



PAPER

[View Article Online](#)
[View Journal](#) | [View Issue](#)Cite this: *Nanoscale Adv.*, 2022, 4, 3928

Shape dependent sensing potential of gold nanoparticles in etching based multicolorimetric plasmonic-ELISA†

Sangeeta Yadav ^a and Jitendra Satija ^{*b}

In the present study, a systematic investigation has been carried out for the first time to assess the potential of three different shapes of gold nanoparticles (AuNPs), viz. nanorods (AuNRs), nanotriangles (AuNTs), and nanospheres (AuNSs), to develop a horseradish peroxidase (HRP) enzyme-mediated etching-based plasmonic ELISA (p-ELISA) strategy. The etching of the AuNPs in ELISA is achieved by 3'-3'-5'-tetramethylbenzidine (TMB²⁺), which is produced by the biocatalytic conversion of chromogenic TMB via HRP. All three types of AuNPs were interacted with varying concentrations of TMB²⁺ (7–131 μM) (product of HRP enzyme reaction) and characterized for visible color change and by UV-Vis spectroscopy and transmission electron microscopy (TEM). From the comparative analysis of all three shapes of AuNPs, AuNRs exhibited vivid visible color change and absorbance intensity change compared to spherical and triangle-shaped nanoparticles. The TEM analysis of the etched nanoparticles revealed the gradual etching pattern of AuNRs compared to AuNTs which resulted in multicolor generation as opposed to AuNTs where the etching was relatively very fast and thus shows a faster shape transformation and poor color discrimination. Further, the potential of the AuNR etching-based optimized strategy was successfully demonstrated to develop an indirect competitive p-ELISA for human IgG detection. The developed p-ELISA showed an ultra-low visual limit of detection of 1 fg mL⁻¹ (~6.54 aM) without the aid of any sophisticated instruments. In the future, the developed competitive p-ELISA strategy can be easily employed to develop cost-effective, portable, and point-of-care assays for the detection of various disease biomarkers with ultra-high sensitivity.

Received 29th April 2022
Accepted 16th August 2022

DOI: 10.1039/d2na00266c

rsc.li/nanoscale-advances

Introduction

Plasmonic-enzyme linked immunosorbent assay (p-ELISA) has garnered immense interest in the last decade towards the development of ultrasensitive visual biosensors for various disease biomarkers, environmental pollutants, and food adulterants.^{1–6} This strategy relies upon the modulation in the localized surface plasmon resonance (LSPR) properties of the noble metal nanoparticles (MNPs) through a biocatalytic-triggered reaction that transforms their shape, size, composition, or agglomeration state.^{7–10} Since the LSPR property of the nanoparticles is size/shape and composition-dependent, a very minute structural change can give rise to a noticeable signal. Another important advantage of p-ELISA is the high extinction coefficient of the metal nanoparticles (e.g. gold nanoparticles (AuNPs) $\epsilon = 10^8$ – 10^9 M⁻¹.cm⁻¹) compared to the traditionally

used chromogenic substrate, i.e. 3,3',5,5'-tetramethylbenzidine (TMB) ($\epsilon = 5.9 \times 10^4$ M⁻¹.cm⁻¹), which make them a prudent choice to produce an intense color change even at a very low concentration of the analyte.^{11,12}

To date, the p-ELISA strategy has been realized by inducing the (i) aggregation of the MNPs,^{13,14} (ii) metallization of the MNPs,^{15,16} and (iii) etching-mediated shape transformation of MNPs.^{17,18} In the first approach, the enzyme-catalyzed reaction induces the aggregation of MNPs via altering their surface charges. The degree of MNPs aggregation depends upon the analyte concentration that correspondingly results in a change in characteristic LSPR peak and colloidal solution color which is observed through the naked eye and ELISA plate optical reader. For instance, Nie *et al.* reported a p-ELISA strategy based on AuNPs aggregation for the detection of syphilis by utilizing the biocatalytic reaction involving acetylcholinesterase mediated generation of cationic thiocholine (TCh) in relation to the analyte concentration.¹⁹ The TCh interacts strongly with citrate-capped AuNPs due to thiol groups and thereby alters the surface charges which eventually triggers the aggregation of AuNPs, causing a visual change in color from red to blue.

The second strategy is typically based on the biocatalytic reaction mediated reduction of metal salts which eventually

^aSchool of Biosciences and Technology, Vellore Institute of Technology (VIT), Vellore-632014, Tamilnadu, India^bCentre for Nanobiotechnology, Vellore Institute of Technology (VIT), Vellore-632014, Tamilnadu, India. E-mail: jsatija11@gmail.com; jsatija@vit.ac.in† Electronic supplementary information (ESI) available. See <https://doi.org/10.1039/d2na00266c>

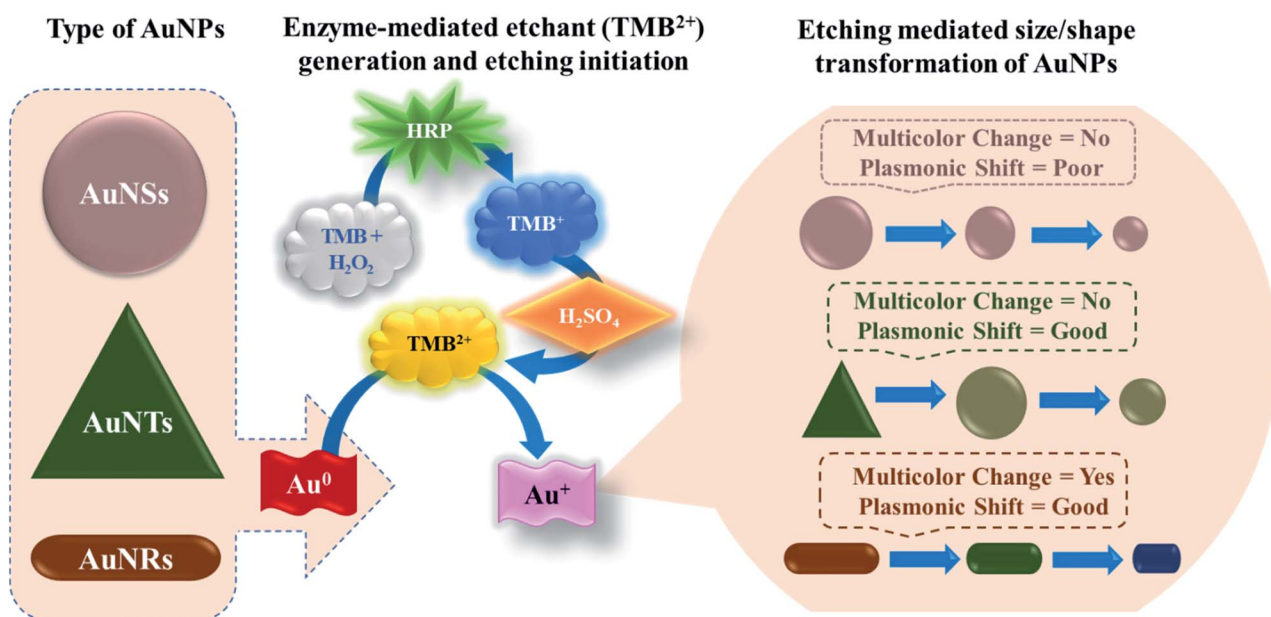
forms a thin metal film (*i.e.* metallization) in a heteroepitaxial manner on the template nanoparticles to produce core-shell type nanostructure.^{20,21} A small difference in the lattice constant of the deposited metal and the template MNPs is an important requirement for the uniform deposition of metal on template nanoparticles. For example, in the case of silver and gold, the lattice constant is as low as 0.25%, thus AuNPs can be easily utilized as a template to grow silver to produce a core-shell nanostructure.²² Using this approach, Yang *et al.* formulated a p-ELISA strategy by depositing silver on the gold nanorods (AuNRs) in a core/shell manner to detect prostate-specific antigen (PSA).²³ The biocatalytic reaction involving alkaline phosphatase (ALP) mediates the generation of dephosphorylated p-aminophenol in relation to the PSA concentration, which eventually reduces silver salt into metallic silver that gets deposited on AuNRs. Accordingly, a significant change in the longitudinal LSPR peak and color of the AuNRs solution from pale red to green, purple and brown was observed. The third strategy is based on the enzyme-mediated generation of the etchant that results in the morphological transformation of MNPs and a visually detectable color change. For example, Yuan *et al.* reported a p-ELISA strategy by oxidative etching of silver nanoprism (AgNPRs) for the qualitative and quantitative determination of danofloxacin (DAN).²⁴ In this indirect competitive p-ELISA, glucose oxidase enzyme-mediated generation of hydrogen peroxide (H_2O_2) triggers the oxidative etching of AgNPRs, which results in a prominent color change from dark blue to colorless.

All three p-ELISA strategies have demonstrated good sensitivity and selectivity without the aid of an optical reader, however, the MNP etching-based color development approach

is the most suitable for the field deployable point-of-care assays. This is based on the fact that the predefined multicolor change in the reaction solution depends upon the shape transformation of MNPs that can be easily correlated with the concentration of the analyte molecules in the sample. Unlike, the aggregation and metallization-based p-ELISA, the effect of reaction conditions and environmental factors such as temperature, is negligible and thus minimizes the chances of false-positive or false-negative results in the case of etching-based p-ELISA strategies.^{25–28} The sensitivity of the etching-based p-ELISAs can be further enhanced by many folds by precise control of the LSPR peak (or the shape) of the MNPs.

