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Triplet dynamic nuclear polarization of pyruvate *via* supramolecular chemistry†

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Dynamic nuclear polarization (DNP) significantly improves the sensitivity of magnetic resonance imaging, and its most important medical application is cancer diagnosis *via* hyperpolarized ^{13}C-labeled pyruvate. Unlike cryogenic DNP, triplet-DNP uses photoexcited triplet electrons under mild conditions. However, triplet-DNP of pyruvate has not been observed because of incompatibility of the hydrophobic polarizing agent with hydrophilic pyruvate. This work demonstrates that supramolecular complexation with β-cyclodextrin can disperse 4,4′-(pentacene-6,13-diyl)dibenzoate (NaPDBA), a pentacene derivative with hydrophilic substituents, even in the presence of high sodium pyruvate concentrations. The polarization of photoexcited triplet electron spins in NaPDBA was transferred to the ^{13}C spins of sodium pyruvate *via* triplet-DNP of ^{1}H spins in water and ^{1}H-to-^{13}C cross-polarization. This provides an important step toward the widespread use of ultra-sensitive MRI for cancer diagnosis.

Introduction

Nuclear magnetic resonance (NMR) is an important non-destructive technique for analyzing chemical structures, and magnetic resonance imaging (MRI) is an essential medical procedure. However, both methods are inherently insensitive because the sensitivity is proportional to spin polarization, which is 0.004% for ^{1}H spins and 0.001% for ^{13}C spins under a 6 T magnetic field at room temperature. Hence, MRI is essentially limited to abundant water molecules.

Dynamic nuclear polarization (DNP) improves the sensitivity of NMR[1–10] because it creates a hyperpolarized nuclear spin state by transferring the high polarization of unpaired electron spins. Dissolution-DNP[11–13] rapidly dissolves hyperpolarized solid samples and has been used for various NMR analyses, such as highly sensitive protein NMR[14,15] and *in vivo* metabolite imaging.[16–20] In particular, [1-^{13}C] pyruvate is the most important probe for high-sensitivity MRI because it is at the center of metabolism and its metabolic kinetics are used in the diagnosis of various diseases, including cancer.[16,17,21–24] Dissolution-DNP has achieved ^{13}C-NMR signal enhancement of more than 10 000-fold;[25] however, it requires severe conditions, such as a high magnetic field (∼7 T) and cryogenic temperatures near 1 K, to use the near-unity electron spin polarization. Alternatively, Overhauser-DNP is a powerful technique that polarizes solutions even at room temperature,[26–29] but the maximum enhancement factor depends on the difference in the gyromagnetic ratio between nuclear spins and electron spins ($\gamma_e/\gamma_H \sim 660$ and $\gamma_e/\gamma_C \sim 2600$).

In contrast, DNP *via* photoexcited triplet electron spins (triplet-DNP) can produce hyperpolarization under milder conditions.[30–34] Photoexcited triplets have large non-equilibrium spin polarizations (∼70% for pentacene[35]) that are independent of temperature, which enables DNP at higher temperatures and lower magnetic fields. Fig. 1A depicts triplet-DNP. After photoexcitation of a polarizing agent, a temporary spin-polarized state is generated by spin-selective intersystem crossing. After the polarization is transferred from the electron spin to ^{1}H spin, it is propagated throughout the solid *via* ^{1}H spin diffusion. Various host molecules and materials have been examined to hyperpolarize drugs,[36–38] water,[39–42] and biologically relevant molecules.[43,44] Dissolution triplet-DNP has been demonstrated.[45,46] However, spin-polarization transfer to lower

