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## A minimal hybridization chain reaction (HCR) system using peptide nucleic acids†

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The HCR represents a powerful tool for amplification in DNA-based circuitry and sensing applications, yet requires the use of long DNA sequences to grant hairpin metastability. Here we describe a minimal HCR system based on peptide nucleic acids (PNAs). A system comprising a 5-mer stem and 5-mer loop/toehold hairpins was found to be suitable to achieve rapid amplification. These hairpins were shown to yield >10-fold amplification in 2 h and be suitable for the detection of a cancer biomarker on live cells. The use of  $\gamma$ -peg-modified PNA was found to be beneficial.

### Introduction

Oligonucleotides are an attractive platform for the design of programmable circuitry, empowering logic gated operations and enzyme-free amplifications. The modular nature of such systems allows a variety of inputs to be integrated into diverse outputs with emerging functions.<sup>1</sup> In addition to logic-gated operations, oligonucleotide circuitry lends itself to the amplification mechanism and is being increasingly embraced for sensing applications and smart diagnostics, integrating logic-based operations with an amplification.<sup>2–5</sup> A particularly important advent for amplification is the development of the hybridization chain reaction (HCR), where a single strand oligonucleotide initiator opens a metastable hairpin (kinetically trapped) freeing a single strand domain capable of opening a second hairpin to repeat the process in a chain reaction (Fig. 1).<sup>6–8</sup> This isothermal polymerization process can be used to amplify the detection of nucleic acids and other biomolecules.<sup>9,10</sup> The HCR has also been shown to proceed in live cells.<sup>11–13</sup> In addition to a simple amplification, the polymerization reaction can be used to turn on diverse outputs such as fluorescence signals (such as an excimer),<sup>14</sup> DNase activity,<sup>15</sup> and pro-drug activation,<sup>16</sup> and deliver drugs for photodynamic therapy.<sup>17</sup> HCRs have been used to detect cell-surface receptors on live cells.<sup>18</sup> Furthermore, the ability to initiate an HCR by the proximity of analytes (AND logic gate) has been harnessed to detect specific protein–protein interactions (PPIs), post-translational modifications<sup>19</sup> and specific biomarkers on cancer cells.<sup>20</sup> Pierce and coworkers' original report of the HCR made use of hairpins that were 48 nt (18 nt stem and 6 nt loop/toehold).<sup>6</sup> Investigations into minimizing this length in order to reduce cost and increase density have been reported with 36–42

nt hairpins.<sup>21,22</sup> It has also been demonstrated that HCR systems with hairpins containing shorter stems (12-mers) show faster kinetics (10-fold)<sup>21</sup> but the shorter stems compromise the metastability resulting in an untriggered HCR. Surprisingly, the performances of DNA mimics have yet to be explored to further minimize the hairpin size. The unique properties of peptide nucleic acids (PNAs)<sup>23–26</sup> are well suited for this goal. PNAs have been shown to form a stable hairpin with just 3 or 4-mer stems with high thermal stability.<sup>27</sup> Moreover, modified monomers can further tune the PNA properties. In particular, modification at the gamma position of the PNA backbone<sup>28</sup> can be used to tune affinities and its chirality can be exploited for orthogonal hybridizations.<sup>29–31</sup> In addition, the enzymatic stability of PNAs against nucleases and proteases would make PNA-based HCRs applicable for *in vivo* applications.

Herein, we report a minimal hybridization chain reaction process enabled by PNAs. Different lengths of hairpin stems and loops were tested, as well as different modifications at the  $\gamma$ -position of PNA monomers (*L*-serine and mini-peg) in order to identify the minimal structure. The kinetics and extent of amplification were characterized indicating more than 10-fold amplification after two hours of incubation. The promising performance of the PNA-based HCR *in vitro* was successfully

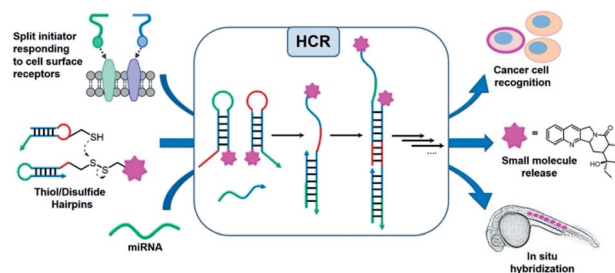


Fig. 1 Schematic representation of different inputs and outputs of the HCR.