To date, various anisotropic MNPs such as nanorods, nanocages, nanocubes, nanoprisms, and nanoflowers have been explored for the development of LSPR based colorimetric assays.^{29–37} Among all other etching processes, the oxidative etching of AuNPs *via* TMB^{2+} has garnered more attention due to their controlled nature of etching and futuristic convenient translation possibilities. Therefore, the reshaping-induced LSPR peak shift can serve as a probe for the development of multi-colorimetric p-ELISA strategies. Although several studies have utilized any single type of AuNPs for the development of TMB^{2+} -mediated etching reaction based on p-ELISA, a detailed comparative analysis of TMB^{2+} mediated re-shaping of different shapes of AuNPs and to answer which shape of the AuNPs shows better sensor performance both in terms of UV-Vis spectral shift and naked-eye detection have not been investigated.

In this study, for the first time, we have reported the systematic comparison of selective etching of three different shapes of AuNPs, *viz.* gold nanospheres (AuNSs), gold nanorods



Scheme 1 Schematic illustration of etching-based p-ELISA strategy developed by employing gold nanospheres (AuNSs), gold nanorods (AuNRs), and gold nanotriangles (AuNTs). The enzyme horseradish peroxidase (HRP) hydrolyses 3,3',5,5'-tetramethylbenzidine (TMB) into TMB⁺, which is oxidized into TMB²⁺ upon H₂SO₄ acid treatment. TMB²⁺ acts as an etchant for the gold nanoparticles and leads to their size and shape transformation.



(AuNRs), and gold nanotriangles (AuNTs), by TMB²⁺ (Scheme 1). The selection of TMB²⁺ as an etchant is based on the fact that most of the commercial ELISA kits employ horseradish peroxidase (HRP) and TMB as enzyme–substrate pair where the TMB (colorless) hydrolyzed into TMB²⁺ (yellow) *via* HRP.³⁸ The TMB²⁺ oxidizes Au(0) into Au(i) in the presence of an optimum concentration of CTAB at room temperature resulting in their shape transformation causing a visual color change and spectral shift.³⁹ The etching process is tracked *via* observing the visual color change in the colloidal solution of AuNPs, by recording the UV-Vis absorption spectra to measure the wavelength shift, and TEM micrograph of AuNPs before and after interaction with TMB²⁺ to assess the level of etching. Amongst the three different shapes, AuNRs showed a gradual change both in the LSPR peak and colorimetric change as a function of etchant concentration. Further, the potential of the AuNRs-etching based optimized strategy was demonstrated by developing an indirect competitive multicolorimetric p-ELISA strategy capable of detecting human IgG (as a model antigen) with a visual detection limit of 1 fg mL⁻¹ (~6.54 aM).

Materials and methods

Materials

Silver nitrate (AgNO₃), gold(III) chloride solution (HAuCl₄), phosphate-buffered saline (PBS, pH 7.4), horseradish peroxidase (HRP), sodium borohydride (NaBH₄), cetyl-trimethyl ammonium bromide (CTAB), 3,3',5,5'-tetramethylbenzidine (TMB), Corning® 96 well microtiter plate, ascorbic acid (AA) and tween20 were procured from Sigma-Aldrich, India. Trisodium citrate (TSC) was procured from Sisco Research Laboratories Pvt. Ltd., India. Human immunoglobulin G (HiGg) and HRP conjugated goat anti-HiGg (GaHiGg@HRP) antibodies were obtained from Bangalore Genei Pvt Ltd., India. Bovine serum albumin (BSA) was purchased from Himedia Labs Ltd., India. Hydrogen peroxide (H₂O₂) (30 wt%) was purchased from Merck Chemicals Ltd. (India). All the other reagents and chemicals used were of analytical grade and utilized as received. Prior to any experiment, all glassware were carefully cleaned to remove any trace of metallic contaminants with aqua regia (3HCl : 1HNO₃). All the aqueous solutions used in the experiments were prepared with ultrapure water (resistivity = 18.2 MΩ cm).

Characterization of gold nanoparticles

The absorption spectra were recorded using Jasco V-630 UV-Vis spectrophotometer (Japan) and Bio-Rad xMark™ microplate absorbance spectrophotometer (India). The transmission electron microscopy (TEM) images were recorded on FEI Tecnai G2 F20 X-Twin transmission electron microscope (USA) and zeta-potential analysis was performed using Nanobrook 90Plus Zeta Brookhaven Instruments (USA). X-ray diffraction (XRD) pattern was recorded on Bruker D8 Advance diffractometer (India).

Synthesis of gold nanoparticles

Synthesis of AuNSs. Citrate-capped spherical AuNPs were synthesized by seed-mediated approach as reported earlier by

Jana *et al.*⁴⁰ Briefly, 0.3 mL of freshly prepared ice-cold NaBH₄ solution (0.1 M) was added to a solution containing 10 mL of TSC (0.25 mM) and 10 mL of HAuCl₄ (0.25 mM) under vigorous stirring. Immediately, the solution color turned from pale yellow to orange-red signifying the formation of Au seeds. These as-prepared seeds were used within 2 h to form AuNSs *via* seed growth method. For this, a growth solution was prepared by gently dissolving 3 g of CTAB in a 100 mL aqueous solution of HAuCl₄ (0.25 mM). Then two sets of 25 mL conical flasks were labeled A and B. In flask A, 50 μL of freshly prepared ascorbic acid solution (0.1 M) was mixed with 7.5 mL of growth solution. This was followed by the addition of 2.5 mL of Au seeds solution under continuous stirring. After 10 min, the solution color changed to wine red indicating the growth of the seed particles. Similarly, for set B, 9 mL of growth solution was mixed with 50 μL of ascorbic acid (0.1 M) solution and to this stirred solution, 1.0 mL of set A solution was added as seed particles. The resultant colloidal solution continued to stir until the color changed to reddish-brown implying the formation of AuNSs and then stored at 4 °C until further use.

Synthesis of AuNRs. CTAB-capped rod-shaped AuNPs were synthesized by a seed-mediated approach as described earlier by Nikoobakht *et al.*⁴¹ In brief, 0.60 mL of freshly prepared ice-cold NaBH₄ solution (10 mM) was injected into a stirred mixture containing 5 mL of each HAuCl₄ (0.50 mM) and CTAB solution (0.20 M). The reaction mixture was continued to stir until the solution color changed to a brownish-yellow indicating the formation of Au seeds. The as-prepared seed solution was allowed to stand without disturbance at room temperature for at least 1 h before being used as seed particles for AuNRs *via* seed-mediated growth method. For growth phase, first 5 mL of CTAB solution (0.20 M) and 0.25 mL of AgNO₃ solution (4 mM) were mixed with 5.0 mL of HAuCl₄ solution (1 mM) under continuous stirring. To this reaction mixture, 70 μL of ascorbic acid solution (78.8 mM) was added which changed the growth solution color from dark yellow to colorless. Lastly, 12 μL of as-prepared seed solution was added which changed the solution color gradually from colorless to brown within 10–20 min, suggesting the formation of the AuNRs. The resultant AuNRs were preserved at 4 °C until further use.

Synthesis of AuNTs. Citrate-capped triangle-shaped AuNPs were prepared by seed-mediated approach as reported earlier by Duchene *et al.*⁴² For seed preparation, 1 mL of freshly prepared ice-cold NaBH₄ solution (100 mM) was added to 37 mL of an aqueous solution containing TSC (0.02 mM) and HAuCl₄ (0.02 mM). An immediate color change was observed from faint yellow to ruby red indicating the formation of Au seeds. The reaction solution was stirred for an additional 5 min and then stored at room temperature for 2–3 h before being used as seed particles for AuNTs synthesis by seed growth method. To prepare the growth solution, 550 μL of each ascorbic acid (100 mM) and NaOH (100 mM) were added to 100 mL of a solution containing CTAB (50 mM) and HAuCl₄ (0.25 mM). Thereafter, 10 μL of NaI solution (100 mM) was added and followed by the addition of 100 μL of Au seeds solution. After two minutes of additional stirring, the reaction mixture was kept under static condition in water bath (maintained at 25 °C) overnight.



Thereafter, the growth solution was poured out to extract the AuNTs in the precipitate which were re-dispersed in 10 mL of CTAB solution (10 mM) solution with quick sonication to achieve high-purity uniform AuNTs. The experimental methods including synthesis protocols for various shapes of AuNPs and characterization techniques are described in the materials and method section in the supplementary section of this manuscript.

