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1 **Title page**

2 **Magneto-separation of Genomic Deoxyribose Nucleic Acid using pH Responsive**
3 **Fe₃O₄@silica@chitosan Nanoparticles in Biological Samples**

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23 **Magneto-separation of Genomic Deoxyribose Nucleic Acid using pH Responsive Fe₃O₄**
24 **@silica@chitosan Nanoparticles in Biological Samples**

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29 **Abstract**

30 Magnetic adsorption technology of polymer functionalized superparamagnetic
31 nanoparticles is showing great potential in biomedical applications because of their facile “on
32 and off” state of magnetization.Highly magnetized superparamagnetic nanoparticles based
33 magnetic adsorption technology was employed for the purification of DNA. The core-shell
34 Fe₃O₄ nanoparticles were synthesized by alkaline precipitation and subsequently coated with
35 silica by sol gel method. Further, silica coated Fe₃O₄ nanoparticles functionalized with
36 chitosan was used as an adsorbent for DNA. The surface adsorption of DNA onto the
37 modified nanoparticles was optimized as a function of pH, time and temperature. The
38 adsorption efficiency of Fe₃O₄@silica@chitosan nanoparticles was examined by U.V visible
39 spectroscopy. Fe₃O₄@silica@chitosan nanoparticles with the high adsorption efficiency of~
40 88% and a high elution efficiency of ~ 98% were employed for DNA isolation from human
41 saliva. Agarose gel electrophoresis was used to validate the quality and quantity of DNA
42 isolated from human saliva. Square wave voltammetry was carried out for monitoring the
43 quantitative information about DNA fragments concentration. This method has potential
44 application in the field of bioelectrochemical analysis. The isolation results of genomic DNA
45 from saliva indicated that the Fe₃O₄@silica@chitosan nanoparticles have outstanding
46 advantages in operation, selectivity, and capacity over the present existing isolation protocols
47 (Phenol–chloroform extraction). Furthermore, it opens up new opportunities in detection and
48 isolation of nucleic acid.

49
50 **Keywords:** Fe₃O₄ nanoparticles, Chitosan, DNA adsorption, Genomic DNA isolation, Square
51 Wave Voltammetry.

52

53 **1. Introduction:**

54 Magnetic adsorption technology has become a promising tool for the separation of
55 biological molecules. Robinson.et.al. used magnetic separation for the first time in
56 biotechnological context [1]. Materials employed for this are defined as magnetisable, which
57 can become magnetic under the influence of an external magnetic field and can facilitate the
58 isolation or extraction of a target molecule. The nonmagnetic target binds to the surface of
59 magnetisable solid phase support, either through a specific affinity interaction or other
60 mechanism,for example ion exchange or hydrophobic interaction so that it can then be
61 isolated or extracted by application of an external magnetic field [2].Nano-size magnetic
62 adsorbents have attracted wide attention owing to their high surface to volume ratio, which
63 result in a higher binding rate, and magnetically controllable aggregation, making the
64 separation easier [3].

65 In order to improve the colloidal stability, biocompatibility and reduce toxicity,the
66 nanoparticles are often encapsulated with suitable biocompatible polymers [4].Coating of
67 polymers over magnetic nanoparticles induces interparticle repulsion and thereby lowers the
68 magnetic attraction between particles which prevents them from agglomeration in presence of
69 an external magnetic field [5]. Surface functionalized magnetic nanomaterials have been
70 widely used in biotechnological and clinical applications, such as bioseparation[6,7,8], drug
71 and gene deliverysystem [9], enzyme and protein immobilization [10], and hyperthermia
72 treatment [11-13] along with DNA separation and adsorption studies [14 ,15] and biosensing
73 [16]. The nucleic acids can be isolated directly from crudesample materials such as blood,
74 tissue homogenates,cultivation media and water.

