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# Electrochemical biosensor based on cellulose nanofibers/graphene oxide and acetylcholinesterase for the detection of chlorpyrifos pesticide in water and fruit juice†

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In this work, cellulose nanofibers and graphene oxide are used to fabricate a simple and reliable electrochemical biosensor, based on acetylcholinesterase (AChE) for the detection of highly dangerous organophosphates (OPs), utilizing chlorpyrifos as a representative sample. AChE is an enzyme that is essential for neurotransmission and catalyzes the conversion of acetylcholine (ATCh) into thiocholine and acetic acid. The pesticide used in this work, chlorpyrifos, inhibits the catalytic activity of AChE on ATCh, and this inhibition can be measured using square wave voltammetry (SWV). Utilizing a process of surface modification, layers of cellulose nanofibers, graphene oxide, a chitosan-graphene oxide composite, and acetylcholinesterase (AChE/CS-GO/GO/CNFs) were immobilized on a screen-printed carbon electrode (SPCE). The modified SPCE working electrode was characterized using scanning electron microscopy and graphene oxide trapped in the cellulose nanofibers was found to increase the sensitivity of the biosensor. The modified biosensor demonstrated good performance for detection of chlorpyrifos over a linear range of 25–1000 nM under optimum conditions, and the limits of detection and quantification were 2.2 nM and 73 nM, respectively. Our sophisticated technique might offer a more precise, straightforward, quick, and environmentally friendly way to assess chlorpyrifos contamination in water and juice samples.

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## 1. Introduction

To protect crops from insects and pests, organophosphates (OPs), esters of phosphoric acid derivatives, are frequently employed today in agriculture, primarily in developing nations. Due to their effectiveness at killing and controlling insects and other pests, OPs are employed in 30% of global pesticide sales.<sup>1–4</sup> OPs have the advantages of being simple to synthesize, highly soluble in water and easy to biodegrade, as well as effectively killing pests, and thus OPs are increasingly the first option for farmers and agricultural workers.<sup>5</sup> On the other hand, overuse of OPs damages the environment, because of

their relatively harmful effects, and leaves residues and contaminants in water, vegetables and fruits.<sup>6,7</sup>

Chlorpyrifos (*O,O*-diethyl *O*-3,5,6-trichloro-2-pyridyl phosphorothioate) is an organophosphorus pesticide, one of several types of pesticides, that is mostly used in residential applications, such as building maintenance, agriculture, plant and animal production to eliminate pests including insects and worms. It is typically used on crops including almonds, maize, cotton, peaches, and fruit trees, like apple, orange and banana trees, mostly in agricultural countries.<sup>8,9</sup> The widespread, abundant and long-term use of chlorpyrifos causes health problems and neurological illnesses, by blocking the activity of the acetylcholinesterase enzyme, in humans and other living creatures, especially in those with pre-existing medical conditions, infants, children and pregnant women.<sup>10,11</sup> Humans who are exposed to chlorpyrifos may experience acute poisoning, which manifests as nausea, vomiting, increased perspiration, muscle spasms, unconsciousness, convulsions and even death.<sup>12–14</sup> Acetylcholinesterase (AChE) is an essential enzyme involved in the transmission of brain impulses. AChE can also speed up the breakdown of the central neurotransmitter acetylcholine (ATCh) into acetic acid and choline.<sup>15</sup> Pesticides like chlorpyrifos can impair the vital AChE activity that causes

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the disorders and diseases mentioned above. Because of its impact on humans and the environmental harm it causes, the use of chlorpyrifos needs to be restricted.

To identify pesticide contamination in the environment, a number of techniques have been developed, including immunoassays such as ELISA (enzyme-linked immunosorbent assay),<sup>16</sup> FIA (fluorescence immunoassay),<sup>17</sup> chromatographic assays like high-performance liquid chromatography (HPLC),<sup>18</sup> gas chromatography (GC),<sup>19</sup> gas chromatography-mass spectrophotometry (GC-MS),<sup>20</sup> colorimetric and fluorometric biosensors,<sup>21,22</sup> dual-signal sensors with both colorimetric and fluorometric techniques<sup>23,24</sup> and electrochemical biosensors.<sup>25–27</sup> In recent years, biosensors containing AChE as a bio-recognition element,<sup>28</sup> and a signal transducer<sup>29</sup> based on an enzyme inhibition method have become rapid, highly sensitive and specific, time-saving, cost-effective and reliable methods for the detection of OP compounds. In this work, chlorpyrifos was detected based on its inhibition of the catalytic activity of AChE on ATCh, where AChE catalyzes the conversion of ATCh into thiocholine (TCh), as measured using a modified electrochemical biosensor.

Given that the use of nanomaterials in the biosensor fabrication process improves the conductivity, sensitivity, stability and biosensor performance, whilst compensating for the poor conductive activity of AChE, electrochemical biosensors with nanomaterial applications have become increasingly popular.<sup>4,26</sup> AChE immobilization and signal amplification are perpetual issues that necessitate taking the biocompatibility and conductivity of an AChE biosensor into account. In order to improve the performance of biosensors for the detection of OPs, nanomaterials and nano-composites, such as 3D graphene,<sup>30</sup> multi-walled carbon nanotubes (MWCNTs),<sup>31</sup> NiO nanoparticles,<sup>32</sup> CuO nanowires,<sup>33</sup> gold-platinum (Au-Pt) bimetallic nanoparticles<sup>34</sup> and CdS quantum dots,<sup>35</sup> have been frequently used.

“Nanocellulose” refers to tiny fibers with nanoscale dimensions that are produced from cellulose using a variety of processes, the most popular of which is alkali or acid hydrolysis.<sup>36</sup> Nanocellulose has emerged as a valuable green material for a wide range of applications, from reinforcement materials to sensing platforms that are particularly important for the food, pharmaceutical and environmental protection industries.<sup>37</sup> Additionally, biomass-derived renewable nanocellulose has a low density, an anisotropic structure, good optical properties, superior mechanical properties, and is chemically resistant.<sup>38,39</sup> Cellulose nanomaterials have attracted interest for their applications in everything from paper, textile, packaging, sensors, water purification, drug delivery and biomedical devices, due to their advantageous qualities like low density, high surface area, and good mechanical strength with excellent biocompatibility and renewability.<sup>40–42</sup> Due to the extremely large surface area of cellulosic nanofibers, their adhesion properties are the major element that must be managed for their use in nanocomposite applications.<sup>43</sup> Therefore, we opted to use cellulosic nanofibers as a foundation material in our electrode fabrication system, along with graphene oxide and an electrode modification approach in this work that uses cellulose

nanofibers made by ultrasonication from the biomass “sugarcane bagasse”.<sup>44,45</sup> We have discovered, *via* electrochemical analysis, that the conductivity of graphene oxide is also enhanced and promoted by the cellulose nanofibers synthesized from sugarcane bagasse. The sensing platform of our biosensors was a screen-printed carbon electrode (SPCE) modified using cellulose nanofibers (CNFs), graphene oxide (GO), graphene oxide-chitosan (CS-GO) and acetylcholinesterase (AChE) (AChE/CS-GO/GO/CNFs) composites. We then tested the biosensor as a chlorpyrifos biosensor (Scheme 1). The AChE/CS-GO/GO/CNFs layers demonstrated excellent surface conductivity due to the presence of the GO, which has a large surface area, high electrical conductivity, a high electron transfer rate, and the ability to immobilize various molecules.<sup>46</sup> AChE was loaded deeply into the layers with the aid of a chitosan adhesive agent,<sup>47</sup> enhancing the sensitivity and stability of the modified electrode. Then, in order to confirm the sensitivity and viability of our biosensor for the detection of chlorpyrifos and other metal ions in actual applications, we tested it on commercial drinking water and juice samples.