Preparation of TMB²⁺ stock solution

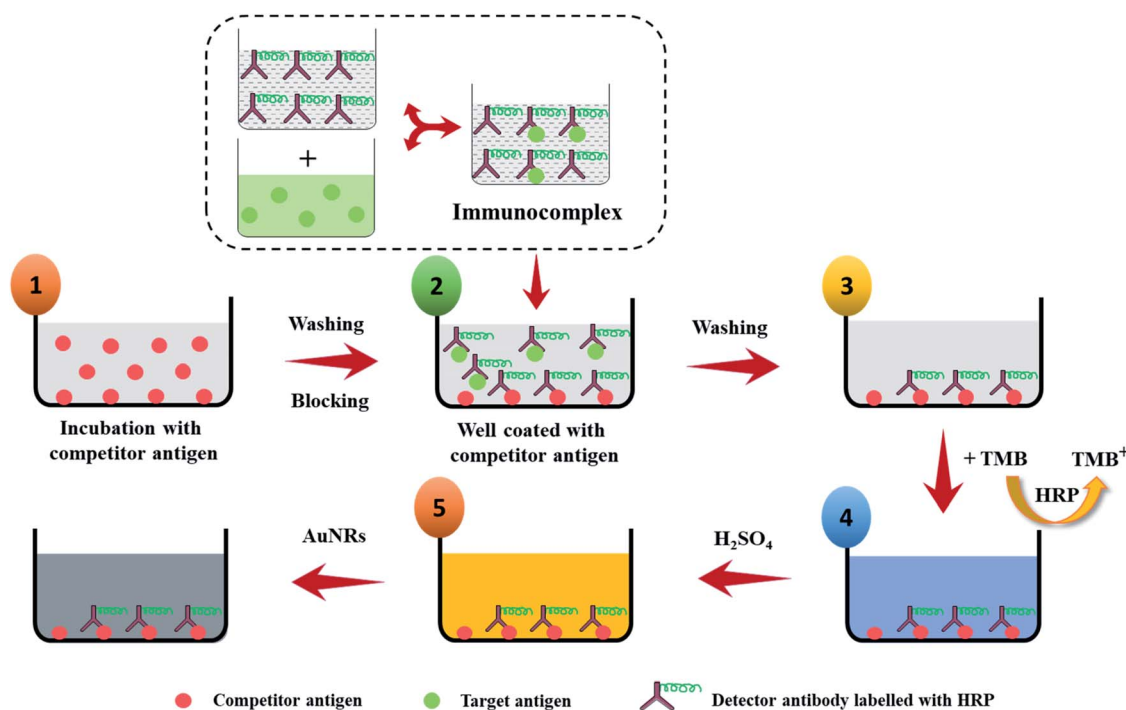
To prepare the TMB²⁺ stock solution, 500 μ L of HRP (100 mU) was mixed with TMB substrate solution which was prepared by mixing 5 mL of TMB (0.83 mM) with 1.23 μ L of H₂O₂ (9.7 mM). An immediate change in the solution color from colorless to blue was observed which indicates the oxidation of TMB into TMB⁺ by HRP. The reaction was continued for about 10 min to ensure the complete conversion of reactant to the product (*i.e.* TMB to TMB⁺). Thereafter, to stop the HRP-mediated oxidation reaction and to initiate the acid-triggered oxidative conversion of TMB⁺ to TMB²⁺, 1.25 mL of H₂SO₄ solution (2 M) was added. An instantaneous change in solution color from blue to yellow was observed which indicates the successful conversion of TMB⁺ (blue) to TMB²⁺ (yellow). The concentration of TMB²⁺ was determined using UV-Vis spectroscopy and Beer–Lambert law by measuring the absorbance at 450 nm (Table S1†).¹¹

Interaction of AuNPs with TMB²⁺

To investigate the interaction behavior of different types of AuNPs with TMB²⁺, the working solutions of all three types of nanoparticles were prepared separately. For this, 2 mL of the as-prepared AuNPs were centrifuged (8000 rpm \times 10 min) followed by discarding of the supernatant and re-dispersion of the settled nanoparticles in 1 mL of CTAB solution (0.06 M). For interaction study, 100 μ L of working solution of all three types of AuNPs were incubated separately with 150 μ L of varying concentrations of TMB²⁺ solution (7 μ M to 131 μ M) in separate vials. A control sample was prepared by mixing 100 μ L of working solution of AuNPs with 150 μ L of DI water. All the samples were incubated at room temperature for 10 min on a rotary mixer, observed for any visible color change, and then characterized using UV-Vis spectrophotometer.

Validation of developed strategy for visual quantification of biomolecules

To realize the potential of the developed strategy towards a biosensor development, an indirect competitive p-ELISA assay was adopted using HlgG as a target antigen and HRP conjugated goat anti-HlgG antibody (GaHlgG@HRP) as the detector molecule (Scheme 2). First, the wells of the microtiter plate were coated with 100 μ L of competitor HlgG solution (conc. = 10 μ g



Scheme 2 Schematic illustration of the p-ELISA strategy for the detection of HlgG. Step 1: microtiter well plate is immobilized with competitor antigen for overnight and then washed and followed by blocking of active sites using BSA to prevent any non-specific interactions; step 2: the target antigen is incubated with HRP enzyme labelled detector antibody for 2 h at room temperature and then the antibody–antigen complexes are added to the wells of the microtiter plates that have been pre-coated with competitor antigen; step 3: wells are washed to remove unbound antigen–antibody complexes and free target antigen; step 4: enzyme substrate is added to the wells and incubated for 10 min at room temperature; step 5: to stop the enzyme-mediated substrate hydrolysis, H₂SO₄ is added and followed by addition of the AuNRs to each well of the plate and then observed for any color change.



mL^{-1} , prepared in 10 mM PBS) overnight at 4 °C. Afterward, the wells were washed thrice with PBST washing buffer (PBS + 0.01% tween 20) to remove any unbound or loosely bound HgG. This was followed by blocking of the free reactive sites on the polystyrene surface of the wells by treating with 200 μL of BSA solution (conc. = 5 mg mL^{-1} , prepared in PBS) for 1 h as this helps in the preventing of any kind of non-specific interaction. Thereafter, the wells were incubated with 100 μL of premix of sample HgG and GaHigG@HRP for 2 h at 37 °C. This premix was prepared by mixing the 100 μL of GaHigG@HRP detector antibody with 100 μL of sample HgG of different concentrations ranging from 1 to 10^{11} fg mL^{-1} for 2 h, individually in separate vials. The washing process was repeated after each interaction step until the enzymatic reaction with TMB. After the interaction, the wells were incubated with 100 μL of TMB solution for 10 min. Thereafter, 50 μL of H_2SO_4 (2 M) was injected into the reaction mixture to stop the enzymatic reaction for successful conversion of TMB^+ to TMB^{2+} which turned the solution color yellow. Afterward, 100 μL of working solution of AuNRs was added to each well which resulted in a visual color change. The change in the optical density [at 450 nm (λ_{max} for TMB^{2+}) and 688 nm (λ_{max} for AuNRs)] and wavelength shift of the reaction mixture was measured using an ELISA plate reader. To assess the specificity of the developed assay, systematic experiments were conducted with negative and positive controls. For negative control, wells were coated

with BSA (instead of competitor HgG) followed by 2 h interaction with 100 μL of GaHigG@HRP (1 : 15 000 in PBS) detector antibody. For positive control, competitor HgG pre-coated wells were interacted with 100 μL GaHigG@HRP (1 : 15 000 in PBS) antibody for 2 h in two different wells and followed by AuNRs addition only in one well, while the other well was kept undisturbed. The rest of the experimental procedure was the same as followed for the sample analyte.

Results and discussion

Characterization of AuNPs

All types of CTAB-capped AuNPs were characterized using UV-Vis spectroscopy, TEM imaging, X-ray powder diffraction (XRD) and zeta potential (Fig. 1). The characteristic extinction spectrum of AuNSs exhibits the extinction peak at 527 nm (Fig. 1a). On the other hand, the extinction spectrum of AuNRs shows two major plasmon peaks at 513 nm and 684 nm, which are associated with the electron oscillation along the transverse and longitudinal direction, respectively (Fig. 1e). The UV-Vis spectrum of AuNTs displays quadrupole and dipole LSPR modes at 872 nm and 1305 nm, respectively (Fig. 1i). For further experiments, we focused on the longitudinal and dipole LSPR modes of AuNRs and AuNTs, respectively. TEM micrographs revealed the formation of uniformly distributed AuNSs (average size = 21.66 ± 1.20 nm), AuNRs (aspect ratio = 2.89 ± 0.30 ,

