



## Fabrication of Ultra-thin Polyrotaxane-based Films via Solid-state Continuous Assembly of Polymers

Journal:	<i>ChemComm</i>
Manuscript ID:	CC-COM-11-2014-008759.R1
Article Type:	Communication
Date Submitted by the Author:	24-Nov-2014
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## COMMUNICATION

## Fabrication of Ultra-thin Polyrotaxane-based Films *via* Solid-state Continuous Assembly of Polymers

Cite this: DOI: 10.1039/x0xx00000x

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Received 00th January 2012,  
Accepted 00th January 2012

DOI: 10.1039/x0xx00000x

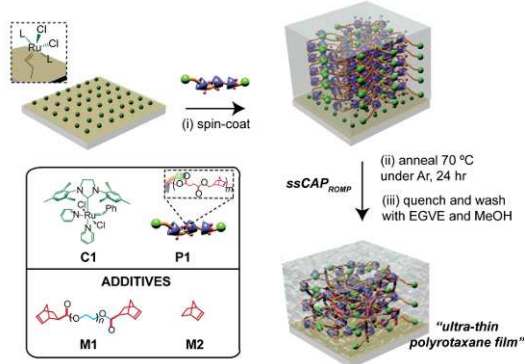
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**Surface-confined ultra-thin polyrotaxane (PRX)-based films with tunable composition, surface topology and swelling characteristics were prepared by solid-state continuous assembly of polymers (ssCAP). The PRX-based films supported cell attachment, and their degradation in biological media could be tuned. This study provides a versatile nano-coating technology with potential applications in biomedicine, including tissue engineering and medical devices.**

The self-assembly of complex multi-molecular systems has received expanding interest in both organic and materials chemistry.<sup>1</sup> This is attributed to the precise nature of the interactions, which leads to functional constructs that are able to rapidly respond to stimuli.<sup>1b</sup> Inclusion chemistry, wherein a 'host' reversibly binds to a 'guest' is a self-assembly process capable of forming highly ordered reversible constructs.<sup>2</sup> Of particular note are cyclodextrin (CD)-based PRXs first discovered by Harada and co-workers.<sup>3</sup> CD-based PRXs are synthesised by threading numerous CD moieties onto a polymeric backbone (e.g., PEG), and subsequently end-capping the polymer with bulky end groups to prevent dethreading.<sup>2b, 3a, b</sup> This allows the supramolecular construct to gain both rotational and translational freedom (*via* the CDs) without disassociation.<sup>4</sup> Since the inception of these constructs, a variety of sophisticated multi-component supramolecular assemblies<sup>2b, 5</sup> and advanced functional materials<sup>6</sup> have been fabricated using PRXs and their derivatives as building blocks. PRXs have been used for a wide range of applications, including drug<sup>7</sup> and gene<sup>8</sup> delivery systems, scaffolds for tissue engineering,<sup>9</sup> highly elastic yet tough 'sliding-ring' materials,<sup>10</sup> and insulated molecular wires.<sup>11</sup> Although much work has focused on the development and characterisation of macroscale CD-based PRX constructs, the study of nanoscale CD-based PRX functional films remains largely unexplored, with only several reports in the literature.<sup>7a, 12a,b</sup> Furthermore, the incorporation of stimuli-responsive polymers may enable triggered release of therapeutics.<sup>12c,d</sup> Recently, we reported the build-up of degradable PRX multilayer films using the layer-by-layer (LbL) technique based upon electrostatic interactions.<sup>12a</sup> The ability to initiate film degradation under biological conditions and the potential to conjugate various drugs and biomolecules onto the CD films highlight their potential in the biomedical field. However, the ability to tailor the composition and physical properties of these films is

complicated by the necessity to have complementary polyelectrolytes. Therefore, novel strategies that provide facile access to PRX-based nanoscale films with tunable properties (i.e., surface morphology, swellability and elasticity) are highly desirable, particularly for biointerfaces whereby cellular interactions and behaviour are dependent on the composition, topography and mechanical properties of the film.<sup>13</sup>

Herein, we report the synthesis of ultra-thin (< 100 nm) PRX-based cross-linked films using a PRX macrocross-linker in combination with the recently developed solid-state continuous assembly of polymers (ssCAP) technique (Scheme 1).<sup>14</sup> Through the simple addition of selected additives during film fabrication, the composition, surface topography, swelling characteristics and degradation rate of the nanoscale PRX films could be controlled. Although predominately composed of low fouling PEG,<sup>15</sup> the PRX-based films were able to facilitate cell attachment and proliferation, which was attributed to the heterogeneity of the PRXs. The ability of the ssCAP technique to produce multi-component PRX-based films with engineered properties makes this approach applicable to the fabrication of functional nanobiotechnology coatings.



