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MXene-derived Potassium Titanate Nanoribbons Decorated Electrode Architecture for Detection of Ciprofloxacin: A Multipurpose Sensing Platform Development

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Abstract

Recent studies have highlighted the promise of MXene-derived titanate nanoribbons (KTNR) as electrode materials for electrochemical sensing applications. This work investigates the electrochemical activity of potassium titanate nanoribbons synthesized from MXene for the development of a voltammetric sensor for ciprofloxacin detection. The sensor offers a sustainable approach for ciprofloxacin quantification, addressing critical needs in food safety, environmental monitoring, and healthcare diagnostics, ultimately contributing to the United Nations' Sustainable Development Goals by mitigating antimicrobial resistance and supporting the One Health initiative. To initiate the experiments, the structural, stability/energetics, and electronic features of two dimer complexes, KTNR/ciprofloxacin and MXene/ciprofloxacin, have been computationally inspected using two in-silico tools, and some important electronic parameters such as binding energy, HOMO-LUMO gap, dipole moment show that the former one (KTNR) is significantly more sensitive than the MXene with the ciprofloxacin. 2D Ti₃C₂ MXene served as the precursor for the synthesis of potassium titanate nanoribbons. X-ray diffraction (XRD), field emission scanning electron microscopy (FESEM), high-resolution transmission electron microscopy (HRTEM), selected area electron diffraction (SAED),

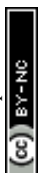


30 elemental mapping, and energy-dispersive X-ray spectroscopy (EDX) techniques were
31 employed to confirm the crystallinity, surface morphology, and layered structure of the
32 synthesized nanoribbons. The electrochemical and sensing properties of the materials were
33 further evaluated using cyclic voltammetry (CV), differential pulse voltammetry (DPV), and
34 electrochemical impedance spectroscopy (EIS). Subsequently, the nanoribbons were deposited
35 onto a glassy carbon electrode (GCE) surface. The electro-oxidation behaviour of ciprofloxacin
36 was then investigated using CV, DPV, and square wave voltammetry (SWV) in an optimized
37 0.1 M phosphate buffer solution (pH 8). The developed sensor exhibited a remarkable linear
38 detection range of 0.6 μM ($\approx 0.03 \mu\text{g mL}^{-1}$) to 147.2 μM ($\approx 7.18 \mu\text{g mL}^{-1}$) for ciprofloxacin.
39 Additionally, the limit of detection (LOD) achieved was 0.07, 0.0608, and 0.0264 μM for CV,
40 DPV, and SWV, respectively. Notably, the electrodes demonstrated excellent selectivity
41 towards ciprofloxacin detection in complex matrices, including marine water, river water,
42 agricultural soil, organic fertilizer, milk, honey, poultry eggs, and simulated body fluids.

43 **Keywords:** MXene derivative, Potassium titanate nanoribbons, electrochemical sensor,
44 ciprofloxacin, healthcare monitoring, food and environmental safety.

46 1. Introduction

47 Ciprofloxacin is a double-edged sword. While it's a crucial antibiotic, its overuse and presence
48 in the environment and food contribute significantly to the global antimicrobial resistance
49 (AMR) crisis. It's an antibiotic with the ability to inhibit bacterial DNA gyrase. It is used to
50 treat humans against a variety of bacterial infections, including urinary tract infections,
51 respiratory tract infections, skin infections, and certain sexually transmitted diseases. It is also
52 evident, that like the other broad-spectrum fluoroquinolone group of antibiotics, ciprofloxacin
53 is also predominantly effective in growth promotion and treating several deadly infections in
54 animal husbandry, including cattle farms, poultry farms, fisheries, and apiculture. However,
55 overuse and misuse of antibiotics like ciprofloxacin are responsible for the development of
56 (AMR). The relationship between AMR and ciprofloxacin lies in the selective pressure exerted
57 by the widespread use of this antibiotic. When bacteria are exposed to ciprofloxacin, some of
58 them may possess genetic mutations or acquire resistance genes that enable them to survive the
59 antibiotic's effects. Through natural selection, these resistant bacteria can then proliferate and
60 spread, leading to the emergence of ciprofloxacin-resistant strains. Ciprofloxacin-resistant
61 bacteria pose a significant challenge. Infections caused by them become more difficult to treat,
62 requiring stronger antibiotics, alternative therapies, and precision dosing through therapeutic



63 drug monitoring. This can lead to longer hospital stays, increased healthcare costs, and even
64 higher mortality rates¹⁻⁹.

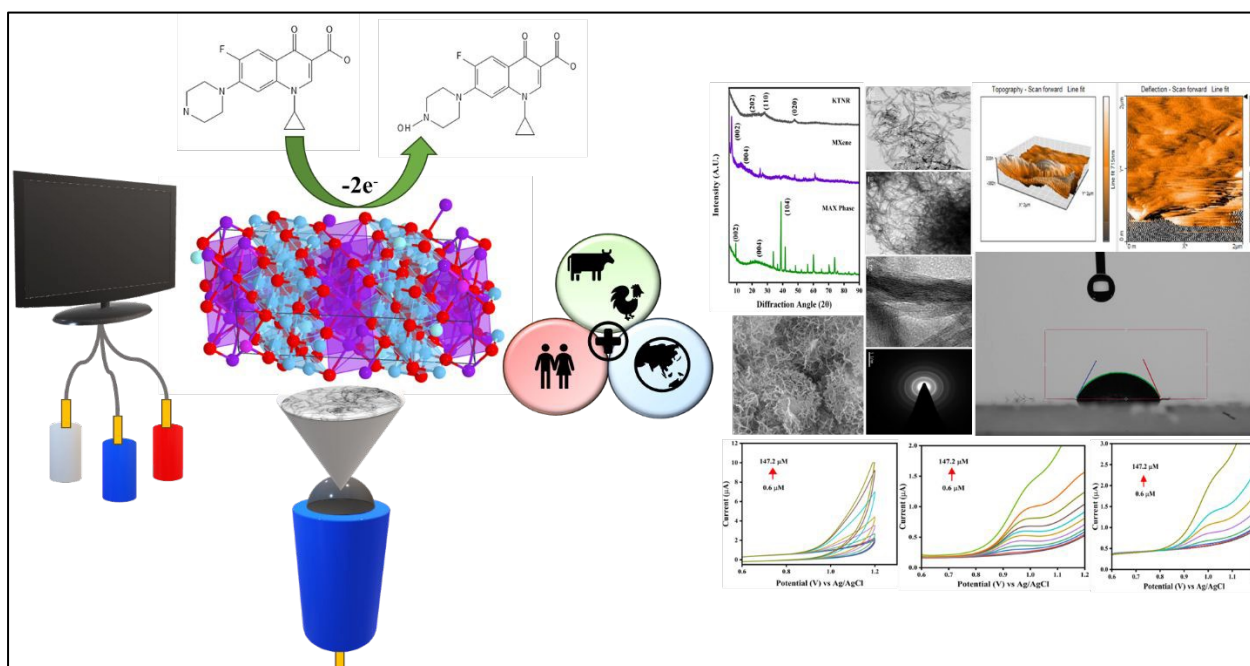
65 The WHO reports show variations, but ciprofloxacin resistance in bacteria like *E. coli* and
66 *Klebsiella pneumonia* can range from 4% to 93% across countries¹⁰. This highlights the
67 growing global problem. Traces of ciprofloxacin can end up in rivers and marines through
68 wastewater. Studies suggest even low concentrations of ciprofloxacin in the environment can
69 promote AMR in *E. coli* present there. In brief, it can affect the whole marine and freshwater
70 ecosystem. Through the food chain, the resistant bacteria and the antibiotic residues enter to
71 human system, even animal-based foods like eggs, meat, milk, and honey also contain
72 ciprofloxacin residues. This further significantly complicates the same global challenges¹¹⁻¹⁶.

73 As a diagnostic analytical approach to measuring the concentration of different bio-
74 analytes^{17,18} and antibiotics¹⁹⁻²³, specifically ciprofloxacin, several versatile and efficient
75 analytical tools have been developed like ultra-high performance liquid chromatography-mass
76 spectrometry, quadrupole time of flight mass-spectroscopy, liquid chromatography-mass
77 spectrometry, which are recognized as a gold standard tool to measure ciprofloxacin
78 concentration in food (viz. milk, eggs, meat, fish, honey), environmental (wastewater, river and
79 marine water, agricultural soils, organic fertilizers), and biomedical (viz. body fluids like blood
80 serum, urine) samples²⁴. Though these tools are highly reliable, sensitive, and efficient in
81 measuring a wide concentration range; due to the high expenditure, and maintenance these
82 techniques are unable to be installed in resource-limited settings. In this context, the
83 development of alternative versatile technology is highly required to measure ciprofloxacin
84 concentration in various real matrices. Thus, a cost-effective electrode material has been
85 reported (**as shown in Scheme. 1**) by using MXene-derived potassium titanate nanoribbons.
86 Here, the electro-catalysis of ciprofloxacin has been demonstrated as a fundamental
87 mechanistic approach.

88 In our study, we have already explored the potential of novel nanoribbons derived from
89 MXene (titanium carbide) as an electrochemical sensing platform to provide food safety. These
90 nanoribbons possess several unique characteristics that make them ideal for this application.
91 Firstly, they possess an intrinsic ability to amplify signals within the material itself, eliminating
92 the need for separate amplifiers. They exhibit exceptional stability over the time, ensuring
93 reliable performance, and demonstrated high sensitivity toward analytes crucial for food safety,
94 as reported by Mini and Raghavan (2024)²⁵. The specific structure of these nanoribbons, with
95 their layered morphology and abundant hydroxyl groups on the surface, provides a large



96 surface area, making them well-suited for ciprofloxacin detection. In addition to that, the
 97 presence of polar bonds in ciprofloxacin is due to the electronegativity difference between the
 98 atoms involved in its chemical structure. Here, the presence of polar bonds leads to an uneven
 99 distribution of electron density within the molecule, resulting in regions of partial positive and
 100 partial negative charge. This polarity allows ciprofloxacin to interact with other polar
 101 molecules or ions, which is important for its mechanism of action as an antibiotic and for its
 102 solubility in aqueous environments, as well as facilitating its electrocatalytic behaviour^{1–3,25–33}.
 103 Interestingly, our research shows that ciprofloxacin, a molecule with polarity, triggers a
 104 decrease in the resistance of these nanoribbons during the catalytic events. This finding
 105 contributes to a deeper understanding of electrochemical sensing mechanisms that exploit
 106 proton conduction. Our work highlights the promise of this electrocatalytic approach for
 107 achieving ultra-low limits of ciprofloxacin detection with exceptional selectivity even in
 108 different real and complex matrices. These are again related to ciprofloxacin sensing for food
 109 and environmental safety along with biomedical purposes like therapeutic drug monitoring
 110 (TDM).



112
 113 **Scheme 1. Schematic illustration of KTNR fabricated multi-purpose electrochemical**
 114 **sensor for ciprofloxacin detection.**

115
 116 **2. Experimental Section**

117 **2.1. Computational Methodology**



118 Computational tools have imperative role in understanding and unraveling the quantum (atomic
119 and molecular) level features. Due to the large size of both dimer complexes (KTNR-
120 ciprofloxacin and MXene-ciprofloxacin) consisting of a large number of heavy metals (like K
121 and Ti in the KTNR and Ti in the MXene), the calculations demanded high computational
122 costing. The optimization and frequency calculations have been executed using the
123 semiempirical approach however, an ab-initio, Hartree-Fock (HF) functional and 6-31G basis
124 set have been used for single point calculations for the F, O, N, C, N, H, and K atoms and SDD
125 for the Ti (transition metal) atom. Since, by keeping the experimental facets, this report
126 discusses some important geometry, energetic/stability, and electronic parameters using
127 molecular modelling and electronic feature analyses in the framework of semiempirical and
128 ab-initio modeling approaches. All quantum chemical calculations have been executed using
129 the immensely used Gaussian 09 electronic structure calculations package ³⁴

130 2.2. Reagents and Equipments

131 Ciprofloxacin ($\geq 99.0\%$; pharmaceutical secondary standard), enrofloxacin ($\geq 99.0\%$),
132 norfloxacin ($\geq 98\%$, TLC), ofloxacin ($\geq 98\%$; Pharmaceutical Secondary Standard), nafion, uric
133 acid ($\geq 99\%$, crystalline), urea (99.0-100.5%, ACS reagent), dopamine hydrochloride ($\geq 98\%$;
134 Pharmaceutical Secondary Standard), diclofenac sodium ($\geq 98\%$; Pharmaceutical Secondary
135 Standard), D-glucose ($\geq 99.5\%$ - GC, BioXtra), 48% hydrofluoric acid ($\geq 99.99\%$ trace metals
136 basis), Titanium aluminium carbide MAX phase (910775; $\geq 90\%$, $\leq 40 \mu\text{m}$ particle size), and
137 ascorbic acid ($\geq 98\%$; Pharmaceutical Secondary Standard) were purchased from Sigma
138 Aldrich, India. Other supporting reagents were procured from SD Fine Chemicals, Mumbai,
139 India; Avra Synthesis Pvt. Ltd. India. All the chemicals were used without any further
140 purification. 0.1 M NaH_2PO_4 and 0.1 M Na_2HPO_4 were used to prepare a phosphate buffer
141 solution with the required pH.