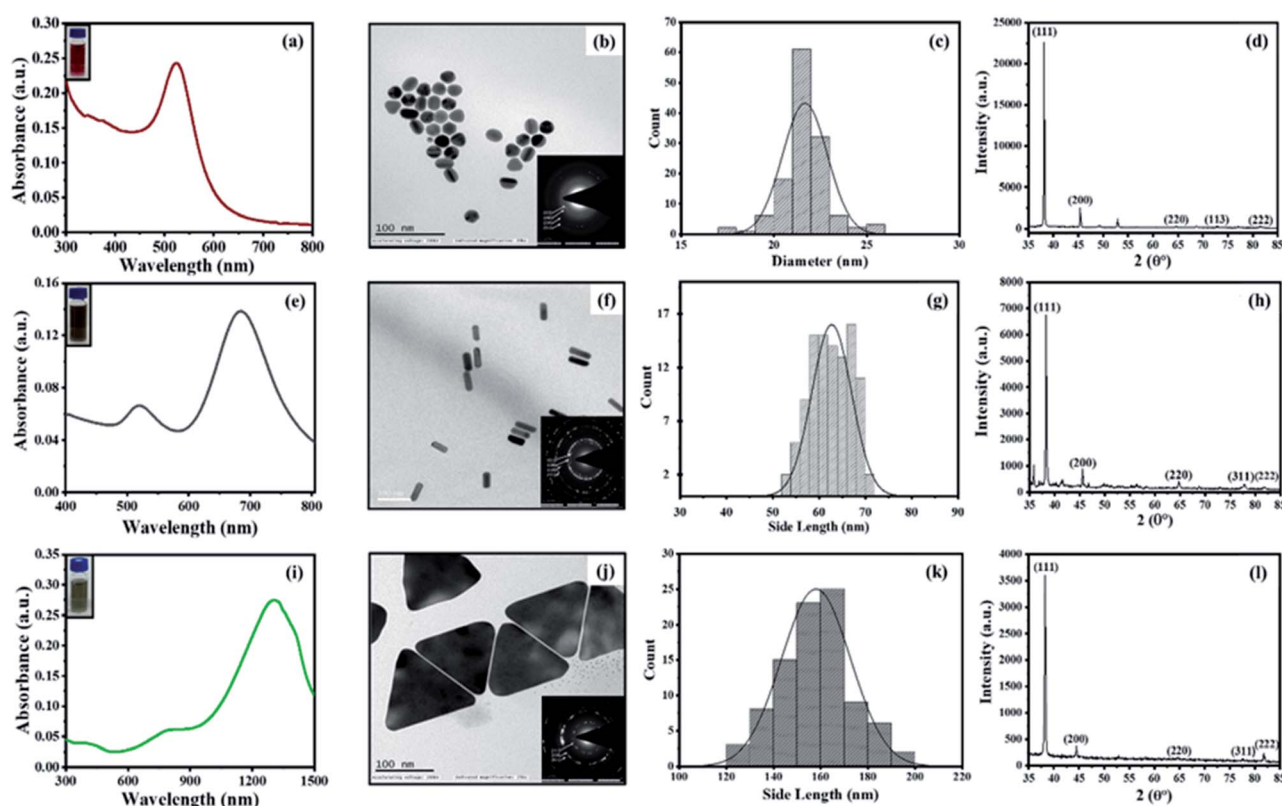


Fig. 1 UV-Vis absorption spectra, transmission electron micrographs, particle size distribution histogram and X-ray diffraction pattern of AuNSs (a–d), AuNRs (e–h), and AuNTs (i–l). The insets of (a, e and i) and (b, f and j) are the photographic images of the corresponding colloidal solution and selected area electron diffraction (SAED) pattern of AuNPs.



average length = 63.27 ± 4.23 nm, average width = 21.96 ± 1.69 nm) and AuNTs (edge length = 157.98 ± 14.65 nm) (Fig. 1b, f and j). The XRD and selected area electron diffraction (SAED) analysis of the AuNPs revealed the crystalline nature of all three AuNPs. The XRD pattern displays four prominent peaks at 38° , 44° , 64° , and 77° , corresponding to (111), (200), (220), and (311) Bragg reflection planes of the face-centered cubic lattice of Au (Fig. 1d, h and l). This indicates that all three shapes of AuNPs consist of pure crystalline Au (JCPDS card no. 04-0784) and the high intensity at (111) reflection plane compared to other planes suggests the predominance of (111) orientation. The clear rings in the SAED patterns, due to sharp reflection from the lattice planes, further confirm the crystalline nature of the AuNPs (Fig. 1b, f and j inset). The zeta potential values of AuNPs were found to be $+65.17 \pm 2.74$ mV, $+20.24 \pm 8.35$ mV, and $+9.31 \pm 0.92$ mV for AuNss, AuNRs, and AuNTs, respectively, which strongly evidence the presence of positively charged CTAB as capping agent on all types of nanoparticles.

Optimization of AuNP dose and interaction time towards the etching of nanoparticles

To obtain the maximum response and prominent color change, the AuNPs dose and interaction time were optimized using AuNRs as representative plasmonic nanoparticles. For the dose optimization, a series of AuNRs solutions of varying concentrations in the range of 0.13 to 0.55 nM were prepared in the individual wells (in both lines A and B) by diluting 25, 50, 75, and 100 μ L of AuNRs with DI water to the final volume of 100 μ L (Fig. 2a). This was followed by the addition of 150 μ L of TMB^{2+} (50 μ M) solution in the wells of line A, while for line B (*i.e.* control experiment), 150 μ L of DI water was added. A gradual increase in the solution color intensity was observed with an increase in the dose of AuNRs (well 1–4 in Fig. 2a). A prominent color change was observed between the TMB^{2+} treated AuNRs (line A) and control AuNRs (line B, without TMB^{2+} treatment) at all the dose levels of AuNRs, however, the color intensity was quite evident at high AuNR dose (*i.e.* AuNR conc. = 0.55 nM). This is due to the fact that at a lower dose of AuNRs (*i.e.* AuNR conc. = 0.13 and 0.28 nM), the TMB^{2+} present in the reaction mixture can completely etch the AuNRs and the solution appears yellow due to the presence of residual TMB^{2+} in the reaction mixture. In contrast, as the concentration of AuNRs increased to 0.40 nM and 0.55 nM, the color of the reaction mixture changed from brown to blue indicating that the TMB^{2+} present in the reaction mixture is not sufficient enough to completely etch the AuNRs and it can only etch them to produce NRs with lower aspect ratios (Fig. 3b). Further, the color intensity of the blue color was found to be relatively more for 0.55 nM of AuNR dose compared to 0.40 nM dose. This is purely associated with an increase in the AuNRs concentration or the number of AuNRs available for TMB^{2+} mediated etching reaction which results in more intense color (Fig. 3a). This is in good agreement with the spectral shift observed after the interaction of 0.55 nM of AuNRs with TMB^{2+} compared to the untreated AuNRs sample (Fig. 2b).

To optimize the reaction time, 150 μ L of two different concentrations (28 μ M and 110 μ M) of TMB^{2+} mixed with 100 μ L

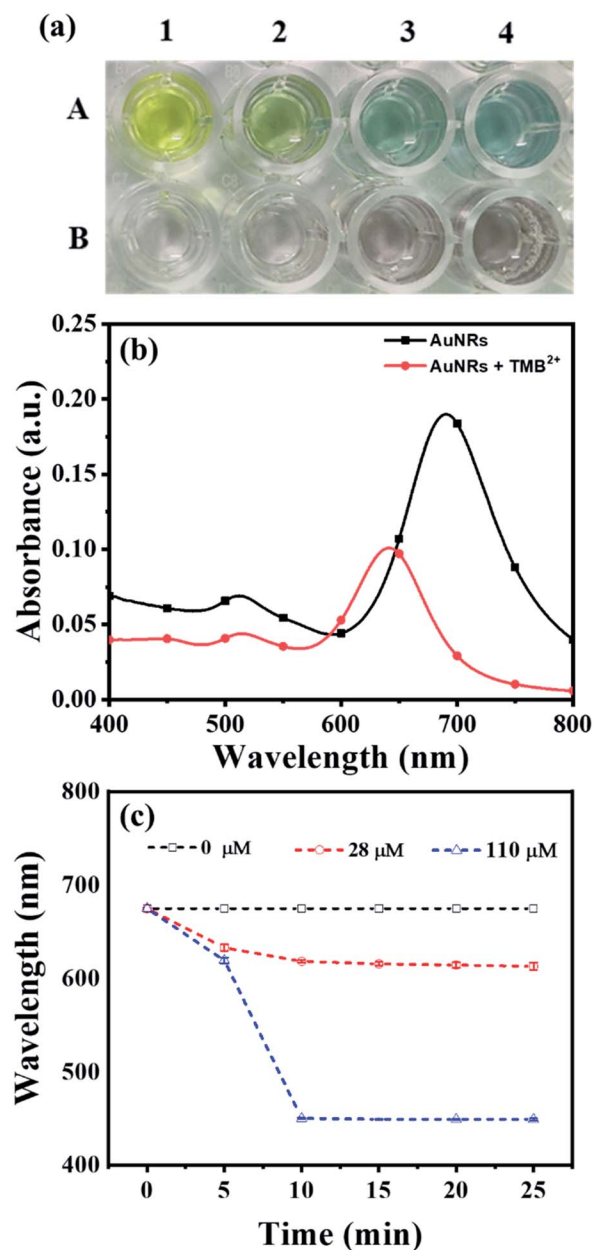


Fig. 2 Optimization of the AuNRs dose; (a) photograph image of the AuNRs sample of varying concentration (0.13, 0.28, 0.40 and 0.55 nM) interacted with 150 μ L of 50 μ M of TMB^{2+} (A₁–A₄), and 150 μ L of water (B₁–B₄), respectively (total volume = 250 μ L with water); (b) UV-Vis spectra of the AuNRs (0.55 nM) after interaction with 150 μ L of each water (black line) and TMB^{2+} (red line) and (c) optimization of the etching time; AuNRs (0.55 nM) were interacted with 150 μ L of water (black dotted line), 28 μ M TMB^{2+} (red dotted line), and 110 μ M TMB^{2+} (blue dotted line).

of AuNRs solution. For the control study, 150 μ L of water was mixed with 100 μ L of AuNRs solution. Fig. 2c shows a time-dependent blue-shift in the longitudinal LSPR peak of AuNRs, which reaches a saturation level at 10 min for both the concentration levels indicating that the etching reaction kinetics has reached to a balanced state. However, in the absence of TMB^{2+} (control experiment), no change in the plasmonic peak was observed suggesting the essential requirement



