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# Selective placement of functionalised DNA origami *via* thermal scanning probe lithography patterning†

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Here we present a nanopatterning strategy utilising thermal scanning probe lithography (t-SPL) for the precise organisation of DNA origami into nanoarrays. The aim of this approach is to demonstrate control in the fabrication of nanoarray platforms exhibiting single-molecule accuracy. Combining the inherent programmability of DNA origami structures with t-SPL nanopatterning, we demonstrated the controlled immobilisation on surfaces of functionalised DNA origami – as proof of concept we employed gold nanoparticles (AuNPs) and quantum dots (QDs) – at predefined positions and in nanoarray configurations. This method holds great potential for the construction of hetero-functionalised biomolecular nanoarrays with single-molecule control, with applications in bionanotechnology and (nano)materials science.

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## 1. Introduction

The ability to control the patterning of single molecules/moieties with nanoscale spatial resolution, is of great interest in a variety of fields, from optoelectronics to biomedicine.<sup>1–3</sup> In this context, the integration of DNA nanotechnology approaches and lithographic patterning methodologies has allowed the development of large-scale nanoarrays of single molecules, enabling high-throughput designs and assays.<sup>4</sup> Notable examples include the construction of nanoparticles arrays,<sup>5–9</sup> the linking of molecular emitters to photonic crystal cavities as an ideal technique for the fabrication of hybrid nanophotonic devices,<sup>10</sup> and the fabrication of biomimetic nanoarrays for multivalent investigations of ligand–receptor interactions in cancer cell spreading.<sup>11,12</sup>

Due to its high programmability and remarkable chemical flexibility, DNA has indeed become a highly desirable material for the organisation of individual molecules and nanostructures with nanoscale spatial resolution and single-molecule control.<sup>13,14</sup> DNA origami, a bottom-up construction approach, utilises a long viral DNA strand as a scaffold that can be folded

into a predetermined shape by incorporating specifically designed short staple strands.<sup>15,16</sup> Modular DNA origami nanostructures, comprising various moieties, such as biomolecules (proteins, aptamers, or RNA),<sup>17,18</sup> nanoparticles (metal particles, quantum dots)<sup>19–21</sup> and organic dyes,<sup>22</sup> can be assembled with a resolution of 3–5 nm.<sup>14</sup> This precision is achieved by attaching distinct molecules to the staple strands through site-specific modifications.

Large-scale organization of modular DNA origami can then be achieved through electrostatic or covalent immobilization onto activated binding sites, which have been lithographically defined on substrates.<sup>6,23–28</sup> Top-down approaches for manufacturing and immobilising nanostructures have received great attention in chemical and biological research as they can attain nanoscale resolution and allow the hierarchical organisation of molecules and nanoscale moieties. Various techniques have been employed to this end, including electron-beam (e-beam) lithography,<sup>25</sup> focused ion beam (FIB) lithography,<sup>11,29</sup> nanoimprint lithography,<sup>23,30</sup> colloidal lithography,<sup>7,31</sup> scanning probe lithography,<sup>32,33</sup> biotemplated lithography,<sup>34,35</sup> and dip-pen nanolithography.<sup>36</sup>

In previous studies, we employed e-beam lithography and FIB patterning, to selectively fabricate and organize functionalised DNA origami scaffolds on surfaces in array configurations, in order to fabricate single-molecule nanoarrays of quantum dots,<sup>37</sup> proteins,<sup>38</sup> and cell-binding ligands for the investigation of cancer cells spreading<sup>11</sup> and cardiomyocytes mechano-signaling.<sup>12,39</sup> Although e-beam and FIB lithography techniques are reliable and commercially available, they are costly,

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time-consuming and have several drawbacks such as the requirement of ultrahigh vacuum, limiting their scale-up and application.<sup>40</sup> Here, we employed thermal scanning probe lithography (t-SPL)<sup>41</sup> as an alternative nanopatterning strategy. In this technique thermal energy from a heated tip is used to induce local material modifications, typically a removable thermolabile resist.<sup>41</sup> t-SPL distinct qualities, including high-resolution nanolithography, closed-loop operation enabling simultaneous reading and writing for characterisation without prior development step, and non-invasiveness (avoiding proximity effects), have allowed its use for a variety of applications, from sub-10 nm resolution patterning,<sup>42</sup> to nanoscale precise 3D fabrication,<sup>41–43</sup> nanoelectrode patterning for 2D electronics,<sup>44</sup> high-throughput protein nanopatterning,<sup>45</sup> and the nanoscale tuneable reduction of graphene oxide.<sup>46</sup>

