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Real-time detection of acetone gas molecules at ppt levels in an air atmosphere using a partially suspended graphene surface acoustic wave skin gas sensor†

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To improve the quality of modern life in the current society, low-power, highly sensitive, and reliable healthcare technology is necessary to monitor human health in real-time. In this study, we fabricated partially suspended monolayer graphene surface acoustic wave gas sensors (G-SAWs) with a love-mode wave to effectively detect ppt-level acetone gas molecules at room temperature. The sputtered SiO₂ thin film on the surface of a black 36°YX-LiTaO₃ (B-LT) substrate acted as a guiding layer, effectively reducing the noise and insertion loss. The G-SAWs exhibited enhanced gas response towards acetone gas molecules (800 ppt) in a real-time atmosphere. The high sensitivity of the G-SAW sensor can be attributed to the elasticity and surface roughness of the SiO₂ film. In addition, the G-SAW sensor exhibited rapid response and recovery at room temperature. This study provides a potential strategy for diagnosing different stages of diabetes in the human body.

1 Introduction

With the development of modern urbanization, humans are struggling with numerous health and environmental problems. Owing to these issues, the lifespan and health condition of human beings have been gradually declining in recent years.1-4 To improve the lifespan and health conditions of human beings, an advanced device that can monitor their health conditions regularly in a real-time environment is required. Exhaled breath (EB) and skin gas analyses are effective approaches that can alter traditional medical diagnostic methods and revolutionize medical devices by providing timely reports and portable functions.5-7 Moreover, compared to traditional healthcare services, skin gas analysis is cheap, noninvasive, and can diagnose diseases in their early stages. Thus, the skin gas technique is promising and effective for the detection and diagnosis of various diseases by detecting biomarkers on the human skin. The skin gas analysis technique is considerably easier and more effective than the EB method for collecting skin gas molecules without any burden on patients. Diabetes is the primary cause of cardiovascular

diseases and diabetic retinopathy. Recently, the number of

Surface acoustic waves (SAWs) have received considerable attention in the field of gas sensing owing to their superior thermal stability, lower phase noise compared to crystal resonators, high quality, and superior temperature characteristics. ^{21–24} The SAW resonator works on the surface, making it highly sensitive to external changes in the environment, such as temperature, gases, and humidity. Therefore, any disturbance or change on the surface of the sensing layer (e.g., mass loading, electrical loading, and elastic loading) has

people affected by diabetes has surged by approximately 500 million, making it a major global disease. The concentration of acetone emitted from the skin of diabetic patients exceeds approximately 77-97 parts per billion (ppb), which is quite low compared to exhaled breath (0.3-0.9 ppm).8-10 Therefore, realtime monitoring of the acetone concentration in human skin can be used as an effective diagnostic criterion for the detection of diabetes in its early stages. Hence, an efficient and meticulous design of an acetone gas sensor is required to detect parts per billion to parts per trillion (ppb-ppt) of gas molecules in the skin and exhaled breath. To identify biomarkers in human breath and skin, different types of gas sensors have been utilized, such as electrical resistance change semiconductors or metal oxides and electrochemical, optical, capacitance, calorimetric, and surface acoustic wave gas sensors. 11-20 However, they are insufficient for detecting low concentrations of skin gas molecules.

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a significant effect on the propagation of acoustic waves, resulting in changes in frequency, phase, and amplitude.25 However, the SAW sensor exhibited lower sensitivity and selectivity towards low-concentration gas molecules. Therefore, researchers have explored different technologies, such as lamp mode, Rayleigh mode, and Love mode SAW sensors, to improve the detection limit.26-29 Among the above-mentioned techniques, the Love-wave-mode SAW sensor is one of the preferred SAW gas sensors because of the effective guidance of the waves close to the sensor surface. When the Love wave propagates along the surface of the guide layer, the lower velocity guide layer produces an impedance mismatch at the boundary, which helps limit the Love wave energy to the surface rather than penetrating the main body of the material, resulting in a lower insertion loss than body wave propagation. Certain conditions are required to generate the Love-wave mode in the SAW sensor. In the Love wave mode, the shear velocity in the guiding layer should be smaller than the shear velocity in the substrate. It is important to choose an overlay material which has low shear velocity, low density, and low acoustic absorption. Fused silica (SiO₂) satisfies these conditions for the existence of Love waves with excellent elastic and thermal properties compared to other materials (polymers, ZnO, etc.) besides low acoustic losses, excellent abrasion resistance to water, and chemical degradation.30 Hence, the Love-wave sensor with a SiO2 thin film as the guiding layer will achieve high sensitivity and low noise in chemical gas sensing.31-35

In this study, monolayer chemical vapor deposition (CVD) graphene Love-wave SAW sensors were fabricated for effective real-time detection of ppt-level acetone gas molecules. The ${\rm SiO_2}$ guiding layer deposited on the surface of the black ${\rm 36^{\circ}YX-LiTaO_3}$ (B-LT) substrate effectively decreased the insertion losses and noise levels in the device. It is worth mentioning that a CVD graphene sensor with a 3 μ m ${\rm SiO_2}$ guiding layer exhibited an excellent gas response as low as 800 ppt, which can detect skin gas molecules and meet the needs of diabetes monitoring in medical diagnosis applications. The enhanced gas response mechanism is briefly explained based on the roughness of the ${\rm SiO_2}$ film and the adsorption orientation.

2 Experimental

2.1 Device fabrication

An 80 nm (Cr/Au) thick interdigital transducer (IDT) pattern was fabricated using photolithography, followed by lift-off. We designed different distances (30, 60, and 90) between the IDT electrode and 30 pairs of reflective grids behind the IDT to improve the stability of the SAW device, as listed in Table 1. The design with a 32 μm period distance and 60 pairs of reflective

Table 1 Structural parameters of the G-SAW device

SAW wavelength λ	32 μm
Acoustic aperture	4 mm
IDT's finger pair number	30, 60, 90
Reflector's electrode number	30
IDT thickness (Cr/Au)	80 nm

grids demonstrated better stability than the other designs. The central sensing area was designed to be 4 \times 4 mm which functioned as the gas-adsorption area.