## 2. Materials and methods

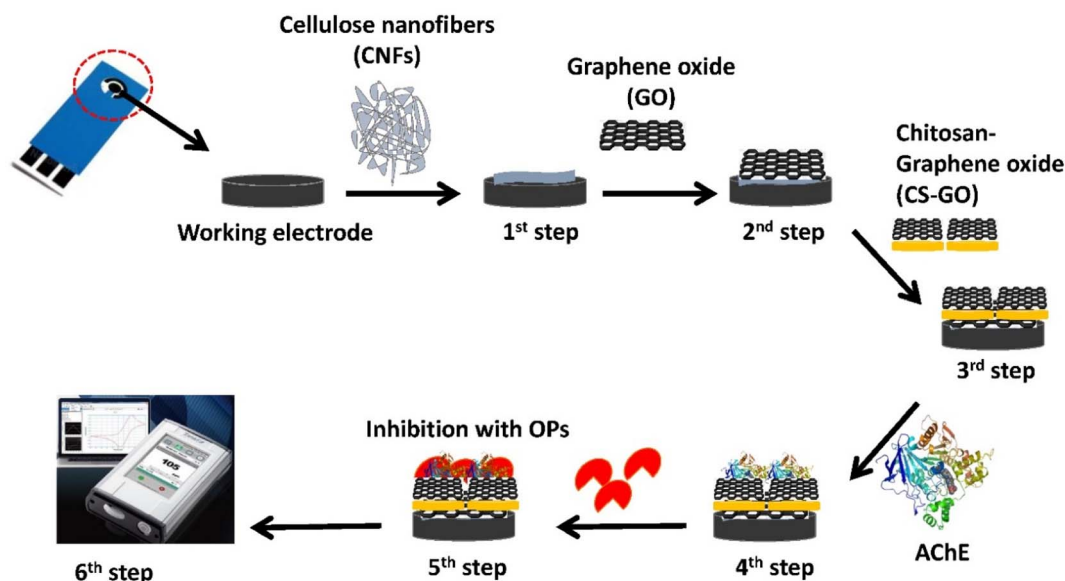
### 2.1 Materials

Acetylcholinesterase (AChE) from electric eels, acetylthiocholine chloride (ATCh), potassium ferricyanide ( $K_3Fe(CN)_6$ , 99%) and chlorpyrifos were purchased from Sigma-Aldrich Co, Ltd, China. Hydrochloric acid (HCl, 37%), sodium chloride (NaCl, 99%), potassium chloride (KCl, <100%), acetone ( $CH_3COOH_3$ ,  $\geq 99.8\%$ ), and ethanol ( $C_2H_5OH$ ,  $\geq 99.7\%$ ) were purchased from RCI Labscan, Thailand. Magnesium nitrate ( $Mg(NO_3)_2$ ,  $\geq 99.4\%$ ) and cobalt(II) nitrate hexahydrate ( $Co(NO_3)_2 \cdot 6H_2O$ ,  $\geq 98\%$ ) were purchased from Univar, Australia. Calcium chloride ( $CaCl_2$ ,  $\geq 95\%$ ) was purchased from Scharlau, Spain. Mercury(II) chloride ( $HgCl_2$ ,  $\geq 99.5\%$ ) was purchased from QRec<sup>TM</sup>, New Zealand. Chitosan ( $[(C_6H_{11}O_4)_n]$ , 100 000–300 000) was purchased from ACROS, China. Phosphate buffer saline (PBS, 1× concentration, osmolarity 280–315 mOsm  $kg^{-1}$ ) was purchased from Cepham Life Science, USA. Hydrogen peroxide ( $H_2O_2$ , 30%, ISO grade) was purchased from Merck Millipore, USA. Deionized water (DI) with specific resistivity of 18.2 MΩ cm was obtained from a RiOs<sup>TM</sup> Type I Simplicity 185 Millipore water purification system. Alkaline hydrogen peroxide (AHP) solution was prepared by adding 1 N NaOH to a 3%  $H_2O_2$  solution, adjusted to a pH of 11.5. Water and juices were bought from a convenience store in Khon Kaen, Thailand. Sugarcane bagasse was bought from a local market in Khon Kaen, Thailand.

### 2.2 Instrumentation and cell setup

The surface morphology of the synthesized cellulose nanofibers was characterized using focused ion beam scanning electron microscopy (FIB-SEM, FEI Helios NanoLab G3 CX, Czech Republic) and field emission scanning electron microscope (FE-SEM, TESCAN, Model: MIRA). Size distribution plot of cellulose nanofibers was done by using Image J and Origin programs.





Scheme 1 Schematic diagram showing the process of modifying a screen-printed carbon electrode (SPCE).

Characterization of each layer of the modified electrodes was performed using scanning electron microscopy (SEM) Brand LEO Model 1450V. The surface functional groups on the CNFs were determined using attenuated total reflection-Fourier transform infrared (ATR-FTIR) spectroscopy (Bruker TENSOR 27 scanning from 4000 to 600  $\text{cm}^{-1}$ ). Square wave voltammetry (SWV) was performed using an electrochemical workstation (ECAS100, Zensor Co., Ltd, Taichung, Taiwan). The biosensors were fabricated on screen-printed carbon electrodes (SPCEs, Zensor Co., Ltd, Taichung, Taiwan) with a three-electrode system: a carbon electrode ( $d = 3.0 \text{ mm}$ /active surface area =  $0.071 \text{ cm}^2$ ) was used as the working electrode, another carbon electrode was used as a counter electrode, and an Ag/AgCl electrode was used as a reference electrode. Solution pH was determined using a HI 5221 pH meter (Hanna Instruments, Thailand). A laboratory centrifuge (Rotina 380 R) was used for the purpose of precipitation of the c-AgNPs solution. The CNF extraction process was achieved using an ultrasound processor (Sonics and Materials Inc., Vibra Cell, VC-750, USA).