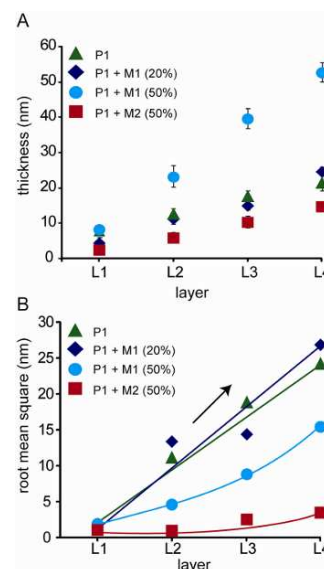
**Scheme 1.** Synthesis of ultra-thin PRX-based films *via* ssCAP<sub>ROMP</sub>. The physical properties of the resulting films were tailored by the addition of selected additives, including the norbornene end-functionalized PEG **M1** or the monomer norbornene **M2**.

The ultra-thin PRX-based films were prepared *via* the ssCAP approach (Scheme 1) as attempts to prepare analogous films from solution state CAP approaches<sup>16</sup> were unsuccessful. Ring-opening metathesis polymerization (ROMP) was used to mediate the ssCAP<sub>ROMP</sub> process to afford surface-confined PRX-based films, whereby the PRX **P1** acts as a macrocross-linker. Film formation was performed on silicon wafers that were pre-functionalised with an initiating layer of the ruthenium (Ru) catalyst **C1** (refer to Supporting Information (SI) for details). The PRX macrocross-linker **P1**, with and without additives (PEG cross-linker **M1** or norbornene **M2**), were deposited onto the substrate *via* spin-coating, which resulted in a 60 nm film (SI, Fig. S1). Subsequently, the films were annealed under an argon atmosphere at 70 °C (i.e., above the melting temperature ( $T_m$ ) of **P1** (SI, Fig. S2)) for 24 h (Scheme 1). The resultant cross-linked films were then washed in methanol containing di(ethylene glycol) vinyl ether (EGVE) to detach the Ru catalyst from the film and to remove any uncross-linked material prior to analysis. Multilayer films were prepared using a previously described re-initiation method.<sup>14, 16</sup>

The PRX-based macrocross-linker **P1** was synthesised in two steps by slight modification of methods reported in the literature.<sup>17</sup> Briefly,  $\alpha,\omega$ -dialkyne PEG<sub>10K</sub> was threaded with  $\alpha$ -CDs to yield a polypseudothaxane as a precipitate. The product was lyophilised prior to end-capping *via* copper catalyzed azide-alkyne cycloaddition (CuAAC) with an azido-anthracene derivative. This resulted in PRXs bearing anthracene end-caps at the PEG chain ends. From <sup>1</sup>H NMR spectroscopic analysis, the inclusion ratio and the end-capping efficiency of the PRX were determined to be *ca.* 3 CDs per PEG chain and 80%, respectively (SI, Fig. S3a). Polymerizable pendent norbornene groups were then conjugated onto the PRX by partial esterification of the primary hydroxyl groups of the threaded CDs with a norbornene acid derivative to afford PRX **P1** (Scheme 1). <sup>1</sup>H NMR spectroscopic analysis of **P1** (SI, Fig. S3b) revealed the presence of *ca.* 3 CD moieties per PRX and an average of 3 polymerizable norbornene moieties per CD (i.e., 5 mol% of norbornene relative to CD primary hydroxyl groups).

Thickness analysis of the PRX-based films was conducted *via* atomic force microscopy (AFM). Fig. 1A illustrates the growth profile of a range of nanoscale PRX-based films consisting of various weight percentages (wt%) of **P1** with and without additives (**M1** or **M2**), with respect to the polymeric layer (L) (where L1 denotes the first ssCAP reaction from the initial Ru-modified Si substrate). For the L1 film prepared from the PRX macrocross-linker **P1** alone, the initial film thickness was determined to be *ca.* 10 nm. Upon re-initiation (L2-L4), the thickness of PRX **P1** based films increased by *ca.* 6 nm per layer to yield an *ca.* 25 nm film after four layers (L4) (Fig. 1A). This is in contrast to control experiments (i.e., **P1** annealed in the absence of catalyst **C1**) that provided a thickness of *ca.* 2.5 nm, which was attributed to the physical adsorption of polymers (SI, Fig. S4). The surface roughness (Fig. 1B) of the **P1** film was found to increase significantly with each additional layer (L1: 1.5 nm to L4: 25.7 nm), which correlated to the presence of relatively large particles with diameters ranging from *ca.* 1-1.4  $\mu$ m was observed on the surface topography of the air-dried films (SI, Fig. S5, **P1** dry-state). The presence of such particles was attributed to the aggregation of the PRXs as previously reported.<sup>12a</sup> To assess whether the bulky threaded CDs of **P1** influence film growth, ssCAP<sub>ROMP</sub> films were also prepared from a linear PEG macrocross-linker **P2** with pendent norbornene groups (5 mol % with respect to total amount of hydroxyl groups) (Fig. 2A). Both **P1** and the linear PEG macrocross-linker **P2** have approximately the same amount of hydroxyl and norbornene groups as evaluated by <sup>1</sup>H NMR spectroscopy (SI, Fig. S3b and S6, respectively). Whereas **P1** provided a film thickness of *ca.* 10 nm after one layer (Fig. 1A), the