In the study presented here, we demonstrate the organisation of heterogenous functionalised DNA origami, incorporating AuNPs and QDs, in predefined positions within a nanoarray pattern created using t-SPL. This strategy allows for the construction of versatile and tuneable DNA-templated surfaces, that hold considerable promise for the fabrication of hetero-functionalised single-molecule nanoarrays, with broad applications in bionanotechnology and materials science.

## 2. Materials and methods

### 2.1. Preparation of DNA origami

DNA origami assembly *via* combining 10 nM single-stranded M13mp18 scaffold DNA and 100 nM staple strands in a 50  $\mu$ L volume of 1 $\times$  assembly buffer (1 $\times$  TAE with 12.5 mM MgCl<sub>2</sub>) and annealed from 95  $^{\circ}$ C to 20  $^{\circ}$ C in a thermal cycler at a cooling rate of 1  $^{\circ}$ C per minute and keep in 4  $^{\circ}$ C after annealing. The mixture solution of self-assembled DNA origami was purified with Millipore Amicon Ultra 100 kDa spin columns in a centrifuge at 10 000 rpm for 4 min, three times, to remove unassembled staple strands. A UV-Vis spectrophotometer was used to detect the rough concentration of DNA origami products.

### 2.2. Preparation of AuNPs-ssDNA

Following mixing 1 mL of AuNPs with 4  $\mu$ L Tween 80 (10% v/v, in water), the mixture was allowed to react for 30 min at room temperature. Next, 0.1 M PBS was added to the mixture. Thiol-ssDNAs were subsequently introduced into the AuNPs solution, resulting in a final DNA concentration of 10  $\mu$ M. The mixture was then incubated for 2.5 hours at 50  $^{\circ}$ C. Any unbound ssDNAs were separated by centrifugation at 16 000g for 15 minutes and washed three times with 1 $\times$  assembly buffer. Finally, the resulting conjugates were re-dispersed in 1 $\times$  assembly buffer.

### 2.3. DNA origami functionalisation

Amino anchors were assembled onto DNA origami for surface covalent immobilisation. The modification of the amino group on DNA origami is achieved by modified of an amino group at the 3' end of 15 chosen staple strands (A05, B05, C05, A13, B13,

C13, A33, B33, C33, A42, B42, C42, A50, B50, C05, and C50) which are all positioned in the inner edges of triangular DNA origami.

To modify DNA origami with AuNPs, AuNPs were conjugated with thiol single-stranded DNA (ssDNA-SH) through thiol-Au interactions. The resulting AuNPs-ssDNA complexes were designed to be complementary to the sticky ends predefined on the staple strands A48, A49, and A56 of DNA origami. AuNPs-ssDNA were then mixed with DNA origami in a 5:1 ratio in 1 $\times$  assembly buffer. The mixture was incubated in the fridge overnight to allow for complete complementary binding with the sticky ends.

To modify DNA origami with streptavidin-QDs, commercially available streptavidin-modified QDs were directly attached to the biotinylated sticky ends on the DNA origami (located at B32 in a corner of the triangle). Streptavidin-QDs were mixed with biotinylated DNA origami in a 10:1 ratio in a 1 $\times$  assembly buffer. The mixture was then incubated at room temperature for 30 minutes. Subsequently, the functional DNA origami was cast onto the surface of a freshly clean mica and characterised using atomic force microscopy (AFM).