2.2 Deposition of the SiO₂ layer

 SiO_2 layers with different thicknesses (1, 2, 3, and 4 μ m) were deposited using magnetron sputtering technology. Before deposition of the SiO_2 layer, the B-LT substrate was cleaned using a standard chemical process. The substrate was precisely placed above the target with a 50 mm distance between them. An RF power of approximately 80 W was used to deposit the SiO_2 layer in an Ar atmosphere (20 sccm).

2.3 Graphene transfer process

Commercially available CVD graphene is utilized as a sensing layer to fabricate G-SAW sensor devices. Polymethylmethacrylate (PMMA) was spin-coated on a copper/graphene substrate and heated at 150 °C for 2 min. Furthermore, the copper foil was etched with oxygen plasma and 0.1 M of ammonium persulfate solution. The graphene was transferred to the ${\rm SiO}_2$ thin film/B-LT substrate as depicted in Fig. 1. The substrate was immersed in the acetone at 60 °C to remove the PMMA on the surface of the graphene.

2.4 Gas sensing measurement

We designed a printed circuit board (PCB) and 3D-printed gas chamber for gas-sensing measurements (Fig. 1). The response of the SAW sensor is defined as $\Delta f = f_{\rm s} - f_{\rm o}$, where $f_{\rm s}$ is the oscillation frequency of the sensor when exposed to the test gas and $f_{\rm o}$ is the center frequency of the sensor in the ambient environment, respectively. The oscillation frequency of the SAW sensor was recorded using a network analyzer (PNA-N5222B). The standard gas was diluted with N₂ and the measurements were performed in an air atmosphere. The SAW waveform characteristics of the graphene were measured before and after the introduction of the target gas molecules. N₂ gas molecules were purged into the chamber to recover the device to its original stage.

3 Results and discussion

The surface morphology was investigated using atomic force microscopy (AFM) to determine the surface roughness of the sputtered SiO₂ thin films. Fig. 2(a–d) illustrate the 2D AFM images of deposited (1, 2, 3, and 4 μ m) SiO₂ guiding layers on the surface of the substrate, respectively. The AFM image indicates that the roughness of the film increased as the thickness of SiO₂ increased. In addition, a considerable number of SiO₂ nanoparticles were uniformly distributed on the surface, and the diameter of the nanoparticles increased with the SiO₂ thickness. The uniformity of the prepared SiO₂ films is illustrated in Fig. S1a,† the root mean square (RMS) roughness increased as the thickness of SiO₂ increased from 3.9 to 5.5 nm. Fig. S1b† shows that the grain size decreased as the temperature increased. These results indicate that a uniform film was grown at higher temperatures. Fig. S2† shows an AFM image of a 3 μ m

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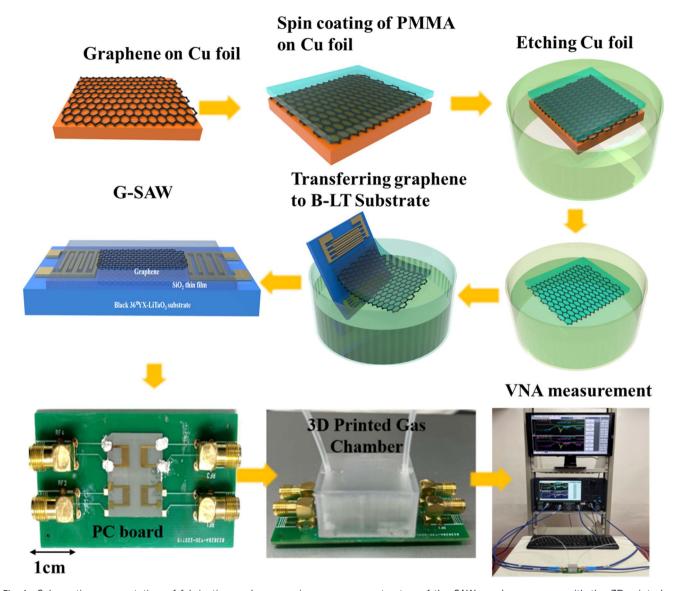


Fig. 1 Schematic representation of fabrication and gas sensing measurement setup of the SAW graphene sensor with the 3D printed gas chamber.

SiO₂ film deposited at different temperatures. The results indicated that temperature played a vital role in the formation of a uniform film and reduced the roughness of the film. The surface morphology of the sputtered SiO₂ thin film was further analyzed using scanning electron microscopy (SEM), as shown in Fig. 2(e and f). The results indicated that the SiO₂ thin film was uniformly deposited on the surface of the substrate and between the gaps of the IDT. The IDT pattern is completely covered with a SiO₂ layer (3 µm) compared to 2 µm which can enhance and guide the Love mode surface acoustic wave to travel within the guiding layer. Fig. 3(a) shows an optical image of the graphene transferred onto the SiO₂/B-LT substrate. The image shows that the graphene was successfully transferred without any cracks or voids. Raman analysis is an efficient technique for analyzing the optical properties, lattice structure, phonon modes, and electronic properties of a material. The Raman spectrum of the G-SAW device shows major peaks which

correspond to the G band (1587 cm⁻¹) and 2D band (2687 cm⁻¹). The G band is attributed to the sp²-bonded carbon atoms in the graphite ring and the 2D band corresponds to the double-resonant Raman scattering of the two phonon emissions, respectively, and the intensity ratio $2D/G \approx 2$, indicating that the CVD graphene is a monolayer (Fig. 3(b)). In addition, the additional peaks, aside from the main peak, were substrate peaks attributed to B-LT. Initially, drain current (I_d) and drain voltage (V_d) measurements were performed on the fabricated G-SAW device using a semiconductor analyzer. The device exhibited ohmic conductance, as shown in Fig. 3(c).