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translated *in cellulo*, where the PNA HCR was applied for the visualization of carbonic anhydrase IX (CA IX) expressed on the surface of cancer cells. Taken together, our results suggest that PNAs are a valid alternative to DNA for the construction of complex networks with a minimal hairpin length.

## Results and discussion

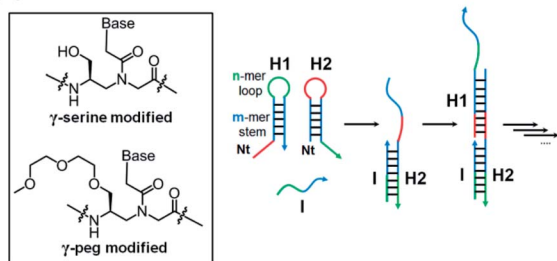
For the HCR to proceed selectively upon addition of a trigger sequence the hairpins must have sufficient metastability (length of the stem). Based on previous results showing that a stem with four G:C pairs can induce stable hairpin structures ( $T_m = 75^\circ\text{C}$ ),<sup>27</sup> we investigated PNA hairpins having a 3-mer loop and 4-mer stem (3,4-system), 4-mer loop and 5-mer stem (4,5-system), and 5-mer loop and 5-mer stem (5,5-system) as HCR scaffolds (Fig. 2A; see Table S1† for full sequences) to gain insight into the minimum length required for a PNA-based HCR. A  $\gamma$ -serine modified PNA backbone was first utilized as it improves the solubility and duplex stability compared to unmodified PNAs.<sup>28,32,33</sup> To evaluate the stability of the hairpins (H1 and H2) and the product of the reaction with the initiator strand (I), the PNAs were labelled with fluorescein (FITC), to confer negative charges and thus allow the PNAs to migrate in polyacrylamide gel electrophoresis (PAGE). In a desirable

system the initiator strand strongly hybridizes to the first hairpin to form an I:H2 duplex, which in turn opens the second hairpin (H1) for the HCR. Gel analysis conducted on these three systems showed that the 5,5-system gave a >90% hybridization yield for the first reaction step (H2 + I) and that the metastability was sufficient to preclude an untriggered HCR (H1 + H2 does not react, Fig. 2B and S1†). In the case of the 3,4-system, the metastability was sufficient, but the H2 + I product was not observable by gel analysis (Fig. S1†). However, the HCR mixture (H1 + H2 + I) yielded species with a higher molecular weight, suggesting that the duplex H2 + I is present in solution but it is too dynamic to withstand migration through the gel. The 4,5-system showed results that were intermediate between the 3,4- and 5,5-systems, with partial formation of the H2:I duplex observed by PAGE (Fig. S1†). Based on these results, the 5,5-system was adopted as a basic design for further investigations.

The addition of 1 equivalent of I (FserI) to H1 and H2 (FserH1 + FserH2) affords a mixture of products as could be anticipated for a statistical reaction, if the rate of initiation is comparable to the rate of the HCR, with higher order HCR oligomers appearing as a smear band. Triggering the HCR with a sub-stoichiometric initiator (0.1 or 0.01 equivalent) led to complete consumption of the initiator but not of H1 and H2 suggesting that the reaction terminates. Moreover, the precipitation of bigger size products was observed in the loading zone of the gel, possibly due to the low solubility of long HCR products (Fig. 2B, red box). These results suggested that the I strand produces desired HCR products; however, the elongation yield of the HCR appeared prematurely terminated (estimated fewer than 10 HCR cycles based on the fact that 0.1 equivalent of initiator did not consume all the hairpins).