75 The magnetic properties of the solid materials provide an additional advantage due to
76 their possibility of adjusting magnetization and demagnetization that, they can be removed
77 relatively easily and selectively evenfrom viscous sample suspensions. In fact, magnetic
78 separationis the method of choice for the recovery of smallparticles in the presence of
79 biological debris and other fouling material of similar size.Furthermore, the efficiency of
80 magnetic separation isalso suited for large-scale purifications [17].

81 Generally, interactions of biological macromolecules with surfaces are of great
82 significance in nature and biotechnology. DNA immobilization and adsorption on surfaces
83 have direct applications in biosensing, DNA purification, and nanofabrication [18]. Many
84 methods of DNA immobilization were developed, including cross-linking, electrostatic
85 adsorption, self-assembled monolayer, and entrapment in porous magnetic silica microspheres
86 surface [15]. DNA is a negatively charged biomolecule due to the deprotonation of
87 the phosphate groups above pH 1.0 [8]. Exploiting the property of DNA, the use of
88 electrostatic capture of DNA has been shown by decreasing the solution pH below the pKa of
89 the immobilized residue. Further, in order to release the DNA from these devices, it is
90 necessary to switch the charge on support by increasing the pH above pKa of immobilized
91 residue [19]. Wanget al. [20] have reported extraction of calf thymus DNA using ionic liquid
92 1-butyl-3-methylimidazolium hexafluorophosphate. A high binding efficiency (~90%) was
93 achieved, which mainly resulted from the strong electrostatic attraction between the cationic
94 groups and the phosphate groups of DNA [21]. However, low back extraction efficiency has
95 been faced also due to the strong electrostatic forces.

96 In the present work, a study on the adsorption of DNA on surface of Fe₃O₄
97 @silica@chitosan nanoparticles and its elution in the medium was conducted. The silica
98 coating on iron oxide nanoparticles is employed in order to screen the magnetic dipolar
99 interactions between the MNPs. Moreover, silica shells present other advantages arising from
100 their chemical stability, easy surface modification (reactive surface silanol groups) and
101 biocompatibility, thus offering the possibility of introducing new functionalities onto the
102 nanoparticle surface [22]. The core shell nanoparticles were further functionalized with
103 chitosan to exploit the positive amino group of chitosan for DNA adsorption. The amine
104 activated surface can be used to covalently link specific biomolecules [23]

105 The work reports the utility of Square-Wave Voltammetry, for measurements of
106 nucleic acids at glassy carbon electrodes. The adsorption efficiency of ~ 87% is obtained with
107 high elution efficiency of ~ 98% which is a desirable parameter. The high adsorption
108 efficiency as well as high elution efficiency of the proposed nanoparticles makes it an
109 appropriate candidate to be used in bioseparation. The high adsorption efficiency of the
110 nanoparticles was tested for DNA isolation from human saliva. The proposed method is
111 suitable for both miniscale as well as large scale DNA purification.

112 2. Materials and Methods

113 2.1 Chemicals

114 Calf thymus DNA and Low molecular weight Chitosan (>90% degree of
115 deacetylation) were procured from Sigma Aldrich. Acetate buffer for electrochemical analysis
116 was used (0.2 M CH₃COOH + 0.2 M CH₃COONa, pH 5.0). Ferrous chloride (FeCl₂),
117 polyethylene glycol (PEG, M_w = 6000), sodium chloride (NaCl), Tris-HCl, ethylene
118 diaminetetraacetic acid (EDTA), sodium dodecyl sulphate (SDS), sodium hydroxide (NaOH),
119 hydrochloric acid (HCl), were purchased from Hi media, India. All solutions were prepared
120 using double distilled water.

121

122 2.2 Fabrication of Fe₃O₄@silica@chitosan Nanoparticles.

