

# Analytical Methods

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## Development and validation of dot-ELISA on modified cellulose filter paper: A simplified novel approach

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## Abstract

Graft polymerization of glycidyl methacrylate (GMA) onto cellulose filter paper (CFP) was carried out by free-radical polymerization process and grafted surfaces were characterized by standard polymer characterization techniques. Reactional profiles of GMA and cellulose were elucidated using molecular mechanics energy relationships by exploring the spatial disposition of molecular entities. CFP-g-GMA surfaces with different graft levels of GMA were evaluated and standardized for their application in dot-ELISA in two steps. In the first step, sensitivity, specificity and reproducibility of the assay on GMA grafted cellulose surface was evaluated through a model system using rabbit anti-goat IgG, goat anti-rabbit IgG and goat anti-rabbit IgG HRP-conjugate. Variety of blocking agents and different levels of conjugate dilutions were screened to standardize the assay. Rabbit-anti-goat IgG antibody at a concentration as low as  $6\text{ngmL}^{-1}$  was efficiently detected on CFP with 70% GMA graft level using 5% skimmed milk as blocking agent and antispecies-IgG-peroxidase conjugate diluted 2000 times. In the second step, sensitivity and specificity of the developed system was established with human blood and finally used to identify the source of mosquito blood meal, an important parameter in epidemiological studies, particularly in determining the role of mosquito in malaria transmission. Time duration of standardized assay reduced to 90 min compared to 3-4 h of usual dot-ELISA. For mass screening, as for epidemiological studies in field conditions, sheet of higher dimensions – instead of small strips as utilized by the researchers for laboratory studies – can be used for multiple spotting.

**Keywords:** *Dot-enzyme linked immunosorbent assay; Glycidyl methacrylate; Cellulose filter paper; Blocking agents; Mosquito blood meal; Molecular mechanics energy relationships.*

## 1. Introduction

Immunodiagnostic methods have long been used in the diagnosis of various diseases. Among these, the solid phase – heterogeneous – immunoenzymatic (IE) assays have become one of the most powerful tools for the laboratory diagnosis of infectious diseases, autoimmune disorders, immune allergies and neoplastic diseases. Such immunoassays require a solid phase, to which are adsorbed the antigen/antibody that recognizes and binds to its complementary antibody/antigen in the sample. The result of binding reaction between the antibody and analyte (antigen) is made visible by means of enzymatic markers.<sup>1</sup> These solid phase IE assays include conventional ELISA (enzyme linked immunosorbent assay) and dot-ELISA which generally utilizes polystyrene (PS) plates and nitrocellulose (NC) membrane, respectively, as the solid phase, to which the adsorption of biomolecules is due to intermolecular attraction forces.<sup>2-4</sup> But these adsorption based procedures suffer from non-specific binding and desorption of biomolecules during incubation and washing steps.<sup>5</sup> It has also been observed that short peptides often do not bind well to the surface of PS-based microtiter plates in solid phase immunoassay.<sup>6,7</sup> In addition, PS plates pose an environmental hazard as, although being disposable, they produce huge amount of carbon monoxide and other toxic gases during incineration due to thermal degradation of PS.<sup>8,9</sup> Modified PS plates, developed and reported by a number of research groups to overcome some of the problems, still have certain drawbacks.<sup>7,10,11</sup> NC membrane on the other hand is costly and requires surface treatment for better attachment of immunoreactants.<sup>12</sup>

A range of synthetic (polypropylene, PS, nylon) and natural polymers (chitosan and cotton) have long been investigated for their use as matrix and support material for enzyme immobilization and in immunoassays.<sup>2,5,13-16</sup> However, in recent years there has been considerable interest and stress on the use of biodegradable polymers. Different polymers, apart from chitosan and cotton, are therefore being explored and applied after suitable modification to have potential end use in these areas. A highly selective glucose biosensor has been prepared by immobilization of glucose oxidase on biodegradable  $\gamma$ -polyglutamic acid film.<sup>17</sup> Microtiter plates based on renewable resource, polylactic acid (PLA) have been patented and launched recently. These are reported to be fully biodegradable and possess an antigen binding efficiency equally well or better than conventionally used polystyrene.<sup>8</sup> An innovative immunostick-cuvette-system has also been reported, in which the stick is made of

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3 the renewable poly(hydroxybutyrate).<sup>8</sup> Cellulose derivatives with different surface properties  
4 that has been used as matrix support include cellulose acetate, amino cellulose acetate,  
5 cellulose nitrate, etc.<sup>18-20</sup>  
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9 Filter paper, a form of cellulose - a natural carbohydrate polymer - is an inexpensive,  
10 easily available, degradable and renewable biopolymer with very good mechanical properties.  
11 However, its application in several technologically important fields is limited due to the lack  
12 of reactive functional sites and thus the desirable surface properties. The use of cellulose-  
13 based materials could thus be extended to new areas by altering and tailoring its chemical and  
14 physical properties through the incorporation of functional moieties onto its surface. Grafting  
15 is one of the promising and attractive methods to introduce a variety of functional groups to a  
16 polymer. Of the various techniques used for grafting, chemical grafting is generally reported  
17 to give higher graft levels and has efficiently been used to graft monomers like acrylamide on  
18 polyethylene oxide, methyl methacrylate (MMA) onto silk sericin, poly(ether glycol) methyl  
19 ether methacrylate on polyether sulfone, poly(N-phenylethylene diamine methacrylamide) on  
20 PS microplate and acrylamide on CFP.<sup>21-26</sup>  
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24 Glycidyl methacrylate (GMA) is an interesting monomer with pendant epoxy groups that  
25 directly reacts with sulfhydryl, amino and carboxyl groups to form stable covalent bonds with  
26 biomolecules.<sup>27-32</sup> The monomer has therefore been used for grafting and such epoxy-  
27 modified polymer surfaces have also been reported to be resistant against hydrolysis and  
28 stable during long storage periods.<sup>33-36</sup>  
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31 Dot-ELISA - a highly versatile solid phase immunoassay for antibody or antigen detection  
32 - has been widely employed in several serological tests because of its sensitivity and  
33 specificity in addition to being practical and less expensive diagnostic test, not requiring  
34 either sophisticated equipment or trained technical personnel.<sup>37</sup> The present paper aims at the  
35 evaluation and standardization of GMA grafted CFP (with GMA graft % from 10 to 100),  
36 developed and reported earlier by the same group of investigators, in dot-ELISA.<sup>38</sup> The paper  
37 also describes the practical application of CFP-g-GMA surfaces for identification of human  
38 blood and the source of mosquito blood meal (species on which mosquito fed).  
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## 54 55 56 **2. Experimental**

### 57 58 59 **2.1 Materials**

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3 Glycidyl methacrylate (GMA), Bovine serum albumin (BSA), Tween-20, 4-chloro-1-  
4 naphthol and hydrogen peroxide (H<sub>2</sub>O<sub>2</sub>) were purchased from Sigma-Aldrich (USA) and used  
5 as received. The CFP (No. 393) used for grafting was obtained from Sartorius, Germany.  
6  
7 Nitrocellulose membranes (0.45µm pore size) were supplied by Advanced Microdevices  
8 (pvt.), Ambala Cantt, India. Cerric ammonium nitrate, nitric acid, acetone and all other  
9 analytical grade chemicals were purchased from CDH, India. Immunoglobulins (Ig): Goat  
10 anti-rabbit (GAR IgG), rabbit anti-goat (RAG IgG), and horseradish peroxidase (HRP)  
11 conjugated to: GAR IgG, RAG IgG and rabbit anti-human (RAH) IgG were purchased from  
12 Bangalore Genei, India.