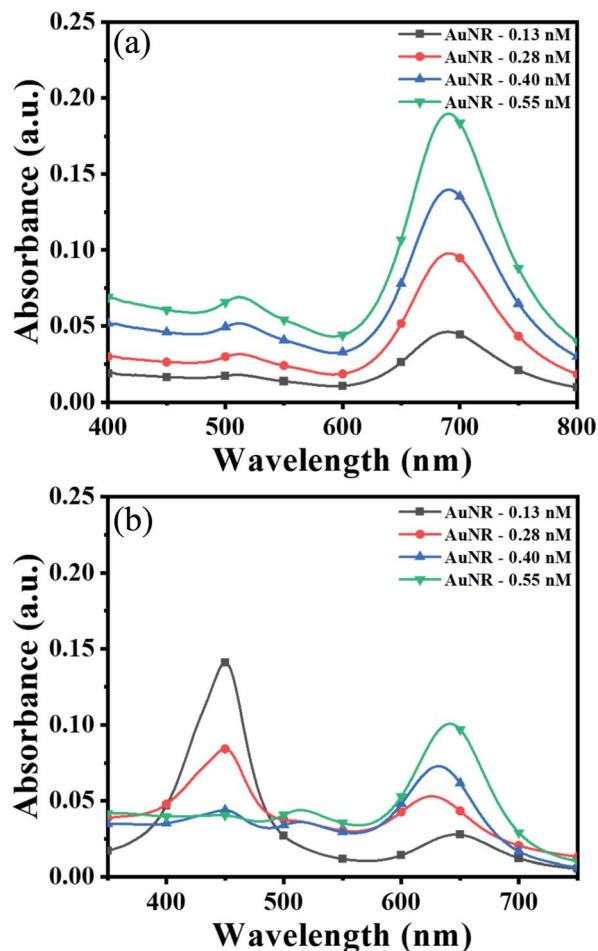


Fig. 3 UV-Vis spectra of (a) AuNRs of 0.13, 0.28, 0.40 and 0.55 nM after interaction with 150 μL of water and (b) 150 μL of 50 μM conc. of TMB^{2+} (for all the samples, total volume was made up to 250 μL with water).

of TMB^{2+} for the etching of the AuNRs. Hence, 100 μL of AuNRs dose and 10 min interaction time was selected as optimum parameters for TMB^{2+} mediated etching.

Interaction analysis of different AuNPs with TMB^{2+}

Prior to the interaction study, it is important to establish that enzyme and residual H_2O_2 (present in the TMB^{2+} stock solution) have neither direct interaction with AuNPs nor interfere with the etching reaction. To assess this, 100 μL of colloidal AuNRs solution interacted with 150 μL of each of H_2O_2 (1.2 mM), 10 mU of HRP enzyme, and TMB^{2+} (110 μM) for 10 min at room temperature. Both H_2O_2 and HRP interacted samples did not show any shift in the LSPR peak indicating that the chosen concentrations of both H_2O_2 and HRP neither affect the stability of AuNRs nor cause their etching (Fig. 4). In contrast, TMB^{2+} treated sample showed a prominent blue shift in the longitudinal plasmon band of AuNRs suggesting their geometrical transformation. Hence, the obtained results established that the HRP and residual H_2O_2 , present in the TMB^{2+} solution, have no direct effect on AuNRs and also their presence does not influence the TMB^{2+} mediated etching process.

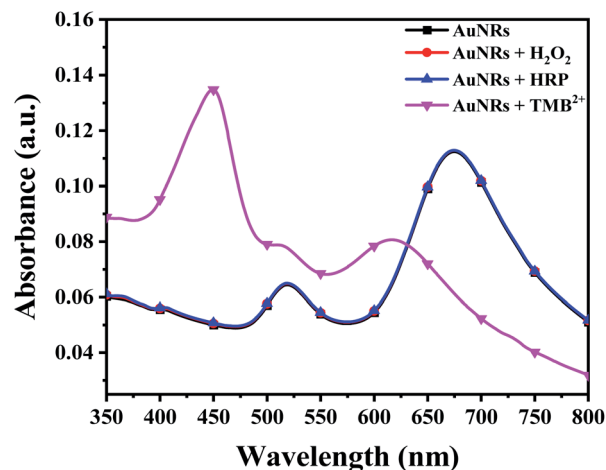


Fig. 4 UV-Vis spectra AuNRs interacted with DI water (black curve), H_2O_2 (red curve), HRP (blue curve) and TMB^{2+} (pink curve) to study the effect of different reagents on TMB^{2+} mediated oxidation of AuNRs. (Note: black, blue and red curves are difficult to discern due to overlapping).

To investigate the effect of nanoparticle shape on their etching pattern, TMB^{2+} solution of varying concentrations (0–131 μM) interacted with all three types of AuNPs individually. The UV-Vis spectra of the interacted samples, the percentage shift in their respective LSPR peak and absorbance ratio ($A_{\text{plasmonic peak}}/A_{450 \text{ nm}}$) as a function of TMB^{2+} concentrations are displayed in Fig. 5. The LSPR peak of the interacted AuNPs appeared significantly blue-shifted with a prominent decrease in the absorbance intensity at their respective plasmonic peak as a function of TMB^{2+} concentration (Fig. 5a–c and S1†). However, the pattern and magnitude of LSPR peak shifts were found to be different for all three shapes of AuNPs. For instance, in the case of AuNSs, at a lower concentration ($\leq 21 \mu\text{M}$) of TMB^{2+} , the LSPR peak did not show any considerable shift in the wavelength, however, a prominent change in the absorbance intensity ($\lambda_{\text{max}} = 527 \text{ nm}$) was observed due to their homogeneous etching without any shape-transformation (Fig. 5d and g).⁴³ This can be easily correlated with the visual change in the color of the AuNSs solution from dark pink to light pink after interaction with $\leq 21 \mu\text{M}$ concentrations of TMB^{2+} . In contrast, at a higher concentration of the TMB^{2+} ($> 21 \mu\text{M}$), the plasmonic peak gradually disappeared with a significant drop in the absorbance intensity at peak plasmonic wavelength, and a new peak at 450 nm was observed corresponding to TMB^{2+} (Fig. 5d and g). This was evident also from the change in color of the reaction solution from pink to yellow. This is due to the fact that at high concentrations of TMB^{2+} , the AuNSs (Au^0) are completely etched into Au^+ resulting in their depletion from the reaction mixture and thereby disappearance of their plasmonic peak.⁴⁴ Simultaneously, the unreacted or remaining yellow color TMB^{2+} level increases, which exhibits its characteristic peak at 450 nm.

In contrast to AuNSs, both AuNRs and AuNTs showed a TMB^{2+} concentration-dependent blue-shift along with a decrease in the absorbance intensity at their respective plasmonic peaks even at