123 Fe₃O₄@silica@chitosan nanoparticles were synthesized by alkaline precipitation
124 method as per previously reported method [24]. 2 g of FeCl₂.4H₂O was dissolved in 50 mL of
125 1 M HCl by heating up to 70 ° C. 50 mL of 3 M NaOH was added to it at 60° C drop by drop
126 with constant stirring. The appearance of black precipitate indicated the formation of iron
127 oxide nanoparticles. The precipitate was magnetically separated and washed thoroughly with
128 water. The synthesized Fe₃O₄ nanoparticles were silica coated in an acid catalyzed sol-gel
129 reaction. Magnetic suspension (0.1 gm/10 mL Fe₃O₄) was ultrasonically dispersed in a round
130 bottomed flask. Acid catalysis was done by adding 0.1 mL of HCl vigorously. After one hour 3
131 mL of water, 5 mL of ammonium hydroxide and 3 mL of TEOS was added to the flask in 5 mL
132 of methanol. The hydrolysis of TEOS was carried out for 7 h at 80 ° C under continuous
133 stirring at 550 rpm. The resultant product was separated by an external magnet and washed
134 thoroughly with double distilled water thrice. Silica coated Fe₃O₄ nanoparticles (0.2 gm) were
135 dispersed in 7.5 mL of chitosan solution (4 mg/mL chitosan dissolved in 2 % acetic acid).
136 Suspension was mixed by sonication for 30 min. Finally, the chitosan functionalized silica
137 coated Fe₃O₄ nanoparticles were dried at room temperature.

138 2.3 Size distribution and colloidal stability

139 Size distribution and colloidal stability of the sample was performed on PSS/NICOMP
140 380 ZLS particle sizing system (Santa Barbara, CA, USA) with a red He-Ne laser diode at

141 632.8 Å in affixed angle 90° plastic cell was used for the measurement of surface charge and
142 colloidal stability.

143 **2.4 Procedure for adsorption and desorption of DNA from Fe₃O₄@silica@chitosan** 144 **Nanoparticles:**

145 Study on the adsorption of DNA, from aqueous solutions, on the surfaces of
146 nanoparticles was investigated batch-wise. The Aliquot of known volume of DNA solution,
147 with selected initial concentration and pH, was transferred into a beaker. A known dosage of
148 the magnetic nanoparticles was added to the beaker. After mixing time elapsed, the
149 nanoparticles were separated magnetically. The concentration of the DNA residue in the
150 supernatant was determined by measuring absorbance before and after adsorption of DNA by
151 UV-vis spectrometer at 260 nm. The percent adsorption of DNA on nanoparticles was
152 calculated using the following equation:

$$153 \text{ \% Adsorption} = (C_0 - C_f) / C_0 * 100\% \quad (1)$$

154 where C₀ and C_f, respectively, represent the initial and final (after adsorption)
155 DNA concentration (in mg L⁻¹) in the aqueous phase. For potential applications, regeneration
156 and reusability of an adsorbent are important factors to be reported. The desorption ratio was
157 calculated using the following equation:

$$158 D = C_i * V / Q * 100 \quad (2)$$

159 Where C_i is the concentration of DNA in the desorption media, V is the volume of this media,
160 and Q is the amount of DNA in the solid phase.

161 **2.5 Time, temperature dependent relative DNA isolation studies:**

162 The effect of adsorption time was studied by keeping the DNA with magnetic
163 nanoparticles at optimized pH for different time. The role of temperature on adsorption of
164 DNA to the surface of magnetic nanoparticles was studied at selected experimental
165 temperatures ranging from 25°C to 90°C. All the experiments were performed batch wise.

166 **2.6 Reusability study**

167 In order to test the reusability of magnetic nanoparticles, DNA adsorption and elution
168 procedure was repeated 5 times by using same group of magnetic nanoparticles. Each
169 experiment was repeated in triplicate to validate the reproducibility.

170 2.7 XRD analysis

171 X-ray diffraction (XRD) patterns of Fe₃O₄@silica@chitosan and DNA adsorbed
172 Fe₃O₄@silica@chitosan nanoparticles were recorded on a Rigaku D/MAXIIA diffractometer
173 using Cu K α radiation ($\lambda = 1.5406\text{\AA}$), operating at 40 kV and 40 mA in the 2θ range from 20°
174 to 80° .