142
143 Powder X-ray diffraction (XRD) (Bruker D8 Advance, Panalytical X Pert3, Germany,
144 Netherlands), field emission scanning electron microscopy (FE-SEM), and energy-dispersive
145 X-ray analysis (EDAX) (Thermo Fisher, FEI QUANTA 250 FEG), high-resolution
146 transmission electron Microscope (HR-TEM) and selected area electron diffraction (SAED)
147 (FEI –TECNAI, G2-20 TWIN - Operating voltage 200 kV) have been used to characterize
148 materials and provided the high-resolution images of the internal structures of the active
149 electrode material, including details of its crystal lattice, atomic arrangements, and defects
150 down to the atomic level. The CHI 660C electrochemical workstation has been used for all



151 electrochemical measurements including cyclic voltammetry (CV), differential pulse
152 voltammetry (DPV), square wave voltammetry (SWV), and electrochemical impedance
153 spectroscopy (EIS). The fabricated electrode surfaces were characterized by the atomic force
154 microscope (Nanosurf AFM, Nanosurf, Switzerland), surface profilometer (Marsurf XR20,
155 Mahr), wettability test (contact angle metre HO-IAD-CAM-01A, HOLMARC). Throughout the
156 experiments, 0.3 μm alumina slurry was used to polish the active surface of glassy carbon
157 electrodes (GCE) to make it used as a working electrode, while Ag/AgCl (3 M KCl) and
158 platinum wire performed as a reference and counted electrode in a three-electrode system.

160 2.3. Synthesis of MXene and MXene-derived Potassium Titanate Nanoribbons (KTNR)

161 MXene was synthesized by the priorly optimized HF etching of the MAX phase and
162 delaminated by DMSO^{35,36}. Potassium titanate nanoribbons (KTNR) were synthesized via a
163 well-established methodology employing MXene as the precursor³⁷. In the initial stage, 100
164 mg of MXene was incorporated into a mixture comprised of 30 mL of 1 M KOH solution and
165 0.68 mL of 30% H₂O₂. This resultant mixture was subsequently transferred to a 50 mL Teflon-
166 lined stainless-steel autoclave. The autoclave underwent hydrothermal treatment at 150°C for
167 a duration of 16 hours, facilitating the transformation of MXene into KTNR. Following natural
168 cooling of the autoclave to ambient temperature, the uppermost layer, containing a white
169 suspension, was isolated using vacuum filtration. The obtained KTNR sample was then
170 subjected to rigorous washing with deionized (DI) water and ethanol to eliminate any residual
171 byproducts from the reaction. Finally, the purified KTNR was desiccated in an oven at 60°C
172 for 12 hours to remove any remaining solvent molecules^{25,38,39}.

174 2.4. Preparation of complex matrices

175 The performance of the fabricated KTNR electrochemical sensor was evaluated in various real-
176 world matrices with clinical significance for trace ciprofloxacin detection. These matrices
177 included simulated body fluid (SBF) to mimic physiological conditions and animal-derived
178 food samples (honey, milk, and eggs) obtained from local markets in Kerala and Tamil Nadu,
179 India. Environmental water samples were also tested, encompassing river water (Ganga) and
180 marine water (Bay of Bengal) collected from West Bengal, India. Additionally, agricultural
181 soil and organic fertilizer were analyzed, and sourced from local agricultural fields and farms
182 in Vellore, India.



183 A standardized sample preparation procedure was employed for food and environmental
184 samples. Briefly, samples were homogenized and filtered using a 0.22 μm nylon filter.
185 Subsequently, they underwent a 10-fold dilution with phosphate buffer (pH 8) before being
186 spiked with ciprofloxacin to achieve a concentration (including 15 μM). For agricultural
187 samples, 1 g of the solid material was ultrasonicated in 10 ml of deionized (DI) water, followed
188 by centrifugation at 3000 rpm for 10 minutes. The resulting supernatant was collected, filtered
189 with a 0.22 μm nylon filter, diluted 10-fold with phosphate buffer (pH 8), and spiked with
190 ciprofloxacin to reach a final concentration of 15 μM .

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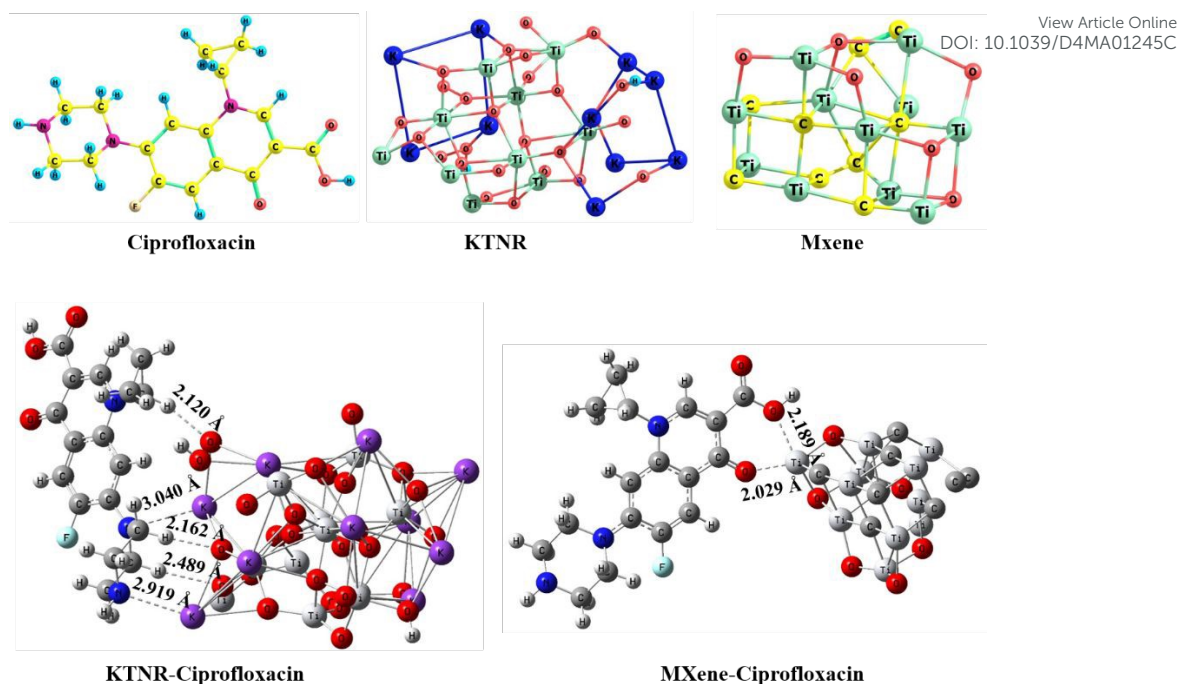
193 3. Results and Discussions

194 3.1. Computational Studies

195 Comprehensive computational studies on the structural, stability/energetic, and electronic
196 features of a variety of molecular systems can be viewed in the reports along with biomaterials
197 ^{40,41}. All optimized structures (monomer constituents and dimer complexes) are shown in
198 **Figure 1**. Here in this report, a few chosen structural/geometrical parameters (particularly, the
199 bond distance between the atoms of two interacting monomer constituents) had been calculated
200 for both dimer complexes (KTNR/Ciprofloxacin and MXene/Ciprofloxacin) which are shown
201 in **Figure 1**. Having a look into the first case as the KTNR/Ciprofloxacin dimer complex, a
202 total of five nonbonding interactions between two components (KTNR and Ciprofloxacin)
203 were shown in the dotted line. The bond lengths of the two K---N (3.040 Å and 2.919 Å) and
204 three weak C-H---O (2.120 Å, 2.162 Å, and 2.489 Å) H-bonding interactions involved in the
205 KTNR/Ciprofloxacin dimer complex can be seen in **Figure 1**. However, only two metal-
206 nonmetal interactions (Ti---O) could be discerned for the MXene-Ciprofloxacin dimer complex
207 whose bond lengths are 2.029 Å and 2.189 Å. The structural parameters appeared to indicate
208 that the former one (KTNR/Ciprofloxacin) could be structurally more favorable than the latter
209 one (MXene/Ciprofloxacin).

210





211
212 **Figure 1. Optimized Structures of the Monomer Constituents (ciprofloxacin, KTNR, and**
213 **MXene) and Dimer Complexes (KTNR-ciprofloxacin and MXene-ciprofloxacin).**

214 In order to inspect the sensitivity/binding feature (also, linked to the structural features)
215 of both dimer complexes (KTNR-ciprofloxacin and MXene-ciprofloxacin), the binding
216 energies (BEs) had been analyzed which can be seen in **Table 1**⁴². The semiempirical approach
217 (PM6) showed that the BE of the KTNR-ciprofloxacin complex (254.6 kcal/mol) was found to
218 be five times greater than that of the MXene-ciprofloxacin complex (-50.6 kcal/mol). Very
219 importantly and notably, the HF/6-31G method also showed that the BE of the former one (-
220 501.8 kcal/mol) was found to be 5.4 times stronger than that of the latter one (-92.7 kcal/mol).
221 Such BE-based findings clearly demonstrated that the KTNR was more sensitive than the
222 MXene with the ciprofloxacin which also supports to the experiment-based outcomes in the
223 later part of research.

224

225 **Table 1. Some Important and Chosen Electronic Parameters of the KTNR-Ciprofloxacin**
226 **and MXene-Ciprofloxacin Dimer Complexes**

System	KTNR-ciprofloxacin	MXene-ciprofloxacin
BE (PM6)	-254.6 kcal/mol	-50.6 kcal/mol
BE [HF (SP)/6-31G]	-501.8 kcal/mol	-92.7 kcal/mol



HOMO	-5.480	-5.818	View Article Online DOI: 10.1039/D4MA01245C
LUMO	-0.610	0.250	
E_{Gap}	4.87	5.568	
Dipole Moment	32.1	23.8	
Natural Charge (e)	KTNR (0.023e) and ciprofloxacin (-0.023e)	MXene (0.415e) and ciprofloxacin (-0.415e)	

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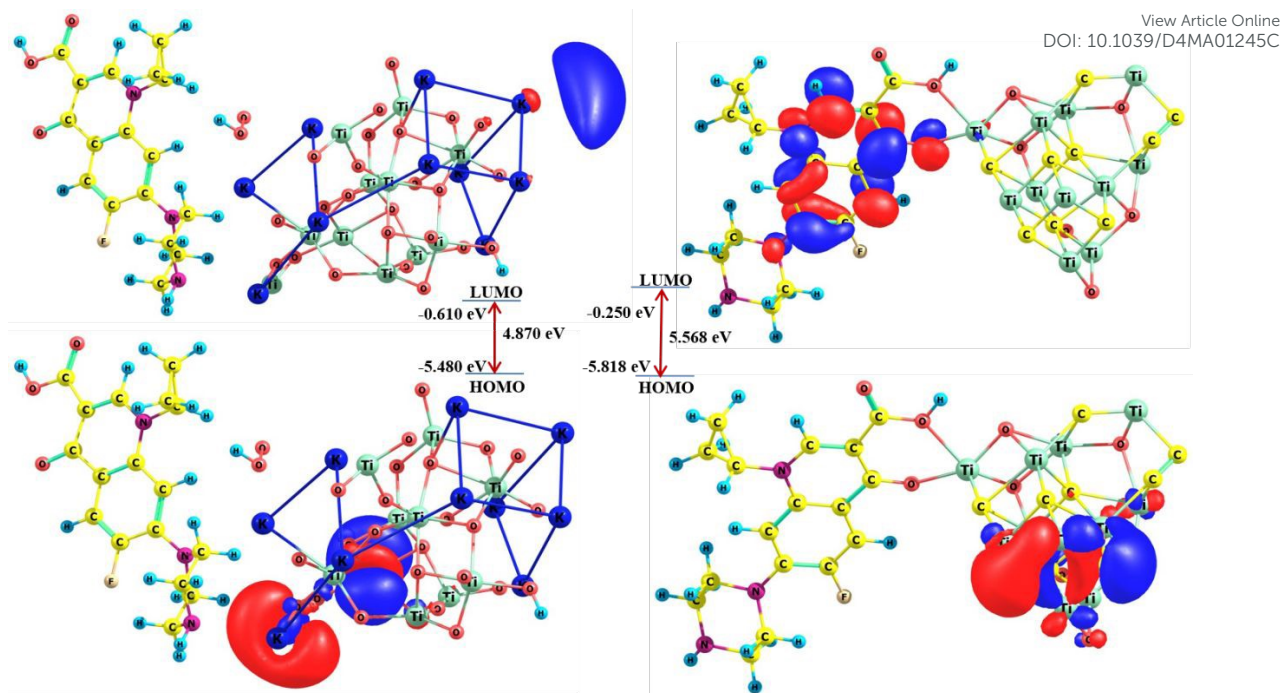
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244

Moreover, as the Frontier molecular orbitals (FMOs), like highest occupied molecular (HOMO) and lowest unoccupied molecular orbital (LUMO), and the associated HOMO-LUMO energy gap (E_{Gap}) being useful diagnostics of showing the sensitivity/reactivity features, such parameters (HOMO, LUMO, and E_{Gap}) had been probed. A system having low E_{Gap} value showed that the system was more sensitive/chemically reactive. The E_{Gap} of both KTNR-ciprofloxacin and MXene-ciprofloxacin complexes had been detected as 4.87 eV and 5.568 eV, respectively which further validated that the former one was more sensitive than the latter one. Interestingly, a system consisting of a large dipole moment (DM) indicated it's more sensitivity/chemical reactivity. Here, in this report the DMs of the KTNR- and MXene-based complexes were computed as 32.1 Debye (D) and 23.8 D which also assured about the more sensitivity of the former one. Additionally, the natural charges on each monomer constituents of both dimer complexes have been examined and it was found that the ciprofloxacin consisted of negative charge (-0.023e) and KTNR had a positive charge (+0.023e). A similar trend can be viewed in the case of the MXene-ciprofloxacin complex where a significant large charge difference (MXene: +0.415e and ciprofloxacin: -0.415e) was therein. Such findings illustrate that the charge transfer (CT) took place from KTNR/MXene to the ciprofloxacin component.