To corroborate the results obtained by PAGE, we also sought to analyse the reaction by SDS-PAGE gel electrophoresis and in addition, immobilize the initiator strand on streptavidin beads. In this case, the initiator sequence was labelled with a biotin

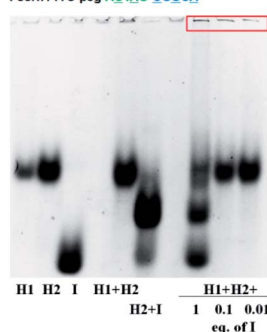
### (A) Scheme for PNA HCR (n m-system)



### $\gamma$ -serine modified, 5-mer stem, 5-mer loop hairpins

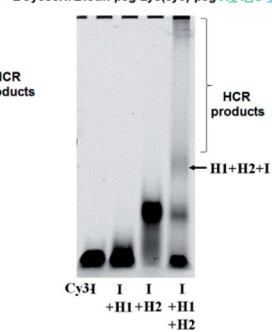
#### (B) 5% PAGE (Fl. of FITC)

FserH1: FITC-peg-GAATG-TGCCG-ACTAG-CGGCA  
FserH2: FITC-peg-CGGCA-CATTG-TGCCG-CTAGT  
FserI: FITC-peg-ACTAG-CGGCA



#### (C) SDS-PAGE (Fl. of Cy3)

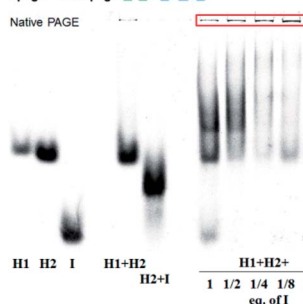
serH1: NH<sub>2</sub>-peg-GAATG-TGCCG-ACTAG-CGGCA  
serH2: NH<sub>2</sub>-peg-CGGCA-CATTG-TGCCG-CTAGT  
Bcy3serI: Biotin-peg-Lys(cy3)-peg-ACTAG-CGGCA



### $\gamma$ -peg modified, 5-mer stem, 5-mer loop hairpins

#### (A) 5% PAGE (Fl. of FITC)

FpegH1: FITC-peg-GAATG-TGCCG-ACTAG-CGGCA  
FpegH2: FITC-peg-CGGCA-CATTG-TGCCG-CTAGT  
FpegI: FITC-peg-ACTAG-CGGCA



#### (B) SDS-PAGE (Fl. of Cy3)

pegH1: NH<sub>2</sub>-peg-GAATG-TGCCG-ACTAG-CGGCA  
pegH2: NH<sub>2</sub>-peg-CGGCA-CATTG-TGCCG-CTAGT  
Cy3pegI: Cy3-peg-ACTAG-CGGCA

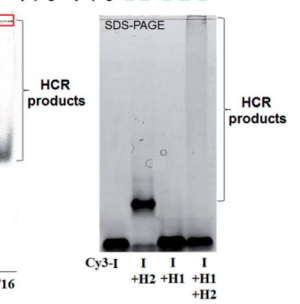


Fig. 2 (A) Basic design of the PNA HCR and structures of  $\gamma$ -modified PNA backbones used in this study. (B) 5% PAGE analysis of the HCR using FITC-labelled  $\gamma$ -serine modified-PNAs. Conditions for the reaction: pH 7.5 0.1 $\times$  PBS, 0.02% tween-20, 1  $\mu\text{M}$  of each component, 20  $\mu\text{L}$ , r.t., and 2 h of incubation. (C) SDS-PAGE analysis of the HCR using  $\gamma$ -serine modified-PNAs, Bcy3serI, serH1, and serH2. Conditions for the reaction: pH 7.5 0.1 $\times$  PBS, 0.02% tween-20, 1  $\mu\text{M}$  of each component, 15  $\mu\text{L}$ , r.t., and 3 h of incubation.

Fig. 3 (A) 5% PAGE analysis of the HCR using FITC-labelled  $\gamma$ -peg modified-PNAs. Conditions for the reaction: pH 7.5 0.1 $\times$  PBS, 0.02% tween-20, 500 nM of each component, 20  $\mu\text{L}$ , r.t., and 2 h of incubation. (B) SDS-PAGE analysis of the HCR using  $\gamma$ -peg modified-PNAs, Cy3pegI, pegH1, and pegH2. Conditions for the reaction: pH 7.5 0.5 $\times$  PBS, 0.02% tween-20, 500 nM of each component, 15  $\mu\text{L}$ , r.t., and 2 h of incubation.