The effect of SiO₂ thickness of a guiding layer was analyzed using a vector network analyzer (VNA), as shown in Fig. 4(a-d). The results indicate that the noise of the SAW waveform is significantly reduced, with the center frequency (130 MHz to 129 MHz) and insertion loss (-15.7 dB to -12.4 dB) as depicted in Fig. 4(a) and S3.† This indicates that the acoustic energy can

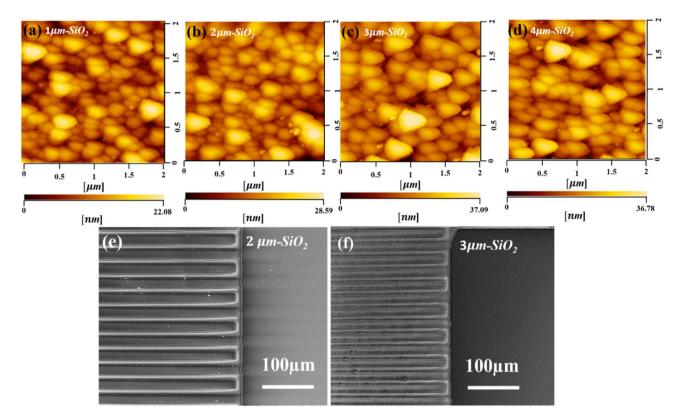


Fig. 2 (a-d) AFM and (e and f) SEM analysis of the SiO₂ layer on a black-36°YX LiTaO₃ substrate with different thicknesses respectively.

be easily captured on the surface by the guiding layer. In addition, the SiO_2 guide layer with 3 $\mu\mathrm{m}$ shows further reduction in the noise level due to the acoustic energy aggregation, resulting in an increased insertion loss of -9.6 dB compared to other thicknesses. The reduction in insertion loss and noise may be due to the effective guidance of acoustic energy and the enhanced electromechanical coupling of elastic waves by the IDTs in the superposition. Strong electromechanical coupling can be achieved when the maximum acoustic energy is between the substrate and layer interface. In addition, the surface acoustic wave tends to propagate more in the waveguide layer; therefore, the acoustic energy is more concentrated in the

waveguide layer and is less likely to leak into the substrate, which enhances the performance of the fabricated SAW sensor with high insertion loss. ³⁰ As shown in Fig. 4(b), a further increase in the thickness resulted in a decrease in the insertion loss, possibly due to the lower coupling effect. Fig. 4(c) shows the Love-wave propagation velocity as a function of the deposited thickness of the SiO₂ guiding layer. The velocity decreases with an increase in the thickness of the SiO₂ guiding layer since the shear wave velocity of the B-LT substrate has a higher shear velocity (4202 ms⁻¹) than the SiO₂ guiding layer (2850 ms⁻¹) which reduces the acoustic attenuation and increases mass sensitivity in the Love wave mode SAW sensor. ^{32,37} Fig. 4(d)

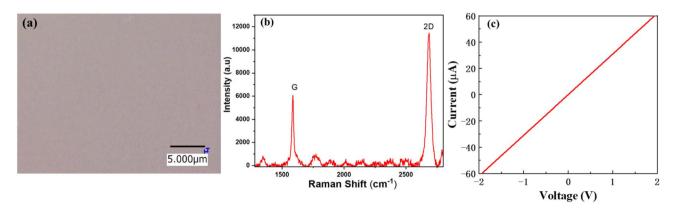


Fig. 3 (a) Optical image of transferred CVD graphene on the $SiO_2/black-36^\circ YX$ LiTaO₃ substrate. (b) Raman spectrum of the CVD G-SAW sensor. (c) I-V characteristics of the fabricated G-SAW sensor.

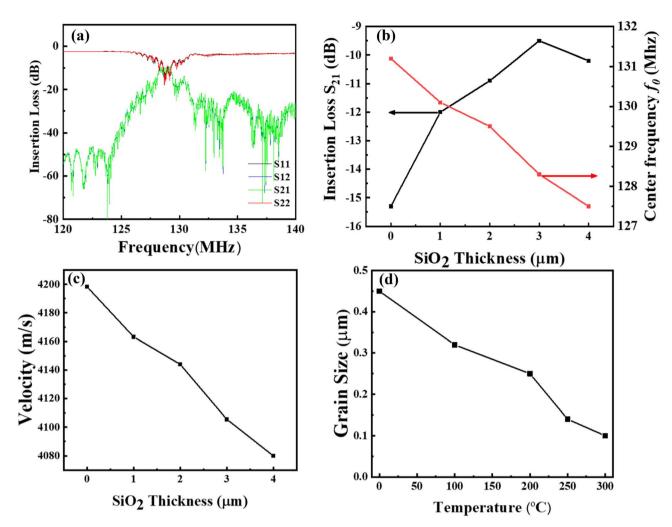


Fig. 4 (a) Surface acoustic wave spectra of 3 μm deposited SiO₂, (b) loss reduction and center frequency shift of different thicknesses of the deposited SiO₂ layer, (c) Love wave propagation velocity vs. thickness of the SiO₂ layer, (d). The temperature dependence of grain size corresponds to 3 µm SiO₂.

shows the grain size of the deposited SiO2 guiding layer deposited at different temperatures. The grain size of the film quickly decreased with increasing temperature, indicating the formation of a uniform film.