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14 Mosquito blood meal samples of laboratory reared *A. stephensi* deliberately fed on human  
15 and buffalo host were taken from Malaria Research Centre (ICMR), New Delhi, India. Blood  
16 samples directly taken from human and buffalo were also provided by the same centre. All  
17 the buffers were prepared in Milli Q water. All samples prepared in % were taken w/v, unless  
18 otherwise stated.

## 29 2.2 Graft polymerization

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31 Grafting of GMA monomer on CFP was carried out by chemical initiation using cerric  
32 ammonium nitrate (CAN) as an initiator. Grafting was undertaken in a glass ampoule under  
33 nitrogen atmosphere as detailed in earlier publication and represented in Scheme 1.<sup>38</sup> GMA  
34 grafted CFP was cut in thin strips to be used for dot-ELISA.

## 40 2.3 Characterization

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42 GMA grafting on CFP was confirmed by various standard techniques ATR-FTIR, SEM and  
43 TGA analysis.<sup>38</sup> Thickness of the ungrafted and GMA grafted CFP samples were measured  
44 using an Essdiel Thickness gauge at 20 gfc<sup>2</sup> pressure.

## 49 2.4 Static lattice atomistic simulations

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51 Molecular simulations were performed using commercial softwares: HyperChem<sup>TM</sup> 8.0.8  
52 Molecular Modeling System (Hypercube Inc., Gainesville, Florida, USA) and ChemBio3D  
53 Ultra 11.0 (Cambridge Soft Corporation, Cambridge, UK). The structure of poly(GMA) was  
54 built in its syndiotactic stereochemistry as 3D model using ChemBio3D Ultra while the  
55 structure of the cellulose (CEL) was generated using the built-in polysaccharide builder  
56 module of HyperChem. The models were energy-minimized using a progressive-  
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4 convergence-strategy where initially the MM+ force field was used followed by energy-  
5 minimization using the Amber 3 (Assisted Model Building and Energy Refinements) force  
6 field. The conformer having the lowest energy was used to create the polymer-polymer  
7 complex. A complex of one polymer molecule with another was assembled by disposing the  
8 molecules in a parallel way, and the same procedure of energy-minimization was repeated to  
9 generate the final models: PGMA, CEL, CEL-CEL (CEL<sub>2</sub>) and PGMA-CEL<sub>2</sub>. Full geometry  
10 optimization was carried out in vacuum employing the Polak–Ribiere conjugate gradient  
11 algorithm until an RMS gradient of 0.001 kcal/mol was reached. For molecular mechanics  
12 calculations in vacuum, the force fields were utilized with a distance-dependent dielectric  
13 constant scaled by a factor of 1. The 1-4 scale factors were electrostatic 0.5 and van der  
14 Waals 0.5.<sup>39</sup>

#### 23 24 **2.4.1 Molecular mechanics assisted model building and energy refinements**

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26 A molecular mechanics conformational searching procedure was employed to acquire the  
27 data employed in the statistical mechanics analysis, and to obtain differential binding energies  
28 of a Polak–Ribiere algorithm and to potentially permit application to polymer composite  
29 assemblies. MM+ is a HyperChem modification and extension of Norman Allinger's  
30 Molecular Mechanics program MM2, whereas AMBER is a package of computer programs  
31 for applying molecular mechanics, normal mode analysis, molecular dynamics and free  
32 energy calculations to simulate the structural and energetic properties of molecules.<sup>40,41</sup>

#### 33 34 35 36 37 38 39 40 41 **2.5 Evaluation and standardization of CFP-g-GMA surface for dot-ELISA with model** 42 **system**

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44 GMA grafted CFP strips were dipped in PBS (pH 7.4) for 5 min and dried at 37°C for next 10  
45 min. Various dilutions of RAG IgG (prepared in PBS) were spotted on to the strips as 2μL  
46 spots each, while PBS was used as control dot. The applied dots were allowed to air dry at  
47 37°C for 20 min. Non-specific protein binding sites left on the strips were then blocked by  
48 incubating in 10 mL of blocking solution for 30 min at 37°C. Strips were then briefly washed  
49 in PBS-Tween (0.05%) to remove the blocking solution and thereafter incubated with 10mL  
50 of peroxidase labeled antispecies IgG conjugate (GAR IgG HRP) for 30 min at 37°C. The  
51 unbound conjugate was aspirated off and strips were washed with PBS-Tween for 30 s with  
52 gentle shaking. Finally, the strips were dipped in covered tray containing the freshly prepared  
53 4-chloro-1-naphthol substrate solution: 6 mg of 4-chloro-1-naphthol dissolved in 2 mL  
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methanol and added to 8 mL PBS containing 100  $\mu\text{L}$  of 3%  $\text{H}_2\text{O}_2$  (v/v). Reaction was allowed to proceed for 5 min in the dark to develop the color, where after the enzyme reaction was stopped by washing with water. Positive results were indicated by the development of a purple-blue color on the spotted site. Sensitivity of the polymeric surfaces was evaluated by spotting serial dilutions of RAG IgG as model antibody in a concentration range from 200  $\text{ngmL}^{-1}$  to 6  $\text{ngmL}^{-1}$ . Different blocking agents like ethanolamine, bovine serum albumin (BSA) and skimmed milk were tried in varied percentages for their efficacy to block the remaining non-specific sites. GAR IgG HRP-conjugate was used in dilutions ranging from 1:1000 to 1:5000. In order to optimize the time duration of the immunoassay, the incubation periods at various steps were varied from 15 min to 1 h. Specificity of the assay was tested using GAR IgG HRP-conjugate against RAG IgG and GAR IgG. Two concentrations (100  $\text{ngmL}^{-1}$  and 50  $\text{ngmL}^{-1}$ ) of both the antibodies were spotted onto the polymeric strip followed by the usual assay steps with standardized solutions.

## 2.6 Specimen of blood samples and preparation of elutes

Human and buffalo blood samples were taken and spotted on separate filter papers as 10  $\mu\text{L}$  dots. The spotted specimen samples were dried at 37°C for one hour and then stored in desiccator at 4°C until further use. When required, a filter paper disc of 10 mm diameter was cut from the middle of a blood spotted specimen sample using a paper punch. All the blood spotted disc samples were then eluted in 100  $\mu\text{L}$  of PBS, pH 7.4 at room temperature for 1h. Eluate thus obtained was serially diluted in PBS from 2 to 10,000-fold (1:1 to 1:10,000). Samples were also taken from different mosquitoes, which have fed either on human or buffalo, by quashing the mosquitoes onto the whatman filter paper no.1. Drying, storage, elution and dilution of mosquito blood meal samples taken on filter paper was done as mentioned above for other blood samples. Specificity test with human and buffalo blood and the identification of the source of mosquito blood meal was carried out at the best dilution identified with human blood sensitivity studies.

## 2.7 Dot-ELISA on CFP-g-GMA surface for identification of human blood and mosquito blood meal source

GMA grafted CFP strips were dipped in PBS solution for 5min and dried at 37°C for another 10 min. Micropipette was used to transfer various eluted blood samples (2  $\mu\text{L}$ ) onto the strips and air dried at 37°C for 20 min. Samples spotted on strips were washed with PBS-Tween

twice for 30 s each with gentle shaking. The strips were then incubated with 10 mL of 5% skimmed milk for 30 min for blocking nonspecific protein binding sites. After removing the blocking solution, strips were incubated with 10 mL of peroxidase labelled RAH IgG HRP-conjugate for 30 min at 37°C. The unbound conjugate was washed with PBS-Tween (30 s) at 37°C and the strips were dipped in dark in 10 mL of freshly prepared chloro-naphthol substrate solution and the reaction was stopped by washing with water. To determine the sensitivity of grafted CFP strips for human blood, the eluted and then serially diluted human blood samples were applied as 2  $\mu$ L dots followed by above mentioned dot-ELISA steps. For the specificity test, RAH IgG HRP-conjugate was tested against eluates from human and buffalo blood samples taken separately. From both the type of blood samples (human and buffalo) two dilutions of the eluate (100 and 1000-fold) were spotted each of 2  $\mu$ L, followed by above mentioned dot-ELISA steps.