175 2.8 DNA isolation using Fe₃O₄ @silica@chitosan magnetic nanoparticles from Human 176 saliva.

177 The saliva (3 mL) was collected and mixed with 500 μL of cell lysis buffer (1 % SDS
178 and 0.2 M NaOH solution) for 2 min at 50°C . The tubes were vortexed and centrifuged. The
179 saliva lysis buffer mixtures were transferred to fresh Eppendorf tubes, and 200 μL of magnetic
180 nanoparticles were added. Magnetic solid phase adsorption of genomic DNA was done by
181 adding nanoparticles to the lysed solution. Then the Binding buffer (25 % PEG- 6000 and 2.0
182 M NaCl, pH 8.5) was added. After that the mixtures were placed at room temperature for 10
183 minutes to ensure target DNA was completely bonded onto the surface of the magnetic
184 nanoparticles. After placing the tube beside a magnet for 20 seconds to attract the
185 nanoparticles, the supernatant was discarded with a pipette and DNA pellet was retained. The
186 DNA pellet was resuspended in 100 μL of 70% ethanol to purify it, and was then centrifuged
187 at room temperature for 20 seconds at 600r/min and then returned to the magnetic to attract
188 the beads for 20 seconds. The supernatant was discarded again. The purification procedure
189 was repeated once to remove any residual contaminants. The purified DNA was eluted by the
190 addition of 50 μL of elution buffer (10 mM Tris HCl, 1.0 mM EDTA , pH 8.5) dissociate the
191 bonded DNA from the magnetic nanoparticles, then vortexed until the pellet was (visually)
192 completely resuspended. With this approach, the DNA could be isolated and purified from
193 saliva samples and stored at 4°C until use. The DNA concentration was measured by
194 spectrophotometer (DN-1000 spectrophotometer, NanoDrop, Wilmington, DE, USA) and
195 verified by agarose gel electrophoresis.

196

197 2.9 Agarose gel Electrophoresis and Electrochemical analysis

198 The isolated DNA was analyzed by 1.2% agarose gel electrophoresis. The running
199 buffer was TAE (40mM Tris, 40mM acetic acid, 1mM EDTA, pH8.0. DNA ladder (New
200 England BioLabs) within the size range from 0.5 to 1.5 kb was used to monitor the size of
201 analyzed fragment The electrophoresis (Bio-Rad) was running at 100 V and 6 °C for 45 min.
202 The bands of interest were cut out with a sterile blade and transferred to a microcentrifuge
203 tube was divided into three aliquots and TE buffer (10 mM Tris–HCl pH 8, 1 mM EDTA,
204 ACS purity, Sigma-Aldrich) was added (dilution gel:TE buffer 1:0.5, 1:1 and 1:2)

205 . Electrochemical measurements were performed using a CHI660C electrochemical
206 workstation (CH Instruments, Shanghai, China). A three-electrode system was employed,
207 including a working GCE electrode, an Ag/AgCl reference electrode and a platinum wire
208 counter electrode using a standard cell with three electrodes. The adsorptive transfer technique
209 is based on the sample accumulation (120 s) onto the working electrode surface and
210 consequently on the electrode washing and square wave voltammetric (SWV) measurement.
211 All experiments were carried out at room temperature (21°C). SWV measurements were
212 carried out in the presence of acetate buffer pH 5.0. SWV parameters: start potential -0.65V,
213 end potential 0.15, potential step 4 mV, frequency 150 Hz, and amplitude 25.05 mV. In this
214 study, we demonstrate that the electrochemical analysis is a sensitive and powerful tool for
215 this type of investigations.