245
 246 **Figure 2. The three-dimensional (3D) HOMO-LUMO Isosurface Maps of the Dimer**
 247 **Complexes (left: KTNR-ciprofloxacin and right: MXene-ciprofloxacin) (bottom: HOMO**
 248 **and top: LUMO).**

249 Finally, the FMOs such as HOMO, LUMO, and single-occupied molecular orbital
 250 (SOMO) have had a significant role in electronic transition phenomenon⁴³. The HOMO of the
 251 KTNR-ciprofloxacin complex was distributed over only some of the Ti-metals of the KTNR
 252 component whereas importantly, a SOMO appeared to be located near a single K-metal atom.
 253 Very interestingly, the HOMO of the MXene-ciprofloxacin was spread over the some of the
 254 Ti-C bonds while the LUMOs were revealed to distributed over the C-atoms of two benzene
 255 rings which demonstrated to show π to π^* transition.

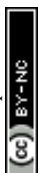
256 3.2. XRD Analysis

257 The XRD pattern in the image is consistent with the conversion of Ti_3AlC_2 MAX Phase to
 258 $\text{Ti}_3\text{C}_2\text{T}_x$ MXene followed by conversion to KTNR (**Fig. 3(A)**). The presence of a high-intensity
 259 peak of the precursor Ti_3AlC_2 MAX phase at an angle of $2\theta = 38.9^\circ$ at (104) signifies elemental
 260 Al. After being etched with HF, the layers become more separated and the peak (104)
 261 disappears which denotes the removal of Al. The diffraction peaks at (002), and (004) were
 262 assigned for $\text{Ti}_3\text{C}_2\text{T}_x$ MXene. This increases the d-spacing of the (002) peak, which can be
 263 observed as a shift of the peak to a lower angle in the XRD pattern⁴⁴. The successful synthesis
 264 of delaminated Mxene was followed by hydrothermal synthesis of KTNR.



265 To comprehend the structure in details, $K_2Ti_4O_9$ crystallizes in the monoclinic $C2/m$ space
266 group⁴⁵. There are two inequivalent K^{1+} sites. In the first K^{1+} site, K^{1+} is bonded in a 8-
267 coordinate geometry to eight O^{2-} atoms. There are a spread of K-O bond distances ranging
268 from 2.78-3.01 Å. In the second K^{1+} site, K^{1+} is bonded in a 6-coordinate geometry to six O^{2-}
269 atoms. There are a spread of K-O bond distances ranging from 2.68-3.08 Å. There are four
270 inequivalent Ti^{4+} sites. In the first Ti^{4+} site, Ti^{4+} is bonded in a 6-coordinate geometry to six
271 O^{2-} atoms. There are a spread of Ti-O bond distances ranging from 1.76-2.27 Å. In the second
272 Ti^{4+} site, Ti^{4+} is bonded to six O^{2-} atoms to form a mixture of distorted corner and edge-sharing
273 TiO_6 octahedra. The corner-sharing octahedral tilt angles are 32°. There are a spread of Ti-O
274 bond distances ranging from 1.77-2.22 Å. In the third Ti^{4+} site, Ti^{4+} is bonded in a 6-coordinate
275 geometry to six O^{2-} atoms. There are a spread of Ti-O bond distances ranging from 1.73-2.35
276 Å. In the fourth Ti^{4+} site, Ti^{4+} is bonded to six O^{2-} atoms to form a mixture of distorted corner
277 and edge-sharing TiO_6 octahedra. The corner-sharing octahedral tilt angles are 30°. There are
278 a spread of Ti-O bond distances ranging from 1.79-2.19 Å. There are nine inequivalent O^{2-}
279 sites. In the first O^{2-} site, O^{2-} is bonded in a distorted rectangular see-saw-like geometry to two
280 equivalent K^{1+} and two Ti^{4+} atoms. In the second O^{2-} site, O^{2-} is bonded in a distorted single-
281 bond geometry to six K^{1+} and one Ti^{4+} atom. In the third O^{2-} site, O^{2-} is bonded to two
282 equivalent K^{1+} and two Ti^{4+} atoms to form distorted OK_2Ti_2 tetrahedra that share corners with
283 two equivalents OK_2Ti_2 tetrahedra, corners with five OTi_4 trigonal pyramids, and an edge-
284 edge with one OTi_4 trigonal pyramid. In the fourth O^{2-} site, O^{2-} is bonded in a distorted
285 rectangular see-saw-like geometry to two equivalent K^{1+} and two Ti^{4+} atoms. In the fifth O^{2-}
286 site, O^{2-} is bonded in a distorted linear geometry to two equivalent K^{1+} and two Ti^{4+} atoms. In
287 the sixth O^{2-} site, O^{2-} is bonded in a 4-coordinate geometry to four Ti^{4+} atoms. In the seventh
288 O^{2-} site, O^{2-} is bonded to four Ti^{4+} atoms to form distorted OTi_4 trigonal pyramids that share
289 corners with three equivalents OK_2Ti_2 tetrahedra, corners with three OTi_4 trigonal pyramids,
290 and edges with two equivalent OTi_4 trigonal pyramids. In the eighth O^{2-} site, O^{2-} is bonded in
291 a 3-coordinate geometry to three Ti^{4+} atoms. In the ninth O^{2-} site, O^{2-} is bonded to four Ti^{4+}
292 atoms to form distorted OTi_4 trigonal pyramids that share corners with two equivalents OK_2Ti_2
293 tetrahedra, corners with three OTi_4 trigonal pyramids, an edge-edge with one OK_2Ti_2
294 tetrahedra, and edges with four OTi_4 trigonal pyramids.

295 The XRD also suggested a Monoclinic phase indexing having a Bravais lattice space group
296 $C2/m$. The unit cell had parameters $a=18.25$ Å, $b=3.791$ Å, $c=12.01$ Å, $\beta=106.4$ Å, and volume



297 \AA^3 . The diffraction angles with corresponding $h k l$ values and d -spacing was calculated as (2
298 $0\ 2$), $2\theta = 20.696$, $d = 4.2882$ nm; ($1\ 1\ 0$), $2\theta = 23.997$, $d = 3.705$ nm; ($0\ 2\ 0$), $2\theta = 47.953$, $d =$
299 1.8955 nm. There are also some unidentified peaks present in the XRD pattern, which could
300 be due to impurities or minor phases in the sample. It was evident that MXene had been
301 successfully converted to KTNR after undergoing oxidation and alkalization²⁶ considering that
302 the measured peak positions and intensities are consistent with those of JCPDS No: 32-0861
303 for $\text{K}_2\text{Ti}_4\text{O}_9$ (KTNR).

304 3.3. FESEM, EDAX, and Mapping analysis

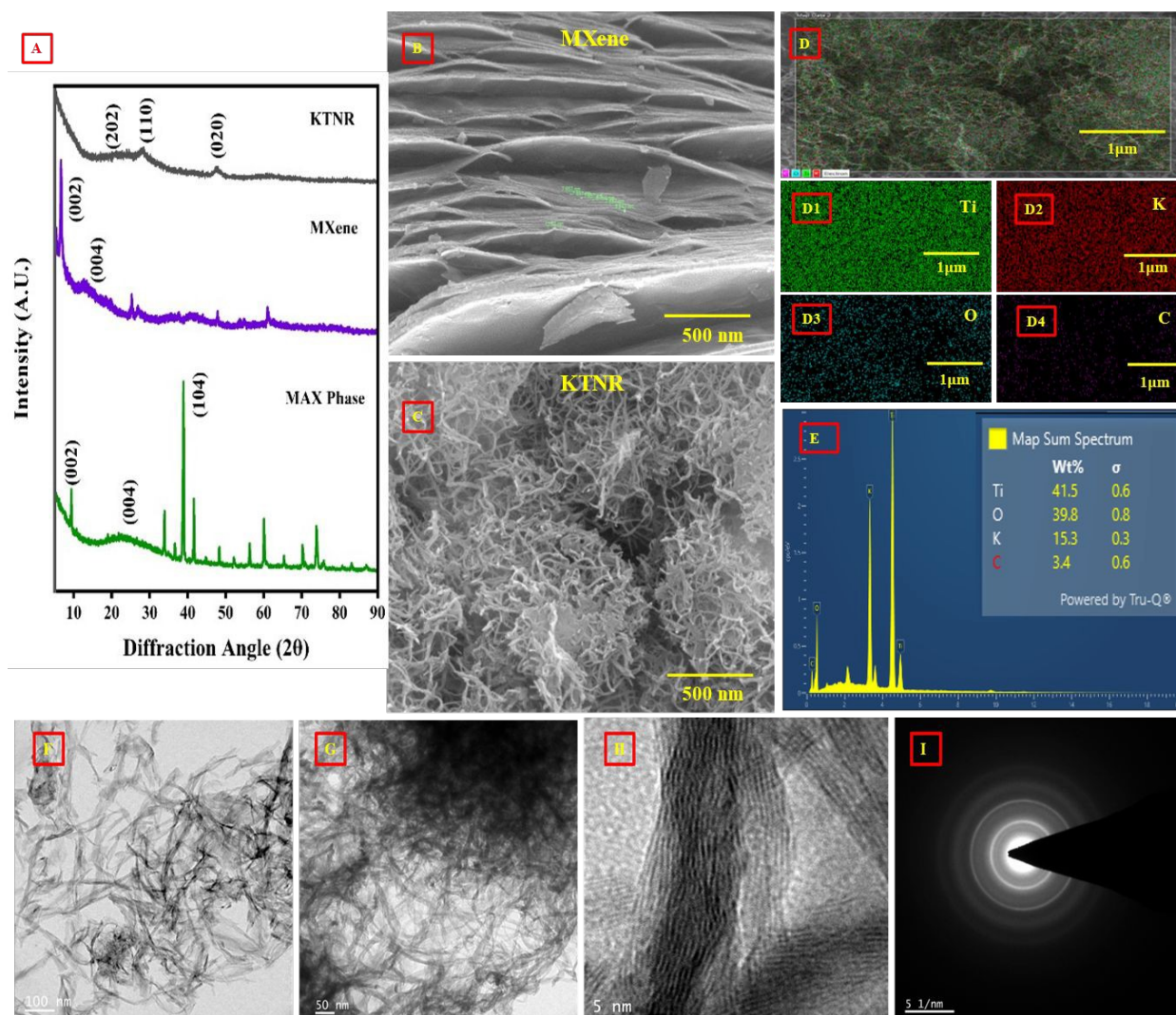
305 The surface morphology of the materials was confirmed using FESEM performed for $\text{Ti}_3\text{C}_2\text{T}_x$
306 MXene which clearly showed stacking between the multi-layered structure (**Fig. 3(B)**)⁴⁶. The
307 width of ultrafine layers corresponded to a range varying from 6.76 nm to 12.62 nm. The inter-
308 spacing between the layers ranged from 20 nm to 550. The FESEM images of KTNR depicted
309 a distinct webbed-like complex network of nanoribbons having high surface area and porosity
310 (**Fig. 3(C)**). The width/diameter of nanoribbons ranged from 9.7 nm to 16.4 nm indicating the
311 uniform morphology. Further, the EDAX and Mapping was done to obtain the atomic weight
312 distribution (Wt%) K, Ti, and O relating to 41.5 %, 39.8 % and 15.3% respectively throughout
313 the matrix correlating to successful synthesis of KTNR. The uniform abundance of all procured
314 elements K, Ti, and O (**Fig. 3(D-E)**) which makes it a perfect candidate to achieve enhanced
315 electrocatalytic activity of the nanocomposite especially due to notable presence of bimetallic
316 Potassium and Titanium in the matrix. The presence of Carbon (3.4 Wt%) as recorded in EDAX
317 was subjected probably due to some incomplete alkalization its precursor MXene.

318 3.4. HRTEM and SAED pattern analysis

319 HRTEM images further revealed the structural evolution from MXene nanosheets to KTNR
320 nanoribbons. As simultaneous oxidation and alkalization process, the KTNR was assumed to
321 have a diameter of around 10 nm (**Fig. 3(F-H)**). As shown in Fig. , HRTEM images validated
322 the ultrafine widths as low as that of ~ 2.3 nm and ultrathin thickness of ~ 1.6 nm while the
323 lattice spacings averaged at 0.745 nm. The width or thickness is comparatively lesser than that
324 of precursor Ti_3C_2 MXene and thereby demonstrating the advantages of the morphological
325 advancement in the nano-scale. Also, the HR-TEM results suggests that the KTNR exists in
326 single or few layers which is practically impossible to achieve in MXene. In a polycrystalline
327 material having monoclinic phase, the electrons will diffract at a range of angles, producing



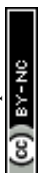
328 rings on the SAED pattern. KTNR also showed multiring SAED pattern that confirmed the
 329 polycrystalline nanostructures with distinct phases (Fig. 2(I)).



330
 331 **Figure 3.** (A) XRD analysis of KTNR, Mxene and, MAX Phase in the range of (2θ) 5-90°;
 332 FE-SEM images of (B) MXene, (C) KTNR; Elemental mapping of (D) all elemental
 333 compositions together in KTNR; Atomic distribution of (D1) Titanium, (D2) Potassium,
 334 (D3) Oxygen, and (D4) Carbon in a selected section of the matrix of KTNR; (E) EDAX
 335 spectrum of elements of K:Ti:O:C; HR-TEM of KTNR at (F) 100 nm, (G) 50 nm and, (H)
 336 5 nm scales showing different lattices including multiring SAED pattern (I) to confirm its
 337 polycrystallinity.