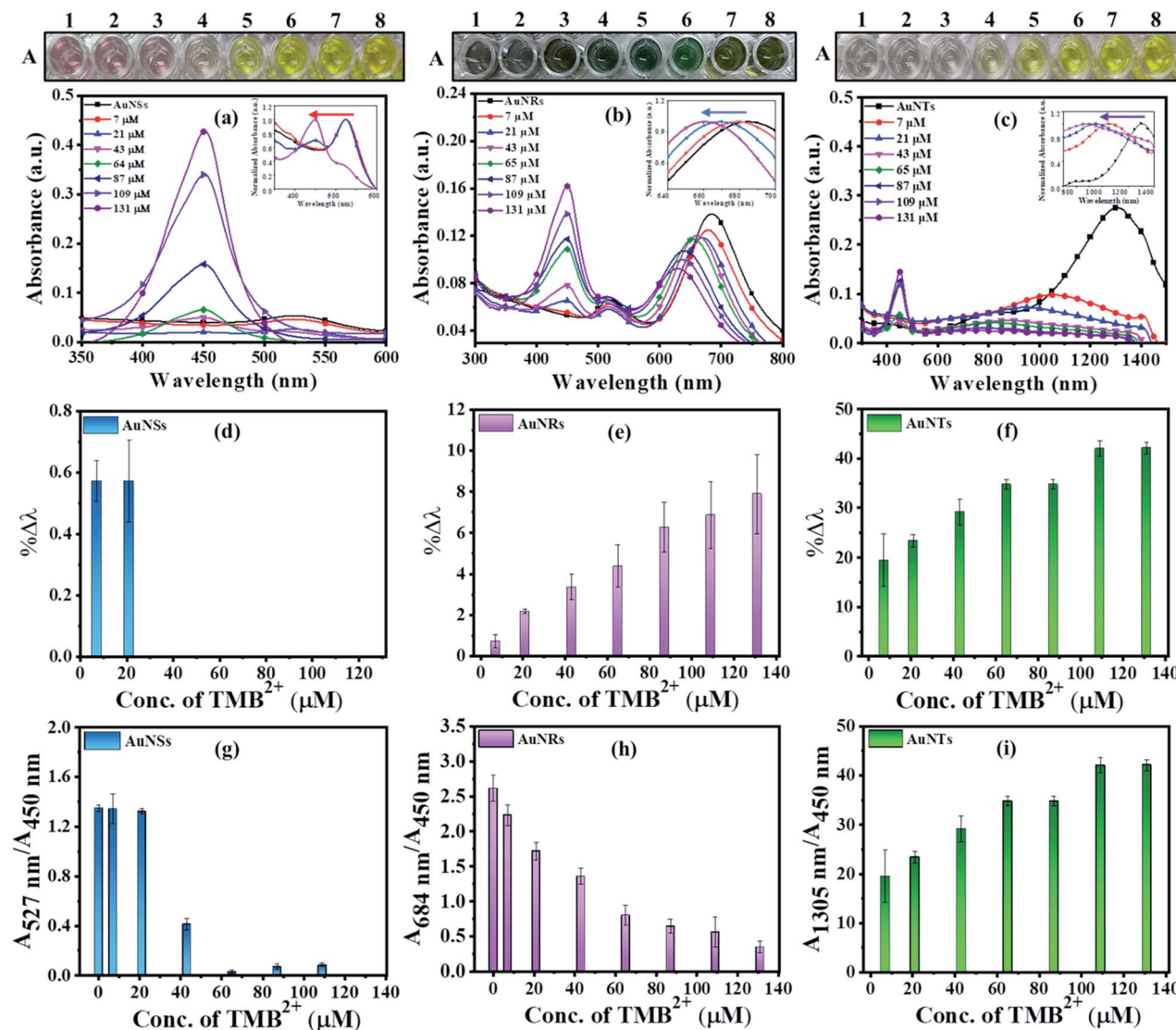


Fig. 5 AuNPs and TMB^{2+} interaction analysis. The photographic image, UV-Vis spectra, percentage shift in the LSPR peak wavelength and absorbance ratio (absorbance at LSPR peak to absorbance at 450 nm) of AuNSs (a, d and g), AuNRs (b, e and h), and AuNTs (c, f and i) after interaction with different concentrations of TMB^{2+} (0–131 μM). (Note: The LSPR plasmonic peak of AuNSs completely disappeared at higher concentrations of the TMB^{2+} (>21 μM) and a new peak at 450 nm was observed corresponding to TMB^{2+} , therefore $\% \Delta \lambda$ calculated at those concentrations is zero in fig (d)).

lower concentrations of TMB^{2+} (*i.e.* ≤ 21) (Fig. 5b and c). Similar to AuNSs, in both cases, the appearance of a new peak at 450 nm with a gradual increase in its intensity was observed with an increase in the TMB^{2+} concentration to 43 μM onwards, indicating the presence of unreacted TMB^{2+} in the reaction mixture. As presented in Fig. 5(e and f), $\% \Delta \lambda$ was found to increase from 0.73–7.87% and 19.54–42.14% for AuNRs and AuNTs, respectively as the concentration of TMB^{2+} increased from 7–131 μM . This indicates that the LSPR peak shift value was observed to be more in the case of AuNTs than AuNRs. This can be easily correlated with a multicolor and single-color change observed for AuNRs and AuNTs, respectively (Fig. 5). This might be due to the presence of sharp curved tips/features of the AuNTs at the corners ($\sim 60^\circ$) which are possibly hot regions towards the etching owing to lesser capping coverage.⁴⁵ Additionally, as a result of the finite

thickness of the AuNTs, a little change in the edge length of AuNTs by means of TMB^{2+} mediated etching induces a large change in their aspect ratios and thus a sharper LSPR shift.⁴⁶ Conversely, in the case of AuNRs, the etching reaction is not isotropic in all directions and these are preferentially etched along the axial direction. This can be ascribed to lesser CTAB capping density at the tips as compared to the sides of the AuNRs which favors the greater interaction with TMB^{2+} at tips, resulting in AuNRs with different aspect ratios.¹⁷

In addition to the sharp surface feature of AuNPs, differences in the crystal facets of the nanoparticles may also have a significant role towards different surface binding and reactivities, contributing to variations in etching.⁴⁷ For instance, the surface energies of metal crystal planes are in order of (110) > (100) > (111) and depending on this, they possess different



reactivities and stability. In the case of AuNTs, the bottom and side edge surfaces are composed of (111) and (110) crystal facets, respectively. The atoms at the corner areas and (110) facet possess higher energy than those at the (111) facet due to their lower coordination numbers. Therefore, the corners and side edges of the NTs are more prone to be etched compared to other areas. As the etching reaction continues, morphological changes occur in NTs starting from sharp triangle prisms and progressing to “snipped” triangular, hexagonal, and eventually, disk-like nanoplates. On the other hand, in the case of AuNRs, the side surface is surrounded by (110) and the tip is enclosed by (111) and (001) crystal facets.⁴⁷ As the (111) facet is considered to be the highly stable surface and least reactive, the (110) facet is extremely reactive and the most prone to reconstructions. However, owing to the presence of CTAB molecules, the (110) and (100) facets of AuNRs become more stable than (111) planes, therefore, the tip of AuNRs with (111) facets might be potentially etched during the reaction.^{48,49} This is reflected by the gradual change in the color of AuNRs and AuNTs solution during the etching reaction. To further support, TEM analysis of the AuNTs and AuNRs before and after interaction with TMB²⁺ was carried out which revealed a significant decrease in the aspect ratio of AuNRs (AR = from 2.89 ± 0.30 to 2.16 ± 0.23) and edge length (from 157.98 ± 14.65 nm to 57.84 ± 5.59 nm) of AuNTs (Fig. 6). These results strongly support the crystal facet-dependent preferential etching of the AuNRs and AuNTs.

Conclusively, all three shapes of AuNPs show geometrical transformation in their shape due to etching by TMB²⁺, however, the change in the plasmonic peak is more prominent for AuNRs and AuNTs. Further, the AuNRs displayed a gradual change in LSPR peak shift, absorbance intensity ratio and visually detectable multicolor change compared to the AuNSs and AuNTs, which showed only single-color transformation (from pink to yellow for AuNSs and green to yellow for AuNTs). Hence, these results indicate that the TMB²⁺ mediated etching of AuNPs is significantly influenced by their shape which would also reflect during visual detection-based biosensor development when such etching reaction is employed in the reaction.

Immunoassay and detection principle

To demonstrate the feasibility of the AuNRs-etching mediated biosensing, we applied this method to develop an indirect competitive p-ELISA for visual detection of HlgG. The samples containing known concentrations of HlgG (conc. = $1-10^{11}$ fg mL⁻¹) interacted with GaHlgG@HRP (enzyme-linked specific detector antibody) in separate vials which form a stable HlgG-GaHlgG@HRP immunocomplex in proportion to the HlgG concentration present in the sample. Thereafter, this pre-mix was introduced in the microtiter plate wells pre-coated with competitor HlgG so that the free GaHlgG@HRP can interact with the competitor HlgG, *i.e.* pre-coated on the microplate. Subsequently, HRP catalyzed the conversion of TMB into TMB⁺ which is followed by the addition of concentrated H₂SO₄ to obtain TMB²⁺. The generated TMB²⁺ mediates the oxidative etching of AuNRs, resulting in distinct color changes which are accompanied by a blue shift in their longitudinal plasmonic peak. The solution displays a multicolor change as the concentration of HlgG decreases in the sample (Fig. 7a). As the HlgG concentration in the sample increases, lesser GaHlgG@HRP will be available for binding to the pre-coated competitor HlgG. As a result, lesser or no enzymatic conversion of TMB to TMB⁺ takes place and thereby no etching of the AuNRs and therefore the solution color remained unchanged.

The instrumental analysis of the interacted samples corroborated the visual detection findings. The absorbance spectra of the developed competitive p-ELISA showed an increase in the absorbance intensity at 688 nm and a corresponding decrease in the absorbance intensity at 450 nm as a function of HlgG concentration in the sample (Fig. 7b). This is due to the fact that with an increase in the concentration of HlgG, the number of detector antibodies available to interact with pre-immobilized competitor antigen reduces concurrently and this consequently minimizes the conversion of TMB into TMB⁺ *via* HRP and thereby the etching of the AuNRs.

To evaluate the selectivity of the developed sensing strategy, both positive and negative control studies were carried and the results are shown in Fig. 7a and S2.† For positive control studies (*i.e.* in the absence of HlgG in the sample), two different experiments were performed. In the well A₁, AuNRs were added to the biocatalytically produced TMB²⁺ reaction mixture, while in the well A₂, AuNRs were not added and thus exhibited the characteristic yellow color of the TMB²⁺. The absorbance at

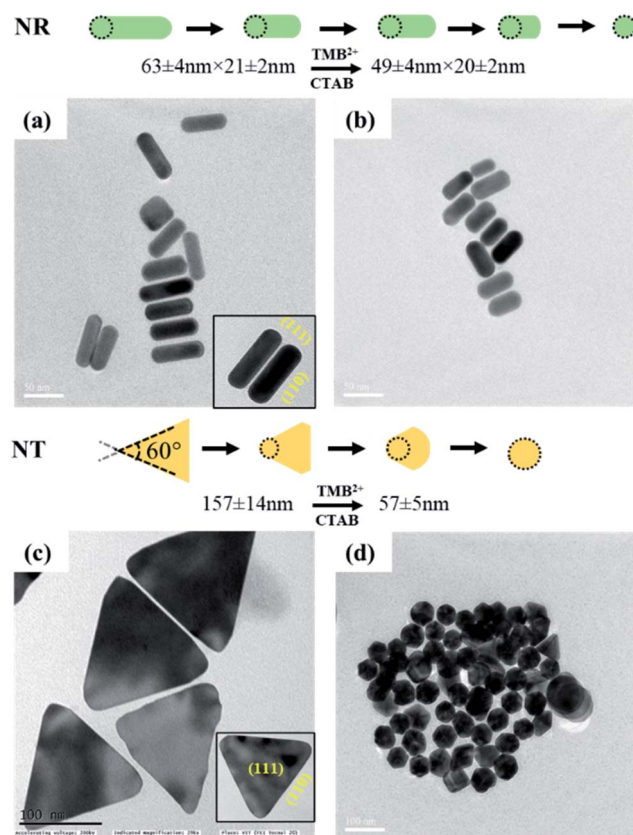


Fig. 6 TEM images of AuNRs (top) and AuNTs (bottom) (left, a and c) before and (right, b and d) after interaction with TMB²⁺.