Investigation of the gas sensor

Fig. 5(a-c) illustrate the center frequency response plots of the G-SAW sensor towards acetone, ethanol, and ammonia gas molecules, respectively, at room temperature and relative humidity (10-95%). The peak corresponds to the center frequencies f_0 and f_s of the waveform under an ambient atmosphere and gas molecules. As evident from the sensing results, the positive frequency shift of Δf gradually increases as the concentrations of gas molecules increase. Fig. S4† shows the dynamic frequency response curves of the G-SAW sensor towards acetone, ethanol, and ammonia gas molecules at different concentrations, which exhibited a linear relationship when the concentrations varied between 800 and 100 ppm, respectively. However, the G-SAW sensor showed a higher sensitivity towards acetone gas molecules than to other gas

molecules (Fig. 5(d)). Fig. 5(e) shows the SAW devices without a CVD graphene sensing layer toward acetone molecules. The results revealed no shift in frequency even towards higher concentrations of acetone gas molecules. This demonstrates the role of graphene in sensing gas molecules in our experiments. Fig. S4† shows the effect of the temperature of the gas sensor toward acetone and ammonia gas molecules. The results reveal that the gas response of acetone gas increases monotonically up to 60 °C and decreases slightly above that temperature. However, ammonia exhibited a lower response than acetone gas molecules. Fig. S5† shows the response to acetone gas (100 ppm) under different humidity and temperature conditions. As humidity increases, water molecules are physisorbed on the surface of graphene, leading to a slight decrease in sensitivity. When the relative humidity was further increased, the multilayer water molecules were adsorbed. This results in a mass effect in the graphene SAW sensor. Fig. 5(f) shows the response and recovery curves of the acetone gas molecules at room temperature. The results indicated that acetone gas exhibited a quick response and recovery at very low concentrations. The

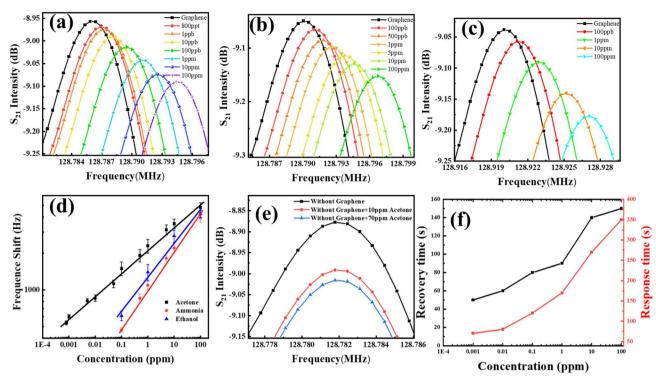


Fig. 5 Gas sensing analysis of the G-SAW sensor: (a) acetone, (b) ammonia, (c) ethanol. (d) Comparative study of frequency shifts toward different concentrations of acetone, ammonia, and ethanol gas molecules. (e) Acetone gas sensing analysis without CVD graphene. (f) Recovery time of the G-SAW sensor in response to acetone, ethanol, and ammonia gas molecules.

acetone gas molecules take a long time to recover, which may be due to the stronger van der Waals (vdW) interactions between the graphene and acetone gas molecules. The observed sensitivity was significant compared to that of other recent SAW gas sensors (see Table 2).

4 Discussion of the sensing mechanism

In this study, the G-SAW device showed a slight shift in the center frequency when exposed to gas molecules. This shift in the center frequency can be attributed to various phenomena, such as the elasticity effect, mass effect, and acoustoelectric effect, as shown in eqn (1) ^{45,46}

$$\frac{\Delta f}{f_0} = C_e h f_0 \Delta \left(\left(\frac{4u}{v_0^2} \right) E \times \frac{4u - 5}{5v^2 u + 2\lambda} \right) + C_m f_0^2 \Delta \rho$$

$$- \frac{k^2}{2} \Delta \left(\frac{1}{1 + \frac{v_0}{\sigma_e}} \right)^2 \tag{1}$$

 f_0 : fundamental frequency of the SAW sensor, ρ : the mass surface density of the sensitive coating (mass per unit area), k^2 (9%): the electromechanical coupling coefficient, v_0 (4200 ms⁻¹): the undisturbed SAW velocity, σ_s : the sheet conductivity of the sensitive layer, E: Young's modulus of the materials, v: Poisson's ratio of the materials, u: the shear modulus of elasticity, C_e : the coefficients of elasticity, C_m : the coefficients of elasticity, C_s (4 pF cm⁻¹): the capacitance per unit length of the piezoelectric substrate.

Table 2 Comparison of acetone gas sensing: prior SAW sensors reported vs. current work^a

Туре	Sensing film	Temperature (°C)	Target gas	Concentration	Ref.
SAW	Рру	RT	Acetone	5.5 ppm	38
SAW	Cu/SWCNTs	RT	Acetone	100 ppm	39
CR	NiO/ZnO	RT	Acetone	0.8 ppm	40
CR	ZnO/S, N: GQDs/PANI	RT	Acetone	5.5 ppm	41
CR	W ₁₈ O ₄₉ /Ti ₃ C ₂ Tx Mxene	RT	Acetone	0.17 ppm	42
SAW	QDs/Ppy	RT	Acetone	0.5 ppm	43
QCM	PDA-GO	RT	Acetone	400 ppm	44
SAW	Suspended graphene	RT	Acetone	0.008 ppm	This worl

^a CR - Chemo-resistive, RT - room temperature.