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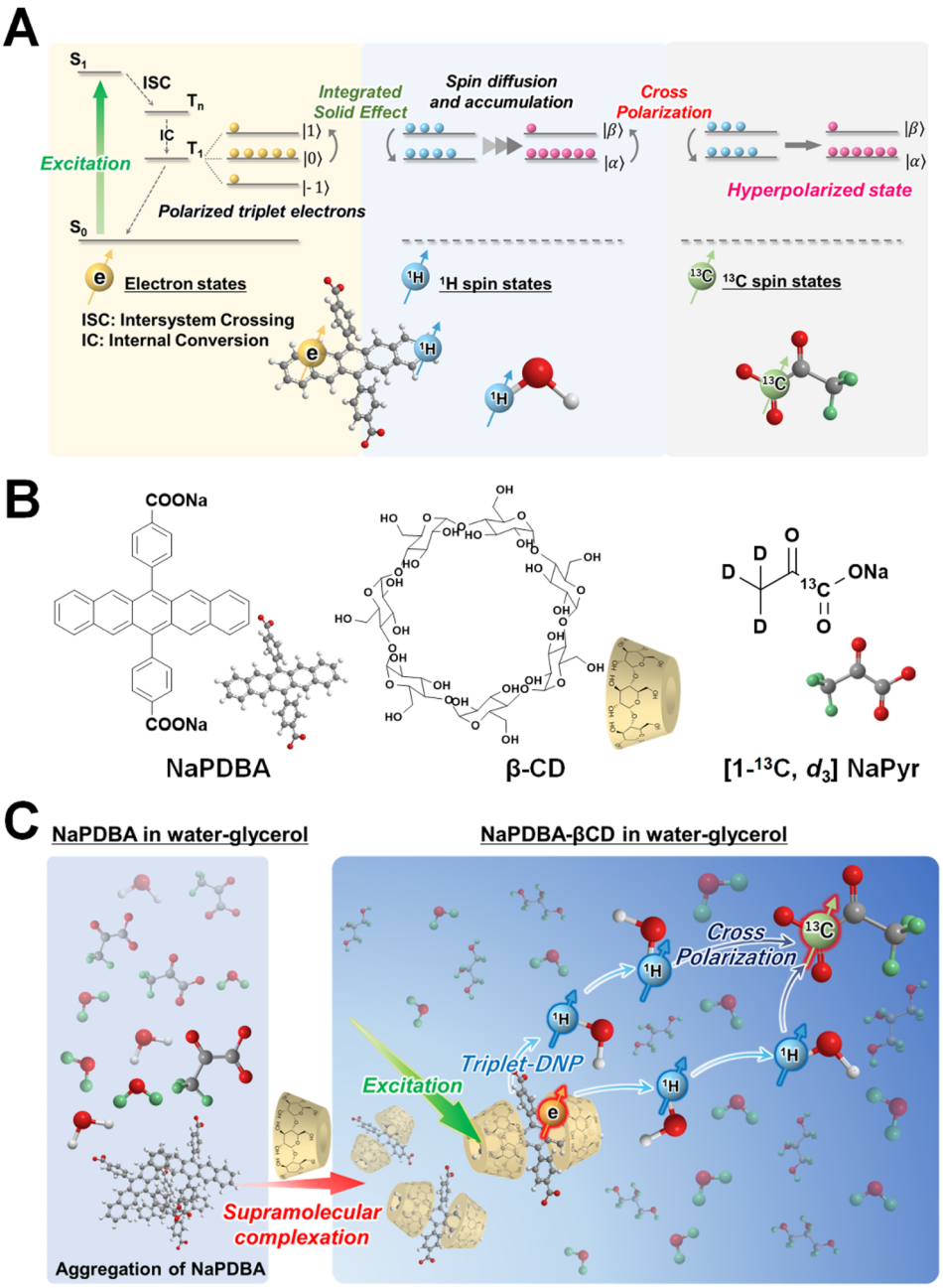

Fig. 1 Hyperpolarization of [1-^{13}C, d_3] sodium pyruvate (NaPyr) by triplet dynamic nuclear polarization (DNP) and cross polarization (CP). (A) Scheme of triplet-DNP and CP. (B) Molecular structures of NaPDBA, βCD, and [1-^{13}C, d_3] NaPyr. (C) NaPDBA aggregate in DNP juice in the absence of β-cyclodextrin (βCD), but the dispersibility is significantly increased by supramolecular complexation with βCD. Polarization transfer from photoexcited triplet electron spins to ^{1}H spins of water and then to ^{13}C spins of [1-^{13}C, d_3] NaPyr.

gyromagnetic ratio spins such as in ^{19}F and ^{13}C *via* cross polarization (CP) has been limited to aromatic molecules,[33,36,37,47] and triplet-DNP of [1-^{13}C] pyruvate has never been demonstrated because of poor miscibility between the hydrophobic polarizing agent and hydrophilic pyruvate.