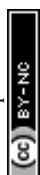
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339 3.5. Surface optical profilometry, AFM, and Contact angles

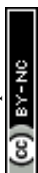


340 The **Fig. 4(A1 and A2)** showed a line profile obtained from surface profilometry, likely
341 representing the height variations along a specific line on the GCE surface. The provided data
342 likely corresponded to specific roughness parameters measured by the profilometer. The
343 roughness of the surface can influence the performance of the electrode in electrochemical
344 applications. A moderately rough surface can provide more active sites for reactions compared
345 to a flat surface. The both MXene (41319.6231 nm) and KTNR (41249.6805 nm) showed
346 similar R values, indicating comparable overall roughness across the measured profiles.
347 MXene (44811.3649 nm) has a higher M value compared to KTNR (43641.228 um). A higher
348 M value signifies more prominent height variations throughout the profile. Both materials
349 likely introduce roughness, potentially increasing the surface area for improved sensor
350 performance. MXene might have had a surface with sharper peaks and valleys compared to
351 KTNR, based on the higher M value. The width values (around 0.89 um for both) might
352 represent the width measured at a specific height threshold and may not reflect the actual width
353 of the MXene sheets or the average width of the KTNR nanoribbons. The position values
354 (around 1.56 um for both) corresponded to the location where the ASH (average surface height)
355 was measured. MXene (3491.74 nm) has a higher ASH compared to KTNR (2391.91 nm).
356 This suggested that the MXene layer sits higher on average relative to the reference plane
357 compared to the potassium titanate nanoribbons. Increased surface roughness and higher ASH
358 could be beneficial for electrochemical sensors by providing more sites for analyte molecules
359 to adsorb. This could potentially improve the sensitivity of the sensor. However, the optimal
360 surface characteristics depend on the specific target analyte and the desired electrochemical
361 process. Both MXene and KTNR appeared to introduce roughness to the GCE surface, which
362 could be advantageous for sensor applications. MXene might offer a slightly higher surface
363 area due to its roughness characteristics and higher average surface height. However, further
364 analysis and testing are necessary to determine how these surface properties translate to sensor
365 performance for specific target molecules. However, excessively rough surfaces can hinder
366 electron transfer kinetics.

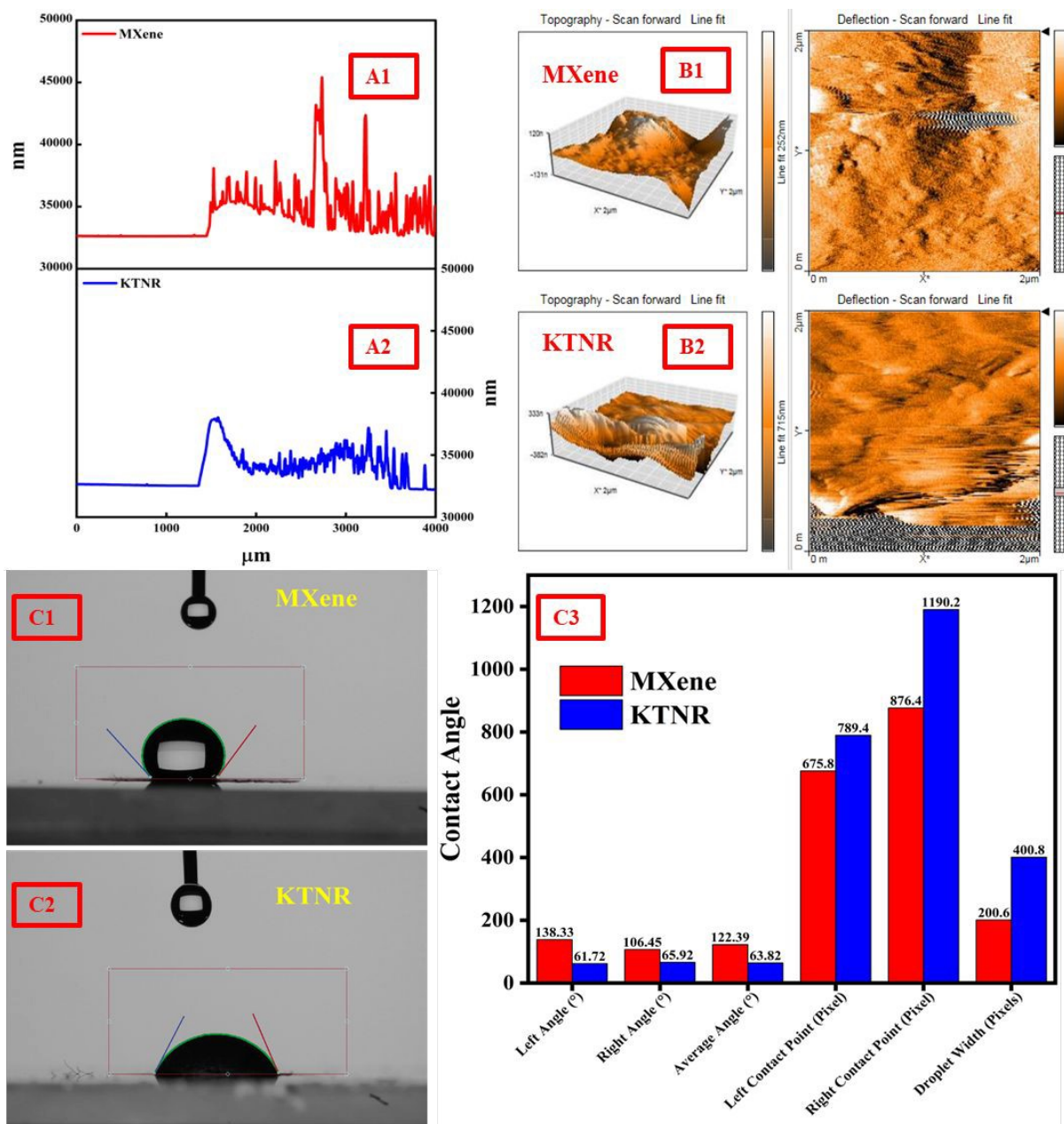
367 To consider AFM, both MXene and KTNR had an image size of 2 μm , indicating the area
368 scanned by the AFM tip (**Fig. 4(B1-B2)**). This allowed for a direct comparison of the surface
369 features within this defined area. The area (4.031 pm^2) was identical for both samples as it
370 represents the total analysed surface area by the AFM, which was likely the same for both
371 measurements. The surface topography parameters i.e., Sa (Surface Area) for MXene (73.43
372 nm) had a significantly higher Sa compared to potassium titanate nanoribbons (30.255 nm).



373 This suggested a much larger projected surface area for MXene within the scanned area. This
374 might be due to the inherent roughness of multi-layered MXene sheets compared to the
375 smoother surface of individual few-layered KTNR nanoribbons. MXene (108.56 nm) also had
376 a higher Sq (Root Mean Square Roughness) value compared to KTNR (42.233 nm). This
377 confirmed that the MXene surface exhibited more significant height variations, indicating a
378 rougher topography. A much higher Sy (Skewness) value for MXene (1057.6 nm) was
379 compared to KTNR (332.57 nm). Both values were positive, suggesting surfaces with more
380 frequent peaks than valleys. However, the significantly higher value for MXene indicated a
381 much stronger tendency towards a peak-dominated surface profile. MXene (436.12 nm) also
382 had a higher Sp (Peak Area Fraction) value compared to potassium titanate nanoribbons (181.4
383 nm). This aligned with the other parameters and suggested that the MXene surface has a larger
384 portion covered by peaks compared to valleys. Both Sv (Valley Area Fraction) values were
385 negative, which might be an artifact as discussed previously. However, the absolute value of
386 Sv was much higher for potassium titanate nanoribbons (-151.17 nm) compared to MXene (-
387 621.52 nm). It might also suggest a slightly higher portion of the scanned area for potassium
388 titanate nanoribbons was covered by valleys compared to MXene. Sm (Mean Height) values
389 were negative, indicating the surfaces were lower than the reference plane on average.
390 However, the MXene surface has a slightly more negative Sm value (-10.028 pm) compared
391 to potassium titanate nanoribbons (-10.015 pm). The AFM data suggested a clear difference in
392 surface topography between MXene and potassium titanate nanoribbons. MXene exhibited a
393 significantly rougher surface with larger height variations, a stronger tendency for peaks, and
394 a larger portion of the surface covered by peaks. In contrast, the potassium titanate nanoribbons
395 appeared to have a smoother surface with less pronounced height variations and a more
396 balanced distribution of peaks and valleys (considering the uncertainty with Sv). The rougher
397 surface of MXene, characterized by its higher Sa, Sq, Sy, and Sp values, could potentially offer
398 a higher surface area for improved performance in electrochemical sensor applications. This
399 increased surface area can provide more active sites for analyte molecules to adsorb, leading
400 to potentially higher sensitivity. However, considering thin film formation, the higher surface
401 roughness of the MXene film suggested a potentially larger effective surface area for
402 applications like catalysis or electrochemical sensing. However, it might also hinder electron
403 transport in electronic devices. The flatter and smoother potassium titanate nanoribbon film
404 might offer less surface area but could potentially allow for more efficient electron transfer



405 across the electrode surface. Further analysis and testing are necessary to determine how these
 406 surface properties translate to sensor performance for specific applications.

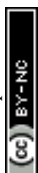


407

408 **Figure 4. Surface optical profilometry of (A1) MXene and (A2) KTNR; AFM (3D) plot to**
 409 **show roughness characteristics and topography for (B1) MXene (B2) KTNR; Contact**
 410 **angle of 0.1 M phosphate buffer on the surface of (C1) MXene and (C2) KTNR fabricated**
 411 **GCE; (C3) Bar graph comparing parameters for Contact angle analysis.**

412

413 The provided **Fig. 4(C1 and C2)** presented the contact angles measured between a drop of 0.1
 414 M Phosphate buffer electrolyte and the surface of the MXene and KTNR fabricated GCE. The

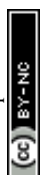


415 average contact angle for MXene (122.39°) indicated a hydrophobic surface whereas the
416 average contact angle of KTNR (63.82°) suggested a hydrophilic surface. Generally, a
417 moderately hydrophilic surface was preferred for electrochemical sensors. This allows for good
418 wettability by the electrolyte solution while maintaining some degree of control over the
419 adsorption/desorption processes of analyte molecules at the electrode surface. A low contact
420 angle like that of KTNR indicates good wettability, meaning the electrolyte can easily penetrate
421 the electrode pores and reach the active material. This is essential for efficient ion transport
422 and redox reactions. Proper wetting ensures good contact between the electrolyte and the
423 electrode surface, facilitating fast charge transfer and improving the overall kinetics of the
424 electrochemical process. Highly hydrophobic surfaces can hinder electrolyte interaction and
425 limit sensor performance. Highly hydrophilic surfaces might allow for excessive non-specific
426 adsorption of molecules from the electrolyte, leading to background noise and decreased sensor
427 sensitivity⁴⁷. Based on the contact angle data, KTNR with a more hydrophilic surface (average
428 angle of 63.82°) appeared to be a better candidate for an electrochemical sensor compared to
429 MXene (average angle of 122.39°). A bar graph is provided to represent the parameters owing
430 to calculation of contact angle (**Fig. 4(C3)**). The surface roughness could influence the effective
431 contact angle. Rougher surfaces could exhibit higher contact angles even for hydrophilic
432 materials like MXene in this case. The specific target analyte and the desired electrochemical
433 process could also play a role in determining the optimal surface wettability. Other factors like
434 surface chemistry and charge distribution could also influence the interaction between the
435 electrode surface and the analyte/electrolyte. While the contact angle data suggested KTNR
436 might be more favourable due to their hydrophilicity, further testing with the target analyte and
437 optimization of the electrode surface properties would be necessary to achieve the best
438 performance for a specific electrochemical sensing application.

439 **3.6. Material characterizations and electrochemical techniques**

440 **3.6.1. Stability study for MAX Phase, MXene, and KTNR fabricated GCE**

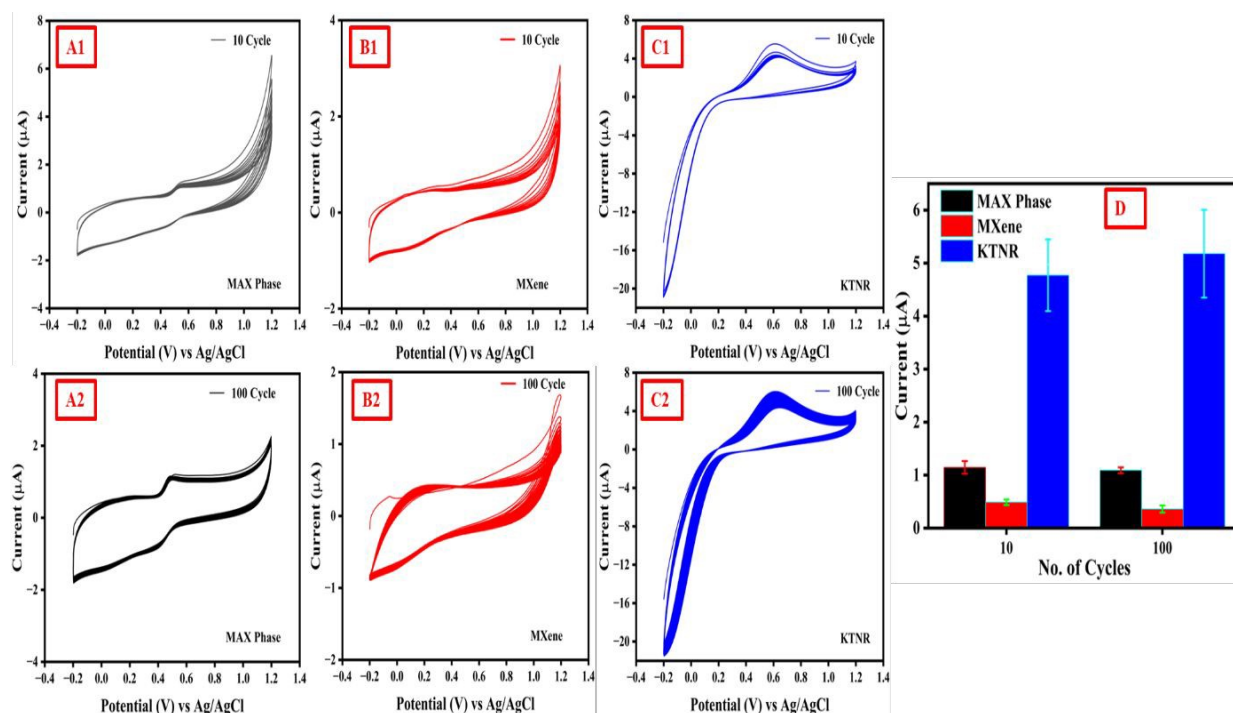
441 The experiment was performed to compare the stability of MAX Phase, MXene and KTNR
442 and electrodes for 5 mM $K_3[Fe(CN)_6]$ oxidation in 0.1 M KCl solution over multiple CV cycles
443 (10 and 100 cycles) ((**Fig.5A(1-2)**, **Fig.5B(1-2)** and **Fig.5C(1-2)**)⁴⁸. The current values and
444 their standard deviations were provided for each electrode at different cycle numbers. All
445 electrodes fabricated with MAX Phase, MXene, and KTNR showed a decreasing trend in
446 current with increasing cycle number. For MAX phase, MXene, and KTNR, the current value