### 2.4. AFM characterization of DNA origami

Dimension icon AFM (Bruker) was used to characterize the DNA origami structures. The DNA origami solution is diluted by 1 $\times$  assembly buffer to around 1 nM for getting a good separation of the DNA nanostructures. Five micro liters of diluted DNA origami solution were cast on freshly cleaned mica and left to adsorb on the surface for 5 min. Subsequently, the substrate was washed with distilled water to remove non-absorbed origami and then blown dry by compressed air. ScanAsyst-Air tips with 0.4 N m<sup>-1</sup> spring constant were used to scan the sample by AFM under ScanAsyst™ Mode. A resolution of 512 pixels per line with a 1 Hz scan rate was chosen for appropriate imaging of the DNA origami nanostructures.

### 2.5. t-SPL nanopattern fabrication

Silicon chips are soaked and sonicated in acetone for 5 minutes, then rinsed with isopropanol. The silicon chips were dried with compressed air and cleaned using 2 minutes of Harrick plasma treatment. The resist films were prepared by spin coating polyththalaldehyde (PPA, 5% in anisole). To achieve 80 nm thick films, PPA was spun at 3000 rpm for 35 s at ambient conditions, followed by incubation at 110  $^{\circ}$ C for 2 minutes to remove residual solvent. The substrate, patterned by t-SPL, was designed to match the size of the DNA origami. Nanoapertures for DNA origami placement was created by selectively removing the PPA resist. The PPA resist can be removed if needed *via* the use of *N*-methyl-2-pyrrolidone. All t-SPL processes were conducted using the NanoFrazor Explore system, Heidelberg Instruments, following the manufacturer's instructions. The generated patterns were packed in a clean 24-well plate and prepared for DNA origami immobilization.

### 2.6. DNA origami covalent immobilisation

After oxygen plasma treatment, a 0.1% solution of carboxyethylsilane (CTES) in 5 mM Tris buffer (pH 8) was incubated on a



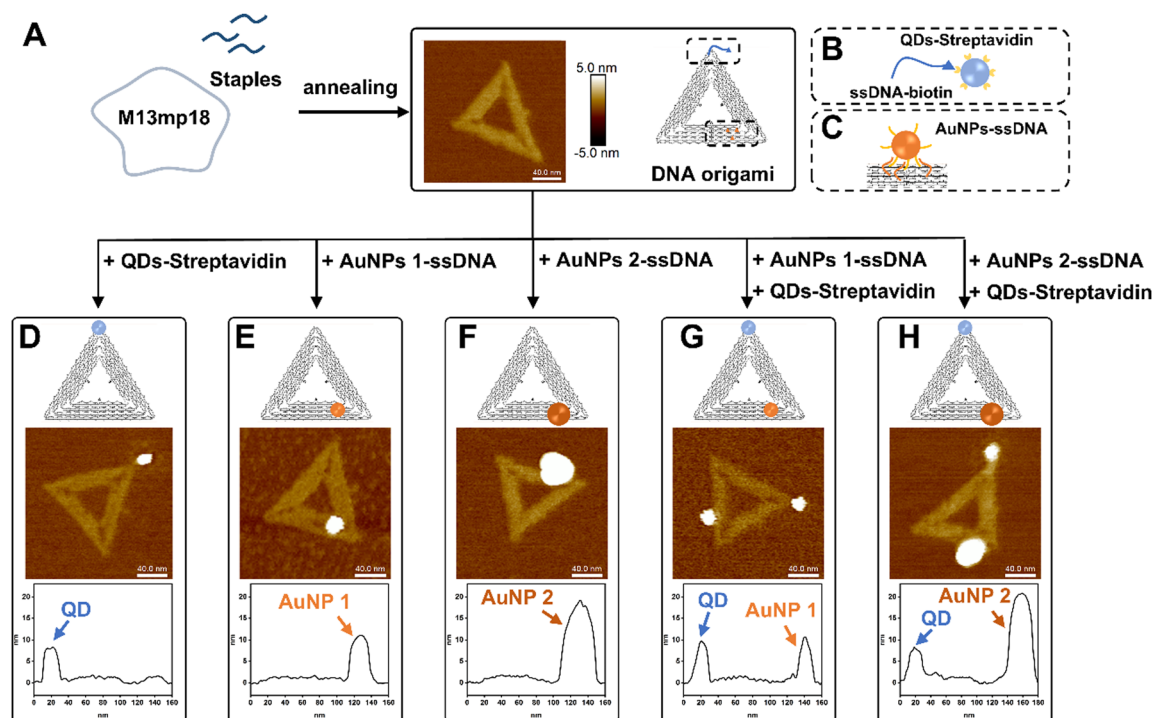
shaker for 30 minutes to form carboxyl groups on the activated binding sites. The substrates were then washed three times with  $1\times$  assembly buffer to remove any free CTES. To covalently binding DNA origami to carboxyl sites, fifteen amino anchors along the inner edges of the triangular DNA origami were functionalised. One hundred microliters of the DNA origami solution (300 pM) were deposited onto the substrate and incubated on a shaker for 1 hour in a 24-well plate with a moist Kimwipe. After placement, the substrates were washed three times with 10 mM MOPS buffer (pH 8.1) containing 125 mM  $MgCl_2$ . An equal volume of 50 mM EDC and 100 mM NHS in MOPS buffer was added to the substrates and incubated on a shaker for 10 min for covalent conjugation. The DNA origami covalently conjugated substrates were washed with 10 mM MOPS buffer (pH 8.1) containing 150 mM NaCl, then rinsed with PBS containing 125 mM NaCl to remove any noncovalently bound DNA origami, and subsequently rinsed with water and dry with compressed air. The samples were checked under AFM.