Here, we report triplet-DNP of [1-^{13}C, d_3] sodium pyruvate (NaPyr) at ~100 K and 0.64 T. Higher concentrations of NaPyr are desired for dissolution-DNP application because the polarized spins are diluted after dissolution.[20] Water-soluble polarizing agents were developed and used for triplet-DNP in aqueous matrices,[41,43,48] but hydrophilic polarizing agents easily aggregate with high concentrations of polar pyruvate. To solve this problem, we used supramolecular chemistry to increase the dispersion of the polarizing agent (Fig. 1B). Cyclodextrin can encapsulate hydrophobic dyes in water,[49,50] and the triplet-DNP of water was observed by using 4,4′-(pentacene-6,13-diyl) dibenzoate (NaPDBA) as a guest in cyclodextrin.[48] NaPDBA aggregation was prevented by supramolecular complexation with β-cyclodextrin (βCD) with a saturated concentration of 1.5 M NaPyr in DNP juice (H_2O/D_2O/glycerol-d_8 = 1/3/6, v/v/v),

a general glass forming solvent.[20] The well-dispersed NaPDBA–βCD complex generated polarization of triplet electron spins, which was transferred to the ^{1}H spins of water in DNP juice by triplet-DNP and then to the ^{13}C spins of [1-^{13}C, d_3] NaPyr by CP (Fig. 1C).

Results and discussion

Evaluation of dispersibility of polarizing agents

The dispersed state of NaPDBA in DNP juice was evaluated *via* absorption spectra (Fig. 2) since random aggregation of polarizing agents could induce rapid relaxation of photoexcited triplet electron-spin polarization, significantly decreasing triplet-DNP efficiency. The π–π* absorption peak of 1 mM dispersed NaPDBA in methanol was observed at 593 nm (Fig. S5†). A red-shift to 604 nm was observed in DNP juice, indicating NaPDBA aggregation (Fig. S6†).[48] When 1.5 M of NaPyr was dissolved in DNP juice, the NaPDBA peak exhibited a large red shift to 614.5 nm, turning the solution blue (Fig. 2). This indicated that the NaPyr salt disrupted NaPDBA hydration and increased its aggregation.[51] The absorption peak was blue-shifted to 603 nm by adding 5 mM of βCD in DNP juice, in the presence of NaPyr (Fig. 2 and S7†). Previously, the 1 : 2 inclusion complex of NaPDBA–βCD was formed in a water–glycerol mixture [glycerol/H_2O (5/5, v/v)],[48] and the absorption peak was also blue-shifted by adding 5 mM of βCD in DNP juice [glycerol/H_2O (6/4, v/v)] in the absence of NaPyr (Fig. S8†). No significant change in the absorption spectra of NaPDBA–βCD in DNP juice was observed with or without NaPyr (Fig. 2). Here, the NaPDBA–βCD inclusion complex was intact at high NaPyr concentrations because the addition of salt increased water structuring and shifted the equilibrium toward the bound state.[52,53]