Mosquito blood meal source identification with modified CFP surface was also carried out utilizing samples of mosquito blood meal of known source (human or buffalo). Blood meal eluate for spotting was used at 100-fold dilution and RAH IgG HRP-conjugate was used for detection.

### 3. Results and discussion

#### 3.1 Graft polymerization

Grafting of GMA monomer on CFP was carried out by free radical polymerization using CAN as chemical initiator in aqueous medium. The probable reaction mechanism is presented in Scheme 1 and detailed studies of various parameters of grafting *i.e.* concentrations of monomer (1 to 10%) and initiator ( $1.0-6.0 \times 10^{-3} \text{ molL}^{-1}$ ), the polymerization temperature (40-70°C) and time (5-30 min) is reported in our earlier publication.<sup>38</sup> The degree of grafting of GMA onto cellulose filter paper varied from 10 to 102 $\pm$ 3%, under different reaction conditions and a maximum of 102 $\pm$ 3% was recorded at 60°C in 25 min with  $4 \times 10^{-3} \text{ molL}^{-1}$  of initiator (CAN) concentration and 5% GMA monomer.

#### 3.2 Characterization

The GMA grafting was confirmed by chemical analysis of ungrafted and various grafted surfaces using ATR-FTIR. Apart from the characteristic absorptions of filter paper surface at 3400 and 2920  $\text{cm}^{-1}$  because of O-H stretching and C-H stretching vibrations respectively and at 1426 and 1023  $\text{cm}^{-1}$  of C-H bending and O-H bending respectively, the grafted surface

exhibited additional peaks characteristic of GMA (Fig. 1(a)). The peaks at 906 and 845  $\text{cm}^{-1}$  are assigned to epoxide group while the peak at 1730  $\text{cm}^{-1}$  corresponds to the carbonyl functional group of grafted GMA. The scanning electron micrographs showed an introduction of heterogeneity along and across the fibres which increased with the increase in graft level which may be the outcome of incompatibility of the hydrophobic poly(GMA) graft with the hydrophilic cellulosic filter paper matrix (Fig. 1(b)). The thickness of unmodified CFP was recorded as 0.19 mm which increased from 0.21 to 0.54 mm with an increase in the graft level from 10 to 100% (Fig. 1(c)).

### 3.3 MMER analysis

Molecular mechanics energy relationship (MMER), a method for analytico-mathematical representation of potential energy surfaces, was used to provide information about the contributions of valence terms, noncovalent Coulombic terms, and noncovalent van der Waals interactions for polymer/polymer interactions. The MMER model for potential energy factor in various molecular complexes can be written as:

$$\mathbf{E}_{\text{molecule/complex}} = V_{\Sigma} = V_b + V_{\theta} + V_{\varphi} + V_{ij} + V_{hb} + V_{el} \dots (1)$$

where,  $V_{\Sigma}$  is related to total steric energy for an optimized structure,  $V_b$  corresponds to bond stretching contributions (reference values were assigned to all of a structure's bond lengths),  $V_{\theta}$  denotes bond angle contributions (reference values were assigned to all of a structure's bond angles),  $V_{\varphi}$  represents torsional contribution arising from deviations from optimum dihedral angles,  $V_{ij}$  incorporates van der Waals interactions due to non-bonded interatomic distances,  $V_{hb}$  symbolizes hydrogen-bond energy function and  $V_{el}$  stands for electrostatic energy.

In addition, the total potential energy deviation,  $\Delta E_{\text{total}}$ , was calculated as the difference between the total potential energy of the complex system and the sum of the potential energies of isolated individual molecules, as follows:

$$\Delta \mathbf{E}_{\text{Total(A/B)}} = \mathbf{E}_{\text{Total(A/B)}} - (\mathbf{E}_{\text{Total(A)}} + \mathbf{E}_{\text{Total(B)}}) \dots (2)$$

$$\mathbf{E}_{\text{GMA}} = 543.925V_{\Sigma} = 2.444V_b + 511.545V_{\theta} + 27.634V_{\varphi} + 2.302V_{ij} \dots (3)$$

$$\mathbf{E}_{\text{CEL}} = -4.641V_{\Sigma} = 1.477V_b + 8.718V_{\theta} + 6.145V_{\varphi} + 13.110V_{ij} - 34.094V_{el} \dots (4)$$

$$\mathbf{E}_{\text{CEL2}} = -20.212V_{\Sigma} = 1.404V_b + 8.624V_{\theta} + 7.617V_{\varphi} + 4.778V_{ij} - 42.036V_{el} \dots (5)$$

$$E_{\text{GMA-CEL}_2} = 475.869V_{\Sigma} + 5.275V_b + 526.026V_{\theta} + 44.213V_{\varphi} - 9.053V_{ij} - 90.592V_{el} \dots (6)$$

$$\Delta E = -47.844 \text{ kcal mol}^{-1}$$

The molecular stability can then be estimated by comparing the total potential energies of the isolated and complexed systems. If the total potential energy of the complex is smaller than the sum of the potential energies of isolated individual molecules in the same conformation, the complexed form is more stable and its formation is favoured.<sup>42</sup>

### 3.3.1 Formation of polymeric assemblies

The GMA was modeled as a polymer - PGMA - with monomer chain length of 4 monomer contents for better efficiency in terms of computational time and modeling space. The cellulose based polysaccharide platform was built by modeling two parallel cellulose chains with 4 oligosaccharide contents in each chain. The energetic profiles of the formation of the polymeric assemblies viz. CEL-CEL (CEL<sub>2</sub>) and PGMA-CEL<sub>2</sub>, in vacuum, are represented by energy equations 3-6 and the conformational profile for the same are depicted in Fig. 2. The energy equations demonstrated that the polymeric systems were highly stabilized in terms of respective bonding and non-bonding energy factors. The energy stabilization with negative steric energies in all case of PGMA-CEL<sub>2</sub> suggested good compatibility and reactivity. Additionally, the geometric conformation and the hydrogen bonding suggest the involvement of C3-C2 bond of cellulose with the reactive functionalities of PGMA. The geometric stabilization displayed  $\Delta E \sim -48 \text{ kcal mol}^{-1}$  wherein the PGMA-CEL<sub>2</sub> complex was destabilized by all bonding energy contributions viz. bond stretching, bond angle and torsional constraints and stabilized by van der Waals forces and electrostatic interactions (non-bonding interaction). Strikingly, introduction of the acrylic polymer introduced deviations from optimum dihedral angles and bond positions with values in the range of  $\sim 2 \text{ kcal mol}^{-1}$  to  $\sim 10 \text{ kcal mol}^{-1}$  which lead to a highly strained molecular geometry. This may explain the experimental observation “heterogeneity along and across the fibres with an increase in graft level which may be the outcome of incompatibility of the hydrophobic poly(GMA) graft with the hydrophilic cellulosic filter paper matrix”. However, the van der Waals interactions ( $\sim -15 \text{ kcal mol}^{-1}$ ) and electrostatic contributions ( $\sim -50 \text{ kcal mol}^{-1}$ ) added to the stabilization and retrieved high negative values which may be due to PGMA acting as filler in the space lattice of the binary system (Fig. 2). This in turn explains the notion of “an increase in adsorption properties of CFP with grafted GMA” as predicted in the experimental