### 2.3 Synthesis of the cellulose nanofibers (CNFs) from sugarcane bagasse

Cellulose nanofibers were synthesized from sugarcane bagasse (SCB) *via* the alkaline hydrogen peroxide (AHP) hydrolysis method and extraction of the CNFs was achieved using ultrasonication.<sup>48,49</sup> The raw bagasse from the sugarcane must first be washed and cleaned before being dried completely prior to synthesis of the cellulose nanofibers. Following that, raw bagasse was broken into pieces 2–5 cm in length and pulverized into a fine powder, sieved through a 250  $\mu\text{m}$  diameter mesh, and then stored in a desiccator for further use. Secondly, the alkaline hydrogen peroxide (AHP) hydrolysis was performed to remove hemicellulose and lignin from the SCB. Then the dry powder was mixed constantly in an AHP solution at a temperature of 40  $^{\circ}\text{C}$  for

four hours using a magnetic stirrer. The pH of the solution was periodically adjusted to 11.5 during the AHP hydrolysis. After pulping, 2 N  $\text{H}_2\text{SO}_4$  was added to the mixture to bring the pH level to a neutral range. To get rid of all the soluble elements, the insoluble residue was collected using vacuum filtering and rinsed three times with deionized water. The residual white residue from the cellulose pulp was dried and given the name “cellulose”. Finally, low-frequency (20 kHz) ultrasound was used to ultrasonically irradiate the AHP-hydrolyzed cellulose (0.5% w/v) for 2 hours in a 1%  $\text{H}_2\text{O}_2$  solution on an ice bath support to prevent overheating the samples. A 13 mm diameter cylindrical titanium alloy probe tip was installed in the processor. Other processor requirements included a 750 W output power, a 60% amplitude, and a 10 s on/5 s off cycle. To avoid the agglomeration of fragmented fibers, a few drops of 2 N  $\text{H}_2\text{SO}_4$  were added to the suspension (pH 5.0) after the sonication treatments were complete. The suspension was then aggressively agitated using a vortex for two minutes. After ultrasonication,  $\text{H}_2\text{SO}_4$  was added to avoid potential equipment corrosion. The obtained gel-like suspension was labelled “cellulose nanofiber” suspension and some amounts of the suspension were dried in order to perform characterization of the cellulose nanofibers.

### 2.4 Preparation of graphene oxide solution and chitosan-graphene oxide solution

2 mg of graphene oxide (GO) was dissolved in 5 mL of deionized water to obtain a GO concentration of  $0.4 \text{ mg mL}^{-1}$  and this GO solution was sonicated for 15 min. 0.1 g of chitosan was dissolved in 10 mL of 1% glacial acetic acid to obtain a 1% chitosan solution. For the mixture of chitosan and graphene oxide, 500  $\mu\text{L}$  of the GO solution was mixed with 2.5 mL of chitosan solution and the mixture was sonicated for 15 min in order to dissolve the GO in chitosan completely. The prepared solutions were stored in a refrigerator at 4  $^{\circ}\text{C}$ .



## 2.5 Preparation of acetylcholinesterase (AChE), acetylthiocholine (ATCh) and chlorpyrifos solutions

A solution of 0.3 mg mL<sup>-1</sup> of AChE was prepared by weighing 0.0015 g of AChE, dissolving it in 1 mL of DI water and storing at 4 °C. Next, 1.0 M of ATCh solution was prepared by dissolving 0.1980 g of ATCh in 1 mL of DI water. This solution was kept as a stock solution for the preparation of solutions with various ATCh concentrations, which were stored at 4 °C. For the preparation of 1 mM stock solution of chlorpyrifos, 0.0035 g of chlorpyrifos was dissolved in 10 mL of acetone, and various concentrations of chlorpyrifos solutions were prepared from this stock solution. Chlorpyrifos is a colorless to white crystalline solid with an odor resembling mercaptan. It is only weakly soluble in water, but is soluble in the majority of organic solvents like acetone, dichloromethane, ethyl acetate and methanol.<sup>50</sup> In addition, the preparation of all chlorpyrifos solutions was performed within a biosafety cabinet. All prepared solutions were stored at 4 °C for further experiments.

## 2.6 Preparation for the detection of chlorpyrifos in drinking water and juice samples

For the detection of chlorpyrifos in drinking water and juice samples, 100 µL of chlorpyrifos from a prepared 1 mM stock chlorpyrifos solution was spiked into 1 mL of drinking water and juice to obtain 1 µM chlorpyrifos-spiked drinking water and juice samples. From those spiked samples, 30 nM and 50 nM of chlorpyrifos solutions were prepared again and mixed with 1 mM ATCh and 2.5 mM ferri-ferrocyanide solutions. The modified SPCEs were incubated with the solutions for 15 min. Then, SWV analysis of the detection of the chlorpyrifos-incubated electrodes was performed.

## 2.7 Fabrication of the CNFs/GO/CS-GO/AChE-modified SPCE

First, 10 µL of the CNFs suspension was dropped on the surface of the working electrode of the SPCE and dried at room temperature for 1 h. Then, 10 µL of a GO solution was dropped on the SPCE as a second layer just before the layer of CNFs had dried entirely, and this second layer was allowed to dry at RT for 1 h. After drying the SPCE, 10 µL of the CS-GO solution was premixed with 10 µL of prepared AChE. 10 µL of the mixture of CS-GO/AChE was then immobilized on the surface of the CNFs/GO of the SPCE, dried

and stored at 4 °C for 24 h. The immobilized enzymatic electrochemical biosensors were labelled as CNFs/GO/CS-GO/AChE-modified SPCE. Moreover, CNFs/SPCE, CNFs/GO/SPCE, and CNFs/GO/CS-GO/SPCE were prepared using a similar method for comparison. The diagram of the device and the fabrication process are shown in Scheme 1. Chlorpyrifos was spiked into commercial water and juice samples in order to assess the applicability of our modified electrode. For each concentration and the experiments for parameter screening, three electrodes were prepared and all experiments were repeated three times.

# 3. Results and discussion

## 3.1 Characterizations of the synthesized cellulose nanofibers (CNFs)

Cellulose nanofibers were synthesized from raw sugarcane bagasse by AHP hydrolysis followed by ultrasonication<sup>48</sup> as described in Section 2.3. Following the synthesis, the surface morphology of the cellulose nanofibers was examined under a scanning electron microscope and compared to raw sugarcane bagasse and AHP-hydrolyzed cellulose, as depicted in Fig. 1a–c. Significant changes could be observed when comparing the raw sugarcane bagasse (Fig. 1a) and AHP-hydrolyzed cellulose (Fig. 1b). The intermolecular ester bonds between the lignin and carbohydrate were broken by the alkaline conditions during the hydrolysis of the raw bagasse in AHP solution.<sup>51</sup> The rapid oxidation of lignin into low molecular weight and water-soluble oxidation products, which causes the dissolution of lignin, is caused by the extremely reactive OH radicals released during the degradation of H<sub>2</sub>O<sub>2</sub>.<sup>52</sup> SEM images of the AHP-treated cellulose (Fig. 1b) indicated that most of the lignin and hemicellulose from the raw bagasse were successfully removed during AHP hydrolysis. After the cellulose was ultrasonicated for 2 hours in 1% H<sub>2</sub>O<sub>2</sub> at a low frequency (20 kHz) in an ice bath, the mesh layers of the strongly entangled porous networks of the cellulose nanofibers could be observed, as shown in Fig. 1c. Compared to the cellulose sample, the fiber shapes of the ultrasonicated sample displayed notable changes due to the synergistic effects of the H<sub>2</sub>O<sub>2</sub> and ultrasonication treatments.<sup>48,53</sup> After the ultrasonication process, cellulose nanofibers were generated, which are made up of a bundle of stretched cellulose chain molecules with long, web-like and highly entangled nanofibers. Furthermore, the elongated and