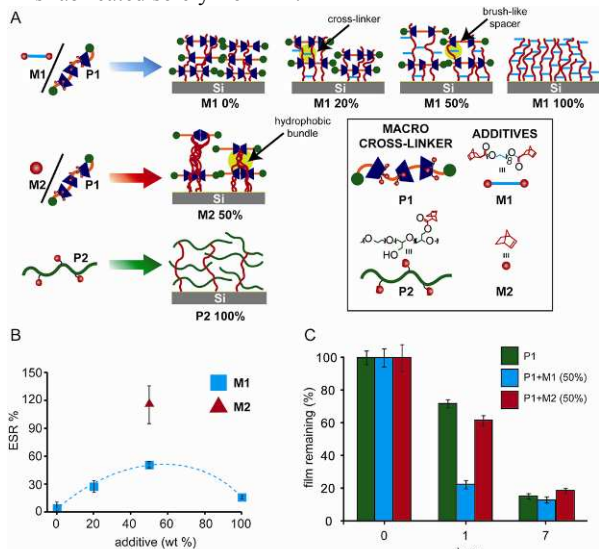
film derived from **P2** was significantly thicker (L1; *ca.* 80 nm, Fig. S7). The significant difference in film growth was attributed to the steric hindrance of the bulky CDs decreasing accessibility to the norbornenes (i.e., polymerizable moieties) during the ssCAP process. Based upon these observations, it was rationalised that the addition of relatively small, mobile and polymerisable additives during the CAP process with **P1** would improve film growth, as well as providing an additional handle to control the films properties. Therefore, the addition of the PEG-based cross-linker **M1** as an additive was studied. **M1** acts as a brush-like spacer, increasing the intermolecular distance between adjacent cross-linkable PRXs whilst also creating additional cross-linking points. Whereas the addition of 20 wt% of **M1** had negligible effect on the **P1** film thickness over multiple layers relative to **P1** alone (Fig. 1), the addition of 50 wt% of **M1** resulted in an increase of 15 nm per layer after the first layer (L1; 8 nm) was deposited (Fig. 1A). Overall, the addition of 50 wt% **M1** assisted film growth, resulting in a 2.5 fold increase in film thickness per layer as compared to **P1** alone. Furthermore, the surface topography of the films prepared with **M1** (20 and 50 wt%) appeared smoother (c.f., **P1** films), which was attributed to the flexible nature of the PEG chains (SI, Fig. S5, **P1+M1** (20 and 50 wt%) dry-state). The monomer, norbornene **M2**, was also selected as an additive for film formation as it may act as a spacer, increasing the intermolecular distance between PRXs. Although the addition of 50 wt% **M2** did not seem to improve film growth compared to **P1** alone (Fig. 1A), a significant decrease in film roughness (Fig. 1B) was noted (SI, Fig. S5, **P1+M2** (50 wt%) dry state). This result is attributed to the ability of free norbornene to connect neighbouring **P1** molecules and occupy voids, thereby resulting in more homogenous films similar to poly(norbornene) brushes synthesised *via* grafting-from techniques.<sup>18</sup>



**Figure 1.** Air-dried PRX-based nanoscale films made *via* ssCAP<sub>ROMP</sub> in the presence of **P1** and different amounts (wt%) of additives (**M1** or **M2**). (A) ‘Air-dried’ film thickness with polymeric layer (L) on planar silica (Si) substrates, as measured in-air by AFM. (B) Film surface roughness (root mean square) with increasing polymeric layer (L), as measured by dry-state AFM. Note, the plotted film thickness values are based upon the measured film thicknesses minus control experiments (that measured physical adsorption), and are the average of 15 independent measurements.

