, discerns crucial information from extensive data regarding the structure and physicochemical properties of M2D NCs. ML not only refines the structure-performance relationships, but also predicts the potential decomposition and metabolic fates within the human body. The notable accuracy of ML models, surpassing that of other simulation methods, is a noteworthy attribute. Moreover, AI can guide each step in the development journey of M2D NCs – from material design and lab synthesis to *in vitro* or *in vivo* performance evaluation and large-scale manufacturing – resulting in an ultra-short research and development (R&D) cycle. Consequently, AI significantly enhances the efficiency of material design, reduces production

1424 | *J. Mater. Chem. B*, 2024, **12**, 1404–1428

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costs, mitigates utilization risks, and unequivocally accelerates the clinical translation of M2D NCs.

The second critical aspect underscores the advantages derived from the advancements in the in-depth understanding of tumorigenesis and metastasis pathology. The ongoing exploration of an expanding array of pathogenic factors and tumor biomarkers, such as diverse kinases, RNA molecules, and cellular signaling pathways, provides a foundation for potential intervention approaches at the cellular and molecular biology levels. This, in turn, catalyzes novel attempts through the utilization of M2D NCs, offering a promising avenue for the development of feasible tumor theranostic schemes. Furthermore, insights gleaned from the study of biological behaviors, encompassing immunoregulation, gene expression, pharmacokinetics, long-term biotoxicity, contribute to a nuanced understanding, promoting the rational design and administration of M2D NCs that are more aptly suited for clinical use in tumor treatment.

The third facet underscores the convenience derived from the widespread utilization of magnetic or optical theranostic devices and other technologies in clinical settings. Electric magnetic instruments and laser therapy apparatuses have become staple tools in clinical physiotherapy and rehabilitation, effectively alleviating inflammation, edema, muscle pain, and other injuries. Moreover, the integration of MRI and magnetic hyperthermia apparatus has proven successful in clinical tumor diagnostics and therapy. Leveraging the synergy of AI and electronics technology has led to the development of more intelligent magnetic and optical medical devices, enhancing precision and personalization in theranostic applications. Consequently, the proliferation of these advanced medical devices establishes a robust foundation for the widespread use of M2D NCs.

In conclusion, owing to their distinctive magnetic responsiveness and intelligent stimuli-response behaviors, including optical and immune modulation, coupled with the inherent biosecurity within the internal environment of the human body, M2D NCs present a promising clinical outlook. With increasing emphasis on controlled synthesis, functionalization, and a deeper comprehension of the mechanisms underlying multimodal antitumor therapy, it is anticipated that novel M2D NCs with tailored pharmaceutical properties will emerge. These advancements are expected to position M2D NCs as qualified multimodal antitumor nanomedicine in practical applications in the near future.

Author contributions

Ying Yuan: investigation, writing – original draft. Bo Chen: conceptualization, resources, investigation, funding acquisition, writing – original draft. Luping Song: investigation. Xingxing An: investigation. Qinrui Zhang: investigation. Hao Lu: writing – review & editing. Chang Ming Li: supervision, writing – review & editing. Chunxian Guo: supervision, funding acquisition, writing – review & editing.

Conflicts of interest

There are no conflicts of interest to declare.

Acknowledgements

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