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3 discussion. Furthermore, a close look at the molecular complex reveals the presence of both  
4 inter- and intra-molecular H-bonding. These non-bonding interactions, from van der Waals  
5 forces to electrostatic contributions, may be due to the hydrophobic interactions arising from  
6 the inclusion of PGMA which can further provide covalent attachment to the antibodies  
7 through the epoxy groups, not involved in the bonding with CEL, leading to the applicability  
8 of PGMA-CEL as a potential substrate for evaluation in ELISA.  
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### 14 **3.4 Evaluation and standardization of CFP-g-GMA surface for dot-ELISA with model** 15 **system** 16 17

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19 For a reliable immunoassay there has to be a balance between sensitivity, background noise  
20 and specificity of the solid phase. Sensitivity of a matrix broadly depends on the surface  
21 binding efficacy of the antigen/antibody, blocking condition (type and amount of blocking  
22 agent) and the concentration of the conjugate used. A model system was designed using  
23 RAG, GAR immunoglobulins and their corresponding HRP-conjugates to standardize the  
24 dot-ELISA assay on the modified CFP polymeric surface.  
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#### 31 **3.4.1 Effect of blocking agent** 32

33 Prevention of non-specific binding of reagents to the matrix is important for a solid phase  
34 immunoassay. Blocking of all protein-binding sites left on the surface after sample spot  
35 application is important and achieved using a proper blocking agent in an appropriate amount  
36 as insufficient blocking may result in a high background while over-blocking may decrease  
37 the sensitivity. For a novel surface before proceeding for immune reaction, its important to  
38 standardize the blocking condition (type and amount of blocking agent). Three different  
39 blocking agents had been investigated in varying percentages (1%, 2% and 5%) for their  
40 efficiency in blocking GMA grafted CFP surface and the results are presented in Fig. 3(a).  
41 Ethanolamine, a commonly employed blocking agent for the epoxy groups (present in grafted  
42 GMA on CFP), was able to block the surface partially. A better signal to noise ratio was  
43 observed at an ethanolamine amount of 1%. For all the concentrations of ethanolamine used,  
44 a background noise was always present, which was higher for modified CFP with low  
45 grafting level. Although ethanolamine is able to react with and block the non-specific GMA  
46 sites present on the grafted CFP, it is not equally effective for the blocking of cellulosic  
47 component of the matrix. This results in background noise when ethanolamine is used as a  
48 blocking agent. BSA, as a blocking agent gave a better signal to noise ratio than  
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3 ethanolamine, and was best at a usage of 2%. These results indicate BSA as a better blocking  
4 agent than ethanolamine for both GMA and cellulose. Although, BSA is generally used for  
5 blocking NC membrane – the widely used membrane for dot-ELISA, its blocking effect on  
6 GMA grafted CFP was although not very profound but, satisfactory. The signals (colored  
7 dots) obtained with different percentages of skimmed milk were almost comparable but, a  
8 higher background noise was observed with 1% skimmed milk, which reduced with an  
9 increase in amount to 2%. Further increase in skimmed milk amount to 5% was able to block  
10 the surface completely without dampening the color dot intensity. This established skimmed  
11 milk as the best blocking agent for the GMA grafted CFP surface at a concentration of 5%.

### 12 13 14 15 16 17 18 19 20 21 **3.4.2 Effect of conjugate dilution**

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23 The conjugate in dot-ELISA is almost always antibody linked to an enzyme. The antibody is  
24 specific to and probes for the analyte of interest in the sample spot while the linked enzyme in  
25 conjugate finally produces a visible signal with chromogenic substrate. A balanced  
26 concentration of enzyme conjugate is required because increase in conjugate concentration to  
27 attain higher sensitivity can lead to higher background and reduced specificity. Conjugate  
28 (GAR IgG–HRP) was therefore diluted to various extents ranging from 1:1000 to 1:5000, in  
29 order to determine the optimal dilution for the system under investigation. All the dilutions  
30 were used in combination with all the three blocking agents at their best blocking  
31 concentration (%) determined in previous section (3.4.1). Conjugate dilutions showed  
32 different results with different blocking agent for detecting various concentrations of RAG  
33 IgG antibody spotted as sample on CFP-g-GMA. The cumulative effect of HRP-conjugate  
34 dilutions with ethanolamine, BSA and skimmed milk as blocking agent has been shown in  
35 Fig. 3(b) (i-iii). With ethanolamine (1%) blocked surfaces, the conjugate dilution of 1:1000 to  
36 1:5000 gave more or less similar results in terms of the lower limit of the analyte (RAG-IgG)  
37 detected ( $25 \text{ ngmL}^{-1}$ ). It is assumed that the lower dilutions of 1:1000 and 1:1500 would have  
38 been able to identify and generate signals for even lower antibody concentrations, but, due to  
39 increased background noise at these dilutions, the positive signals (colored dots) were not  
40 visible. At an increased dilution of 1:2000, the background noise decreased and the signal  
41 intensity remained comparable, while, a further dilution of 1:5000 reduced the intensity of  
42 signals (Fig. 3(b)-i). BSA (2%) blocked CFP-g-GMA strips gave a higher background noise  
43 at a conjugate dilution of 1:1000 which decreased progressively on further dilution from  
44 1:1500 to 1:5000. As with ethanolamine blocked surfaces, the positive signals on strips  
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3 incubated with 1:1000 conjugate dilution were visible only at higher analyte concentration  
4 spots (Fig. 3 (b)-ii). Due to an added effect of increase in conjugate dilution and better BSA  
5 blocking much of the background noise was reduced at a dilution of 1:1500 and 1:2000. The  
6 colored spots were visible for spotted antibody concentration of  $12 \text{ ngmL}^{-1}$ , although the  
7 intensity of these dots was low. When skimmed milk (5%) blocked CFP-g-GMA surfaces  
8 were evaluated in combination with conjugate dilutions, a significant advance in signal to  
9 background noise was observed at a dilution of 1:1500 and a clear background was obtained  
10 at dilutions above 1:2000 (Fig. 3 (b)-iii). As seen in figure, the color intensity of dots  
11 remained comparably same upon increase in dilution from 1:1500 to 1:2000 but on further  
12 dilution to 1:5000 the intensity decreased.  
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### 22 **3.4.3 Sensitivity**

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24 The visibility of a dot depends on the contrast of the color generated against the background  
25 and is thus dependent on the concentration of analyte in a sample spot. The sample is  
26 therefore applied in small volumes of concentrated analyte and the minimum detectable  
27 concentration i.e. sensitivity of any assay system is determined by applying serial dilutions of  
28 the analyte. The GMA grafted CFP with different percent grafting were therefore evaluated  
29 for their sensitivity by using antibody (RAG-IgG) dilutions from 200 to  $6 \text{ ngmL}^{-1}$  in  
30 combination with various blocking agents (used at varied concentrations) and conjugate  
31 dilutions. The cumulative influence of reagents on the detection of antibody spots of different  
32 concentrations applied onto the surface of CFP-g-GMA is shown in Fig. 3(b). With  
33 ethanolamine (1%) as a blocking agent, the highest sensitivity recorded is  $25 \text{ ngmL}^{-1}$  with  
34 fairly clear background at a conjugate dilution of 1:2000. Although the sensitivity remained  
35 comparably same at a higher dilution of 1:5000, the color intensity of the dots weakened (Fig.  
36 3(b)-i). When BSA (2%) was used as a blocking agent the same conjugate dilution of 1:2000  
37 showed improved sensitivity and was able to detect the antibody spot of  $12 \text{ ngmL}^{-1}$ , although  
38 the color intensity of the dots was very low. This established BSA as a better blocking agent  
39 than ethanolamine, for CFP-g-GMA surfaces at a conjugate dilution of 1:2000. On increasing  
40 the conjugate dilution to 1:5000 a decline in the sensitivity of the surface was recorded. (Fig.  
41 3(b)-ii). Skimmed milk at a concentration of 5% effectively blocked the non-specific sites on  
42 the modified CFP and gave the best signal to noise ratio when used in combination with  
43 conjugate diluted to 1:2000. With this set of reagents the intensity of color developed for  
44 RAG-IgG concentration of  $200 \text{ ngmL}^{-1}$  down to  $12 \text{ ngmL}^{-1}$  were strong and very clearly  
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visible on the surface of modified CFP (Fig. 3(b)-iii). The signals at  $6 \text{ ngmL}^{-1}$  antibody concentration were although weak but detectable and visible against the clear background of the developed matrix. The optimized assay protocol for dot-ELISA on GMA grafted CFP therefore required 5% skimmed milk as the blocking agent, a peroxidase labeled antispecies IgG conjugate diluted 2000 times and the standardized incubation period of 30 min in each step. Under these conditions the sensitivity of the surface observed was  $6 \text{ ngmL}^{-1}$ .