**2.6.1 Optional.** Due to the strong binding of DNA origami to the negatively charged silicon surface in a high magnesium concentration, we can also use a non-covalent binding strategy in magnesium buffer as a simple alternative. One hundred microliters of DNA origami in placement buffer (10 mM Tris buffer with 35 mM  $MgCl_2$ , pH 8.3) at a concentration of 300 pM were cast onto the patterning substrate for 1 hour on a shaker. Then, 500  $\mu$ L of placement buffer were added to wash away nonbinding DNA origami. The substrates are dried with an

ethanol gradient, dipped in mixtures of 25%, 50%, 70%, 80%, and 90% ethanol for 10 seconds each, and then air-dried.

### 3. Results and discussion

Triangular DNA origamis were chosen and synthesized in this project due to their inherent advantages such as stiffness and low tendency to folding and aggregation during assembly from solution to surfaces.<sup>15</sup> To verify the construction of these DNA nanostructures, synthesized DNA origamis were cast on clean mica and imaged using atomic force microscopy (AFM). AFM imaging confirmed that triangle DNA origami contain three 120 nm edges and have a height of roughly 1.5–2 nm, which is consistent with the height of dsDNA (Fig. 1A). Different nanoparticles were selected in this proof-of-concept project, namely commercially available streptavidin modified quantum dots (QDs) ( $\sim 9.4 \pm 0.8$  nm) and ssDNA-conjugated gold nanoparticles (AuNPs) of different sizes (AuNPs 1-ssDNA,  $\sim 8.7 \pm 0.5$  nm and AuNPs 2-ssDNA,  $\sim 18.7 \pm 4.8$  nm) [Fig. S1 in the ESI<sup>†</sup>]. The DNA origami scaffold was modified with biotin to the end of a staple located in a corner of its triangular structure, which can bind to streptavidin modified QDs (Fig. 1B). For the binding of AuNPs to the DNA origami, the metal nanoparticles were modified with a thiol single-strand DNA (ssDNA-SH) with the aid of tween 80 (ref. 47) (Fig. S2, ESI<sup>†</sup>), to obtain AuNPs-ssDNA hybrids complimentary to predefined sticky ends on the DNA origami (Fig. 1C). Fig. 1D–H show the schematic design of



**Fig. 1** Synthesis and functionalisation of DNA origami with QDs and AuNPs. (A) Schematic of DNA origami synthesis. (B) Cartoon of DNA origami functionalised with QDs via biotin–streptavidin coupling, and (C) of ssDNA functionalised AuNPs complementary hybridisation on predefined sticky ends of DNA origami. Schematic, topographic AFM image and corresponding height profile of DNA origami modified with (D) one QD, (E) AuNP 1, (F) AuNP 2, (G) AuNP 1 and QD, and (H) AuNP 2 and QD.