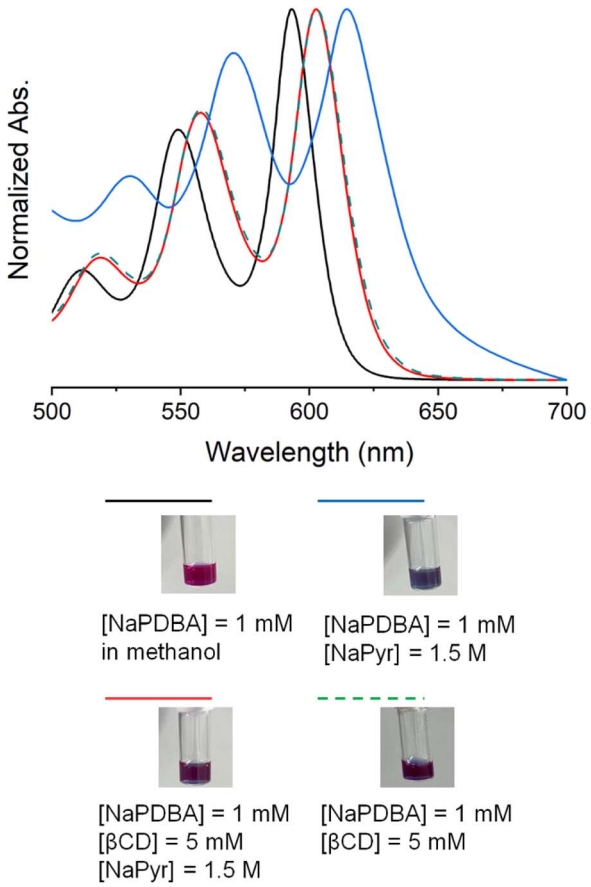

Fig. 2 Dispersion of NaPDBA in the presence of NaPyr. Absorption spectra of NaPDBA in methanol (black line), NaPDBA in DNP juice containing NaPyr (blue line), the NaPDBA–βCD complex in DNP juice (dashed green line) and the NaPDBA–βCD complex in DNP juice containing NaPyr (red line) at room temperature. The concentrations of NaPDBA, NaPyr, and βCD were 1 mM, 1.5 M and 5 mM, respectively. Photographs of each solution are shown.

Evaluation of supramolecular structures

The structure of the NaPDBA–βCD inclusion complex was investigated with NMR and molecular dynamics (MD) simulations. The room-temperature ^{1}H NMR spectra of NaPDBA shifted upfield when adding βCD in glycerol-d_8/D_2O (6/4, v/v) that contained NaPyr, which indicated formation of the inclusion complex (Fig. S9†).[54,55] Nuclear-Overhauser-effect room-temperature NMR of NaPDBA and βCD in D_2O with NaPyr revealed cross peaks between the NaPDBA pentacene skeleton and the βCD inner region (Fig. S10†). This indicated that NaPDBA was incorporated into the βCD hydrophobic cavity. NMR spectra of NaPDBA and βCD with different concentrations in D_2O which contained NaPyr indicated a 1 : 2 molar ratio of NaPDBA to βCD in the inclusion complex (Fig. S11†). In the MD simulations, the 1 : 2 inclusion complex was stable in glycerol/H_2O (6/4, v/v) (Fig. 3A and B), and remained stable in the presence of 1.5 M NaPyr (Fig. 3C and D). These results were

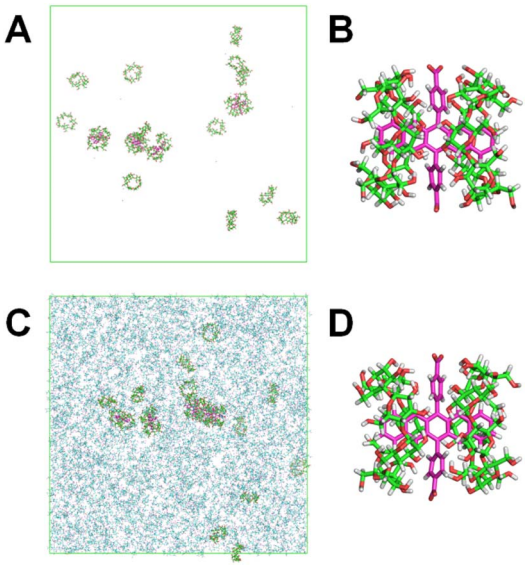

Fig. 3 Molecular dynamics (MD) simulations of NaPDBA–βCD supramolecular complexes. (A and B) MD simulation snapshots of the NaPDBA–βCD complex ([NaPDBA] = 1 mM and [βCD] = 5 mM) in glycerol/H_2O (6/4, v/v) at 300 K. Glycerol and H_2O were omitted for clarity. (C and D) MD simulation snapshots of the NaPDBA–βCD complex with NaPyr ([NaPDBA] = 1 mM [βCD] = 5 mM and [NaPyr] = 1.5 M) in glycerol/H_2O (6/4, v/v) at 300 K. Glycerol and H_2O are omitted for clarity.

consistent with the dispersibility of the NaPDBA–βCD complex with and without NaPyr.