The results of the assay performed on modified CFP, with varying degree of grafting (ranging 10-100%), in accordance to the standardized and established dot-ELISA protocol is presented in Fig. 3(c). As seen in this figure, no defined color dots developed on the CFP surface with grafting level as low as 10%, instead the whole strip takes up the color. On an increase in grafting level to 20%, the color dots become visible but show a diffused boundary, which becomes defined only on the GMA grafted CFP with graft level above 20%. Although the dots with clear boundaries are visible on modified CFP with graft level of 40 to 60%, the dots obtained are larger. A progressive decrease in the size of the dots is observed with an increase in graft level from 40 to 70%, showing confined and sharp dots on modified CFP with GMA graft level of 70% and above. This observation can be explained by the varying protein binding ability of the modified CFP surface with varying graft levels of GMA. The grafted GMA is believed to alter the adsorption properties of CFP on one hand while providing covalent attachment to the antibodies on the other. Since the antibody binding properties of CFP with lower graft level is low, the antibody migrates with the buffer and on color development with the substrate, either the complete matrix takes up the color or larger dots are observed. Additionally, because of the diffusion of sample antibody to larger areas the color intensity dampens. Modified CFP with higher graft level exhibit higher antibody binding properties as can be seen from the development of compact and defined dots (Fig. 3(c)). Best results are visible at the CFP-g-GMA surface with 70% graft level. The surface show good intensity color dots due to the confinement of spotted antibody solution to a smaller region and thus gives the best signal to noise ratio which is comparable to that on standard NC membrane. Good results obtained with GMA grafted CFP at 70% graft level can be explained due to the optimum balance attained between the hydrophobic grafted GMA and hydrophilic properties of the cellulosic matrix, which makes the GMA grafted CFP a suitable matrix for dot-ELISA. Moreover, GMA grafted on CFP provides partial covalent attachment to the antibodies through its active epoxy group and also introduces hydrophobicity to the surface which controls the excessive wicking action of the CFP matrix. The level of

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3 hydrophilicity and adsorption capacity present at 70% GMA grafted CFP due to the inherent  
4 hydrophilic property of CFP backbone is sufficient in providing better diffusion of antibodies  
5 to the matrix. It may also have a role in building a hydrophilic microenvironment around the  
6 hydrophobic GMA in order to maintain the conformational stability of the antibodies attached  
7 to CFP-g-GMA matrix. On increase in graft level beyond 80% the background noise  
8 reappears; this reduces the dot visibility especially at lower antibody concentrations. This  
9 background noise may be attributed to the incomplete blocking due to the highly hydrophobic  
10 nature of the surface (at 100% graft level) which hinders the diffusion of the blocking agent  
11 to the active sites of the matrix.  
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19 The GMA grafted CFP with 70% graft level was therefore established as the best and most  
20 appropriate matrix for the dot-ELISA at optimized and standardized conditions of: 5%  
21 skimmed milk blocking agent, a peroxidase labeled antispecies IgG conjugate diluted 2000  
22 times and the standardized incubation period of 30 min in each step. The developed matrix  
23 has also been compared with the conventionally used NC membrane for dot-ELISA in Table  
24 1. All further experiments were carried out with 70% GMA grafted CFP matrix and the  
25 results of all dot-ELISA experiments undertaken with the model system are presented on this  
26 surface only.  
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### 33 34 **3.4.4 Specificity**

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37 Dot-ELISA specificity test with 70% GMA grafted CFP matrix were conducted for GAR IgG  
38 HRP-conjugate against RAG IgG and GAR IgG and the results are presented in Fig. 3(d). As  
39 can be seen, the color development was clearly observed on both the spots (50 and 100 ngmL<sup>-1</sup>)  
40 of RAG IgG while there was no color development with GAR IgG. The result obtained is  
41 as expected because GAR IgG HRP conjugate used is complementary to RAG IgG and  
42 therefore binds specifically to RAG IgG only and not GAR IgG. This confirms the specificity  
43 of the CFP-g-GMA surface, showing no cross reactivity.  
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## 50 **3.5 Dot-ELISA for detection of human blood**

### 51 52 **3.5.1 Sensitivity**

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55 The results of the sensitivity (lowest detectable limit) of the CFP-g-GMA surface for human  
56 blood (antibodies present in human blood) are given in Table 2 and shown in Fig. 4. The  
57 RAH IgG HRP-conjugate was used which specifically binds to human antibodies. The human  
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blood eluate dilutions ranging from 10 to 100-fold gave strong positive results while any further dilution dampened the color intensity of the dots and finally showed no result at a dilution of 1:10,000. Although the color intensity of dots obtained with neat eluate and that of 2-fold diluted eluate was good, the dots obtained with these eluates were diffuse. This diffuse dot formation may be the result of the presence of higher concentration of antibodies in the sample. The results thus established that a 0.1  $\mu$ L dot of blood on filter paper disc, eluted with 100  $\mu$ L of PBS is sufficient to be identified through dot-ELISA on the developed GMA grafted CFP matrix. The sensitivity results of developed matrices with human blood have been compared to that of the commercially used NC membrane, which shows an absolute correlation (Fig. 4).

### 3.5.2 Specificity

RAH IgG HRP-conjugate was used for the specificity test against human and buffalo blood eluates. Results in Fig. 5(a) show good color intensity dots at both spots of blood eluate (1:100 and 1:1000 diluted) obtained from human and no color development with either of the two buffalo blood eluted spots. The results obtained are as predicted because the conjugate (RAH) has been specifically used against human blood which identifies human antibodies only and does not bind to antibodies from any other organism. This confirms that there is no non-specific reaction to other species' blood samples (eluates). Blood eluate samples from human and buffalo were spotted in replica (n=2) in order to confirm the reproducibility.

### 3.6 Dot-ELISA for detection of mosquito blood meal source

Fig. 5(b) shows the result of identification of source of mosquito blood meal. The blood meal eluate obtained from mosquitoes that have fed on three different human were applied as sample 1, 2 and 3, while the ones fed on two different buffalos were used as sample 4 and 5. Out of all spotted samples only 1, 2 and 3 were identified (by colored dot formation), with RAH IgG HRP-conjugate, which correspond to the blood meal obtained from mosquitoes that fed on humans. The conjugate used is anti to human antibodies and therefore, specifically binds to and identifies human antibodies only. The blood meal eluates of mosquitoes fed on buffalo did not give a positive result thereby showing no color dots in Fig. 5(b) for sample 4 and 5. Thus, the GMA grafted CFP matrix successfully identified the mosquito blood meal source.