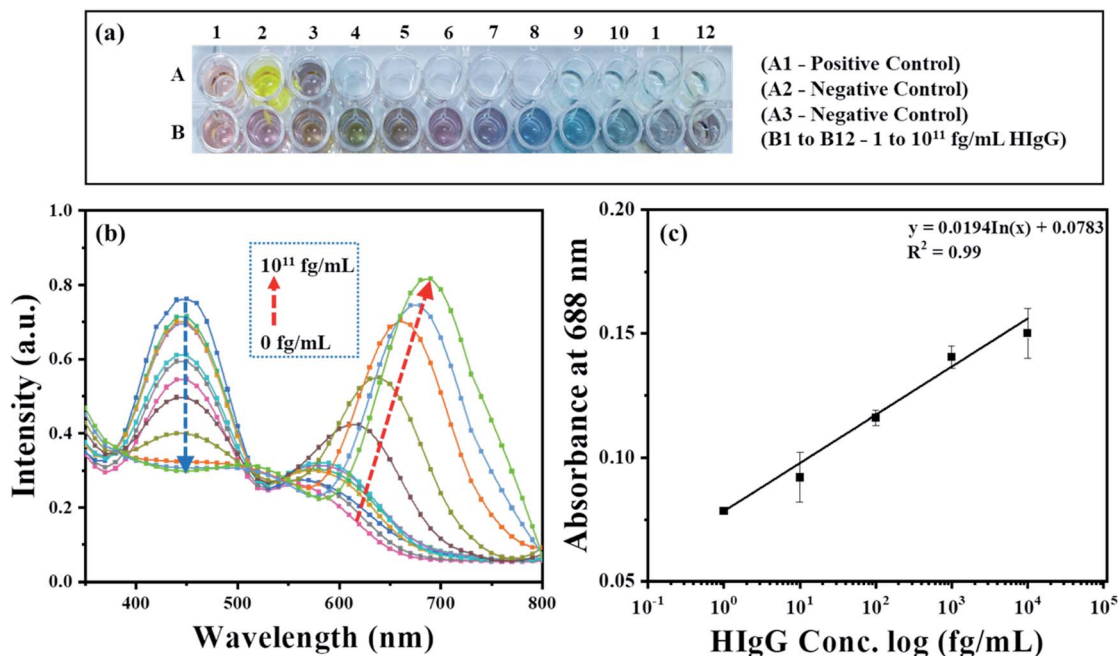


Fig. 7 (a) Photos of microtiter plate wells containing AuNRs interacted with TMB²⁺, produced as a product of the enzymatic reaction in developed competitive p-ELISA and (b) UV-Vis absorption spectra of AuNRs after interaction with different concentrations of HIgG (0 to 10¹¹ fg mL⁻¹). (c) The linear relationship between absorbance change ($\lambda_{\max} = 688$ nm) and log concentration of HIgG.

450 nm was observed to be the highest for both the controls, which is due to the fact that in the absence of HIgG in the sample, the maximum number of standard HIgG-GaHIgG@HRP binding events took place. This resulted in a greater number of HRP molecules available for the conversion of TMB to TMB²⁺ (Fig S2,† black curve). In addition, we observed a prominent change in the color of AuNRs solution from brown to light pink (Fig. 7a, well A₁), indicating the maximum etching of the nanorods as the GaHIgG@HRP was freely available to form the immunocomplex with the standard immobilized HIgG on the well. For the negative control experiment, the standard HIgG (*i.e.* pre-coated on the wells) was replaced with BSA and then interacted with the GaHIgG@HRP. In this case, the AuNRs solution did not show any spectral shift and color change (Fig. 7a, well A₃ and Fig S2,† red curve). This suggests the no binding of the GaHIgG@HRP towards the BSA and thereby no catalytic conversion of TMB into TMB²⁺ and thus no etching and/or color change. This indicates the highly specific nature of the developed plasmonic immunoassay.

For the calibration curve, the absorbance values ($\lambda_{\max} = 688$ nm) were plotted against the logarithm concentration of sample HIgG. As shown in Fig. 7c, the calibration curve exhibits good linearity in ranges from 1 to 10⁴ fg mL⁻¹ of HIgG (Table S2 in ESI†). In contrast, a gradual decrease in the absorbance intensity at 450 nm was observed as a logarithm concentration of HIgG (Fig. S3†). This evidences that visual color changes at fg mL⁻¹ concentration level of the analyte are in accordance with the instrumental results and proves the potential of AuNRs-etching based naked eye detection-based ultra-sensitive biosensor. The etching of AuNRs *via* TMB²⁺ produced multi-color changes in proportion to the concentration of sample HIgG (Fig. 7a). The naked eye detection limit of the developed immunosensing strategy was found to be as low as 1 fg mL⁻¹ (~6.54 aM), which is comparable or better than other instrumentation based biosensing platforms developed by employing different AuNPs (Table 1).^{50–54} In addition, compared to the other reported nanoparticle-based ELISA sensing strategies, the developed method provides several other advantages including

Table 1 Comparative analysis of the analytical performances of different AuNPs based optical sensors for biomolecule detection

Technique/Instrument	AuNPs Type	Target analyte	LoD (aM)	Ref.
SPR	AuCNPs	B-type natriuretic peptide	10	50
Colorimetric/microplate reader	AuNSs	Prostate-specific antigen (PSA)	93	51
Plasmonic fiber optic sensor	AuNSs	PSA	3×10^3	52
SERS/Raman microscope	AuNSs	C-reactive protein	10	53
Plasmonic fiber optic sensor	AuNSs	HIgG	7	54
p-ELISA/naked eye	AuNRs	HIgG	6.54	This study

(i) easy integration with conventional ELISA schemes, wherein HRP-labeled detector antibodies are used,^{55,56} (ii) elimination of false positive and negative signal due to autoaggregation of the nanoparticles,^{57,58} (iii) the greater stability of the AuNRs towards temperature, light and the biological thiols as compared to silver nanoprisms,⁵⁹ and (iv) easy and simple as it does not require any conjugation or surface functionalization of the AuNRs.^{60,61}

Conclusion

In the present work, we have reported the oxidative etching of different shapes of AuNPs *via* TMB²⁺, a product of the enzymatic reaction that is most commonly utilized for ELISA-based detection platforms. All three shapes of the AuNPs showed a spectral shift and change in absorbance at their respective LSPR peak after interaction with different concentrations of TMB²⁺. Amongst all three shapes of AuNPs, TMB²⁺-mediated etching of AuNRs led to a vivid color response in relation to the concentration of the etchant. This was due to the selective etching at the tips of the nanorods that led to the formation of AuNRs of different aspect ratios as a function of TMB²⁺ concentration. This optimized strategy was further realized into a multicolorimetric visual detection system for the sensing of HlgG. The competitive p-ELISA could detect the HlgG with a visual detection limit of 1 fg mL⁻¹ through the naked eye without the aid of any sophisticated instrument. Although AuNR-etching based p-ELISA has the potential for visual detection at a very low level of the analyte, it suffers from manual intervention in order to perform the complete bioassay. It may also pose the risk of manual error and thus may lead to a false signal. Hence, to minimize these risks and reduce manual intervention, efforts must be made to integrate the p-ELISA technique with microfluidic or chip-based technology and realize it into a point-of-care diagnostic system for various disease detection.

Author contributions

Sangeeta Yadav: investigation, methodology, writing – original draft. Jitendra Satija: conceptualization, supervision, writing – review & editing.

Conflicts of interest

There are no conflicts to declare.

Acknowledgements

The authors thank the Vellore Institute of Technology (VIT) for providing Seed Grant (SG20210170) for carrying out this research work.