The PRX **P1**-based nanoscale films obtained after three re-initiations (i.e., L4) were subjected to swelling experiments, whereby

the films were swollen in water for 2 days. The degree of swelling was measured in terms of the equilibrium swelling ratio (ESR %) (SI, Equation 1) using thickness measurements obtained from dry and wet-state AFM analysis (SI, Fig. S8). The addition of additives (**M1** or **M2**) is expected to increase the intermolecular distance between the CD cross-link points, thereby decreasing cross-linking density and allowing for greater swelling of the films in comparison to films fabricated solely from **P1**.



**Figure 2.** (A) Illustration of the PRX-based nanoscale film (L4) morphology in its fully swollen state when additives (**M1** or **M2**) are incorporated at various weight percentages (wt%). (B) Equilibrium swelling ratio (ESR%) of the fully swollen PRX-based nanoscale films measured by AFM. (C) Degradation studies of various films submerged in a mixture of 10 % blood serum and 90 % PBS over 7 days. Percentage degradation was taken as the reduction in film thickness, as measured by wet-state AFM over time.

Fig. 2A is a theoretical illustration of the change in film morphology of a series of swollen PRX-based nanoscale films with different amounts of additives (**M1** or **M2**). It was observed that films prepared with just the PRX macrocross-linker **P1** did not swell significantly (ESR% *ca.* 2.0%, Fig. 2B) as the distance between the CD cross-link points would be very short. Furthermore, as the CDs are significantly larger than the norbornene groups, it is also possible that the ROMP process was sterically hindered. However, when the PEG cross-linker **M1** is introduced, the distance between the CD cross-link points is increased as the PEG acts as a brush-like spacer decreasing the cross-link density of the film (Fig. 2A). Therefore, the incorporation of **M1** (20 and 50 wt%) into **P1** films results in films with ESR% values of *ca.* 30 and 50 %, respectively (Fig. 2B). The increase in ESR% is attributed to a decrease in cross-linking density between adjacent PRXs molecules. For comparison, films prepared solely from **M1** were also analysed, and displayed lower swellability (ESR% of *ca.* 16 %, Fig. 2B) than films prepared from both **P1** and **M1**, which is attributed to a higher cross-linking density. Although PEG is generally hydrophilic in nature, the high cross-linking density and low swellability of pure **M1** (i.e., PEG<sub>400Da</sub>) films most likely results from the low molecular weight of **M1** and high norbornene to ethylene glycol repeat unit ratio (2:9). When the molecular weight of PEG is significantly increased (e.g., with the use of PEG<sub>20kDa</sub> **P2**, Fig. 2A) leading to a decrease in the norbornene to ethylene glycol repeat unit ratio, the resulting films fabricated *via* the same ssCAP process with only one layer are able to swell significantly more (i.e., ESR % *ca.* 167 %, Fig. S9). The significant

increase in swellability compared to pure **M1** films is attributed to the lower cross-linking density (Fig. 2A). It is expected that films fabricated with **M1** and **P1** would possess an increased intermolecular spacing between PRXs resulting from the presence of PEG-based brush-like spacers (Fig. 2A). However, owing to the difunctional nature of **M1**, additional covalent cross-linking sites are also introduced, which contributes to the film cross-linking density, thereby limiting the swellability of the films. To avoid this scenario, the monomer, norbornene **M2**, was added as an additive at 50 wt%. As **M2** is a monomer, it was expected that the norbornene groups would act solely as a spacer increasing the intermolecular distance between PRXs (Fig. 2A). It was observed that films prepared with 50 % **M2** were able to swell significantly more than any other PRX-based films fabricated in the series (ESR %  $\sim$  116 %, Refer to Fig. 2B, red icon). The significant increase in ESR is suggestively attributed to the hydrophobic polynorbornene chains bundling together in a collapsed configuration and creating hydrated pockets throughout the polymeric network. In addition, it is expected that the threaded CDs moieties would slide along the PEG backbone and aggregate. The aggregation of the CDs thus exposes the hydrophilic PEG backbone. These two contributing factors are expected to allow for higher swellability than the other PRX-based films (Fig. 2A and B).