#### 4. Conclusion

GMA grafted CFP molecular mechanics simulations and in silico energy minimizations demonstrated the involvement of C3-C2 bond of cellulose in reaction with the GMA molecule resulting in a stabilized structure of the matrix. The GMA grafted CFP with varying graft level ranging from 10-100% were evaluated for application in dot-ELISA through a model system. The standardized conditions established for carrying out the assay on grafted CFP were: 5% skimmed milk as blocking agent, a peroxidase labelled antispecies IgG conjugate diluted 2000 times and the optimized incubation period of 30 min in each step. Under these conditions, a minimum background noise and the highest sensitivity of  $6 \text{ ngmL}^{-1}$  was recorded at 70% GMA grafted CFP matrix. This standardized CFP-g-GMA (70% graft level) surface and protocol when applied for detection of human antibody in blood by direct ELISA method using blood eluate as sample dots showed that 10  $\mu\text{L}$  dot of blood on whatman filter paper no. 1 eluted with 100  $\mu\text{L}$  PBS gave the best intensity of colored dots although elution with 1000  $\mu\text{L}$  PBS also gave a good intensity. The same graft level was successfully used to identify the source of mosquito blood meal, an important parameter in epidemiological studies, particularly in determining the role of the mosquito in malaria transmission. Therefore, modified CFP with 70% GMA graft level was highly specific as dot-ELISA matrices, showing no non-specific reactions either in a model system or with blood samples. The surface is equally sensitive and specific as nitrocellulose membrane with added advantage of being biodegradable, ecofriendly, many folds less expensive, easier to handle and does not require any special preparation for covalent binding of biomolecules. The prepared surfaces are being explored by the research group for quantitative ELISA and the results are encouraging. The present investigation established the developed surface to possess a strong potential to be used as matrix in dot-ELISA for detection of various diseases to be performed in the field conditions and in minimally equipped laboratories.

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## Schemes

**Scheme 1** Reaction scheme of grafting of GMA on CFP (a) activation of cellulose filter paper surface, (b) Grafting of GMA

**Table Captions**

**Table 1** Comparison of developed and conventionally used dot-ELISA matrix

**Table 2** Sensitivity test with human blood

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### **Figure Captions**

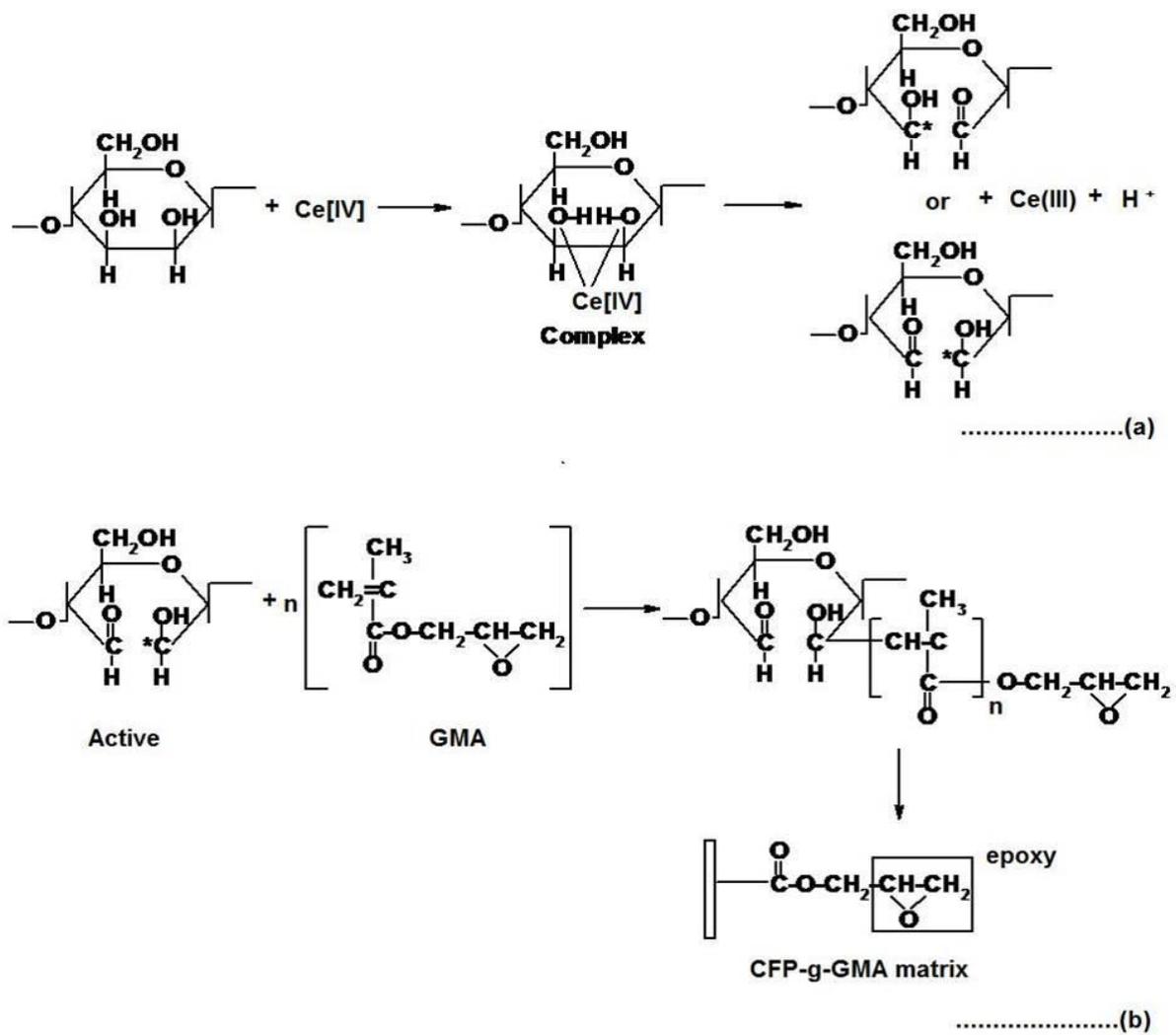
**Fig. 1** Characterization: (a) FTIR spectra of (i) ungrafted CFP and (ii-v) GMA-grafted CFP with varying grafting percentage [(ii) 20%; (iii) 50%; (iv) 70%; (v) 100%](Tyagi et al., 2009b); (b) Scanning electron micrographs of (i) ungrafted CFP and (ii-iv) GMA-grafted CFP with varying percent grafting [(ii) 20%; (iii) 70%; (iv) 100%](Tyagi et al., 2009b); (c) Effect of grafting on thickness of cellulose filter paper

**Fig. 2** Visualization of geometrical preferences of (a) PGMA; (b) CEL-CEL; and (c) PGMA-CEL<sub>2</sub> (d) 3-D ball-and-stick molecular structure of PGMA-CEL<sub>2</sub> matrix in transparent display mode after molecular simulation in vacuum. Color codes: C (cyan), O (red), and H (white).