In our study, the shift in the center frequency (Δf) may be related to the mass loading, elastic properties, or acousticelectric interaction effects of the adsorbed gas molecules on the graphene surface. The acoustic effect is related to the changes in the electrical conductivity and capacitance of the sensing layer. Hence, the acoustic-electric interaction of the fabricated graphene sensor was exposed to acetone gas molecules at room temperature. The change in the resistance was monitored separately using gold electrodes with and without gas molecules. The initial resistance of the graphene sensor was found to be approximately 31.11 k Ω and the resistance slightly increased when exposed to acetone gas molecules (Fig. 6(a)). The calcu-

lated value indicated that the factor $\left(\frac{v_0 C_s}{\sigma_s}\right)^2 \gg 1$, which shows

that the contribution of the acoustic interaction is negligible for the graphene/SiO₂/B-LT sensor device. In addition, the current vs. voltage measurements were augmented by the aforementioned results, as depicted in Fig. 6(a). Hence, the contribution of the gas response may be attributed to other effects. The massloading effect causes a shift in the center frequency towards the negative side, and the elastic effect causes a positive shift in the center frequency. In this study, the resonant frequency of the G-SAW sensor showed a positive shift in the center frequency with an increase in the concentration of acetone gas molecules. Therefore, an elastic effect occurred due to the adsorption of acetone gas molecules onto the surface of the graphene layer.

Fig. 7 indicates that the gas sensitivity of the G-SAW sensor is highly dependent on the surface roughness of the deposited SiO₂ thin film. As shown in the schematic image, graphene is suspended between the nanoparticles of the SiO₂ guiding layer. In the case of suspended graphene, the van der Waals interactions between graphene and the surface atoms of the substrate are removed, leading to enhanced electronic, mechanical, and chemical properties compared to those of non-suspended graphene. In addition, the suspended graphene exhibits fewer

wrinkles and crystal defects, thus enhancing the elastic properties and sensitivity of the G-SAW sensor. It has been reported that electron mobility can be increased up to 200 000 cm² V⁻¹ s⁻¹ and the single molecule can be detected.⁴⁷ When gas molecules are introduced, the graphene membrane undergoes deflection that is approximately two orders of magnitude larger than that of a thin film with lower roughness. The molecules tended to move into a high-propagation area on the graphene surface and lose their kinetic energy. Consequently, molecules can be easily captured by graphene via van der Waals (vdW) interactions. In general, gas molecules can easily escape and desorb from the interaction surfaces of graphene. In contrast, when an SAW Love wave is applied, the adsorbed gas molecules can continuously interact with the graphene surface owing to the reduced kinetic energy. The acetone gas molecule showed higher sensitivity than the other gas molecules because of its molecular size and higher strain on the surface of the graphene. It is also evident that a decrease in the roughness of the film leads to a low gas response, as depicted in Fig. 7(b). The charge distribution of acetone molecules can be distorted from their normal shape by propagation on the graphene surface. In addition, the G-SAW sensor showed higher sensitivity towards acetone gas molecules with higher dipole moments (2.88 D), as shown in Table 3. Acetone gas molecules are preferentially adsorbed on CVD monolayer graphene, with O atoms above the hollow site of the C ring. Acetone adsorbed on graphene with a small binding energy enhances the mobility of graphene at room temperature. This resulted in stronger van der Waals interactions with the graphene surface, leading to increased hardness and compressive stress. Furthermore, the high dipole moment of acetone induces stronger electrostatic interactions with graphene, leading to deformation and surface hardness. These results indicate that the elastic effect plays a major role in the high sensitivity toward acetone gas molecules.

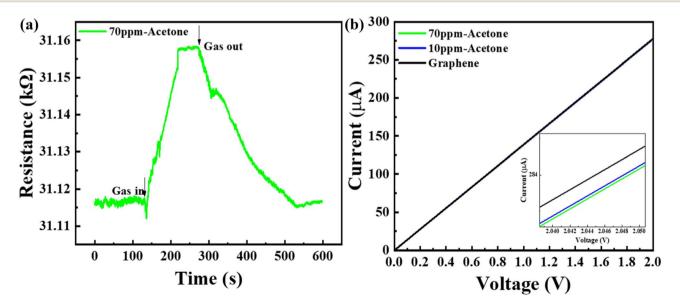


Fig. 6 (a) Electrical resistance of the graphene film when exposed to 70 ppm acetone gas, (b) I-V curve of the graphene film when exposed to 70 ppm and 10 ppm acetone gas

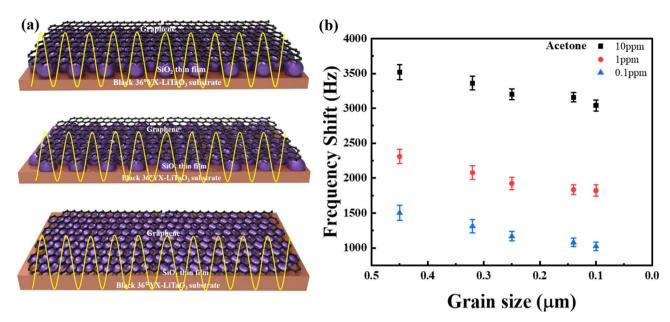


Fig. 7 (a) Schematic representation of the G-SAW sensor device with different particle sizes. (b) Effect of sensing response with respect to the grain size of SiO₂.

Table 3 Basic data table of gas molecules⁴⁸

Analytes	Molecular size (Å)	Molecular weight (g mol ⁻¹)	Dipole moment (D)
Acetone (C ₃ H ₆ O)	4.6	58.8	2.88
Ethanol (C ₂ H ₆ O)	4.3	46.07	1.6
Ammonia (NH ₃)	2.3	17.03	1.48

5 Conclusion

In this study, a Love-wave-based G-SAW gas sensor was fabricated, and its gas-sensing response towards ammonia and acetone was studied at room temperature. The SiO₂ guidance plays a major role in noise reduction and insertion loss. The G-SAW showed remarkable sensitivity toward acetone gas molecules at low concentrations (800 ppt) at room temperature. The acetone gas-sensing mechanism of the G-SAW sensor was based on the graphene partially suspended between the nanoparticles and the dipole interactions between the graphene and gas molecules. The G-SAW sensor exhibited a rapid positive shift in the center frequency, which indicated a change in the Young's modulus when the gas molecules were adsorbed onto the graphene surface. Resistance measurements confirmed the elastic effect of the G-SAW gas sensor.