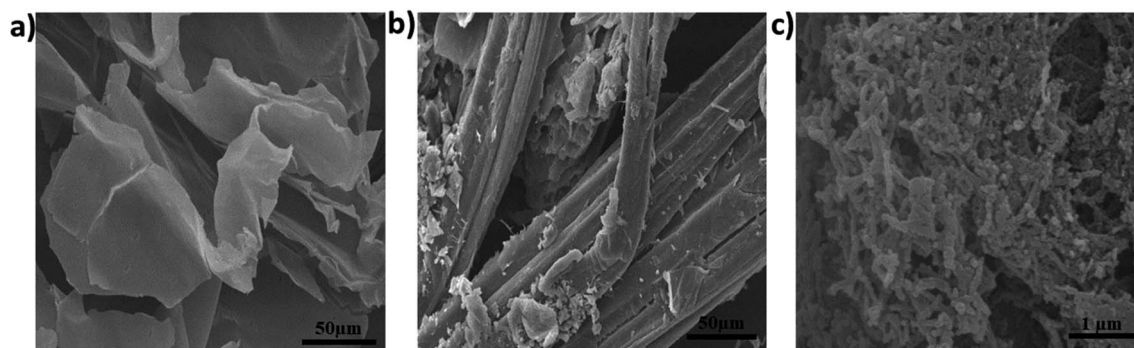


Fig. 1 SEM images of (a) raw sugarcane bagasse, (b) AHP-hydrolyzed cellulose and (c) cellulose nanofibers (CNFs).





intertwined structure of CNFs could be seen as shown in Fig. S1a† and the average diameter of CNFs was calculated using the Image J program; resulting in an average size of  $83.55 \pm 1.32$  nm ( $n = 106$ ) as shown in Fig. S1b.†

Additionally, the functional groups on the surface of the cellulose nanofibers (CNFs) were evaluated using attenuated total reflectance-Fourier transform infrared spectroscopy (ATR-FTIR) (Fig. S1†) by comparison with raw bagasse and AHP-treated cellulose. The results shown in Fig. S2† indicate that the change of lignocellulose composition throughout the AHP hydrolysis process was successful. The prominent peak at  $3354\text{ cm}^{-1}$  in the spectra of all the samples represents the O–H and C–H stretching of the OH- and CH- groups, respectively. The peak seen at  $1024\text{ cm}^{-1}$  in the spectra of all the samples represents the cellulose C–O–C pyranose ring stretching.<sup>54</sup> Another peak at  $2912\text{ cm}^{-1}$  in the spectra of the raw SCB and AHP-treated cellulose samples corresponds to the C–H stretching of the methyl groups that could be present in the hemicellulose and lignin. A sharp peak at  $1701\text{ cm}^{-1}$  in the spectrum of the raw SCB sample represents the C=O–O vibration of the acetyl and uronic ester groups of the hemicelluloses,<sup>55</sup> this peak was not observed in the spectra of the AHP-treated cellulose and CNFs. Similarly, a peak at  $1568\text{ cm}^{-1}$  in the spectra of the raw SCB and AHP-treated cellulose samples represents the aromatic C=C vibration in lignin, and this peak was also not observed in the CNFs spectrum. Other peaks at  $1380\text{ cm}^{-1}$  and  $1249\text{ cm}^{-1}$  represent the C–H bending and C–H stretching of hemicellulose and lignin.<sup>55,56</sup> This indicates that hemicellulose and lignin were successfully removed during the ultrasonication process.

### 3.2 Fabrication of the biosensor and its morphological and electrochemical characterization

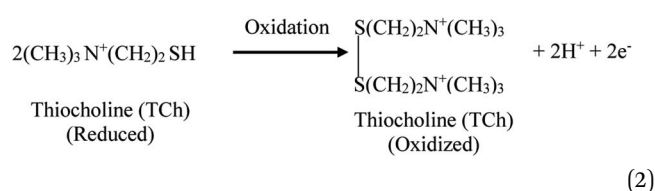
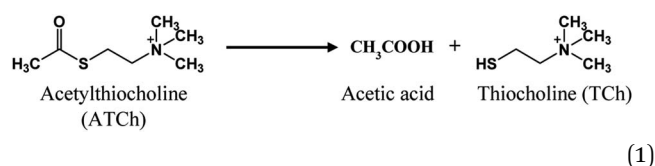
In this study, the nanocomposite materials CS-GO/GO/CNFs were coated on the surface of the SPCE's working electrode *via* a casting method. The enzyme AChE was immobilized on the electrode *via* a physical adsorption approach. Additionally, as our detection method relies on the reversible activity of the AChE enzyme, it is important to increase the AChE activity as much as possible. The enzyme structure was unaltered by this immobilization, allowing the enzyme to maintain its activity and facilitating the delivery of substrates to the enzyme's active region.<sup>57</sup> Surface morphological characterizations at each stage of the SPCE modification, including of the bare SPCE, the CNFs-coated SPCE, GO/CNFs/SPCE and AChE/CS-GO/GO/CNFs/SPCE, were carried out using SEM, as depicted in Fig. 2a–d. On the surface of the SPCE, a highly entangled, mesh-layered, interpenetrated network of CNFs was visible, as shown in Fig. 2b. The enormous surface areas of the GO sheets covered nearly the entire surface of the CNFs when GO was deposited on the CNFs, increasing the large electroconductive working area of the SPCE (Fig. 2c). After AChE was immobilized with the chitosan-graphene oxide mixture, a uniform, smooth and even layer could be seen on the electrode's surface (Fig. 2d).

Cyclic voltammograms (CVs) were measured to characterize the electrochemical reactions of the modified SPCEs. The results shown in Fig. 3a and b, indicate that after the CNFs were

coated on the surface of the SPCE's working electrode, the cathodic current decreased because of the non-conductivity of the CNFs. However, the electro-conductivity and the surface area of the working electrode could be enhanced by coating the CNFs with graphene oxide, as shown by the increase in the peak current of GO/CNFs to  $6.94 \times 10^{-5}$  A (Fig. 3d). The compatibility of the CNFs with GO was confirmed by the morphological characterization using SEM. Additionally, the CS-GO/GO/CNFs peak was clearly visible at  $7.94 \times 10^{-5}$  A (Fig. 3e), indicating that coating with the mixture of chitosan and GO might improve the signal amplification of the electrode's oxidation current. Even when compared with the current of the sample with only GO coated on SPCE, the CS-GO/GO/CNFs peak exhibited a higher current. Finally, when the AChE enzyme was coated on CS-GO/GO/CNFs, curve f in Fig. 3, the current was observed to decrease slightly to  $2.68 \times 10^{-5}$  A, due to the non-conductivity of AChE.