**Fig. 3** Dot-ELISA studies with model system: (a) Effect of different blocking agents; (b) Effect of conjugate dilutions on RAG-IgG spotted CFP-g-GMA surface blocked with (i) ethanolamine (1%) (ii) BSA (2%), (iii) skimmed milk (5%); (c) Dot-ELISA comparison on cellulose filter paper with different graft level of GMA (under standardized condition); (d) Specificity test on CFP-g-GMA surface (70% graft level)

**Fig. 4** Sensitivity test on CFP-g-GMA surface (70% graft level) with human blood

**Fig. 5** Identification of (a) human blood and (b) mosquito blood meal



Scheme 1

Table 1

Property	Developed system (GMA grafted CFP)	Conventionally used system (nitrocellulose membrane)
Sensitivity	Good	Good
Specificity	Good	Good
Time duration		
Incubation	30 min	45 min
Total assay time	1h 30 min	~3 h
Washing	Very short /twice (~30 s each)	Extensive/thrice (1-2 min each)
Photostability	Stable	Unstable
Handling	Easy	With care
Cost	Economic	Costly

Table 2

<b>Dilution of blood eluate</b>	<b>Sensitivity</b>
Neat eluate	++
1:1	++
1:10	+++
1:100	+++
1:1000	+
1:10,000	-

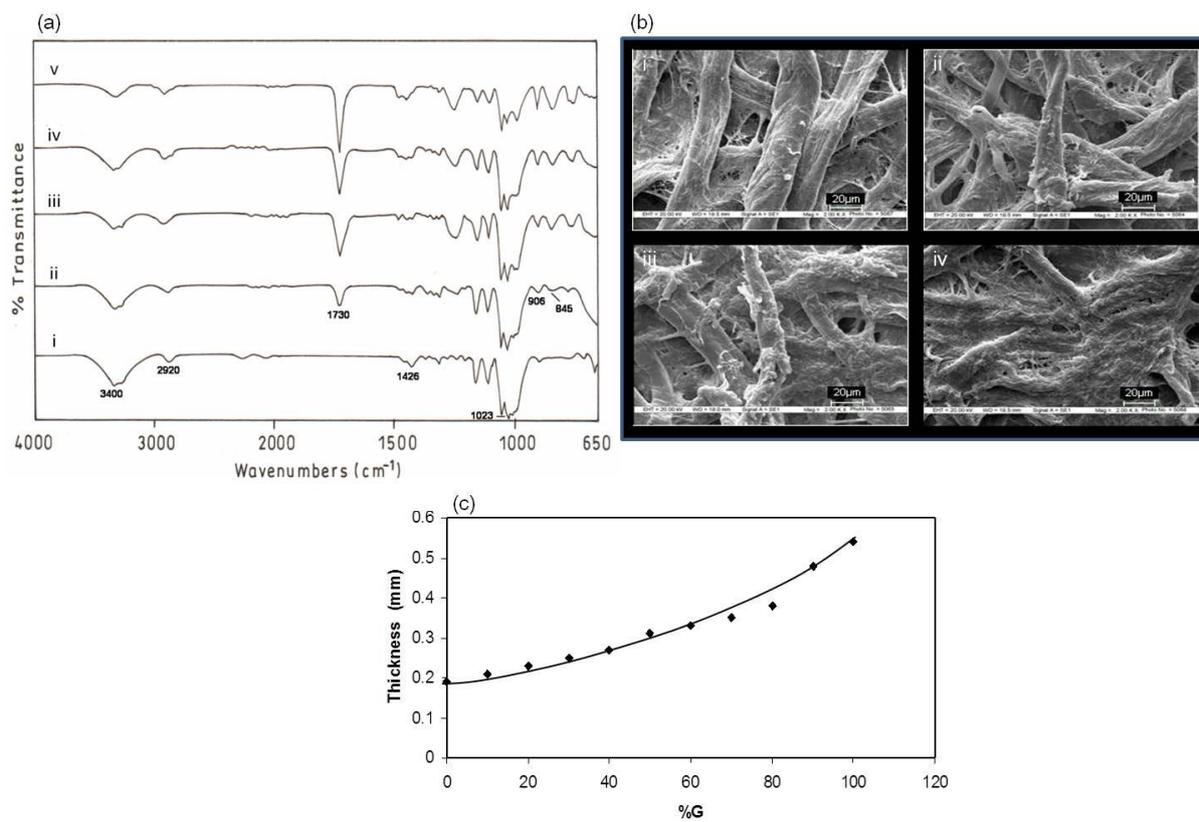


Figure 1

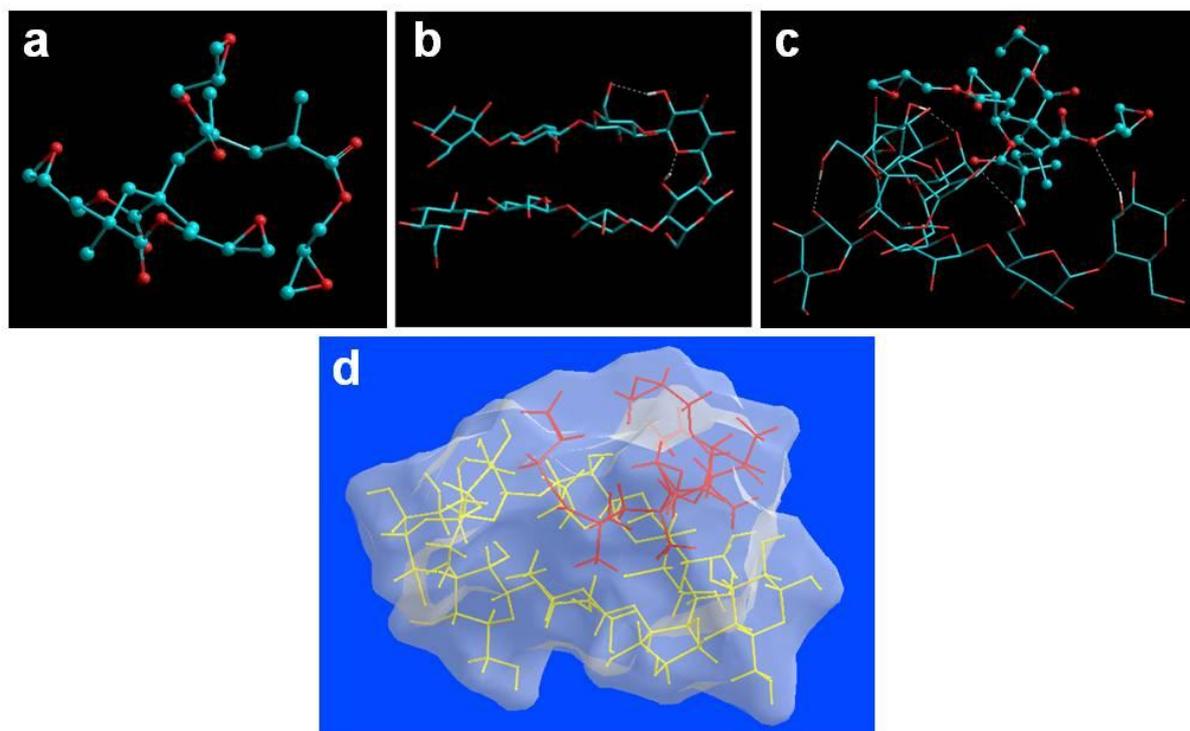
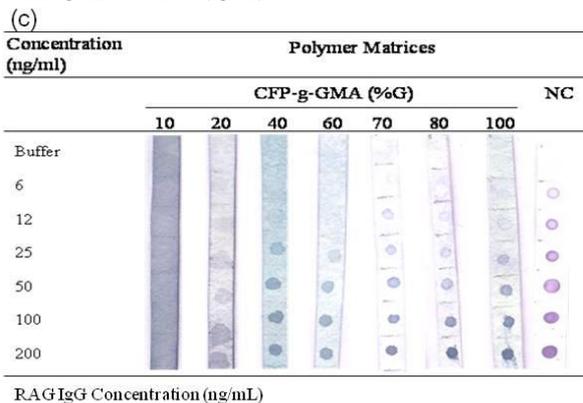
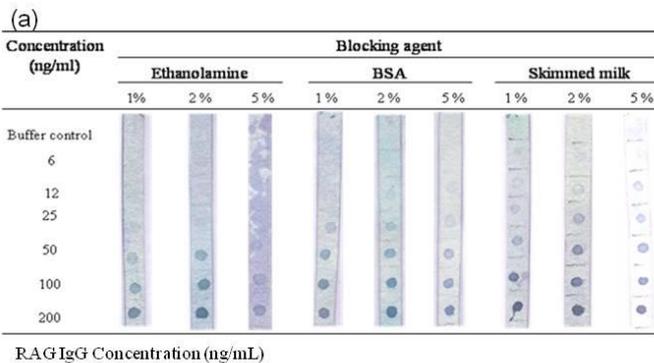
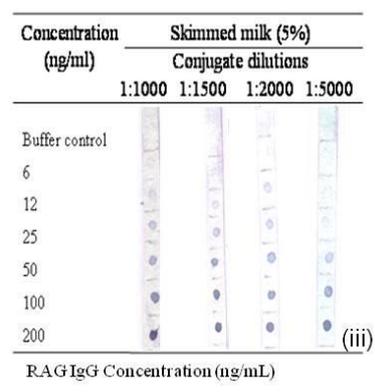
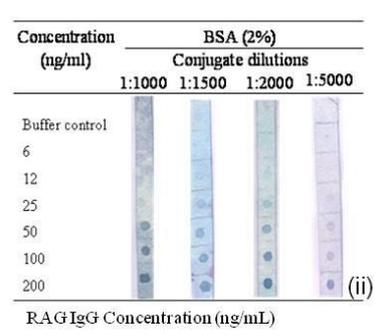
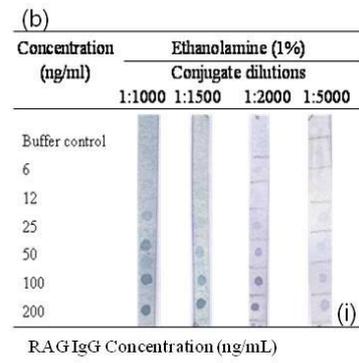