Conflicts of interest

The authors declare that they have no known competing financial interests or personal relationships that could have appeared to influence the work reported in this study.

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References

- 1 R. A. Potyrailo, Multivariable Sensors for Ubiquitous Monitoring of Gases in the Era of Internet of Things and Industrial Internet, *Chem. Rev.*, 2016, **116**, 11877–11923, DOI: **10.1021/ACS.CHEMREV.6B00187**.
- 2 C. Cai, J. Mo, Y. Lu, N. Zhang, Z. Wu, S. Wang and S. Nie, Integration of a porous wood-based triboelectric nanogenerator and gas sensor for real-time wireless foodquality assessment, *Nano Energy*, 2021, 83, 105833, DOI: 10.1016/J.NANOEN.2021.105833.
- 3 Z. Lou, L. Wang, K. Jiang, Z. Wei and G. Shen, Reviews of wearable healthcare systems: Materials, devices and system integration, *Mater. Sci. Eng. R Rep.*, 2020, **140**, 100523, DOI: **10.1016/J.MSER.2019.100523**.
- 4 A. W. Boots, J. J. B. N. Van Berkel, J. W. Dallinga, A. Smolinska, E. F. Wouters and F. J. Van Schooten, The versatile use of exhaled volatile organic compounds in human health and disease, *J. Breath Res.*, 2012, **6**, 027108, DOI: 10.1088/1752-7155/6/2/027108.
- 5 M. Kampa and E. Castanas, Human health effects of air pollution, *Environ. Pollut.*, 2008, **151**, 362–367, DOI: **10.1016/J.ENVPOL.2007.06.012**.
- 6 A. Bajtarevic, C. Ager, M. Pienz, M. Klieber, K. Schwarz, M. Ligor, T. Ligor, W. Filipiak, H. Denz, M. Fiegl, W. Hilbe, W. Weiss, P. Lukas, H. Jamnig, M. Hackl, A. Haidenberger, B. Buszewski, W. Miekisch, J. Schubert and A. Amann, Noninvasive detection of lung cancer by analysis of exhaled breath, *BMC Cancer*, 2009, 9, 348, DOI: 10.1186/1471-2407-9-348.

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7 J. Hunt, Exhaled Breath Condensate: An Overview, *Immunol. Allergy Clin. North Am.*, 2007, 27, 587–596, DOI: 10.1016/ J.IAC.2007.09.001.

- 8 S. Zhang, W. Jiang, Y. Li, X. Yang, P. Sun, F. Liu, X. Yan, Y. Gao, X. Liang, J. Ma and G. Lu, Highly-sensitivity acetone sensors based on spinel-type oxide (NiFe2O4) through optimization of porous structure, *Sens. Actuators*, *B*, 2019, 291, 266–274, DOI: 10.1016/J.SNB.2019.04.090.
- 9 A. M. Diskin, P. Španěl and D. Smith, Time variation of ammonia, acetone, isoprene and ethanol in breath: a quantitative SIFT-MS study over 30 days, *Physiol. Meas.*, 2003, 24, 107, DOI: 10.1088/0967-3334/24/1/308.
- 10 A. A. Baharuddin, B. C. Ang, A. S. M. A. Haseeb, Y. C. Wong and Y. H. Wong, Advances in chemiresistive sensors for acetone gas detection, *Mater. Sci. Semicond. Process.*, 2019, 103, 104616, DOI: 10.1016/J.MSSP.2019.104616.
- 11 R. Sankar Ganesh, M. Navaneethan, V. L. Patil, S. Ponnusamy, C. Muthamizhchelvan, S. Kawasaki, P. S. Patil and Y. Hayakawa, Sensitivity enhancement of ammonia gas sensor based on Ag/ZnO flower and nanoellipsoids at low temperature, *Sens. Actuators, B*, 2018, 255, 672–683, DOI: 10.1016/J.SNB.2017.08.015.
- 12 P. Kirchner, J. Oberländer, P. Friedrich, J. Berger, G. Rysstad, M. Keusgen and M. J. Schöning, Realisation of a calorimetric gas sensor on polyimide foil for applications in aseptic food industry, *Sens. Actuators*, *B*, 2012, 170, 60–66, DOI: 10.1016/J.SNB.2011.01.032.
- 13 M. R. R. Khan, S. Oh, G. Choi and H. S. Lee, Highly sensitive, fast and wide dynamic range lactate sensor containing solvatochromic sensing membrane by combining the capacitance-to-phase conversion technique, *Sens. Actuators*, *B*, 2020, **309**, 127783, DOI: **10.1016/J.SNB.2020.127783**.
- 14 Y. Tan, T. Huang, L.-P. Sun, S. Jiang, Y. Liu, B.-O. Guan and W. Jin, Dispersion turning point-enhanced photothermal interferometry gas sensor with an optical microfiber interferometer, *Sens. Actuators*, *B*, 2023, 133690, DOI: 10.1016/J.SNB.2023.133690.
- 15 J. Zhao, Y. Pan, P. Lu, X. Zhang, T. Li, J. Zhang, C. Sima and D. Liu, Ppb-level all-optical off-axis QEPAS gas sensor based on dual-wavelength demodulation of out-of-plane vibration mode, *Sens. Actuators*, B, 2023, 133689, DOI: 10.1016/ J.SNB.2023.133689.
- 16 B. Kwon, H. Bae, H. Lee, S. Kim, J. Hwang, H. Lim, J. H. Lee, K. Cho, J. Ye, S. Lee and W. H. Lee, Ultrasensitive N-Channel Graphene Gas Sensors by Nondestructive Molecular Doping, ACS Nano, 2022, 16(2), 2176–2187, DOI: 10.1021/acsnano.1c08186.
- 17 N. Sui, P. Zhang, T. Zhou and T. Zhang, Selective ppb-level ozone gas sensor based on hierarchical branch-like In2O3 nanostructure, *Sens. Actuators, B*, 2021, **336**, 129612, DOI: **10.1016/J.SNB.2021.129612**.
- 18 D. Zhang, Z. Yang, Z. Wu and G. Dong, Metal-organic frameworks-derived hollow zinc oxide/cobalt oxide nanoheterostructure for highly sensitive acetone sensing, *Sens. Actuators*, *B*, 2019, **283**, 42–51, DOI: **10.1016**/ **J.SNB.2018.11.133**.