447 starts at 1.27 μA , 5.44 μA , and 5.51 μA in 10 cycles and decreases to 1.15 μA , 4.24 μA and
448 4.37 μA at 100 cycles. This suggests a loss of electrocatalytic activity for KTNR over time.
449 The MAX Phase and MXene fabricated electrodes showed a huge drip in current with
450 consecutive cycles, but the change of current at the oxidation peak is less pronounced while
451 compared to KTNR, which showed a broad error bar. The standard deviations for both
452 electrodes are relatively small compared to the current values, indicating good reproducibility
453 of the measurements. The alternate increase and decrease in current density suggested a loss of
454 electrocatalytic activity over time, could be due to several factors. The MAX Phase, MXene or
455 KTNR nanostructures could be degrading during the cycling process which could be due to the
456 electrochemical breakdown of the materials or the dissolution of metal ions from the electrode
457 ⁴⁹. The surface of the electrodes could be fouled by reaction products or other impurities in the
458 electrolyte ⁵⁰. This would block the active sites on the electrode and hinder electron transfer.
459 Lastly, the electrode-electrolyte interface could be weakening over time. This would lead to an
460 increase in resistance and a decrease in current density. The stability of KTNR can be compared
461 to MXene and MAX Phase by comparing the decrease in current density for both materials
462 over the same number of cycles. A smaller decrease in current density for KTNR indicated
463 better stability. However, if the anodic peak currents of KTNR and MXene are to be compared,
464 KTNR shows much significant current 4-5 folds greater than that of MXene and MAX Phase
465 fabricated electrodes over multiple cycles (**Fig. 5(D)**). The cathodic current represents the
466 reduction process. The cathodic current was observed to be higher for KTNR in both the 10-
467 cycle and 100-cycle tests. The potential range for all three materials was similar, suggesting
468 that the differences in current are not due to a wider electrochemical window for KTNR. The
469 possibilities, owing to large cathodic current, might be related to KTNR, being nanoribbons,
470 likely possessed a higher surface area compared to MXene and MAX Phase fabricated GCE.
471 A larger surface area is ought to provide more active sites for electrochemical reactions, leading
472 to increased current. The potassium ions in KTNR may interact with the redox species
473 ($\text{Fe}(\text{CN})_6^{3-}$) in the electrolyte, leading to a synergistic effect that enhances the reduction
474 process. The unique structure of KTNR might have facilitated faster charge transfer during the
475 reduction process which could be due to efficient ion diffusion within the nanoribbons or other
476 factors related to their crystal structure. Hence, KTNR exhibited better electrochemical
477 stability, especially over multiple cycles. That would mean that the material could maintain the
478 active sites and charge transfer capabilities, resulting in sustained high cathodic current even
479 after repeated cycling ^{51,52}. Also the broad window of MAX Phase and MXene suggested them



480 to be energy storage materials while KTNR exhibits a way better catalytic property as an
 481 electrode material.



482
 483 **Figure 5. Stability Study of (A1-A2) MAX Phase/GCE, (B1-B2) MXene/GCE and KTNR**
 484 **(C1-C2) employing 10-200 cycles in 5 mM $K_3[Fe(CN)_6]$; (D) Error Bar graph showing**
 485 **peak currents against 10 and 100 cycles for MAX Phase, MXene and KTNR.**

486
 487 **3.6.2. Understanding the properties of electrode materials using various electrochemical**
 488 **techniques**

489 The intricate properties of all electrode materials were subjected to electrochemical techniques
 490 such as CV, DPV, and EIS in 5mM $K_3[Fe(CN)_6]$ containing 0.1 M KCl. The electrocatalytic
 491 properties of KTNR, MXene, and MAX Phase were studied through CV and DPV. The CV
 492 and DPV voltammograms suggest that KTNR-fabricated GCE exhibited highest electron
 493 transfer compared to MXene and MAX Phase fabricated GCEs. The CV graph (**Fig. 6(A)**) was
 494 observed to have a sharp peak of KTNR having an I_{pa} almost 4 times anodic peak current (I_{pa}
 495 = 3.96 μA) which demonstrated faster reaction kinetics while MXene and MAX Phase having
 496 I_{pa} = 0.69 μA and 0.38 μA respectively, had much broader peaks, indicating a slower reaction.
 497 It was also confirmed by DPV (**Fig. 6(B)**) where a high peak current in the KTNR (I_{pa} = 1.15
 498 μA) curve was observed compared to MXene (I_{pa} = 0.98 μA) and MAX Phase (I_{pa} = 0.46 μA)



499 indicated greater electrode activity for the redox reaction of $K_3[Fe(CN)_6]$. A more positive peak
500 potential for KTNR ($E_{pv} = 0.39$ V) signified a lower overpotential, meaning the electrode
501 requires less or optimal energy to drive the reduction reaction compared to MXene ($E_{pv} = 0.43$
502 V) and MAX Phase ($E_{pv} = 0.16$)⁵³. The effective surface area by KTNR, MXene and MAX
503 Phase fabricated electrodes were calculated to be 3.47×10^{-8} cm²/s, 1.054×10^{-9} cm²/s and
504 3.196×10^{-10} cm²/s respectively. By considering all parameters, MXene and MAX Phase as
505 electrode materials were ought to be better as energy storage materials while KTNR showed
506 better electro-catalytic performance.

507 The EIS Nyquist plots for KTNR fabricated GCE shows a lower impedance compared to its
508 precursors MXene and MAX Phase. This indicates that the KTNR electrode has a higher ability
509 to transfer charge at the electrode-electrolyte interface. In other words, it has better
510 electrocatalytic activity⁵⁴. In the Nyquist plot, the imaginary impedance (Z'') is plotted on the
511 y-axis and the real impedance (Z') is plotted on the x-axis (**Fig. 6(C)**). The equivalent circuit
512 model simplified KTNR electrode-electrolyte interface and the fitting method used was
513 Randomize + Simplex while the parameters were the values of the components in the
514 equivalent circuit ($R_1 + Q_1 / (R_2 + C_2 / (R_3 + C_3 / (R_4 + W_4))) + C_5 / R_5$) that best match the experimental
515 EIS data. The $R_1 = 2.028 \Omega$ or the solution resistance (R_s) represented the resistance of the
516 electrolyte solution between the working and reference electrodes. A lower R_s suggests a more
517 conductive electrolyte solution. The $R_2 = 195 \Omega$ and $R_3 = 938.9 \Omega$ referred to charge transfer
518 resistance (R_{ct}) that represented the resistance to electron transfer between the electrode and
519 the electrolyte. The Nyquist plot showed a smaller semicircle diameter at low frequencies
520 indicates a lower R_{ct} and faster charge transfer kinetics⁵⁵. In the image, the KTNR electrode
521 has a smaller semicircle diameter compared to MXene and MAX Phase. The diameter of the
522 semicircle for KTNR extends less towards the lower frequencies, it could also indicate faster
523 mass transfer for the KTNR electrode. The value of $R_4 = 23601 \Omega$ suggested a Warburg
524 impedance $W_4 = 0.2033e-9$ Ohm.s^{-1/2} implying to the resistance to mass transfer of ions within
525 the electrolyte which in-turn was related to the rate of the reaction at the electrode surface⁵⁶.
526 The possible film resistance $R_5 = 271304 \Omega$ represented the resistance of Nafion stabilized
527 KTNR thin film formed on the electrode surface. The $C_2 = 0.509e-6$ F or the double layer
528 capacitance represented the capacitance between the electrode-electrolyte interface. The $C_3 =$
529 $0.2197 \mu F$ and $C_5 = 1.287e24$ F represented capacitance associated with the Nafion stabilized
530 film on the electrode surface or porosity of KTNR as electrode material⁵⁷. Lastly, Constant
531 Phase Element ($Q_1 = 4.239e-6$ F.s^{a-1}) was an element that could be used to model a more

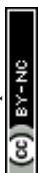


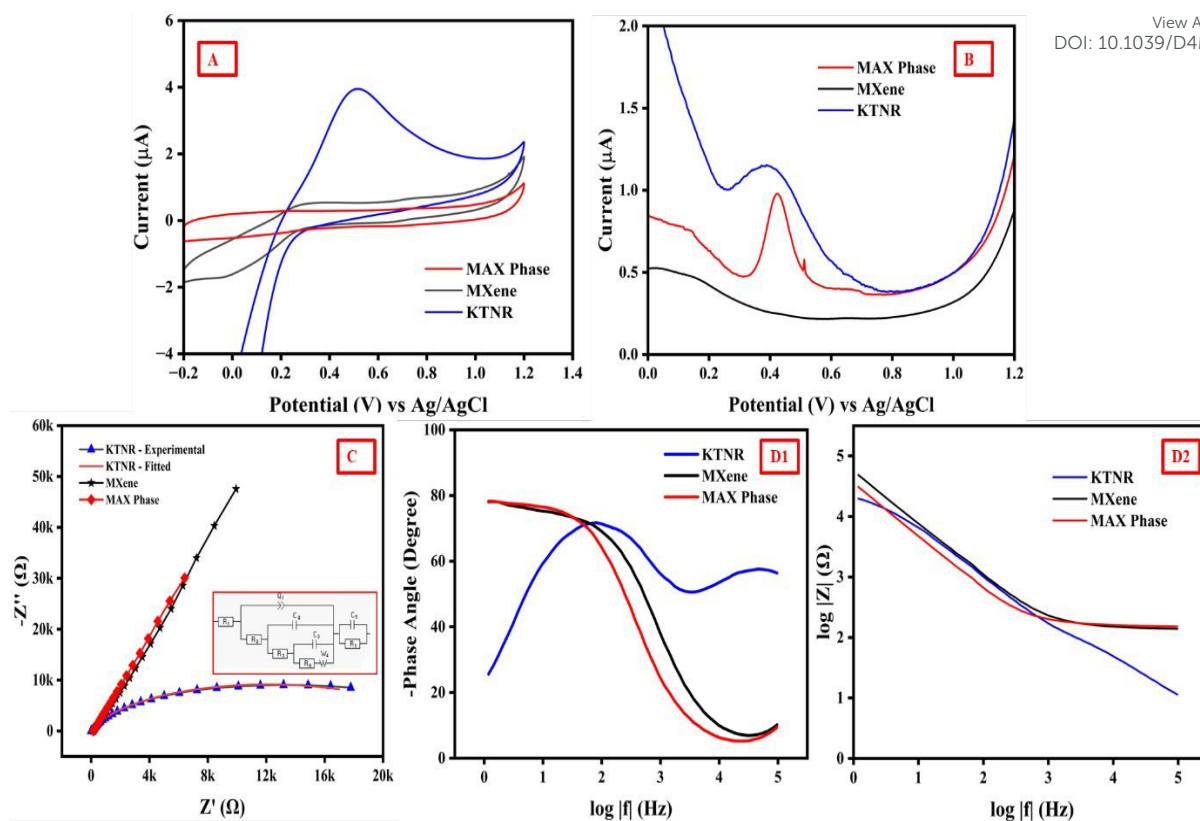
532 complex capacitance where the parameter "a1= 0.7535" determined the deviation from ideal
533 capacitance behaviour of the equivalent circuit. The exchange current density represents the
534 rate of electron transfer at equilibrium, where the forward and reverse reaction rates are equal.

535 It's a fundamental parameter that reflects the intrinsic activity of the electrode material. The
536 key relationship is derived from the Butler-Volmer equation, and under conditions of small
537 overpotential (near equilibrium), it simplifies to $I_0 = RT / (nF R_{ct})$; where I_0 = exchange current
538 density (A/cm^2), R = ideal gas constant ($8.314 J/mol \cdot K$), T = absolute temperature (K), n =
539 number of electrons transferred in the redox reaction, F = Faraday constant ($96485 C/mol$) and
540 R_{ct} = charge-transfer resistance (Ω). The R_{ct} values in this case was calculated to be 938.9Ω ,
541 230346Ω and 326328Ω for KTNR, MXene and MAX Phase respectively which yielded the
542 corresponding I_0 values of $2.75 \times 10^{-5} A/cm^2$, $1.22 \times 10^{-7} A/cm^2$ and $7.92 \times 10^{-8} A/cm^2$. The
543 exchange current density showed KTNR/GCE has much better intrinsic electrocatalytic
544 activity⁵⁸.