DNA origami modified with QDs/AuNPs and the corresponding AFM topographical images confirming DNA origami's heterogeneous functionalisation. AFM imaging allowed us to determine the yield of mono- and multi-valent functionalisation (Fig. S3, ESI<sup>†</sup>): 79.28% (88/111) with a QD (Fig. 1D), 83.77% (294/351) with AuNP 1 (Fig. 1E), 88.89% (176/198) with AuNP 2 (Fig. 1F), 65% (78/120) with QD and AuNP 1 (Fig. 1G), and 70.53% (67/95) for DNA origami with QD and AuNP 2 (Fig. 1H).

In order to organise the functionalised DNA origami in nanoarray configuration on surfaces, we employed t-SPL to nanopattern on silicon chips and create chemically patterned areas capable of selectively binding DNA nanostructures. The silicon substrates were coated with polyphthalaldehyde (PPA), as

illustrated in Fig. 2A; subsequently t-SPL was employed to pattern areas matching the size and shape of the DNA origami we employed. Following the thermal scan probe etching process, the PPA decomposes from polymers into monomers, exhibiting topographic features as designed (Fig. 2B). Subsequently, selective removal of the PPA resist remaining in the nanoapertures was achieved by oxygen plasma etching, creating hydrophilic regions for the subsequent DNA origami placement (Fig. 2C). The initial thickness of PPA was *ca.* 80 nm, as measured by AFM, and was decreased by oxygen plasma treatment at a rate of *ca.* 1.2 nm per second (Fig. S4, ESI<sup>†</sup>). The plasma activated silicon surfaces exhibiting hydroxyl groups were silanised using carboxyethylsilanetriol (CTES) to create

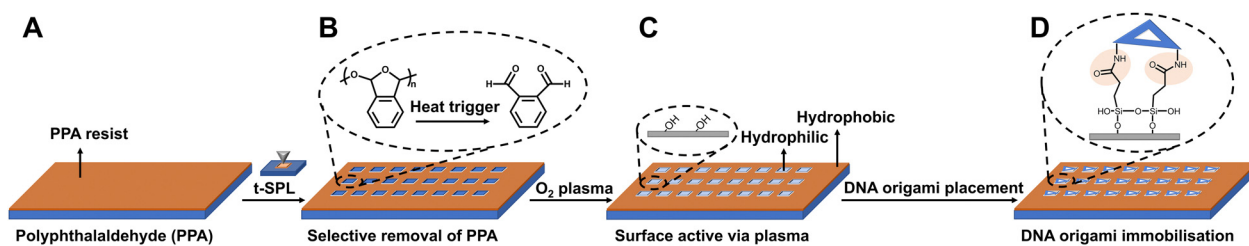


Fig. 2 Schematic of the t-SPL patterning and DNA origami placement process. (A) Polyphthalaldehyde (PPA) spin coating on the silicon substrate; (B) selective removal of PPA via t-SPL; (C) oxygen plasma for removal of PPA in nanoapertures and activation of the surface; (D) activated surface functionalised with carboxyl group via silanisation, and covalent binding with amino-modified DNA origami with the aid of EDC and NHS.