- 19 D. Zhang, Z. Xu, Z. Yang and X. Song, High-performance flexible self-powered tin disulfide nanoflowers/reduced graphene oxide nanohybrid-based humidity sensor driven by triboelectric nanogenerator, *Nano Energy*, 2020, 67, 104251, DOI: 10.1016/J.NANOEN.2019.104251.
- 20 D. Zhang, M. Wang and Z. Yang, Facile fabrication of graphene oxide/Nafion/indium oxide for humidity sensing with highly sensitive capacitance response, *Sens. Actuators, B*, 2019, 292, 187–195, DOI: 10.1016/J.SNB.2019.04.133.
- 21 Z. Oumekloul, S. Pecqueur, A. de Maistre, P. Pernod, K. Lmimouni, A. Talbi and B. Hafsi, A New Approach to Improve the Control of the Sensitive Layer of Surface Acoustic Wave Gas Sensors Using the Electropolymerization, 2022, pp. 1-4, DOI: 10.1109/DTIP56576.2022.9911737.
- 22 Y. Pan, M. Qin, P. Wang, L. Yang, L. Zhang, C. Yan, C. Zhang and W. Wang, Interface and Sensitive Characteristics of the Viscoelastic Film Used in a Surface Acoustic Wave Gas Sensor, ACS Sens., 2022, 7(2), 612–621, DOI: 10.1021/acssensors.1c02509.
- 23 M. Asad and M. H. Sheikhi, Surface acoustic wave based H2S gas sensors incorporating sensitive layers of single wall carbon nanotubes decorated with Cu nanoparticles, *Sens. Actuators, B*, 2014, **198**, 134–141, DOI: **10.1016/J.SNB.2014.03.024**.
- 24 W. Luo, Q. Fu, D. Zhou, J. Deng, H. Liu and G. Yan, A surface acoustic wave H2S gas sensor employing nanocrystalline SnO2 thin film, *Sens. Actuators, B*, 2013, **176**, 746–752, DOI: **10.1016/J.SNB.2012.10.086**.
- 25 Y. Tang, D. Ao, W. Li, X. Zu, S. Li and Y. Q. Fu, NH3 sensing property and mechanisms of quartz surface acoustic wave sensors deposited with SiO2, TiO2, and SiO2-TiO2 composite films, *Sens. Actuators, B*, 2018, 254, 1165–1173, DOI: 10.1016/J.SNB.2017.07.195.
- 26 P. Patial and M. Deshwal, Systematic Review on Design and Development of Efficient Semiconductor Based Surface Acoustic Wave Gas Sensor, *Trans. Electr. Electron. Mater.*, 2021, 22, 385–393, DOI: 10.1007/S42341-021-00332-1.
- 27 L. Zhou, Z. Hu, P. Wang, N. Gao, B. Zhai, M. Ouyang, G. Zhang, B. Chen, J. Luo, S. Jiang, H. Y. Li and H. Liu, Enhanced NO2 sensitivity of SnO2 SAW gas sensors by facet engineering, *Sens. Actuators, B*, 2022, **361**, 131735, DOI: 10.1016/J.SNB.2022.131735.
- 28 W. Wang, X. Liu, S. Mei, Y. Jia, M. Liu, X. Xue and D. Yang, Development of a Pd/Cu nanowires coated SAW hydrogen gas sensor with fast response and recovery, *Sens. Actuators*, *B*, 2019, 287, 157–164, DOI: 10.1016/J.SNB.2019.02.047.
- 29 M. Šetka, F. A. Bahos, D. Matatagui, M. Potoček, Z. Kral, J. Drbohlavová, I. Gràcia and S. Vallejos, Love wave sensors based on gold nanoparticle-modified polypyrrole and their properties to ammonia and ethylene, *Sens. Actuators, B*, 2020, 304, 127337, DOI: 10.1016/J.SNB.2019.127337.
- 30 J. Du, G. L. Harding, J. A. Ogilvy, P. R. Dcnchcr and M. Lake, A study of Love-wave acoustic sensors, *Sens. Actuators, A*, 1996, 56, 21–219.
- 31 M. Šetka, F. A. Bahos, O. Chmela, D. Matatagui, I. Gràcia, J. Drbohlavová and S. Vallejos, Cadmium telluride/ polypyrrole nanocomposite based Love wave sensors highly