Time-resolved ESR measurements

The polarization of photoexcited triplet electron spins in NaPDBA in DNP juice was evaluated by time-resolved X-band electron spin resonance (ESR) at 140 K (Fig. 4) after 527 nm pulsed-laser excitation. Almost no ESR signal was observed for NaPDBA in DNP juice containing NaPyr in the absence of βCD (Fig. 4A). This was because of random NaPDBA aggregation, which induced rapid relaxation of the triplet electron polarization. When a chromophore aggregate is in a random orientation, the photoexcited triplet electron spins hop between chromophores with different orientations, causing the electron spins subject to magnetic field fluctuations and inducing relaxation of electron spin polarization.[56,57] In contrast, the NaPDBA–βCD complex exhibited a clear ESR signal in DNP juice, even with NaPyr, reflecting well-dispersed NaPDBA *via* supramolecular complexation. The ESR spectra were fitted with the EasySpin toolbox in MATLAB.[58] The zero-field splitting parameters and relative populations of the NaPDBA–βCD complex were almost the same with and without NaPyr, and were almost the same as those for dispersed pentacene and its derivatives (Table S1†).[59,60] This confirmed that the supramolecular structure was intact in the presence of NaPyr, consistent with the absorption measurements. Fig. 4B shows the signal decay of the ESR absorption peak. The NaPDBA–βCD complex had 27 μs and 29 μs polarization lifetimes in the presence and absence of NaPyr, respectively. These lifetimes were long enough to use the triplet-DNP sequence.