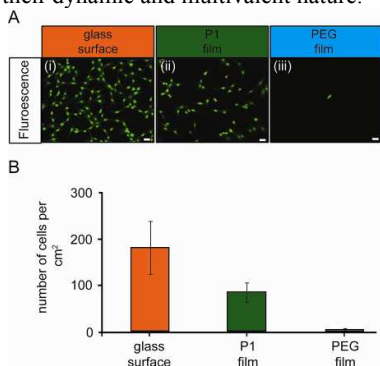
The degradability of the PRX-based nanoscale films was also studied by immersing the films in a mixture of 10 % blood plasma and 90 % PBS. As serum contains a variety of enzymes, including those capable of catalysing hydrolyses of ester bonds, it was hypothesised that the degradation of the PRX films could be tailored by controlling the type and amount of additive (**M1** or **M2**) incorporated. Degradation of the films was measured by thickness analysis at various time points using wet-state AFM (Fig. S10). It was observed that PRX films fabricated with additive **M1** (50 wt%) displayed the highest percentage of degradation (Fig. 2C) after 1 d, which was attributed to the higher content of ester bonds present in the **M1** component. Near complete degradation (> 80%) of all the films was observed after 7 days. The ability to tune the film degradation rate further demonstrates the potential of these films as nano-coatings for various bio-related applications. Thus, by varying the type and amount of additive used, the physical properties of the PRX-based films can be tailored.

Functional materials composed of  $\alpha$ -CD/PEG PRXs have shown potential to control and tune the extent of cell adhesion and proliferation.<sup>9</sup> For example, the incorporation of PRXs into PEG-based hydrogels has led to successful cell attachment and proliferation.<sup>9</sup> This phenomenon is believed to result from the surface heterogeneity generated by the PRXs, rather than the chemical composition of the CD groups.<sup>9</sup> The ability to control heterogeneity by simply varying the amount of PRXs, or the amount of threaded CDs, makes PRX-based materials and interfaces potential candidates for tissue engineering and biomedical coating applications. Therefore, the cell adhesion characteristics of the nanoscale PRX-based film composed purely of **P1** was investigated using mouse embryonic fibroblast (NIH/3T3) cells according to our previously reported assay.<sup>19</sup> Non-modified and PEG-coated (i.e., **P2**-coated) glass slides were used as positive and negative controls, respectively, and cell attachment was quantified by acquiring 10 images from random locations on each substrate using fluorescent microscopy (Fig. 3 and SI, Fig. S11).

Unlike the **P2** PEG films, **P1**-based films were able to support cell adhesion and proliferation, as observed *via* fluorescence microscopy (Fig. 3). The ability of inherently rough **P1** based films to support cell attachment and proliferation was attributed to the heterogeneity of the PRXs, despite the films being predominately composed of PEG (i.e., main-chain of the PRX is PEG (*ca.* 75 wt. %)), which is



low fouling (Fig. 3). The relatively high content of PEG in the **P1** films is also believed to contribute to the 50 % reduction in cell adhesion in comparison to the glass slides (Fig. 3). Interestingly, when cell adhesion studies were conducted using HeLa cell lines, no cell attachment was observed for both PRX **P1** and PEG based films. These promising preliminary results indicate that the ultra-thin PRX-based films could potentially be employed as nano-coatings in various biomedical applications. In addition, the remaining hydroxyl groups on the CD cross-links within the PRX networks could also be used to support the conjugation of various receptors and biofactors that facilitate specific cell interactions and behaviour. The dynamic nature of CDs conjugated with specific receptors further increases the potential of these materials as increased ligand affinity is often seen owing to their dynamic and multivalent nature.<sup>20</sup>



**Figure 3.** (A) Cell (NIH/3T3) attachment on glass, **P1** ssCAP<sub>ROMP</sub> film (L4) and **P2** ssCAP<sub>ROMP</sub> film (L1). (B) Number of cells per surface area attached on the respective substrates. Scale bars are 100  $\mu$ m.

In conclusion, ultra-thin PRX-based networks were fabricated using CD/PEG PRXs as the building block *via* the recently developed ssCAP<sub>ROMP</sub> technique. Using this approach, the composition and resulting physical properties of the PRX-based films could be tuned by the addition of various additives during the fabrication process. In addition, the rate of film degradation in the presence of blood serum was also demonstrated and could be controlled by the choice of additive. Preliminary cell attachment studies using NIH/3T3 cell lines indicated that the nanoscale PRX-based films were also able to support cell adhesion, highlighting their potential application in the field of nanobiotechnology. These promising results highlight the ability of the ssCAP approach to construct multi-compositional PRX films with tunable properties on the nanoscale, providing new avenues for PRX-based technologies to be applied as nano-coatings.

The authors acknowledge the Australian Research Council under the Future Fellowship Scheme (FT110100411, G.G.Q.) and Discovery Project (DP1094147 and DP130101846, F.C., G.G.Q.). K. L., Q.F. and J. C. are the recipients of the Australian Research Council Super Science Fellowship (FS110200025).

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† Electronic Supplementary Information (ESI) available: [details of any supplementary information available should be included here]. See DOI: 10.1039/c000000x/

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