### 3.3 Reaction mechanisms of ATCh and chlorpyrifos on the modified AChE/CS-GO/GO/CNFs/SPCE

The modified AChE/CS-GO/GO/CNFs/SPCE electrode was studied using CV and SWV techniques, with ferri-ferrocyanide as a mediator solution for studying the mechanisms. Since acetylthiocholine serves as the substrate for the mono-enzymatic AChE biosensor, the first objective was to create a highly sensitive enzymatic product thiocholine (RSH) sensor. The major weakness in terms of electrochemical thiocholine detection is the large overpotential required on most common electrode surfaces (gold, platinum and carbon paste), as well as the fouling of the working electrode surface.<sup>58,59</sup> Utilizing nanostructured materials or redox mediators can help to overcome these problems and allow for the electrochemical detection of thiocholine. Our choice was to use cellulose nanofibers and the electrochemical mediator ferricyanide in solution, since it has the ability to electro-catalyze the oxidation of thiocholine.<sup>60–63</sup> ATCh is a substrate that AChE normally catalyzes into acetic acid and TCh. However, the pesticide organophosphate chlorpyrifos can inhibit the enzyme's function, stopping ATCh from being broken down into acetic acid and TCh, and halting the oxidative reaction. Based on the activity of AChE on ATCh, CV and SWV studies of the modified SPCE were performed, as shown in the following equations (eqn (1)–(3)).



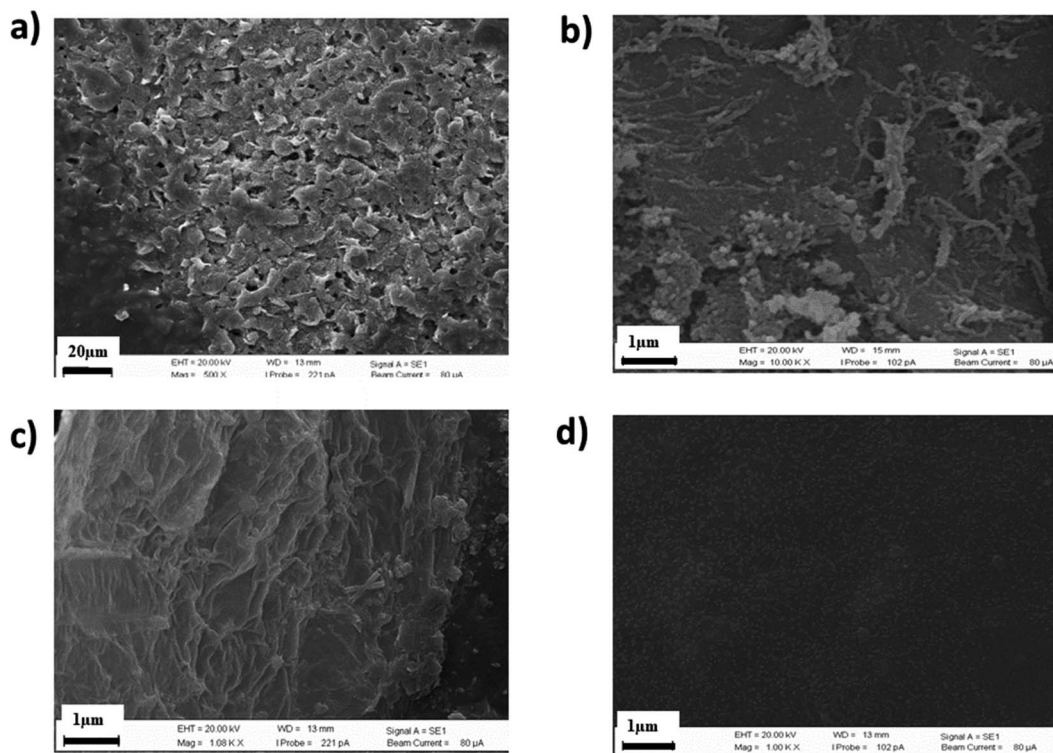


Fig. 2 SEM images of the surface of (a) bare SPCE, (b) CNFs/SPCE, (c) GO/CNFs/SPCE and (d) AChE/CS-GO/GO/CNFs/SPCE.

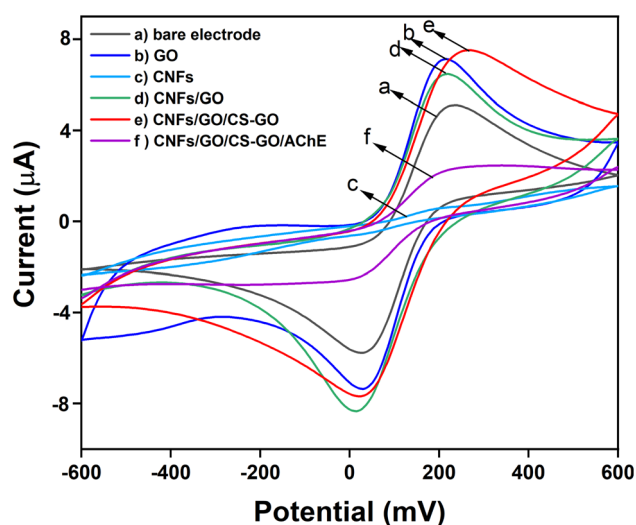


Fig. 3 CV curves for (a) a bare electrode, (b) GO/SPCE, (c) CNFs/SPCE, (d) GO/CNFs/SPCE, (e) CS-GO/GO/CNFs/SPCE, (f) AChE/CS-GO/GO/CNFs/SPCE, in the presence of 5 mM  $K_3[Fe(CN)_6]$ /0.1 M KCl.



While performing the CV on the modified SPCE with ATCh (red line in Fig. 4a), a significant anodic current was observed, compared with the current of the modified electrode (black line). The anodic current of the modified SPCE in the presence of ATCh and chlorpyrifos (blue line) appeared to be reduced

when chlorpyrifos was added, possibly as a result of chlorpyrifos' potential to suppress the activity of AChE. Similarly, the SWV response of the modified biosensor in the presence of ATCh (red line in Fig. 4b) showed the highest current compared with the modified SPCE (black line). The current of the modified SPCE in the presence of both ATCh and chlorpyrifos (blue line) significantly declined because chlorpyrifos inhibited the action of AChE, and the level of inhibition depended on the amount of chlorpyrifos added.

### 3.4 Effect of ATCh concentration and incubation time with ATCh on the modified SPCEs

The effect of various concentrations of ATCh on the modified electrodes immobilized with AChE was examined using SWV. The substrate ATCh can be converted into acetic acid and thiocholine (TCh) in the presence of AChE, as explained in Section 3.3. The TCh oxidation peak can be followed using SWV, as shown in Fig. 5a. The electrode currents gradually decreased as the ATCh concentration was changed from higher to lower concentrations (Fig. 5a and b). These results indicate that the working ability of the AChE-immobilized modified electrodes could be properly examined by using different concentrations of ATCh. With the highest current obtained, 1 mM of ATCh was selected as the optimum concentration for further experiments on our biosensor. Then, the AChE/CS-GO/GO/CNFs modified SPCEs were treated with 1 mM of ATCh and it was observed that the TCh oxidation current peaks increased as a function of time. However, the TCh oxidation peaks stabilized after 15 min, as depicted in Fig. 5c and d. Therefore, the optimal time for