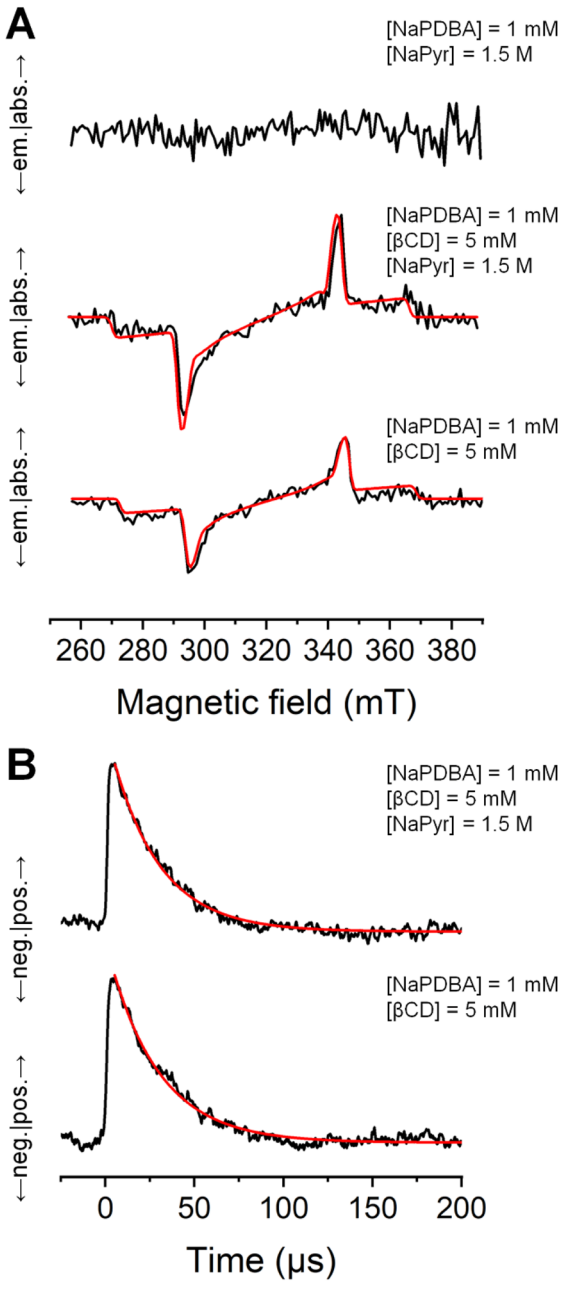

Fig. 4 Time-resolved electron spin resonance (ESR) spectra of NaPDBA and peak signal decays in DNP juice (glycerol/H_2O (6/4, v/v)). (A) ESR spectra of NaPDBA containing NaPyr (top), the NaPDBA–βCD complex containing NaPyr (middle), and the NaPDBA–βCD complex (bottom) after 527 nm photoexcitation at 140 K. The concentrations of NaPDBA, NaPyr and βCD were 1 mM, 1.5 M and 5 mM, respectively. Spectra were fitted with the EasySpin toolbox in MATLAB (red lines). (B) Decays of peak ESR signals (black lines). Single-exponential fits are also shown (red lines).

Evaluation of the spin–lattice relaxation time

Because the accumulation of spin polarization *via* triplet-DNP competes with ^{1}H spin relaxation, a solid sample must have a sufficiently long spin–lattice relaxation time (T_1) for efficient triplet-DNP. The ^{1}H T_1 of glassy DNP juice with NaPDBA and βCD was 46 s at 100 K and 0.64 T, while the addition of NaPyr significantly decreased it to 2 s (Fig. S12†). This was because of increased ^{1}H spin relaxation *via* methyl group rotation in NaPyr.[61] The use of deuterated sodium pyruvate (d_3-NaPyr) recovered the ^{1}H T_1 (26 s), and the difference from ^{1}H T_1 without NaPyr (46 s) may have been because of remaining ^{1}H spins in the methyl groups of [1-^{13}C, d_3] NaPyr.

DNP measurements

Polarization of the photoexcited NaPDBA triplet electron spins was transferred to the ^{1}H spins of water in DNP juice [glycerol-d_8/D_2O/H_2O, 60/30/10, (v/v/v)] by the ISE sequence at 100 K and 0.64 T (see the ESI for details, Fig. S13†).[31,34] NaPDBA was photoexcited with a 527 nm pulsed laser to produce the polarized electron spins. Then, 17.3 GHz microwaves were irradiated to transfer the polarization from electron spins to ^{1}H spins by matching the frequency of the electron spin in the effective magnetic field in the rotating frame with the Larmor frequency of the ^{1}H spins in the laboratory frame. The magnetic field was swept during microwave irradiation to use more electron spin packets, since the resonant field of the triplet electron spins is broadened by the random orientation of the polarizing agents and hyperfine interactions. By repeating the ISE sequence at 500 Hz, the ^{1}H spins were polarized throughout the glassy DNP juice until the accumulation of ^{1}H spin polarization reaches equilibrium with the spin–lattice relaxation. After the triplet-