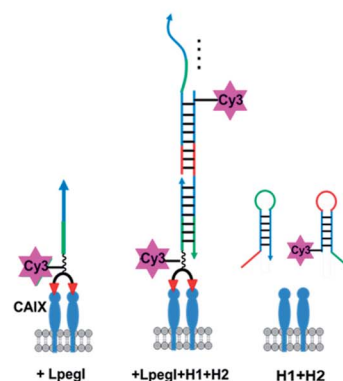
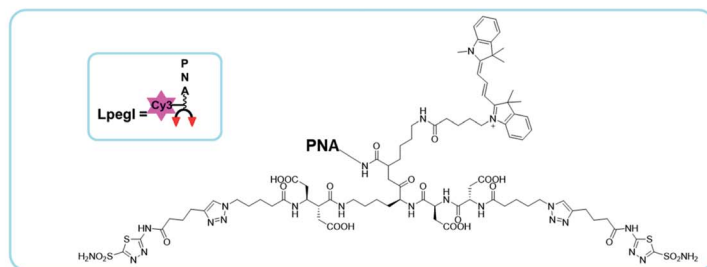
with a low equivalence of I did not result in the complete consumption of the hairpin after 2 h of reaction (Fig. 3A, 1/8 and 1/16 eq. of I). A similar pattern was observed for SDS-PAGE with  $\gamma$ -peg modified-PNA hairpins (Fig. 3B, 87% consumption of hairpins in the reaction of I + H1 + H2 based on fluorescence integration, and Fig. S3†).

Next, the elongation efficiency of the HCR was evaluated by fluorescence-based techniques. First, a fluorescence pulldown assay was utilized to estimate the number of hairpins that participate in the formation of HCR products. In this experiment, a mixture of **pegH1** and **Cy3pegH2** was added to streptavidin beads loaded with a biotinylated initiator (**BpegI**) to trigger the HCR (Fig. 4A). The reaction yield of the HCR was evaluated by the quantification of consumed hairpins upon

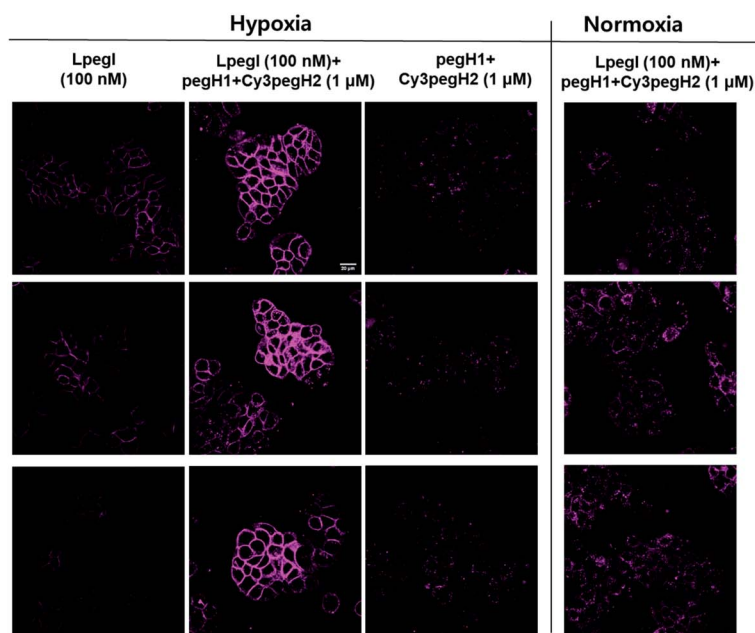
reaction both in the reaction sample (**BpegI** + **pegH1** + **Cy3pegH2**) and in a reference sample lacking the initiator strand. Based on this method, we observed that 90 pmol of **Cy3pegH2** was consumed by 15 pmol of **BpegI**, which indicates 12 cycles of the HCR (Fig. 4A). In addition, the reaction was quantified by fluorescence microscopy analysis of streptavidin beads. In this case, two different biotinylated initiators (**BpegI** and **FBpegI**) were used; each initiator was loaded on separated beads and the beads containing **BpegI** were submitted to a regular HCR with **pegH1** + **Cy3pegH2**, while beads with **FBpegI** (fluorescein labelled) were treated with an excess amount of Cy3-labelled hairpin H2 (**Cy3pegH2**) but not H1 such that only one cycle of the HCR can take place. After incubation, the beads from each reaction were washed, mixed and screened with