Figure 2



(d)

Antibody	Antibody Conc. (ng/ml)	Antibody Conjugate	CFP-g-GMA (70%)
RAG-IgG	100	GAR-IgG-HRP	
	50	GAR-IgG-HRP	
GAR-IgG	100	GAR-IgG-HRP	
	50	GAR-IgG-HRP	



Analytical Methods Accepted Manuscript

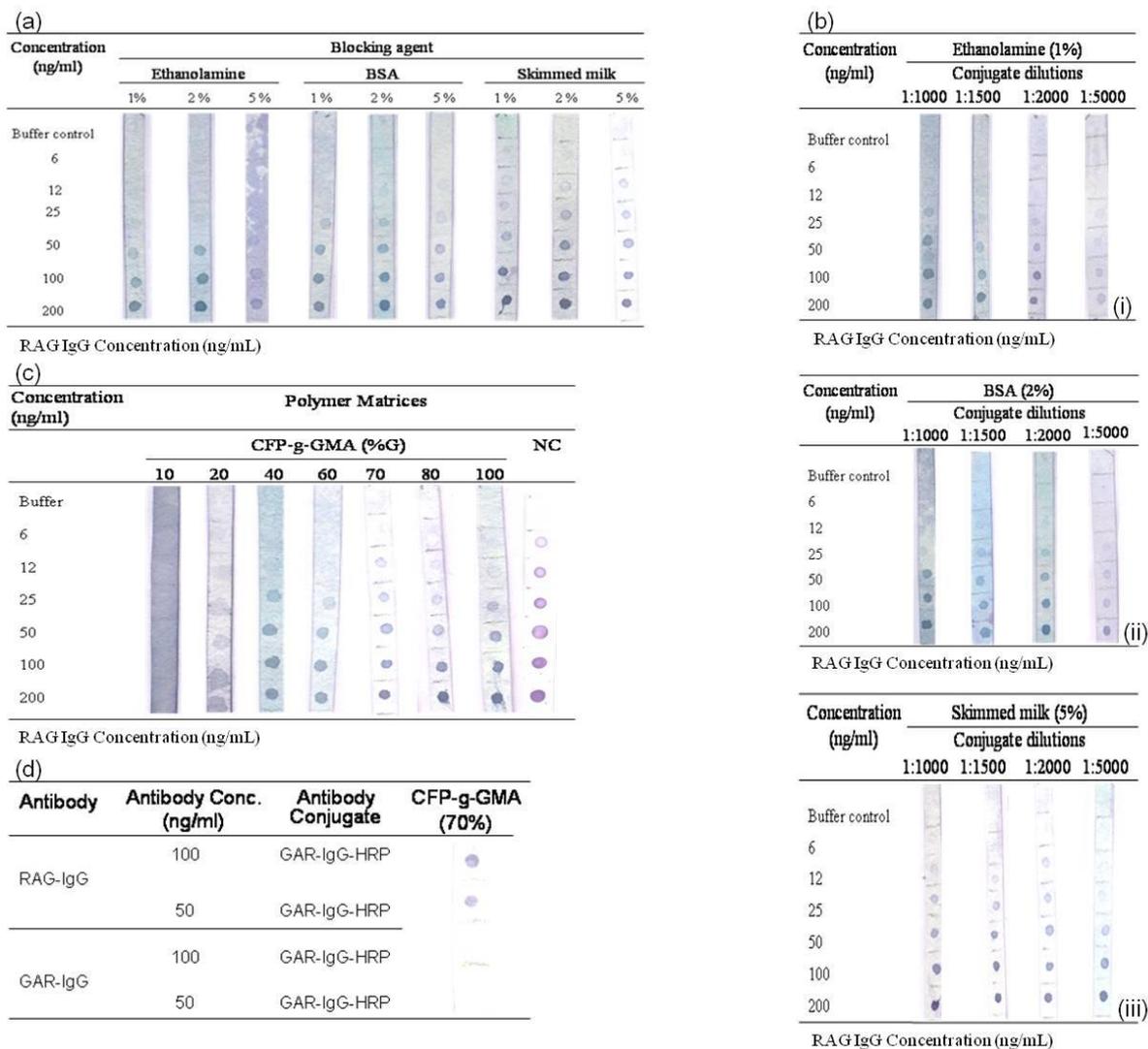
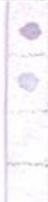


Figure 3

Dilution of Blood Eluate	Solid Phase (Matrix)	
	CFP-g-GMA (70%)	NC
Neat eluate		
1:1		
1:10		
1:100		
1:1000		
1:10,000		

Figure 4

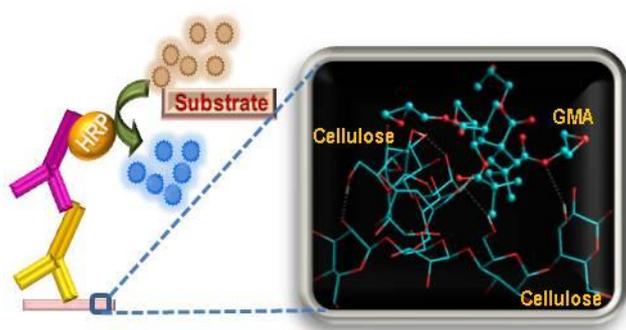
(a)

Blood Source	Blood Eluate Dilution	Antibody Conjugate	CFP-g-GMA (70%)
Human	1:100	RAH-IgG-HRP	
	1:1000	RAH-IgG-HRP	
Buffalo	1:100	RAH-IgG-HRP	
	1:1000	RAH-IgG-HRP	

(b)

Sample No.	Mosquito Blood Meal Source (Dilution of 1:100)	Conjugate	CFP-g-GMA (70%)
1	Human	RAH-IgG-HRP	
2	Human	RAH-IgG-HRP	
3	Human	RAH-IgG-HRP	
4	Buffalo	RAH-IgG-HRP	
5	Buffalo	RAH-IgG-HRP	

Figure 5



Graphical Abstract

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