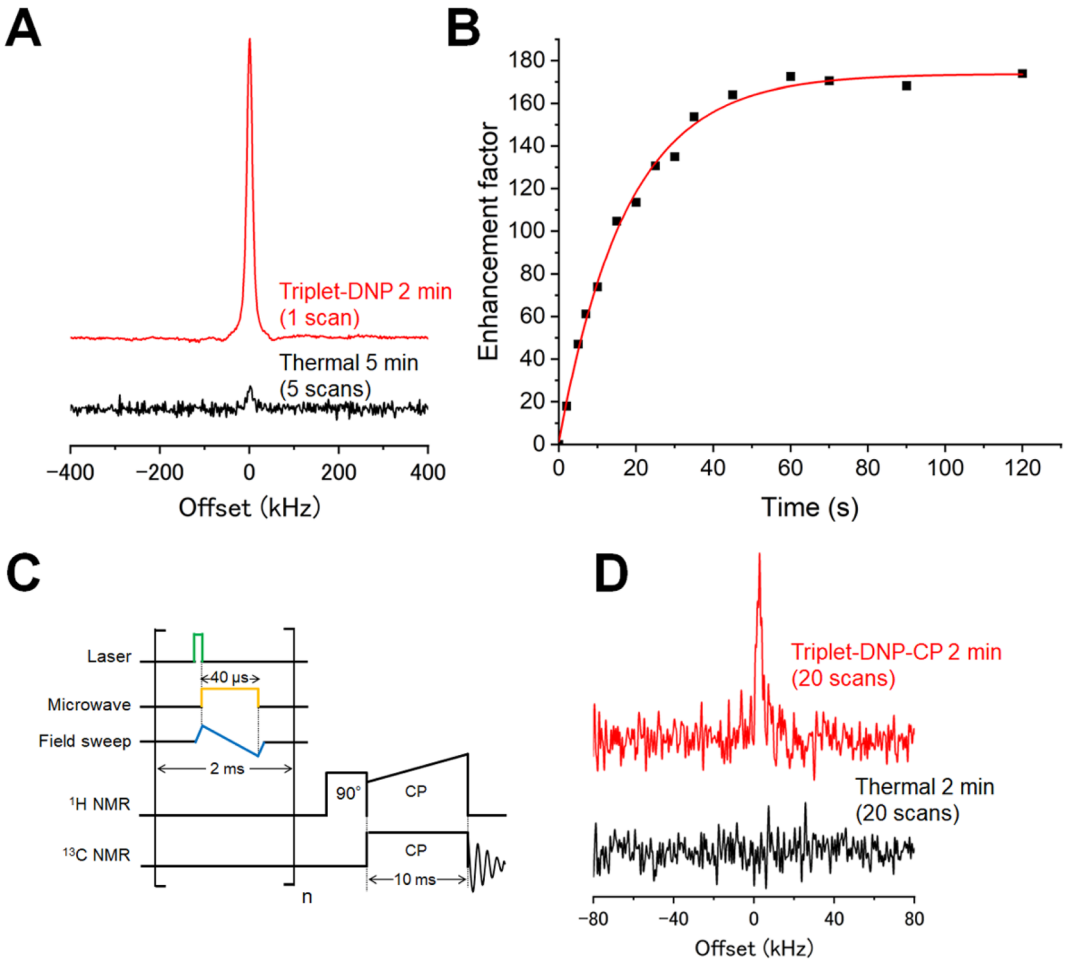

Fig. 5 (A) ^{1}H NMR signals of water in DNP juice (glycerol-d_8/D_2O/H_2O, 60/30/10, v/v/v) containing NaPDBA, βCD and [1-^{13}C, d_3] NaPyr under thermal conditions (five scans every 5 min) and after triplet-DNP (integrated solid effect sequence for 2 min and 1 scan) at 100 K. (B) ^{1}H polarization buildup curve of DNP juice containing NaPDBA, βCD and [1-^{13}C, d_3] NaPyr at 100 K. The enhancement factors were calculated by comparing the peak areas after triplet-DNP with that of thermal equilibrium. The enhancement factor relative to thermal equilibrium at room temperature is shown. (C) Sequence of triplet-DNP and ramped-amplitude cross-polarization (RAMP-CP). (D) 6.864 MHz ^{13}C NMR spectra of [1-^{13}C, d_3] NaPyr. The red line shows the spectra after triplet-DNP and RAMP-CP (integrated solid effect sequence for 2 min, followed by RAMP-CP, 20 scans) and the black line shows the spectra after RAMP-CP with thermal ^{1}H spins (20 scans).

DNP process in a microwave resonator, the sample was shuttled within 1 s to a coil *via* a motor to acquire ^{1}H NMR. Fig. 5A shows ^{1}H NMR of DNP juice containing 1 mM NaPDBA, 5 mM βCD, and 1.5 M [1-^{13}C, d_3] NaPyr obtained at the thermal state after 2 min of triplet-DNP, in which the accumulation of spin polarization and spin relaxation reached equilibrium. Enhancement factors of 58 and 174 were obtained relative to thermal equilibria at 100 K and room temperature, respectively (Fig. 5B).