References

- 1 R. de la Rica and M. M. Stevens, *Nat. Nanotechnol.*, 2012, **7**, 821–824.
- 2 R. Chen, X. Huang, H. Xu, Y. Xiong and Y. Li, *ACS Appl. Mater. Interfaces*, 2015, **7**, 28632–28639.
- 3 C. Yao, S. Yu, X. Li, Z. Wu, J. Liang, Q. Fu, W. Xiao, T. Jiang and Y. Tang, *Anal. Bioanal. Chem.*, 2017, **409**, 1093–1100.
- 4 Q. Yang, R. Cai, W. Xiao, Z. Wu, X. Liu, Y. Xu, M. Xu, H. Zhong, G. Sun, Q. Liu, Q. Fu and J. Xiang, *Nanoscale Res. Lett.*, 2018, **13**, 397.
- 5 L. Wu, G. Li, X. Xu, L. Zhu, R. Huang and X. Chen, *Trends Anal. Chem.*, 2019, **113**, 140–156.
- 6 K. Kołataj, J. Krajczewski and A. Kudelski, *Environ. Chem. Lett.*, 2020, **18**, 529–542.
- 7 J. N. Anker, W. P. Hall, O. Lyandres, N. C. Shah, J. Zhao and R. P. Van Duyne, *Nat. Mater.*, 2008, **7**, 442–453.
- 8 E. Petryayeva and U. J. Krull, *Anal. Chim. Acta*, 2011, **706**, 8–24.
- 9 Z. Zhang, Z. Chen, S. Wang, F. Cheng and L. Chen, *ACS Appl. Mater. Interfaces*, 2015, **7**, 27639–27645.
- 10 J. Li, Y. Y. Wei, X. P. Liu and Z. R. Xu, *Sens. Actuators, B*, 2022, **353**, 131139.
- 11 P. D. Josephy, T. Eling and R. P. Mason, *J. Biol. Chem.*, 1982, **257**, 3669–3675.
- 12 P. K. Jain, K. S. Lee, I. H. El-Sayed and M. A. El-Sayed, *J. Phys. Chem. B*, 2006, **110**, 7238–7248.
- 13 J. Liao, Y. Zhang, W. Yu, L. Xu, C. Ge, J. Liu and N. Gu, *Colloids Surf., A*, 2003, **223**, 177–183.
- 14 K. Sato, K. Hosokawa and M. Maeda, *J. Am. Chem. Soc.*, 2003, **125**, 8102–8103.
- 15 J. Tharion, J. Satija and S. Mukherji, *Plasmonics*, 2014, **10**, 753–763.
- 16 J. Satija, J. Tharion and S. Mukherji, *RSC Adv.*, 2015, **5**, 69970–69979.
- 17 R. Zou, X. Guo, J. Yang, D. Li, F. Peng, L. Zhang, H. Wang and H. Yu, *CrystEngComm*, 2009, **11**, 2797–2803.
- 18 S. A. Alex, J. Satija, M. A. Khan, G. M. Bhalerao, S. Chakravarty, B. Kasilingam, A. Sivakumar, N. Chandrasekaran and A. Mukherjee, *Anal. Methods*, 2015, **7**, 5583–5592.
- 19 X. M. Nie, R. Huang, C. X. Dong, L. J. Tang, R. Gui and J. H. Jiang, *Bioelectron*, 2014, **58**, 314–319.
- 20 N. Toshima and T. Yonezawa, *New J. Chem.*, 1998, **22**, 1179–1201.
- 21 S. S. Shankar, A. Rai, A. Ahmad and M. Sastry, *J. Colloid Interface Sci.*, 2004, **275**, 496–502.
- 22 M. Rycenga, C. M. Cobley, J. Zeng, W. Li, C. H. Moran, Q. Zhang, D. Qin and Y. Xia, *Chem. Rev.*, 2011, **111**, 3669–3712.
- 23 X. Yang and Z. Gao, *Chem. Commun.*, 2015, **51**, 6928–6931.
- 24 M. Yuan, Q. Xiong, G. Zhang, Z. Xiong, D. Liu, H. Duan and W. Lai, *J. Mater. Chem. B*, 2020, **8**, 3667–3675.
- 25 M. R. Ivanov, H. R. Bednar and A. J. Haes, *ACS Nano*, 2009, **3**, 386–394.
- 26 R. Pamies, J. G. H. Cifre, V. F. Espín, M. Collado-González, F. G. D. Baños and J. G. de la Torre, *J. Nanopart. Res.*, 2014, **16**, 2376.
- 27 N. Bizmark and M. A. Ioannidis, *Langmuir*, 2015, **31**, 9282–9289.



- 28 J. Satija, N. Punjabi, D. Mishra and S. Mukherji, *RSC Adv.*, 2016, **6**, 85440–85456.
- 29 E. Hao, G. C. Schatz and J. T. Hupp, *J. Fluoresc.*, 2004, **14**, 331–341.
- 30 C. Yu and J. Irudayaraj, *Anal. Chem.*, 2007, **79**, 572–579.
- 31 N. Jana and T. Pal, *Adv. Mater.*, 2007, **19**, 1761–1765.
- 32 K. M. Mayer, S. Lee, H. Liao, B. C. Rostro, A. Fuentes, P. T. Scully, C. L. Nehl and J. H. Hafner, *ACS Nano*, 2008, **2**, 687–692.
- 33 B. Tang, J. Wang, S. Xu, T. Afrin, W. Xu, L. Sun and X. Wang, *J. Colloid Interface Sci.*, 2011, **356**, 513–518.
- 34 Z. He, J. Zhu, G. J. Weng, J. J. Li and J. W. Zhao, *Nanotechnology*, 2020, **31**, 335505.
- 35 Z. Zhang, Z. Chen, C. Qu and L. Chen, *Langmuir*, 2014, **30**, 3625–3630.
- 36 Z. Zhang, Z. Chen, F. Cheng, Y. Zhang and L. Chen, *Analyst*, 2016, **141**, 2955.
- 37 Z. Zhang, H. Wang, Z. Chen, X. Wang, J. Choo and L. Chen, *Biosens. Bioelectron.*, 2018, **114**, 52–65.
- 38 T. Porstmann and S. T. Kiessig, *J. Immunol. Methods*, 1992, **150**, 5–21.
- 39 L. Guo, S. Xu, X. Ma, B. Qiu, Z. Lin and G. Chen, *Sci. Rep.*, 2016, **6**, 32755.
- 40 N. R. Jana, L. Gearheart and C. J. Murphy, *Langmuir*, 2001, **17**, 6782–6786.
- 41 B. Nikoobakht and M. A. El-Sayed, *Chem. Mater.*, 2003, **15**, 1957–1962.
- 42 J. S. DuChene, *et al.*, *Chem. Mater.*, 2013, **25**, 1392–1399.
- 43 S. Sun, M. Gao, G. Lei, H. Zou, J. Ma and C. Huang, *Nano Res.*, 2016, **9**, 1125–1134.
- 44 X. Ma, Y. Lin, L. Guo, B. Qiu, G. Chen, H.-h. Yang and Z. Lin, *Biosens. Bioelectron.*, 2017, **87**, 122–128.
- 45 J. E. Millstone, W. Wei, M. R. Jones, H. Yoo and C. A. Mirkin, *Nano Lett.*, 2008, **8**, 2526–2529.
- 46 H. Yuan, K. P. F. Janssen, T. Franklin, G. Lu, L. Su, X. Gu, H. Uji-i, M. B. J. Roelfaers and J. Hofkens, *RSC Adv.*, 2015, **5**, 6829–6833.
- 47 T. S. Sreeprasad, A. K. Samal and T. Pradeep, *Langmuir*, 2007, **23**, 9463–9471.
- 48 Z. L. Wang, R. P. Gao, B. Nikoobakht and M. A. El-Sayed, *J. Phys. Chem. B*, 2000, **104**, 5417–5420.
- 49 C. J. Johnson, E. Dujardin, S. A. Davis, C. J. Murphy and S. Mann, *J. Mater. Chem.*, 2002, **12**(6), 1765–1770.
- 50 H. R. Jang, A. W. Wark, S. H. Baek, B. H. Chung and H. J. Lee, *Anal. Chem.*, 2014, **86**, 814–819.
- 51 D. Liu, J. Yang, H.-F. Wang, Z. Wang, X. Huang, Z. Wang, G. Niu, A. R. H. Walker and X. Chen, *Anal. Chem.*, 2014, **86**, 5800–5806.
- 52 M. Sanders, Y. Lin, J. Wei, T. Bono and R. Lindquist, *Biosens. Bioelectron.*, 2014, **61**, 95–101.
- 53 A. Hwang, E. Kim, J. Moon, H. Lee, M. Lee, J. Jeong, E.-K. Lim, J. Jung, T. Kang and B. Kim, *ACS Appl. Mater. Interfaces*, 2019, **11**, 18960–18967.
- 54 R. Bandaru, M. Divagar, S. Khanna, C. G. Danny, S. Gupta, V. Janakiraman and V. V. R. Sai, *Sens. Actuators, B*, 2020, **321**, 128463.
- 55 N. Feng, J. Shen, Y. Chen, C. Li, Y. Hu, L. Zhang, S. Chen, Q. Fan, W. Huang and L. Wang, *Nano Res.*, 2020, **13**(12), 3364–3370.
- 56 Z. Chen, H. wang, Z. Zhang and L. Chen, *Anal. Chem.*, 2019, **91**, 1254–1259.
- 57 Y. Xianyu, Z. Wang and X. Jiang, *ACS Nano*, 2014, **8**(12), 12741–12747.
- 58 Y. Xianyu, Y. Chen and X. Jiang, *Anal. Chem.*, 2015, **87**, 10688–10692.
- 59 B. Tang, S. Xu, X. Hou, J. Li, L. Sun, W. Xu and X. Wang, *ACS Appl. Mater. Interfaces*, 2013, **5**, 646–653.
- 60 Y. Wu, Y. Xiong, X. Chen, D. Luo, B. Goa, J. Chen, X. Huang, Y. Leng and Y. Xiong, *J. Dairy Sci.*, 2019, **102**, 10877–10886.
- 61 Y. Y. Ozawa, N. Lobsiger, Y. Muto, T. Mori, K. Yoshimura, Y. Yano, W. J. Stark, M. Maeda, T. Asahi, A. Ogawa and T. Zako, *RSC Adv.*, 2021, **11**, 11984–11991.