### (A) Sequences and general HCR scheme for visualization of CAIX

**pegH1:** NH<sub>2</sub>-peg-**GAATG-TGCCG-ACTAG-CGGCA**  
**Cy3pegH2:** Cy3-peg-**CGGCA-CATTC-TGCCG-CTAGT**  
**LpegI:** L-peg-**ACTAG-CGGCA**

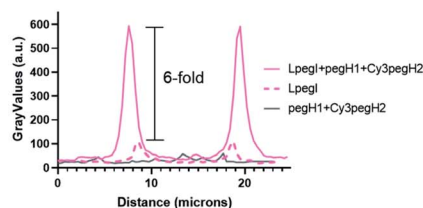


### (B) Imaging CAIX using PNA HCR

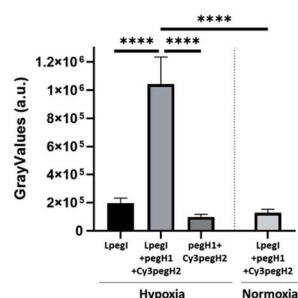


### (C) Quantification of fluorescence

Fluorescence along a line intersecting the cell



Quantified fluorescence on cell membranes



**Fig. 6** PNA HCR on CA IX expressing cells. (A) Sequence information and general scheme of the PNA-HCR system for the visualization of CA IX. CA IX was visualized by 1 : 1 ratio imaging with **LpegI**, PNA HCR (**LpegI** + **pegH1** + **Cy3pegH2**), or only hairpins (**pegH1** + **Cy3pegH2**). (B) Fluorescence pictures of HT-29 cells treated with **LpegI**; **LpegI** + **pegH1** + **Cy3pegH2**; **pegH1** + **Cy3pegH2** under hypoxic conditions or treated with **LpegI** + **pegH1** + **Cy3pegH2** under normoxic conditions. Scale bar: 20  $\mu$ M. (C) Fluorescence intensity profiles recorded along a line intersecting the cell and quantification of fluorescence on cell membranes. Error bars represent standard deviation. Statistics were calculated using an unpaired *t*-test. \*\*\*\**p* < 0.0001.



a confocal microscope for the quantification of the fluorescence. The beads that underwent the HCR were 7-fold more fluorescent in the Cy3 channel than the beads that were treated with only H2, indicating 14 cycles of the HCR, which is consistent with previous quantification accomplished by fluorescence pulldown assay. The elongation efficiency was confirmed by experiments carried out at different concentrations of reagents and for different reaction times (Fig. S4†). Moreover, size-exclusion chromatography (SEC) experiments further supported the formation of H2 + I, H2 + I + H1 and HCR products with a higher molecular weight (Fig. S5†); the estimated size of the HCR product (57 kDa, ~8 HCR cycles) is consistent with previous results obtained by fluorescence measurements. Overall, these quantification experiments suggested that the length of HCR products benefited from the use of peg-modified PNA monomers, enabling more than 10 cycles of the HCR to occur (amplification).

Next, we evaluated the kinetics of hairpin hybridization. FITC or dabcyI quenchers were introduced into PNA strands to monitor the dissociation constants and the rate constants of the first (H2 + I) and second (H2 + I + H1) hybridization steps. The first step was analysed by using a FITC labelled initiator (**FpegI**) and a dabcyI-modified H2 (**DpegH2**). Pseudo-first-order kinetics experiments (dabcyI-PNA in excess) revealed a rate constant of  $4.5 \times 10^4 \text{ M}^{-1} \text{ s}^{-1}$  ( $k_{\text{on}}$ , Fig. 5A) (half-life = 78 s;  $k_{\text{obs}} = 8.9 \times 10^{-3} \text{ s}^{-1}$ , Fig. S6†). Interestingly, the second step (H2:I + H1) showed a 2.6-fold faster reaction rate constant ( $1.2 \times 10^5 \text{ M}^{-1} \text{ s}^{-1}$ , Fig. 5B) (half-life = 30 s;  $k_{\text{obs}} = 2.3 \times 10^{-2} \text{ s}^{-1}$ , Fig. S6†). These kinetic data are in line with those of previously reported DNA HCR systems.<sup>21</sup> The faster reaction for the second may be explained by additional base stacking interaction between **pegIF** and **DpegH1**, mediated by the formation of a **pegIF:pegH2** duplex.<sup>35–37</sup> These results are consistent with previous PAGE results, which showed that some of the initiator remained unreacted when using a stoichiometric ratio of reagents (Fig. 2B, lane H1 + H2 + 1 eq. of I and Fig. 3a), indicating that propagation is faster than initiation.