The ^{1}H spin polarization in DNP juice was transferred intermolecularly to ^{13}C spins in [1-^{13}C, d_3] NaPyr with a ramped-amplitude cross-polarization (RAMP-CP) sequence (Fig. 5C).[62,63] After triplet-DNP at 100 K and 0.64 T, the sample was shuttled into a double-resonance coil with 27.30 MHz and 6.864 MHz resonance frequencies for ^{1}H and ^{13}C spins, respectively. Polarization transfer from ^{1}H spins to ^{13}C spins was conducted using a 10 ms contact. The irradiated field for the ^{13}C spins was fixed at 20 kHz, while that for the ^{1}H spins was swept over the range of 15–25 kHz. After triplet-DNP and RAMP-CP, enhanced ^{13}C NMR of [1-^{13}C, d_3] NaPyr was observed (Fig. 5D). The enhancement was clear from the fact that no ^{13}C NMR peak was observed *via* RAMP-CP when using ^{1}H spins at thermal equilibrium. ^{13}C-methanol at room temperature was used as a reference, and an enhancement factor of 122 was estimated (Fig. S14†). ^{13}C spins in [1-^{13}C, d_3] NaPyr accounted for ∼85% of the total ^{13}C spins in the entire solid sample; thus, the polarization enhancement factor of the ^{13}C spins in [1-^{13}C, d_3] NaPyr should have been close to 122. Because the theoretical ^{13}C NMR enhancement was ∼4 times (γ_H/γ_C) that of ^{1}H NMR with ideal CP, the CP efficiency was 18%. The low efficiency could be attributed to the absence of ^{1}H spins in [1-^{13}C, d_3] NaPyr, because 40–60% efficiencies were observed when ^{1}H spins were present in the target molecule.[64] Furthermore, ideal CP requires that the radiofrequency pulse amplitude be stronger than the ^{1}H NMR linewidth (∼50 kHz).[65] A higher CP efficiency could be obtained by using a stronger radiofrequency pulse.

Conclusions

In conclusion, triplet-DNP of [1-^{13}C, d_3] NaPyr, the most important biomolecular probe in MRI applications, was observed by increasing the polarizing agent dispersion *via* supramolecular complexation. It is important to perform DNP with highly concentrated NaPyr, but the method to disperse the polarizing agent in such a highly polar medium had not been clear. Here, the polarizing agent could be modified with ionic carboxylate moieties and then complexed in supramolecular cyclodextrin, which enabled adequate dispersion. This enabled hyperpolarization of the [1-^{13}C, d_3] NaPyr ^{13}C spins *via* triplet-DNP-CP under a low magnetic field (~0.64 T) and above liquid nitrogen temperatures (~100 K). Since the final polarization obtained by triplet-DNP is determined by the build up time constant, T_b, and T_1, higher ^{1}H and ^{13}C spin polarizations require a shorter T_b and longer T_1. Recently, novel pentacene derivatives showing sharper ESR lines exhibits a shorter T_b than pentacene and the ^{1}H spin polarization is four times higher than that of pentacene.[66] In addition, the polarization increased 10-fold as T_1 increased from 1 to 3 min, and a spin polarization of 8% was achieved in a model amorphous matrix.[66] Higher ^{1}H and ^{13}C spin polarization can be obtained by using such a new polarizing agent instead of NaPDBA to obtain shorter T_b and by diluting the ^{1}H spins or using other matrices with longer T_1. In addition, the implementation of more advanced polarization transfer methods with field/frequency modulation would improve the final spin polarization.[67,68] Hyperpolarized MRI with triplet-DNP will be possible by combining the optimized molecular design of polarizing agents with the key finding of the present study that supramolecular complexation is useful to hyperpolarize NaPyr at high concentrations.

Data availability

All experimental data are available in the article and ESI.†

Author contributions

T. H., Y. K., H. K. and N. Y. designed the research. T. H. and S. K. prepared and characterized the materials. K. T. and T. U. built time-resolved ESR and DNP setups. T. H. and S. K. conducted time-resolved ESR measurements. T. H. and K. N. conducted DNP measurements. S. S. and G. W. carried out MD simulation. T. H., K. N. and N. Y. wrote the manuscript with contributions from all authors.

Conflicts of interest

There are no conflicts to declare.

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