545 A Bode plot ((**Fig. 6(D1-D2)**)) typically shows two key features for EIS data, one being the
546 phase angle which indicates the phase shift between the applied voltage and the resulting
547 current and second is impedance magnitude ($\log |Z|$) which represents the overall resistance to
548 current flow in the system. At high frequencies, the phase angle typically approached towards
549 0 degrees, indicating minimal phase shift. As the frequency decreases, the phase angle becomes
550 more negative, reflecting the increasing influence of capacitive behaviour. At even lower
551 frequencies, the phase angle might approach -90 degrees for a purely capacitive response. At
552 high frequencies, the impedance magnitude was usually dominated by solution resistance and
553 shows a plateau in the $\log |Z|$ vs. $\log |f|$ plot. As the frequency decreases, the impedance
554 magnitude might start to increase due to the influence of charge transfer resistance and other
555 processes. The provided information suggested a complex equivalent circuit model was used
556 to capture the EIS response of the KTNR, MXene, and MAX Phase fabricated GCE.

557





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558

559 **Figure 6.(A) CV (B) DPV (C)EIS Nyquist plots (inset: Equivalent Circuit) (D) Bode Plot**
560 **for KTNR, MXene and MAX Phase fabricated GCE in 5 mM $K_3[Fe(CN)_6]$ in 0.1M KCl**
561 **electrolyte.**

562

563 3.6.3. Mechanism of electro-oxidation of ciprofloxacin on active working surface area of

564 KTNR fabricated electrode

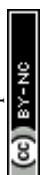
565 Ciprofloxacin is a fluoroquinolone antibiotic known for its broad-spectrum activity. It is a
566 zwitterionic molecule, meaning it can exist with both positive and negative charges depending
567 on the pH. KTNR is a metal oxide material having surface charge which can influence the
568 interaction with ciprofloxacin molecules. The process of electrochemical oxidation involved
569 the transfer of electrons from ciprofloxacin molecules to the electrode surface, resulting in the
570 oxidation of ciprofloxacin. The steps involved were diffusion, adsorption, electron transfer,
571 desorption and diffusion which can be observed in **Fig. 7(C)**. Ciprofloxacin molecules in the
572 bulk solution diffuse towards the surface of the Potassium Titanate electrode. Ciprofloxacin
573 molecules could interact with the electrode surface through various forces like electrostatic
574 interactions, hydrogen bonding, or van der Waals forces. The net charge of ciprofloxacin at pH
575 8 (likely negatively charged) and the surface charge of the KTNR (which could also be pH-



576 dependent) would influence this adsorption process. At the electrode surface, ciprofloxacin
577 molecules lose electrons to the electrode, undergoing oxidation. The specific mechanism of
578 electron transfer could involve direct interaction with the electrode or the participation of
579 intermediate species formed on the electrode surface. The oxidized ciprofloxacin molecules
580 desorbed from the electrode surface and get diffused back into the bulk solution. The factors
581 that could affect the process are pH, electrode potential and scan rate. The pH of the solution
582 could influence the net charge of ciprofloxacin and the surface charge of the KTNR electrode.
583 An optimal pH might exist for balancing the electrostatic interactions and promoting efficient
584 electron transfer. The applied potential at the electrode can influence the rate of electron
585 transfer. A higher positive potential might be required to drive the oxidation reaction. In cyclic
586 voltammetry experiments, the scan rate can affect the observed current response. At faster scan
587 rates, the diffusion process might become limiting, leading to a deviation from the ideal
588 behaviour. The electrochemical oxidation of ciprofloxacin at a Potassium Titanate electrode
589 ought to be a complex process involving mass transport (diffusion), surface interaction
590 (adsorption/desorption), and electron transfer. The efficiency of this process depended on
591 various factors like pH, electrode potential, and surface properties which were studied and
592 optimized in the later part of the research.

593 **3.6.4. Optimization of pH for ciprofloxacin detection using KTNR/GCE**

594 Ciprofloxacin is a zwitterionic molecule, meaning it can exist with both positive and negative
595 charges depending on the pH. At lower pH (around 4), ciprofloxacin is likely mostly protonated
596 (positively charged) due to the acidic environment. As observed in **Fig. 7(A1-A2)** the pH
597 increases from 4 to 11, the solution becomes more basic, and ciprofloxacin loses its protons,
598 becoming increasingly deprotonated (negatively charged). To deal with surface charge
599 interaction KTNR being a metal oxide material that also exhibited a surface charge depending
600 on the pH. At lower pH, the KTNR active surface might be positively charged. As the pH
601 increased, the surface charge of KTNR could become more negative. When the pH was low
602 (acidic), both ciprofloxacin (positively charged) and the KTNR surface (positively charged)
603 experienced electrostatic repulsion. This repulsion could hinder the adsorption of ciprofloxacin
604 molecules onto the electrode surface and slow down the electron transfer process. As the pH
605 increased, ciprofloxacin became increasingly deprotonated (negatively charged). This could
606 lead to attractive forces between the negatively charged ciprofloxacin and the potentially
607 negatively charged KTNR surface at higher pH. This attraction could enhance the adsorption
608 of ciprofloxacin molecules and potentially promote the electron transfer process, leading to a



609 higher current at a slightly less positive potential (anodic shift). The observed optimal pH of 8
610 might be a balance between these two effects. At pH 8, ciprofloxacin might be sufficiently
611 deprotonated to favour adsorption on the electrode surface while minimizing any repulsion
612 from the electrode surface itself. Since the pH 8 is between the reference pKa values (pKa1 =
613 5.17 and pKa2 = 8.74), ciprofloxacin will likely exist in a zwitterionic form in the 0.1 M pH 8
614 phosphate buffer. The carboxylic acid group (pKa1) will likely be deprotonated (negatively
615 charged) as the solution's pH is higher than its pKa. The primary amine group (pKa2) might be
616 partially protonated (positively charged) due to the pH being slightly lower than its pKa2. This
617 could lead to the most efficient electron transfer and the highest anodic peak current for
618 ciprofloxacin oxidation. The anodic peak shifted towards more positive potentials with
619 increasing pH suggesting a change in the rate of the electro-oxidation reaction. The shift likely
620 reflected a slower reaction rate at lower pH (due to electrostatic repulsion) and a potentially
621 faster rate at higher pH (due to enhanced adsorption). Ciprofloxacin might undergo multiple
622 redox reactions involving different electron transfers and protonations. This complex
623 mechanism could lead to non-linear behavior, as the relative contributions of these reactions
624 can vary with pH. Ciprofloxacin, like many drugs, exists in different protonation states
625 depending on the pH of the solution ⁵⁹. These different protonation states could also have
626 varying redox potentials, which might have led to non-linearity ⁶⁰. The nature of the electrode
627 surface, including its composition and roughness, can influence the adsorption of ciprofloxacin
628 and its redox behavior since the fabrication of electrode using drop-casting method might
629 always lead to handling errors ⁶¹⁻⁶³. The ionic strength of the solution could also influence the
630 activity coefficients of the species involved in the redox reaction, leading to deviations from
631 the expected linear relationship ⁶⁴⁻⁶⁶. Temperature could also be a parameter that might have
632 influenced the kinetics of the redox reaction and the stability of the redox species ^{67,68}. This can
633 further complicate the relationship between redox potential and pH .

634 3.6.5. Impact of scan rates on ciprofloxacin detection using KTNR/GCE

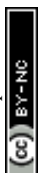
635 The CV curves showed anodic peaks around 0.8 V to 1.0 V at pH 8, which corresponded to the
636 oxidation of ciprofloxacin. As the scan rate increased (from 1 mV/s to 200 mV/s), the following
637 trends were observed (**Fig. 7(B1 and B3)**). The anodic peak current increased and the peak
638 potential (where the current is maximum) shifted slightly towards more positive potentials. The
639 linear regression plots of anodic current (I_p) vs. square root of scan rates ($v^{1/2}$) for three scan
640 rate ranges (1-10 mV/s, 10-100 mV/s, and 100-200 mV/s) suggested a diffusion-controlled
641 electrochemical process for ciprofloxacin oxidation at least for the lower scan rates (1-10



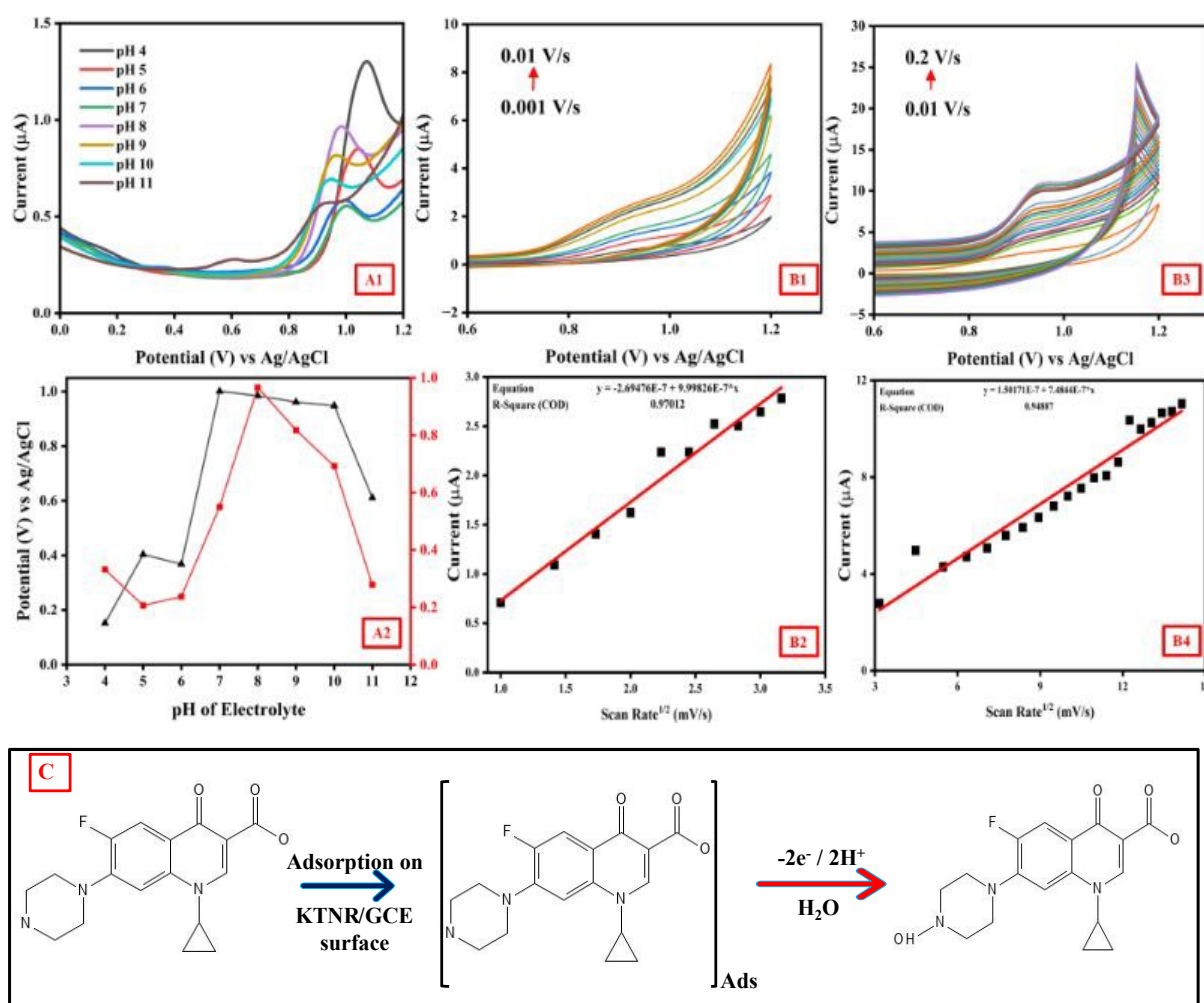
642 mV/s). The high R-squared values 0.97012 and 0.94887 for the linear plots $I_p = 9.99826E-7 * v^{1/2} + 2.69476E-7$ (**Fig. 7(B2)**) and $I_p = 7.4844 - 7 * v^{1/2} + 1.50171E-7$ (**Fig. 7(B4)**) respectively,
643 $v^{1/2} + 2.69476E-7$ (**Fig. 7(B2)**) and $I_p = 7.4844 - 7 * v^{1/2} + 1.50171E-7$ (**Fig. 7(B4)**) respectively,
644 which indicated good linear relationships between the I_p vs $v^{1/2}$ in these two lower scan rate
645 ranges. The deviation from linearity observed at higher scan rates (above 10 mV/s) might be
646 due to limitations in the diffusion process of ciprofloxacin molecules towards the electrode
647 surface at faster scan rates. The regression suggested a diffusion-controlled process. The
648 number of electrons transferred (n) was 1 for ciprofloxacin oxidation and the concentration (C)
649 of analyte was 90 μ M. The electrode surface area (A) was calculated to be 0.071 cm^2 for GCE.
650 The Diffusion coefficient (D) was calculated using Randles-Sevcik equation, with the formula:
651 $I_p = (2.69 \times 10^5) * n^{3/2} * C * A * D^{1/2} * v^{1/2}$. The calculated average diffusion coefficient of
652 $2.21E-11 \text{ cm}^2/\text{s}$ was well consistent within a reasonable range for ciprofloxacin in phosphate
653 buffer electrolyte. Diffusion-Controlled Reactions: At slower scan rates, diffusion processes
654 can become limiting, leading to a more reversible behaviour. As the scan rate increases, the
655 system may not have enough time for the diffusion of reactants and products, leading to a
656 deviation from reversibility and a crossover of the anodic and cathodic peaks.