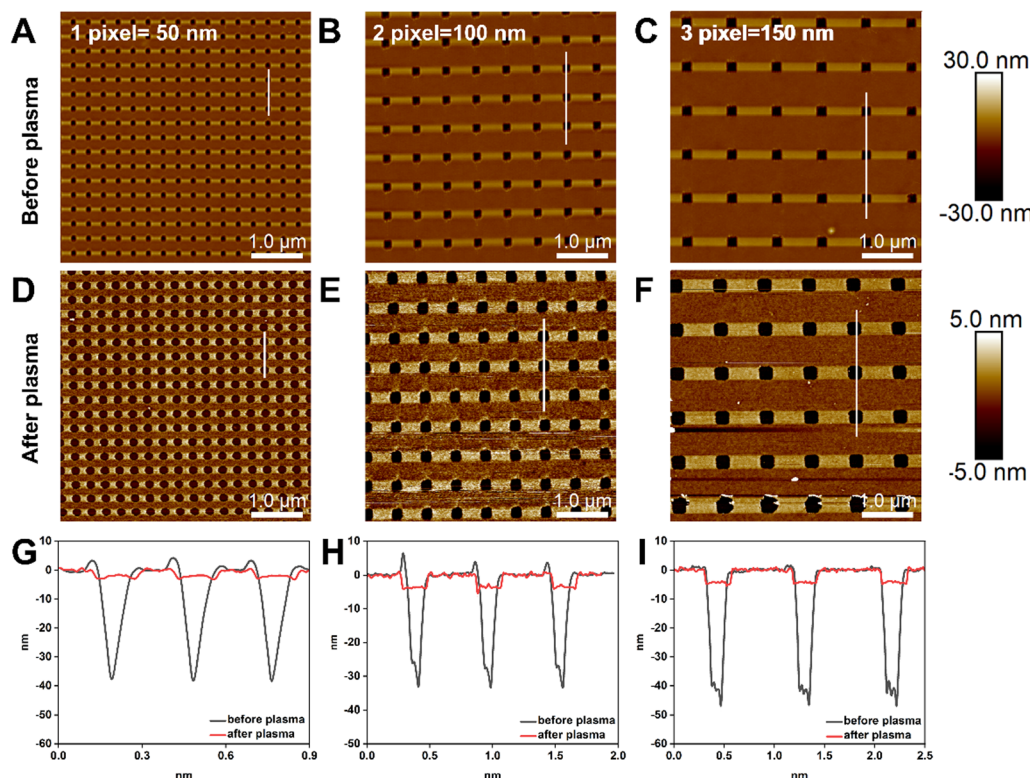


Fig. 3 AFM topographical images and height profiles of nanoapertures activation and enlargement via oxygen plasma etching. (A)–(C) t-SPL patterning nanoaperture nanoarrays with 1-pixel, 2-pixel and 3-pixel, respectively. The resolution of per pixel is 50 nm. (D)–(F) Show each pattern after 60 seconds oxygen plasma leading to apertures of approximately 180 nm, 250 nm, and 300 nm. (G)–(I) AFM height profiles showing the depth and width change of the nanoapertures in each pattern (white lines in A–F), before (black line) and after (red line) oxygen plasma.



carboxylic groups for subsequent immobilisation of amino-terminated DNA Origami, *via* amidation. Fifteen amino groups were introduced onto the inner edges of the triangular DNA origami as binding anchors; this allowed the amino DNA origami to bind covalently to the carboxylic substrates *via* EDC/NHS coupling (see the ESI† for details, and Fig. 2D and Fig. S5A, ESI†). This covalent binding strategy can be successfully achieved on various substrates, such as silicon, silicon dioxide and ITO glass as we show in Fig. S5B (ESI†).

The relationship between the size of the nanoapertures before and after plasma treatment was investigated, as nanoapertures could be activated and enlarged through oxygen plasma etching. To optimise the ideal nanoaperture size for single DNA origami placement, we set the resolution of t-SPL to 50 nm per pixel and patterned each nanoaperture in a size equivalent to one, 2- and 3-pixels. Fig. 3A–C show the patterning results, as imaged and analysed *via* AFM: highly uniform nanoarray apertures were obtained, with diameters of 50 nm, 100 nm, and 150 nm, for the aforementioned one, 2- and 3-pixels experiments, respectively. After oxygen plasma, the size of the nanoapertures increased to approximately 180 nm, 250 nm, and 300 nm, (Fig. 3D–I).

We further proceeded to covalently tether DNA origami onto each activated nanoapertures of varying sizes, in order to confirm the optimal size for single DNA origami placement. DNA origami solutions were dropping cast on the nano-patterned surfaces and imaged *via* AFM in air. Fig. 4A shows *via* AFM imaging- that the 180 nm nanoapertures were the optimal ones for the binding of a single DNA origami per hole (the size of DNA origami is around 120 nm, as shown in Fig. 1A). Differently, the 250 nm and 300 nm nanoapertures lead to the immobilisation of multiple DNA origami per nanoaperture (Fig. 4B and C). The yield of at least one DNA origami immobilisation per nanoaperture was found to be of  $68 \pm 17\%$  (based on 152 nanoapertures), with  $58.8 \pm 13.6\%$  single occupancy, for the 180 nm nanoapertures. Differently, the 250 nm nanoapertures exhibited an occupancy of at least one DNA origami with a yield of  $96 \pm 4\%$  (59 nanoapertures), but only  $13.6 \pm 3.8\%$  showed single occupancy. The 300 nm nanoapertures displayed  $93.3 \pm 11.5\%$  (71 nanoapertures) immobilisation of at least one DNA origami, with only  $11.3 \pm 17.9\%$  achieving single occupancy. These results are shown in Fig. S6 (ESI†).