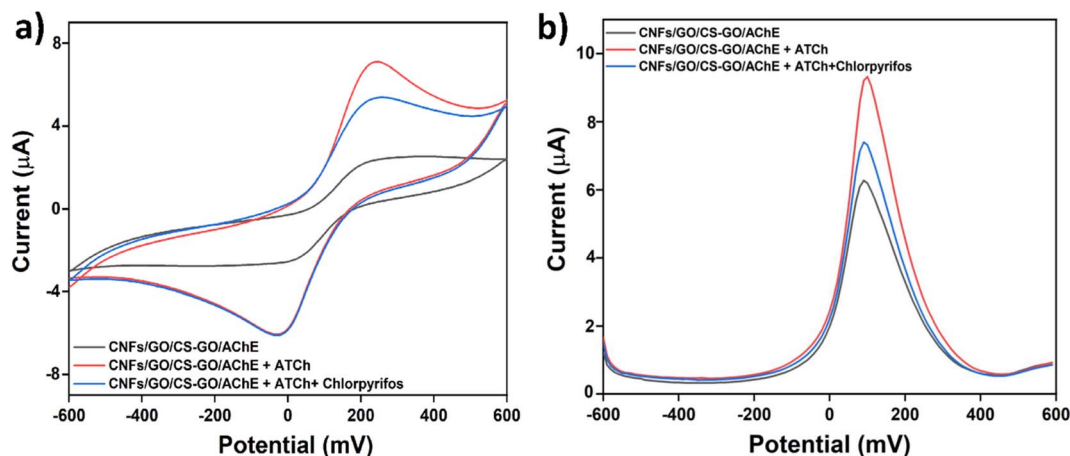


Fig. 4 (a) CV and (b) SWV responses for the modified SPCE in the presence of ATCh (red line) and in the presence of both ATCh and chlorpyrifos (blue line).

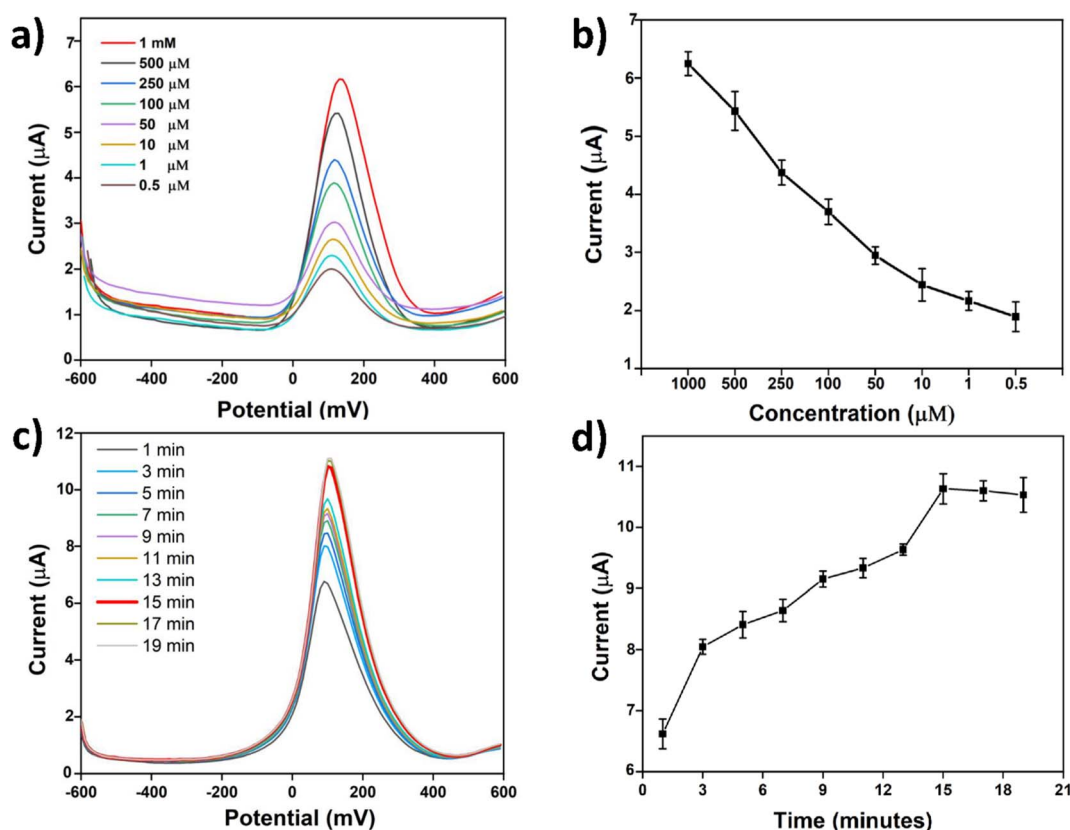


Fig. 5 SWV response for (a) the modified SPCEs to various concentrations of ATCh, (b) the corresponding line graph for the data in (a), (c) the currents of the modified SPCEs after incubation with 1 mM ATCh for different lengths of time, and (d) the corresponding line graph for the data in (c).

incubation of ATCh on the modified electrodes was chosen as 15 min and utilized for further experiments.

### 3.5 Effect of pH on the modified SPCEs

In this experiment, the electrochemical performance of the AChE/CS-GO/GO/CNFs/SPCE modified SPCEs at different pH

values (4, 6, 7, 8 and 10) was studied using the SWV technique. The AChE/CS-GO/GO/CNFs/SPCE modified SPCEs were incubated in 1 : 1 mixed solutions of 1 mM ATCh and 1 M phosphate buffer solutions with various pH values for 15 min. The results shown in Fig. 6a and b indicate that the modified electrodes show the highest current value following incubation in a buffer

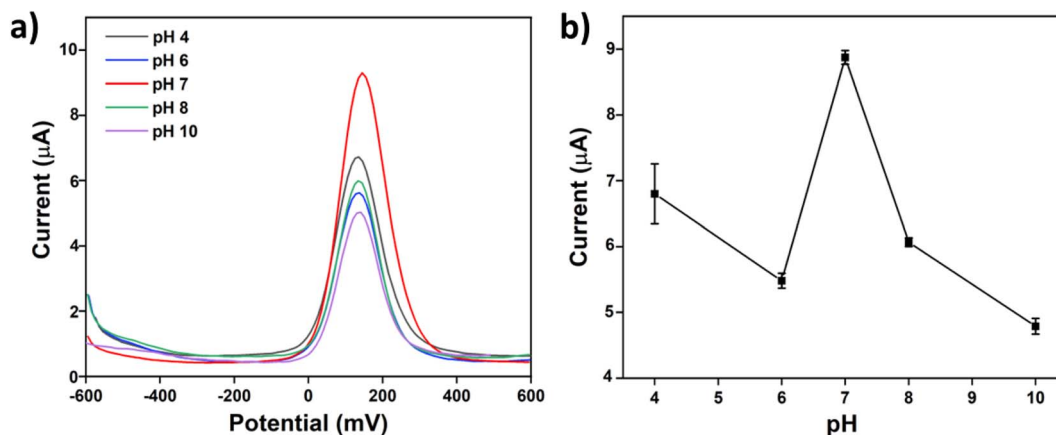


Fig. 6 (a) SWV response of the SPCEs in the presence of 1 mM ATCh and different phosphate buffer solutions (pH 4, 6, 7, 8 and 10). (b) The corresponding line graph for the data in (a).

solution at pH 7. The enzyme activity decreases as the pH value increases above or decreases below the optimal pH. The optimum pH for the AChE enzyme is 7-7 and the catalytic activity of AChE on acetylcholine is at its maximum at the optimum pH. Therefore, the current of the modified SPCE shows the highest peak at pH = 7 in our sensing system. Following this outcome, pH 7 was selected as the optimum pH for further analysis.