657 The crossing of the CV curves at higher potentials in the 10 mV/s to 200 mV/s scan rate range
658 suggested a change in the electrochemical behaviour of the system (**Fig. 7(B3)**). If the charge
659 transfer kinetics were slow, increasing the scan rate could lead to a shift in the peak potentials
660 and a crossover of the curves. At higher scan rates ($>50\text{mV/s}$), the capacitive current associated
661 with double-layer charging became more significant⁶⁹. This could contribute to the observed
662 crossover, as the capacitive current can mask the faradaic current associated with the redox
663 processes. At higher potentials beyond 1V, the electrode surface might undergo oxidation or
664 reduction processes that affected the electrochemical behaviour^{70,71}. These changes could also
665 lead to a shift in the peak potentials and a crossover of the curves^{72,73}. PB electrolyte containing
666 ciprofloxacin could have caused a potential drop (IR drop) across the electrolyte hemisphere,
667 which might have distorted the CV curves, especially at higher scan rates. This IR drop could
668 lead to a shift in the peak potentials and a crossover of the curves⁷⁴.

669 Based on the observed behaviour, a possible mechanism for ciprofloxacin oxidation at the
670 KTNR/GCE could be proposed. Ciprofloxacin molecules in the bulk solution diffused towards
671 the electrode surface. At the electrode surface, ciprofloxacin underwent an electron transfer
672 reaction, getting oxidized. The oxidized ciprofloxacin got desorbed from the electrode surface
673 and diffused back into the bulk solution. At slower scan rates, where the diffusion process was
674 dominant, the current increased as the scan rate increases since there was more time for



675 ciprofloxacin molecules to diffuse towards the electrode surface and get oxidized. At faster
 676 scan rates, the diffusion process might become limited. The ciprofloxacin molecules might not
 677 be able to reach the electrode surface fast enough to keep up with the electron transfer reaction
 678 rate. This could lead to a deviation from the ideal linear relationship between the current and
 679 the square root of scan rate. The CV data suggested that the oxidation of ciprofloxacin at the
 680 KTNR/GCE was an electrochemically active process. The slight shift in the anodic peak
 681 potential with increasing scan rate might be due to kinetic limitations or a combination of
 682 diffusion and kinetic control at higher scan rates.



683
 684 **Figure 7. (A1) Study of pH to optimize the voltammetric detection of ciprofloxacin using**
 685 **KTNR/GCE, (A2) Line + Scatter plot to show the correlation of Peak potential (E_{pv}) and**
 686 **Anodic Peak Current (I_{pa}) vs pH of the 0.1M Phosphate Buffer electrolyte containing**
 687 **ciprofloxacin; Study of different scan rate CV (B1) 0.01-0.01 mV/s and (B3) 0.01-0.2 mV/s**
 688 **in 0.1M Phosphate Buffer at optimized pH =8 and, their corresponding regression plots**



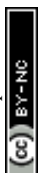
689 **(B2 and B4); (C) Illustration of the mechanism of electro-oxidation of ciprofloxacin at the**
690 **active surface area of KTNR/GCE.**

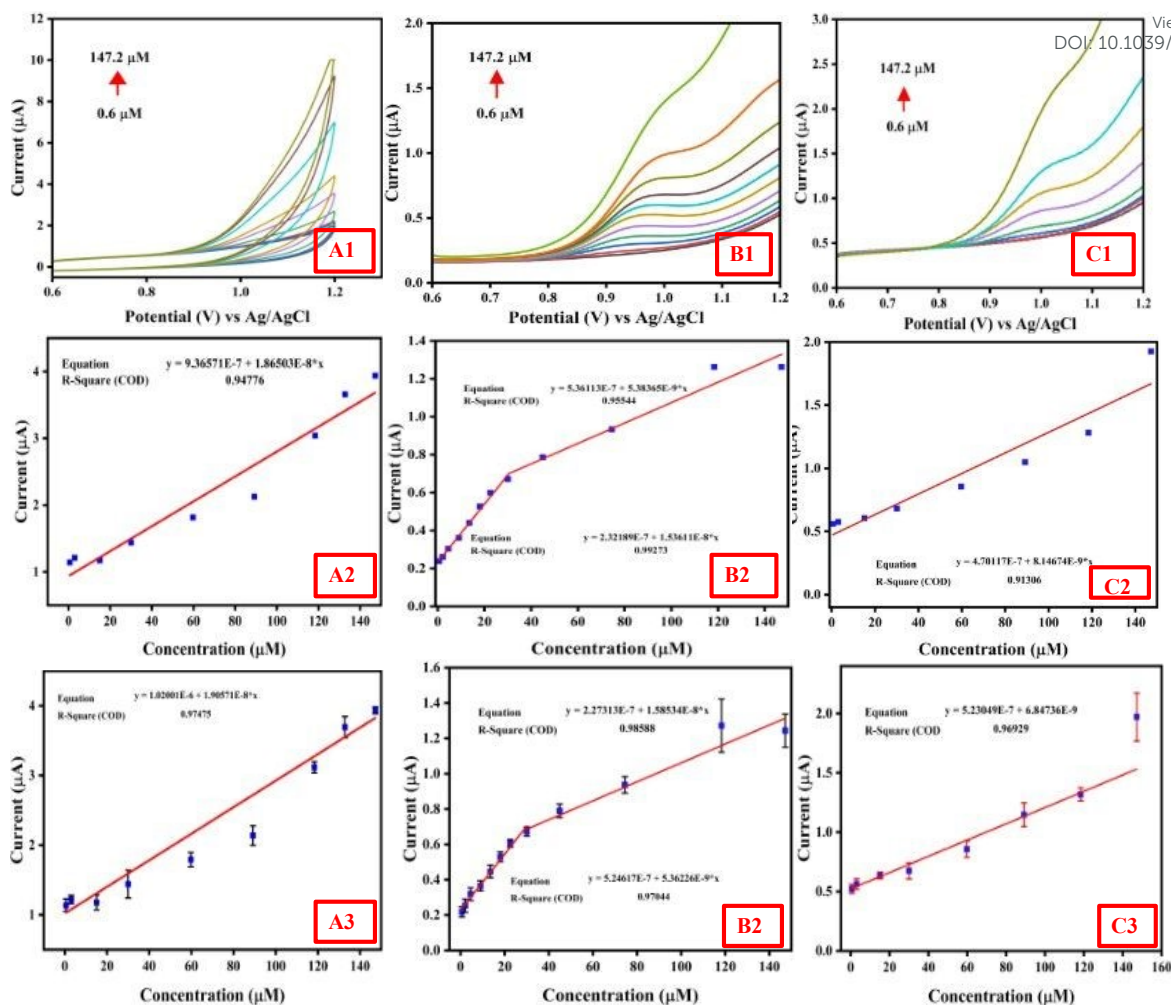
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692 **3.6.6. Electrochemical sensing studies of ciprofloxacin using KTNR/GCE**

693 The CV aimed to investigate the electrochemical response of ciprofloxacin at a KTNR/GCE in
694 a linear concentration range of 0.6 μM to 147.2 μM (**Fig. 8(A1)**). The CV likely showed
695 indistinguishable but linearly increasing oxidation peaks at a specific potential, indicating the
696 electrochemical oxidation of ciprofloxacin at the KTNR/GCE. The position of this peak could
697 be determined at beyond 1.0 V as observed in the voltogram. It was also observed that the
698 oxidation peak current (I_{pa}) increased as the concentration of ciprofloxacin (C) in the electrolyte
699 solution increased. Although no clear peaks were formed, the voltogram suggested that KTNR
700 was actively involved in catalysis which indicated that more ciprofloxacin molecules were
701 being oxidized at the electrode with higher concentrations. Ideally, the plot of peak current vs.
702 ciprofloxacin concentration exhibited a linear relationship having an equation $I_{\text{pa}} = 1.86503\text{E-}$
703 $8 * C + 9.36571\text{E-}7$ with an $R^2 = 0.94776$ (**Fig. 8(A2)**) within a specific concentration range of
704 0.6 μM to 147.2 μM . The LOD was calculated to be 0.07 μM and LOQ was 0.213 μM . The
705 sensitivity of the KTNR/GCE for ciprofloxacin sensing through CV was 0.282 $\mu\text{A uM}^{-1} \text{cm}^{-2}$.

706 DPV was used, which is a more sensitive technique compared to CV for quantitative analysis.
707 The potential range scanned was from 0.6 V to 1.2 V (**Fig. 8(B1)**). The DPV plot showed a
708 well-defined peak at a specific potential, corresponding to the oxidation of ciprofloxacin at the
709 KTNR electrode. The $E_{\text{pv}} = 0.98$ was the peak voltage that could be determined from the
710 voltogram. The image showed that the peak current for the ciprofloxacin oxidation peak
711 increases with the concentration of ciprofloxacin in the electrolyte solution. One could analyze
712 the linearity by plotting the peak current data points for different concentrations and fitting a
713 straight line through them $I_{\text{pa}} = 1.53611\text{E-}8 * C + 2.32189\text{E-}7$ and $I_{\text{pa}} = 5.38365\text{E-}9 * C +$
714 $5.36113\text{E-}7$ (**Fig. 8(B2)**). The respective R^2 value of the fit i.e., 0.99273 and 0.9554, indicated
715 how excellent the data corresponded to a linear relationship. Through DPV, the KTNR/GCE
716 offered a sensitivity of 0.0986 $\mu\text{A uM}^{-1} \text{cm}^{-2}$, while having an LOD and LOQ of 0.0608 μM
717 and 0.184 μM respectively.





718

719 **Figure 8.(A1 and A2) CV response and corresponding regression plot; (B1 and B2) DPV**
 720 **response and corresponding regression plot; (C1 and C2) SWV response and**
 721 **corresponding regression plot of KTNR to obtain the linear concentration range of**
 722 **ciprofloxacin in 0.1 M Phosphate buffer pH = 8; triplicate data on (A3) CV (B3) DPV and**
 723 **(C3) SWV response curves with regression plots showing excellent replicability.**

724 SWV being a variant of pulse voltammetry, was employed to confirm linearity observed in
 725 DPV. It also offers advantages like higher sensitivity and lower background current compared
 726 CV. Each curve in the plot likely corresponded to the SWV response for a different
 727 concentration of ciprofloxacin in the electrolyte solution which also related to the oxidation at
 728 the KTNR active electrode surface (**Fig. 8(C1)**). The equations $I_{pa} = 8.14674E-9 \cdot C +$
 729 $4.70117E-8$ with an R^2 value = 0.91306, shows its consistency with DPV results (**Fig. 8(C2)**).
 730 Also, the LOD and LOQ were calculated which yielded to be 0.0264 μM and 0.08 μM
 731 respectively, while offering a sensitivity of 0.113 μA uM⁻¹ cm⁻². The replicability showed
 732 consistent replicability in data of CV, DPV and DPV as shown in **Fig. 8(A3,B3,C3)**.



733 Overall considering highest sensitivity value and lowest LOD. The DPV data suggested that
 734 the KTNR/GCE electrode was a more promising tool for the quantitative detection of
 735 ciprofloxacin within a certain concentration range of 0.6 μM to 147.2 μM over CV and SWV.
 736 DPV and SWV minimizes the contribution of the charging current by measuring the current at
 737 specific points after the potential step. This led to a sharper and more well-defined peak
 738 compared to CV. The current measured with DPV and SWV was constant throughout the
 739 experiment which reflected the faradaic current at specific points in the potential waveform.
 740 This resulted in a more prominent current response compared to the smooth regular curve
 741 observed in CV. The observed increase in oxidation peak current with increasing concentration
 742 indicated a linear relationship that could be exploited for analytical purposes. This dynamic
 743 range of micromolar concentration can be used for quantitative analysis of ciprofloxacin
 744 concentration in unknown samples using the KTNR/GCE electrode. A comparison with
 745 previous reported non-enzymatic electrochemical sensors for ciprofloxacin detection is
 746 tabulated in **Table 2**.