- sensitive to acetone at room temperature, *Sens. Actuators, B*, 2020, **321**, 128573, DOI: 10.1016/J.SNB.2020.128573.
- 32 W. Wang, S. Fan, Y. Liang, S. He, Y. Pan, C. Zhang and C. Dong, Enhanced Sensitivity of a Love Wave-Based Methane Gas Sensor Incorporating a Cryptophane-A Thin Film, *Sensors*, 2018, **18**(10), 3247, DOI: **10.3390/s18103247**.
- 33 J. H. Choi, J. Lee, M. Byeon, T. E. Hong, H. Park and C. Y. Lee, Graphene-Based Gas Sensors with High Sensitivity and Minimal Sensor-to-Sensor Variation, ACS Appl. Nano Mater., 2020, 3, 2257–2265, DOI: 10.1021/ACSANM.9B02378.
- 34 S. Li, Y. Wan, Y. Su, C. Fan and V. R. Bhethanabotla, Gold nanoparticle-based low limit of detection Love wave biosensor for carcinoembryonic antigens, *Biosens. Bioelectron.*, 2017, 95, 48–54, DOI: 10.1016/J.BIOS.2017.04.012.
- 35 I. Sayago, D. Matatagui, M. J. Fernández, J. L. Fontecha, I. Jurewicz, R. Garriga and E. Muñoz, Graphene oxide as sensitive layer in Love-wave surface acoustic wave sensors for the detection of chemical warfare agent simulants, *Talanta*, 2016, 148, 393–400, DOI: 10.1016/J.TALANTA.2015.10.069.
- 36 S. Lee, K.-B. Kim and Y.-I. Kim, Love Wave SAW Biosensors for Detection of Antigen-antibody Binding and Comparison with SPR Biosensor, *Food Sci. Biotechnol.*, 2011, **20**, 1413–1418, DOI: **10.1007/s10068-011-0194-3**.
- 37 W. Wang, X. Xie, G. Chen, J. Liu and S. He, Temperature-compensated Love wave based gas sensor on waveguide structure of SiO₂/36° YX LiTaO₃, *Smart Mater. Struct.*, 2015, 24, 065019, DOI: 10.1088/0964-1726/24/6/065019.
- 38 F. Li, H. Li, H. Jiang, K. Zhang, K. Chang, S. Jia, W. Jiang, Y. Shang, W. Lu, S. Deng and M. Chen, Polypyrrole nanoparticles fabricated via Triton X-100 micelles template approach and their acetone gas sensing property, *Appl. Surf. Sci.*, 2013, 280, 212–218, DOI: 10.1016/J.APSUSC.2013.04.132.
- 39 M. Asad and M. H. Sheikhi, Surface acoustic wave based H2S gas sensors incorporating sensitive layers of single wall carbon nanotubes decorated with Cu nanoparticles, *Sens. Actuators*, *B*, 2014, **198**, 134–141, DOI: **10.1016/ J.SNB.2014.03.024**.
- 40 C. Liu, L. Zhao, B. Wang, P. Sun, Q. Wang, Y. Gao, X. Liang, T. Zhang and G. Lu, Acetone gas sensor based on NiO/ZnO hollow spheres: Fast response and recovery, and low (ppb) detection limit, *J. Colloid Interface Sci.*, 2017, 495, 207–215, DOI: 10.1016/J.JCIS.2017.01.106.

- 41 D. Zhang, Z. Wu and X. Zong, Metal-organic frameworks-derived zinc oxide nanopolyhedra/S, N: graphene quantum dots/polyaniline ternary nanohybrid for high-performance acetone sensing, *Sens. Actuators*, *B*, 2019, **288**, 232–242, DOI: **10.1016/J.SNB.2019.02.093**.
- 42 S. Sun, M. Wang, X. Chang, Y. Jiang, D. Zhang, D. Wang, Y. Zhang and Y. Lei, W18O49/Ti3C2Tx Mxene nanocomposites for highly sensitive acetone gas sensor with low detection limit, *Sens. Actuators, B*, 2020, **304**, 127274, DOI: **10.1016/J.SNB.2019.127274**.
- 43 M. Šetka, F. A. Bahos, O. Chmela, D. Matatagui, I. Gràcia, J. Drbohlavová and S. Vallejos, Cadmium telluride/polypyrrole nanocomposite based Love wave sensors highly sensitive to acetone at room temperature, *Sens. Actuators*, *B*, 2020, 321, 128573, DOI: 10.1016/J.SNB.2020.128573.
- 44 D. Zhang, X. Song, Z. Wang and H. Chen, Ultra-highly sensitive humidity sensing by polydopamine/graphene oxide nanostructure on quartz crystal microbalance, *Appl. Surf. Sci.*, 2021, 538, 147816, DOI: 10.1016/J.APSUSC.2020.147816.
- 45 D. S. Ballantine Jr, R. M. White, S. J. Martin, A. J. Ricco, E. T. Zellers, G. C. Frye and H. Wohltjen, *Acoustic Wave Sensors: Theory, Design and Physico-Chemical Applications*, 1997, https://books.google.co.jp/books?hl=zh-CN&lr=&id=SXFmxTOP128C&oi=fnd&pg=PP1&dq=Acoustic+wave+sensors:+theory,+design+and+physico-chemical+applic ations&ots=K89Rfh7JmE&sig=YaI95Xsm
 WLJ9Mdgxf2OIWkEBMqw&redir_esc=y#v=onepage&q=Acousticwavesensors%
 3Atheory%2Cdesignandphysico-chemicalapplications&f=false (accessed March 27, 2023).
- 46 W. P. Jakubik, Surface acoustic wave-based gas sensors, *Thin Solid Films*, 2011, **520**, 986–993, DOI: **10.1016**/J.TSF.2011.04.174.
- 47 R. K. Gupta, F. H. Alqahtani, O. M. Dawood, M. Carini, A. Criado, M. Prato, S. K. Garlapati, G. Jones, J. Sexton, K. C. Persaud, C. Dang, U. Monteverde, M. Missous, R. J. Young, S. Boult, N. Dixon, L. Majewski and M. A. Migliorato, Suspended graphene arrays for gas sensing applications, 2D Mater., 2020, 8, 025006, DOI: 10.1088/2053-1583/abcf11.
- 48 J. Park and H. Tabata, Gas Sensor Array Using a Hybrid Structure Based on Zeolite and Oxide Semiconductors for Multiple Bio-Gas Detection, *ACS Omega*, 2021, **6**, 21284–21293, DOI: 10.1021/ACSOMEGA.1C01435.