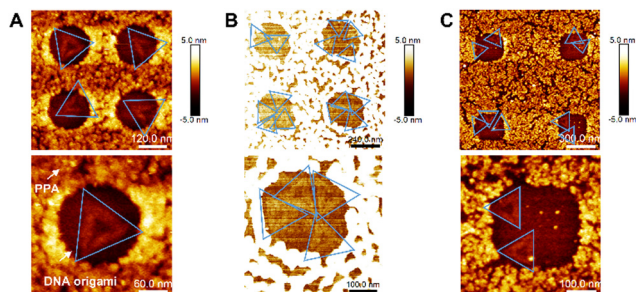


Fig. 4 AFM topographical images of DNA origami placement on nanoapertures. (A) Single DNA origami binding in 180 nm nanoapertures; (B) multiple DNA origamis binding in 250 nm nanoapertures; (C) multiple DNA origamis binding in 300 nm nanoapertures.

We further extended the nanopatterning strategy employed here, to the direct placement of DNA origami into nanoarrays. Fig. 5 demonstrates the successful assembly of DNA origami with a single AuNP1 (Fig. 5A and B) and multiple nanoparticles (AuNP1 and QD, Fig. 5C and D) on different sizes of nanoapertures (180 nm and 250 nm) in arrays. Analysis of the immobilisation yields of DNA origami functionalised with individual (AuNP 1) and multiple (AuNP 1 and QD) nanoparticles (NPs) is shown in Fig. 5E. Compared to unmodified DNA origami, the immobilisation yields of at least one NP(s)-functionalised DNA origami on both 180 nm and 250 nm nanoapertures decreased in all cases (Fig. 5E). For the 180 nm nanoapertures, the yield showed no significant change, remaining at  $68 \pm 6.4\%$  (61 nanoapertures) for DNA origami functionalized with AuNP 1 only, and  $75.3 \pm 13.5\%$  (111 nanoapertures) for multiple NPs-DNA origami architectures (*i.e.* DNA origami with both AuNP 1 and QD). On 250 nm nanoapertures the yield of immobilisation of at least one NP(s)-functionalised DNA origami decreased from  $96 \pm 4\%$  to  $69.3 \pm 17.24\%$  (48 nanoapertures) for DNA origami functionalised with a AuNP 1 only, and down to  $61.2 \pm 12\%$  (104 nanoapertures) for multiple NPs-DNA origami constructs. This observed decrease in immobilisation efficiency is