### 3.6 Effect of chlorpyrifos inhibition time on the modified SPCE biosensors

The organophosphate chlorpyrifos is an inhibitor of acetylcholine esterase, as illustrated above. Here in this part, SWV was used to follow the inhibition of the enzyme by the inhibitor. A solution of 1 mM ATCh and 5 μM chlorpyrifos was incubated on AChE/CS-GO/GO/CNFs modified electrodes in a ferri-ferrocyanide solution and experiments were conducted to determine the optimum time to inhibit the function of AChE. As seen in Fig. 7a, the TCh oxidation peak on the modified SPCEs gradually reduced as

a function of time. The results show that after 15 min, there was no further decrease in current. To simplify the term inhibition, the percentage of inhibition (inhibit%) for the modified SPCEs was calculated and is shown in Fig. 7b (inhibit% was calculated using the equation  $\text{inhibit\%} = I_0 - I/I$ , where  $I_0$  is the peak current of the modified SPCEs in the presence of 1 mM ATCh and in the absence of chlorpyrifos and  $I$  is the peak current of the modified SPCEs in the presence of 1 mM ATCh and in the presence of 5 μM chlorpyrifos). The inhibit% of the modified SPCEs did not rise after 15 min, implying that the activity of the AChE enzyme was completely prohibited by chlorpyrifos. Thus, an inhibition time of 15 min was selected as the optimum time to inhibit the function of the AChE enzyme and was used in further chlorpyrifos detection processes.

### 3.7 Analytical performance of the modified electrode for the detection of chlorpyrifos

After optimization of all the experimental parameters, chlorpyrifos was used as an analyte to determine the performance of

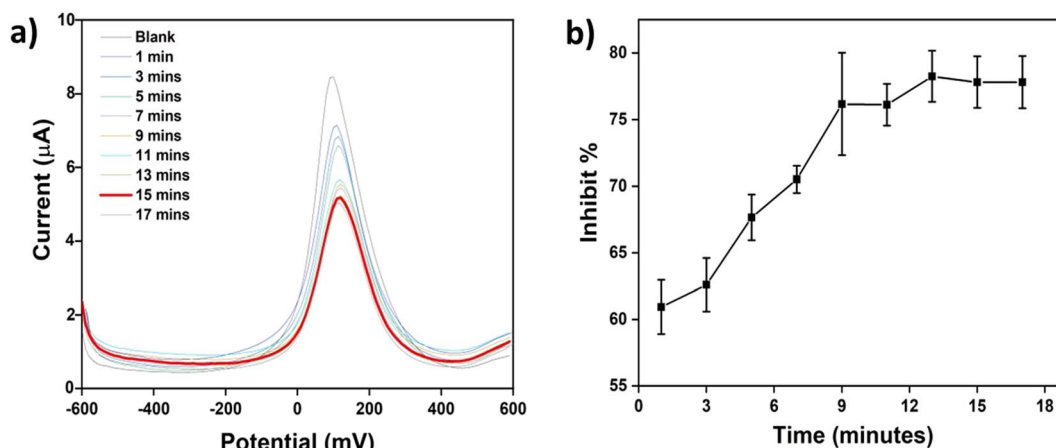


Fig. 7 (a) SWV response and (b) the inhibit% for the modified SPCEs as a function of increasing incubation time with chlorpyrifos. The concentration of chlorpyrifos is 5 μM.





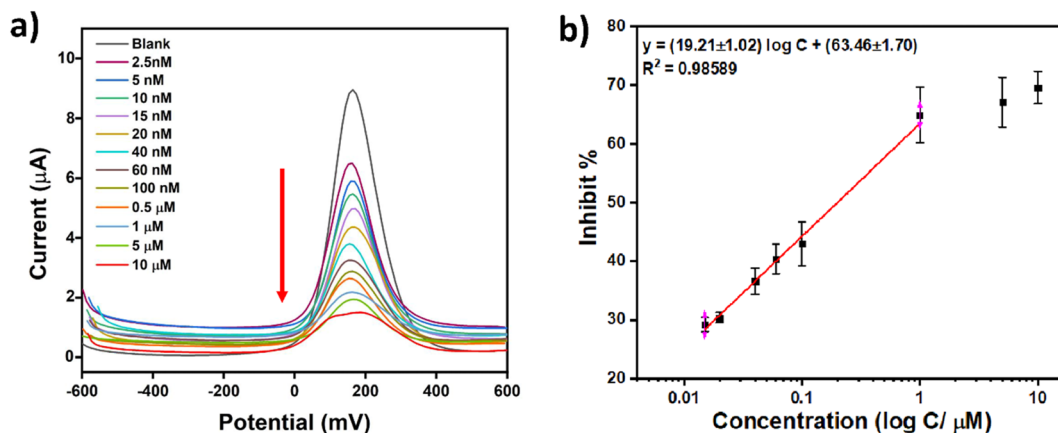


Fig. 8 (a) SWV response for the AChE/CS-GO/GO/CNFs modified SPCE treated with different concentrations of chlorpyrifos and 1 mM ATCh in phosphate buffer at pH 7. (b) The linear graph of chlorpyrifos concentration versus inhibit%.

the modified electrode. The modified AChE/CS-GO/GO/CNFs electrodes were treated with solutions of 1 mM ATCh and the following different concentrations of chlorpyrifos: 2.5 nM, 5 nM, 10 nM, 15 nM, 20 nM, 40 nM, 60 nM, 80 nM, 0.1 μM, 0.5 μM, 1 μM, 5 μM and 10 μM. Then the AChE/CS-GO/GO/CNFs modified electrodes were incubated for 15 min in the presence of chlorpyrifos, and SWV measurements were taken between  $-600$  mV and  $+600$  mV. The TCh peak currents of the modified SPCEs declined gradually as the concentration of chlorpyrifos was increased incrementally, as shown in Fig. 8a. The inhibit% for the enzyme biosensor in the presence of different concentrations of chlorpyrifos was calculated using the equation  $\text{inhibit\%} = I_0 - I/I$ , as defined in the above section, and a linear relationship was obtained as depicted in Fig. 8b. The least squares method was used to obtain the following linear relationship between the inhibition rate and the chlorpyrifos concentration:  $y = (19.21 \pm 1.02) \log C + (63.47 \pm 1.7)$  ( $R^2 = 0.98589$ ). Then the limit of detection (LOD) and limit of quantitation (LOQ) were calculated, resulting in the values 2.2 nM and 73 nM, respectively. These values represent the concentration of chlorpyrifos required to give a current change equal to 3 standard deviations ( $3\sigma$ ; 10 replicate measurements of blank sample ( $I_0$ )) for the LOD, and 10 standard deviations ( $10\sigma$ ) of  $I_0$  for the LOQ.