747 **Table 2. Reported literature on non-enzymatic electrochemical sensors for detection of**
 748 **ciprofloxacin**

Materials/Electrode	Method	Linear Range (μM)	LOD (μM)	Real Samples	References
Co-MOFs/PLA	DPV	0.5–150	0.017	Drug	75
GO/SPCE	DPV	1-8	0.3	Milk	76
TiO ₂ /PVA/GCE	DPV	10–120	0.04	Rain water	77
f-MWCNTs/PANI/GCE	LSV	0.1-1,1-20	0.08	Pharmaceuticals	78
f-MWCNT-coated GCE	SWV	5-100	0.16	Hospital effluent, wastewater, natural water	79
BaCuSi ₄ O ₁₀ /GCE	DPV	0.05-150	0.0009	Pharmaceuticals	80
Pt-RGO/GCE	DPV	10-25	1.53	Tap water, river water	81
CRGO/GCE	SWV	6-60	0.5	Pharmaceuticals, milk	82
Ch-AuMIP/GCE	DPV	1-100	0.21	Tap water, milk, mineral water, pharmaceuticals	83
BiPO ₄ /GO-MMIPs/PGE	SWSV	39-740	0.4	Blood serum, milk	84
Fe-g-C ₃ N ₄ /PGE	DPV	0.001-1	0.0054	Blood serum	85



ChCl/CPE	SWV	0.005 -200	0.00036	CIP eye drops, eggs, river water	View Article Online DOI: 10.1039/D4MA01245C
KTNR/GCE	CV, DPV, SWV	0.6 – 147.2	0.07, 0.0608, 0.0264	honey, milk, eggs, marine water, Ganga water, organic fertilizer, soil, Simulated body fluid	This work

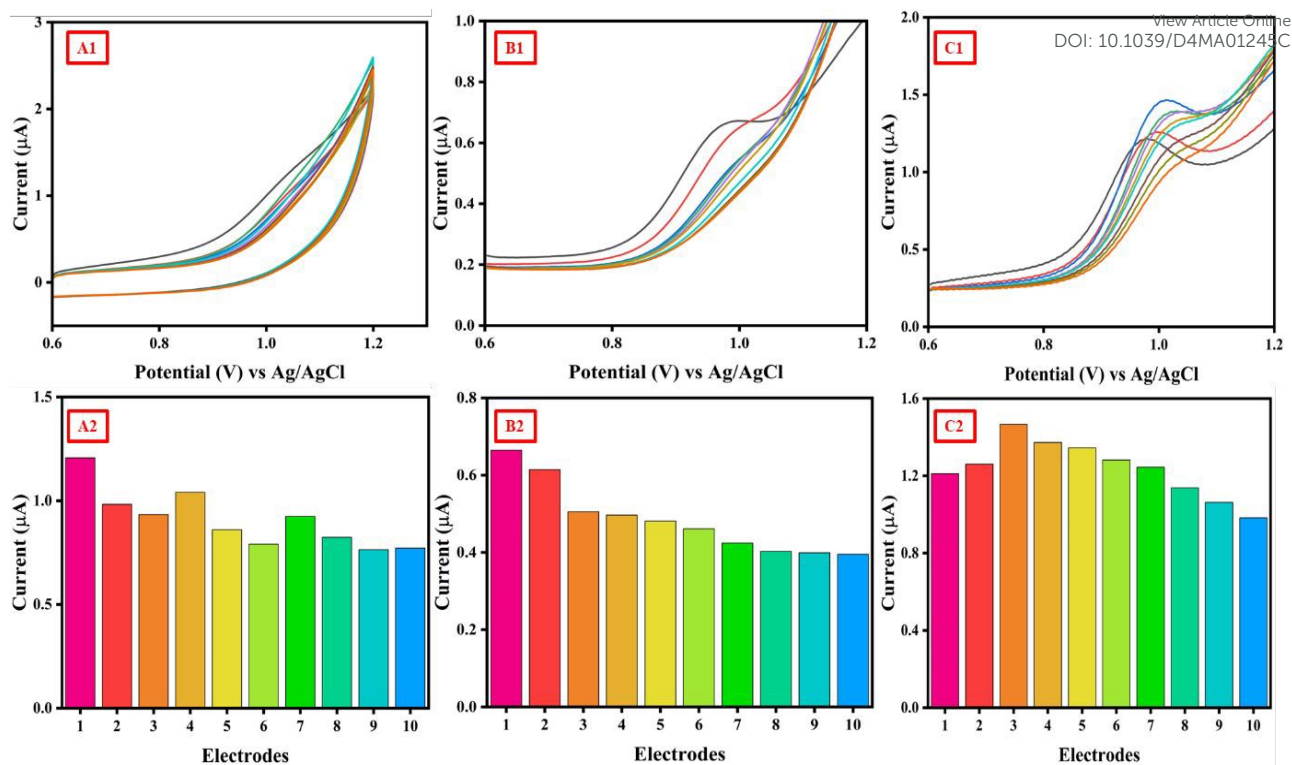
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751 3.6.7. Reproducibility of KTNR/GCE for ultrasensitive detection of ciprofloxacin

752 Freshly fabricated ten KTNR fabricated electrodes were tested through CV, DPV and SWV
 753 (Fig. 9(A1, B1, and C1)) in the same laboratory conditions and room temperature (25°C) to
 754 check the reproducibility of the electrodes towards ciprofloxacin detection using CV technique
 755 at a random concentration. The system's viability was confirmed by an error bar graph (Fig.
 756 9(A2, B2 and C2)) that practically demonstrates the stability of the electrode. The peak
 757 currents averaged at $0.91 \mu\text{A} \pm 0.15\%$, $0.484 \mu\text{A} \pm 0.19\%$ and $1.2 \mu\text{A} \pm 0.12\%$ were obtained
 758 from CV, DPV and SWV. The results showed excellent reproducibility owing to the novelty
 759 of newly developed KTNR based electrochemical sensor. The variation estimated as RSD
 760 values of 0.15%, 0.19% and 0.12% was calculated which could be owed to the handling error
 761 and manual fabrication of the electrodes. However, if the sensor fabrication samples were not
 762 stored properly after preparation, the electrode materials of the sensor could be prone to
 763 oxidation and resulted in the performance might degrade.





764

765 **Figure 9. Reproducibility of KTNR fabricated GCEs based on CV (A1-A2), DPV (B1-B2)**766 **and SWV (C1-C2) towards efficient sensing of ciprofloxacin.**

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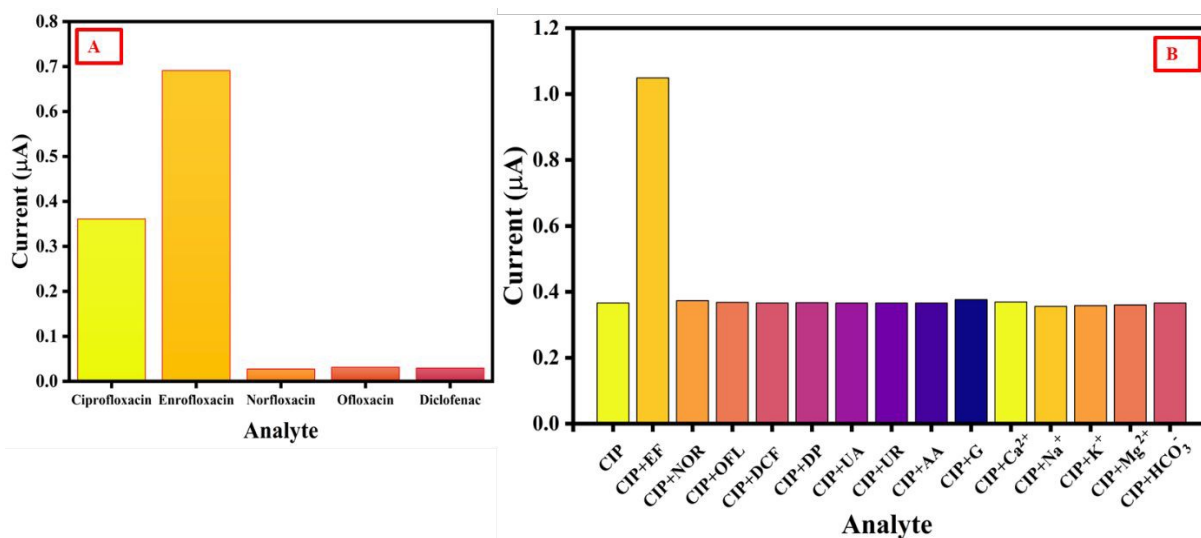
768 **3.6.8. Selectivity of KTNR/GCE and effect of interfering compounds against**
769 **ciprofloxacin detection**

770 To ensure selective healthcare monitoring, the KTNR-modified GCE was expected to present
 771 a high selectivity for ciprofloxacin against other antibiotics and drugs administered to humans
 772 and animals, especially poultry and cattle. To confirm the selectivity of the sensor, the CV was
 773 obtained in solutions containing 10 μM of ciprofloxacin (CIP) against same concentration of
 774 other antibiotics like enrofloxacin (EF), enrofloxacin (NOR), ofloxacin (OFL) and, Diclofenac
 775 (DCF) (**Fig. 10(A)**). In addition to Ciprofloxacin detection, the selectivity of KTNR/GCE was
 776 performed using separate 0.1 M phosphate buffer pH=8 containing ciprofloxacin, norfloxacin,
 777 ofloxacin and, diclofenac individually. The adsorption capacity and selectivity of the
 778 KTNR/GCE for other drug analytes were almost three folds lower compared to ciprofloxacin
 779 which showed the highest peak current at a particular 0.98 V potential window, indicating that
 780 the binding selectivity of KTNR specific to the ciprofloxacin molecules. The high selectivity
 781 can be explained by the unique morphology and high catalytic properties of KTNR. However,
 782 the sensor is not at par selective for ciprofloxacin when it was compared with enrofloxacin



783 which showed twice the amount of current signal within the same potential window. Therefore,
 784 the result has provided evidence that KTNR/GCE was selective to other antibiotic classes and
 785 drugs but not enrofloxacin due to its similar nature to ciprofloxacin oxidation. Both are
 786 zwitterionic molecules that exhibit similar results when tested.

787 The effect of common inorganic ions, compounds and, drugs existing in various real matrices
 788 where ciprofloxacin is detected were also investigated through CV. Compounds like dopamine
 789 (DP), uric Acid (UA), urea (UR), ascorbic Acid (AA), glucose (G), and ions, such as Ca^{2+} , Na^{+}
 790 , K^{+} , Mg^{2+} , HCO_3^{-} were chosen to test while their concentrations were hundred times higher
 791 than that of ciprofloxacin, i.e., by adding 1000 μM of interfering compounds/ions and 10 μM
 792 ciprofloxacin in 0.1M phosphate buffer pH = 8, and the results were shown in **Fig. 10(B)**. Also
 793 to check the effects of co-existence of other drugs in real matrices, enrofloxacin, norfloxacin,
 794 ofloxacin and diclofenac were taken into consideration in the same manner by checking with
 795 10 μM concentration along with 10 μM ciprofloxacin. The only exception that occurred is in
 796 case of enrofloxacin where the interference could be seen to be quite high³⁷. Other than that,
 797 the response of the sensor towards bare 10 μM ciprofloxacin solution is quite similar to that
 798 toward the mixture of ciprofloxacin and interference drugs, compounds and ions, suggesting a
 799 very excellent anti-interfering ability of KTNR/GCE even in the micro-environment where the
 800 amount of interference may be remarkably higher than ciprofloxacin. The DPV results indicate
 801 that the present interfering substances have negligible or no influence on the ciprofloxacin
 802 detection in real matrices other than enrofloxacin being present in them. This also owes that
 803 the sensor has excellent recognition ability toward the ciprofloxacin detection owing to the
 804 unique properties of KTNR.



805



806 **Figure 10. (A) Selectivity of the KTNR/GCE for ciprofloxacin (CIP) against enrofloxacin**
 807 **(EF), norfloxacin (NOR), ofloxacin (OFL), and, diclofenac (DCF); (B) Interference test**
 808 **for electrochemical ciprofloxacin (CIP) a determination under influence of other co-**
 809 **existing compounds like dopamine (DP), uric acid (UA), urea (UR), ascorbic acid (AA),**
 810 **glucose (G), and ions such as Ca²⁺, Na⁺, K⁺, Mg²⁺, HCO₃⁻.**

811

812 3.6.9. Validation of KTNR/GCE for ciprofloxacin detection in complex matrices

813 The ultrasensitive detection of trace ciprofloxacin in complex matrices existing in animal,
 814 environment and human were achieved by the standard addition method. The results are
 815 tabulated in **Table 3**. The developed KTNR based ciprofloxacin sensor was successful in
 816 detecting the trace analyte concentrations in the tested complex matrices of real samples.
 817 Recoveries ranging between 40.13 % to 124 %, are practically viable analytical results for a
 818 potential electrochemical sensing device. Spiked samples of milk and ganga water showed low
 819 recovery rate indicating the possibility of some interfering compounds being adsorbed or there
 820 may be an incident of electro-polymerization of pollutants that causes fouling at the electrode
 821 surface which in-turn is hindering the current flow. However, honey, egg and most importantly
 822 simulated body fluid (SBF) show excellent recovery rate indicating the efficacy of the proposed
 823 sensing device.

824 **Table 3. Electrochemical trace detection of ciprofloxacin spiked in milk, honey and egg,**
 825 **Ganga water, marine water, soil and organic fertilizer samples using KTNR modified**
 826 **electrochemical sensor.**

Samples	Spiked (μM)	Detected (μM)	Variance	STD	RSD (%)	Recovery (%)
Milk	0	0	0	0	0	0
	15	6.02	40.3202	6.349819	60.41693	40.13333
Honey	0	0	0	0	0	0
	15	15.3	0.045	0.212132	1.400211	102
Egg	0	0	0	0	0	0
	15	14.6	0.08	0.282843	1.911099	97.33333
Marine Water	0	0	0	0	0	0
	15	6.56	35.6168	5.967981	55.36161	43.73333
Ganga Water	0	0	0	0	0	0
	15	18.6	6.48	2.545584	15.15229	124
Organic Fertilizer	0	0	0	0	0	0
	15	11.4	6.48	2.545584	19.28473	76



Soil	0	0	0	0	0	0
	15	8.3	22.445	4.737615	40.66623	55.33333
SBF	0	0	0	0	0	0
	15	15.1	0.005	0.070711	0.469838	100.6667

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827

828 **4. Conclusion**

829 In conclusion, this research demonstrated the successful synthesis, characterization and
 830 fabrication of a novel 2D MXene-derived potassium titanate nanoribbon-based electrochemical
 831 sensor for the ultrasensitive detection of ciprofloxacin. The sensor exhibited exemplary
 832 performance in all electrochemical voltammetric techniques (CV, DPV, and SWV) achieving
 833 a remarkably low LOD and LOQ while being highly selective for other antibiotics and
 834 interfering species except enrofloxacin at the particular pH 8. Notably, the sensor demonstrated
 835 practical reliability in complex matrices mainly in egg, honey, and SBF, making it a promising
 836 candidate for real-world applications in on-site food safety, environmental monitoring, and
 837 healthcare diagnostics. Further studies could focus on optimizing sensor stability and exploring
 838 miniaturization techniques for technology readiness level (TLR) upgradation and on-site
 839 detection to combat antimicrobial resistance against ciprofloxacin, thus contributing to One
 840 Health and Sustainable Development Goals.

841

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Data Availability Statement

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To,

The Editor-in-Chief
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The data will be made available on request.

With Kind regards

Dr. Vimala Raghavan

Dr. Sarvesh K. Pandey