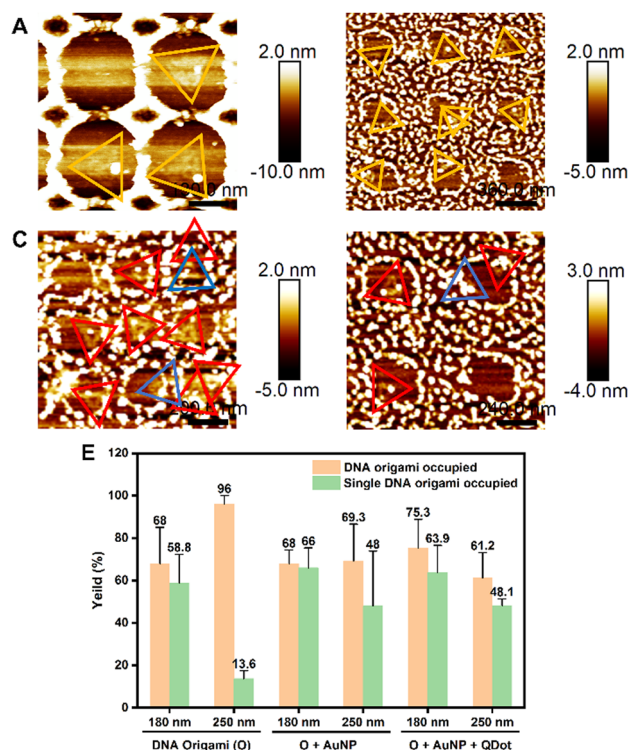


Fig. 5 AFM images of nanoparticle-functionalised DNA origami immobilised on nanoapertures. (A) DNA origami with AuNP 1, immobilised in 180 nm nanoapertures; (B) DNA origami with AuNP1, immobilised in 250 nm nanoapertures; yellow triangle frames indicate DNA origami with AuNP 1; (C) DNA origami with AuNP1 and QD, immobilised in 180 nm nanoapertures; (D) DNA origami with AuNP1 and QD immobilised in 250 nm nanoapertures. Blue triangle frames indicate incomplete functionalised DNA origami (only one or no nanoparticle), while red triangle frames indicate DNA origami with multiple nanoparticles. (E) Analysis of DNA origami immobilization yields for 180 nm and 250 nm nanoapertures.



likely due to the multiple binding sites on each nanoparticle, which may lead to aggregation of DNA origami/nanoparticles in solution, reducing the concentration of individual DNA origami.

Nevertheless, single DNA origami assembly efficiency did not decrease significantly on 180 nm nanoapertures: from  $58.8 \pm 13.6\%$  to  $66 \pm 9.4\%$  in DNA origami-AuNP 1, while multiple NPs-functionalised DNA origami exhibited a yield of single DNA origami occupancy of  $63.9 \pm 12.73\%$ . Notably, on 250 nm nanoapertures the yield of single DNA origami occupancy improved, going from  $13.6 \pm 3.8\%$  to  $48 \pm 25.9\%$  for DNA origami-AuNP 1, and  $48.1 \pm 3.2\%$ , multiple NPs-functionalised DNA origami (Fig. 5E). The increase in single occupancy yields in 250 nm nanoapertures may be due the increase in size for DNA origami-nanoparticle/s hybrids, making them more suitable for the 250 nm nanoapertures, preventing another DNA origami from entering the same nanoaperture. Another reason could be the decrease in concentration of individual DNA origami in the overall solution, caused by the aggregation of DNA origami/nanoparticle complexes. This aggregation reduces the likelihood of multiple DNA origami appearing in the same nanoaperture. Fig. S7 (ESI<sup>†</sup>) show additional representative AFM images of AuNP 1-functionalised DNA origami (Fig. S7A and B, ESI<sup>†</sup>) and multiple nanoparticle-functionalised DNA origami with AuNP 1 and QD immobilised in 180 nm and 250 nm nanoapertures (Fig. S7C and D, ESI<sup>†</sup>).

## 4. Conclusions

In this work we report a strategy for the fabrication of versatile platforms capable of assembling individual nanoscale moieties with precise single-molecule control in array configurations. As a proof of concept, we employed DNA origami functionalised with QDs and AuNPs as modular components, while t-SPL was utilised to pattern nanoapertures arrays for individual DNA origami placement. Following covalent binding aided by carboxyl silanisation on silicon substrates, we systematically investigated the yield of individual DNA origami occupancy per nanoaperture as a function of the parameters employed in the nanopatterning that directly relate to the size of the apertures -from 180 nm to 300 nm- to the yield of placement of 120 nm DNA origami functionalised with QDs and AuNPs. In this way, we demonstrated a high degree of control in the directed assembly in nanoarray configuration of DNA origami functionalised with distinct nanoparticles. Future investigations will likely explore how to better control the number of DNA nanostructures per aperture and their orientation. The methodology presented here, and the findings reported, are of interest for the high-throughput and high-yield construction of single-molecule nanoarrays; these in turn have applications in a variety of fields from information technology to photonics and biomedicine.

## Data availability

Data for this article, including DNA sequences, experimental nanopatterning and functionalisation procedures, and materials are available in the ESI<sup>†</sup> of the article

## Conflicts of interest

There are no conflicts to declare.

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