### 3.8 Selectivity and stability studies of the AChE/CS-GO/GO/CNFs modified SPCE

The selectivity of the modified AChE/CS-GO/GO/CNFs/SPCEs for the detection of chlorpyrifos spiked in water and in the presence of different analytes was measured using SWV. Generally, water samples might commonly contain many organic and inorganic substances which may interfere with the analysis of chlorpyrifos. Consequently, as shown in Fig. S3† and the corresponding histogram summarizing the results in Fig. S4,† the sensing tests were conducted in the presence of potential interfering materials that may coexist with the detection of OPs in water samples, such as  $\text{Na}^+$ ,  $\text{K}^+$ ,  $\text{Mg}^{2+}$ ,  $\text{Mn}^{2+}$ ,  $\text{Ca}^{2+}$ ,  $\text{Zn}^{2+}$ ,  $\text{Co}^{2+}$ ,  $\text{Fe}^{2+}$ ,  $\text{Hg}^{2+}$  and  $\text{As}^{3+}$ . The current response of the electrode modified

with substrate ATCh showed no apparent decrease in the presence of other analytes. The current of CNFs/GO/CS-GO/AChE/SPCE decreased significantly when a modified electrode was treated with chlorpyrifos, as seen in Fig. S3,† and the current difference ( $I_0 - I$ ) for chlorpyrifos on the modified electrode is greater than that of the other analytes, as shown in Fig. S4.† These experiments confirmed that the fabricated biosensors are robust even in the presence of possible interfering ions in the testing samples. Furthermore, the modified areas of the electrode were covered with  $1 \times$  phosphate buffer saline (PBS) solution and stored at  $4^\circ\text{C}$ , then stability tests were performed on the modified AChE/CS-GO/GO/CNFs/SPCEs. The modified electrode's sensing stability was subsequently tested for 21 days (Fig. S5a and b†) using 5 mM  $\text{K}_3[\text{Fe}(\text{CN})_6]/0.1$  M KCl and  $0.5$  μM chlorpyrifos. The study revealed that even after 21 days, the current of the modified SPCEs remained nearly equal to the original current recorded on the first day.

### 3.9 Determination of chlorpyrifos content in water and juice samples

Next, known concentrations of chlorpyrifos (30 nM and 50 nM) were spiked in the water and lychee juice samples (see Section 2.6), and the chlorpyrifos was assayed using the calibration curve shown in Fig. 8b. The results are depicted in Table 1 and reveal a satisfactory recovery percentage of 94.85–101.4% and a relative standard deviation (RSD%) of 3.03–4.39. These results suggest that this fabricated biosensor could be a practical

Table 1 Determination of chlorpyrifos content in water and juice samples

Sample ( $n = 3$ )	Added (nM)	Found (nM)	Recovery (%)	RSD (%)
Drinking water	50	$50.70 \pm 1.56$	101.4	3.08
	30	$29.41 \pm 1.29$	98.03	4.39
Lychee juice	50	$48.86 \pm 1.65$	97.72	3.38
	30	$28.45 \pm 0.86$	94.85	3.03



Table 2 Analytical performance of our fabricated biosensors compared with other methods

Method	Materials	Target OPs	Application	LOD	Linear range	Ref.
Fluorometric assays	Nitrogen-doped graphene quantum dots (N-GQD)	Fenoxycrab	River water	3.15 $\mu\text{M}$	6–70 $\mu\text{M}$	66
	Mn(II)-doped ZnS quantum dots	Chlorpyrifos	River water	17 nM	0.3–60 $\mu\text{M}$	67
Colorimetric assays	Ascorbic acid capped AuNPs	Dichlorvos	Wheat, water (tap, river and canal) and apple juice	42.9 $\mu\text{M}$	N.D.	68
	c-AgNPs	Dichlorvos	Drinking water and lychee juice	0.65 $\mu\text{M}$	1–7 $\mu\text{M}$	69
	Al <sub>2</sub> O <sub>3</sub> sol-gel matrix SPE	Dichlorvos	Sea water	0.01 $\mu\text{M}$	0.1–80 $\mu\text{M}$	70
	Peroxidase like CuFe <sub>2</sub> O <sub>4</sub> /GODs magnetic nanoparticles	Chlorpyrifos	—	10.7 nM	32–600 nM	71
	AChE/Fe <sub>3</sub> O <sub>4</sub> -CH/GCE	Carbofuran	Cabbage	3.6 nM	5.0–90 nM	72
Electrochemical biosensors	MPs-AChE	Carbofuran	—	20 nM	39–625 nM	73
	Molecularly imprinted polymer (MIP)	Chlorpyrifos	River water and lettuce	4.08 nM	0.1 nM–10 $\mu\text{M}$	74
	CNFs/GO/CS-GO/AChE/SPCE	Chlorpyrifos	Drinking water and juice	2.2 nM	2.5 nM–1 $\mu\text{M}$	This work

option for the determination of chlorpyrifos content in water and juice samples.

### 3.10 Comparison with other methods for chlorpyrifos detection

Chlorpyrifos breaks down into the harmless molecule 3,5,6-trichloro-2-pyridinol (TCP), which then gradually breaks down into carbon dioxide and organochlorine chemicals *via* both aerobic and anaerobic processes in the soil; it has a half-life of 60–12 days.<sup>11,64</sup> However, in naturally occurring water systems with microbial activity, chlorpyrifos has a half-life of less than a week and migrates to sediments, thus the risk to aquatic creatures arises from brief exposures to chlorpyrifos. The environmentally acceptable concentration for various applications of chlorpyrifos, as laid out by the World Health Organization, is 1  $\mu\text{g l}^{-1}$ .<sup>65</sup> Organophosphates including chlorpyrifos can be detected using a variety of assay techniques, some of which are electrochemical (amperometric), fluorometric and colorimetric, as listed in Table 2. Of these methods, electrochemical detection provides satisfactory results and has the benefit of being reasonably fast and accurate. We point out that, in comparison to previous approaches, our sensor system's limit of detection (LOD) for chlorpyrifos is lower than for other techniques.

## 4. Conclusions

The biocompatible and biodegradable cellulose nanofibers (CNFs) used in this study were created and loaded onto a screen-printed carbon electrode (SPCE) along with graphene oxide (GO), taking advantage of the compatibility of the CNFs with the GO layer. This increased the working surface area of the electrode, improved the conductivity of the graphene oxide, and increased the electrochemical activity of the electrode, all of which was confirmed using both cyclic voltammetry and square wave voltammetry techniques. The sensor is inexpensive,

operates well at room temperature, and does not require the use of any complicated apparatus. This biosensor is hence disposable; however, it displays great stability for at least 21 days. In addition, a linear relationship between the concentration of chlorpyrifos and the level of acetylcholinesterase (AChE) inhibition was obtained in the range 25–1000 nM. The limit of detection (LOD) and limit of quantitation were observed to be 2.2 nM and 73 nM, respectively, indicating the highly sensitive and selective inhibition of AChE by chlorpyrifos. Furthermore, the biosensor was employed to examine the chlorpyrifos content in actual water samples, producing results that were satisfactory and had a high recovery rate. Our proposed method may provide a more accessible, rapid and inexpensive way of measuring the chlorpyrifos contamination in water and juice. It is expected to be employed for analysis of chlorpyrifos in other environmental samples in the future.

## Conflicts of interest

There are no conflicts to declare.

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