Next, we sought to apply this minimal HCR system for the detection of biomarkers expressed on the surface of cancer cells. We selected carbonic anhydrase IX (CA IX) as the protein of interest based on the fact that it is a marker of hypoxia in various types of solid tumors.<sup>38–40</sup> CA IX has been established as a prognostic marker and imaging target for solid tumors.<sup>41,42</sup> HT-29, a human colon cancer cell line, was selected as it is known to express CA IX under hypoxic conditions. To ensure anchoring of the initiator strand to the target protein, an acetazolamide-based bivalent ligand<sup>43–45</sup> was conjugated to the initiator strand (**LpegI**) (Fig. 6A). **LpegI** was also Cy3-labelled to be able to monitor the fluorescence signal arising from direct binding between the ligand initiator strand conjugate and CA IX (Fig. 6A). Upon binding of **LpegI** (Fig. 6A) to CA IX over-expressing cells (100 nM, 30 min, and hypoxic conditions), treatment with hairpins **pegH1** + **Cy3pegH2** (1  $\mu\text{M}$ , 1 hour, and hypoxic conditions) triggered the HCR (Fig. 6A and B), resulting in a 6-fold increase in the fluorescent signal (corresponding to 12 elongations) localized on the cell membrane (Fig. 6B and C). As a control, cells treated with hairpins **pegH1** + **Cy3pegH2** (1

$\mu\text{M}$ , 1 hour, and hypoxic conditions) but lacking the initiator strand showed no fluorescence upon washing (Fig. 6B and C), highlighting the fact that the PNA HCR is suitable for the recognition of biological markers and that the system is specifically responsive to the initiator trigger. Once again, this result was consistent with the previous experiments using loaded beads. Moreover, the system was tested under normoxic conditions (CA IX weakly expressed), showing a dramatically weaker signal (Fig. 6B and C), confirming the specificity of the HCR event as a consequence of the target protein concentration (8-fold difference between hypoxia and normoxia). Accordingly, the results demonstrate that the PNA HCR system can be used to readily visualize CA IX *in cellulo*. The advantage of an amplified fluorescence signal makes this setup particularly appealing for the imaging of cellular targets with a low expression level. The amplification levels observed are comparable to those of previously reported amplification with a DNA-based HCR.<sup>46</sup>

## Conclusions

In conclusion, we introduced a minimal HCR system based on  $\gamma$ -modified PNAs (including L-serine or peg modification). Among the screened options, a  $\gamma$ -peg-modified 5-mer stem and 5-mer toehold/loop hairpins were found to be better performing, showing the metastability of hairpins together with fast kinetics ( $1.2 \times 10^5 \text{ M}^{-1} \text{ s}^{-1}$ ) in the chain reaction. The elongation efficiency for the PNA HCR was improved to >10-fold by using the  $\gamma$ -peg-modified PNA, by virtue of the increased solubility of HCR products. The optimized 5,5-system was applied to signal amplification and distinct visualization of CA IX (a cancer biomarker) in live cells by fluorescence. Classic DNA HCR systems require long sequences to allow for the formation of elongated products without leakage (hairpin metastability is lost with stems below a 12 nucleobase length); this work demonstrates that PNAs represent a valuable alternative for the design of minimal systems. Moreover, our results suggest the suitability of the PNA HCR for the detection of targets in biological environments. The work enables the power of HCR amplifications to be tapped with an alternative platform that has significantly different physicochemical properties than DNA.

## Data availability

Raw data corresponding to the experiments reported have been deposited at (<https://zenodo.org/record/4740000#.YJ-x36j7Q2x> with DOI: 10.5281/zenodo.4740000).

## Author contributions

The work was conceived by K. T. K., S. A. and N. W., K. T. K. synthesized and characterized the HCR system. S. A. performed in cellulo experiments. K. T. K., S. A., N. W., analysed and discussed the results. N. W. directed the project. K. T. K., S. A., N. W. wrote the manuscript.



## Conflicts of interest

There are no conflicts to declare.

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