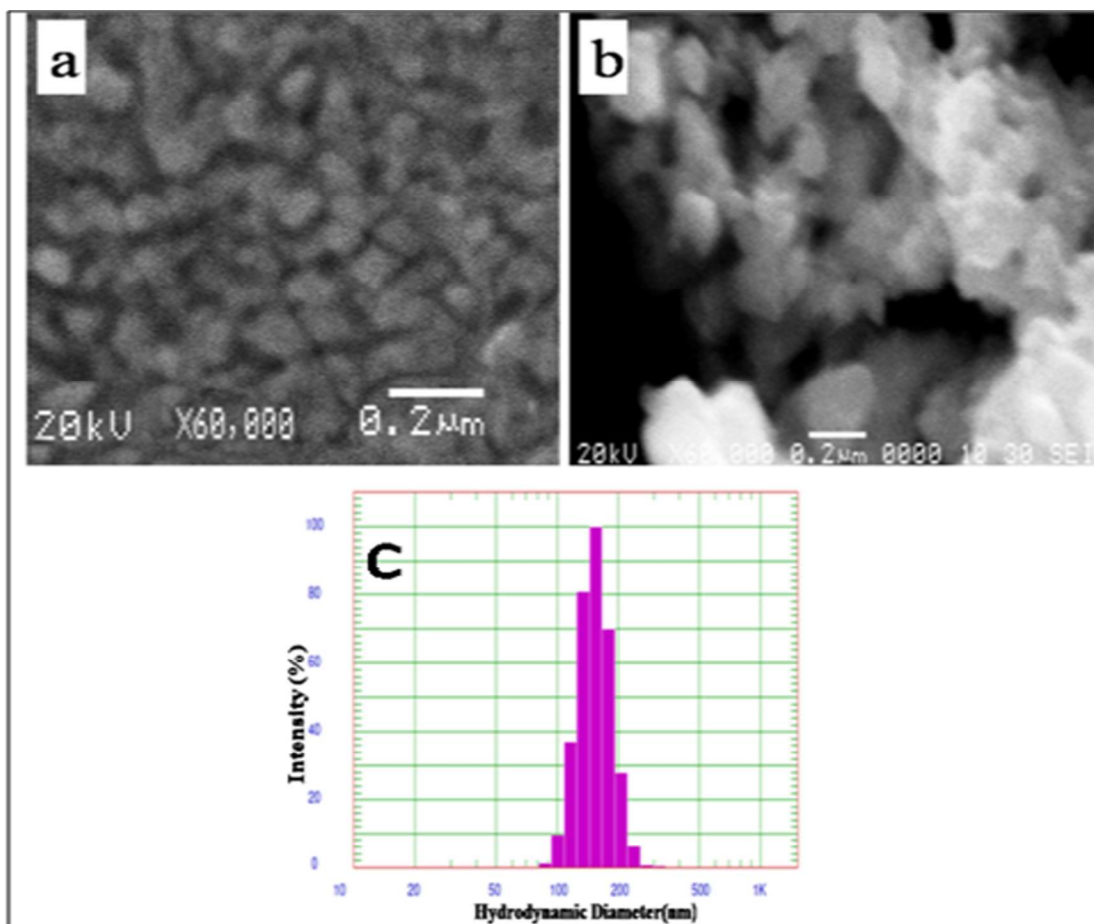
216 3. Results and Discussion

217 3.1 Size distribution and colloidal stability

218 **The morphological characteristics of bare Fe₃O₄ and Fe₃O₄ @silica@chitosan**
219 **Nanoparticles are shown in Fig 1a and b respectively. Spherical morphology was**
220 **observed in SEM images of bare Fe₃O₄ and Fe₃O₄ @silica@chitosan Nanoparticles .It is**
221 **evident that the morphology appearing in SEM images is the surface morphology of the**
222 **clusters of nanoparticles.** Dynamic light scattering analysis of the sample revealed that the
223 nanoparticles were monodispersed with average hydrodynamic diameter of 155.3 nm and a
224 variance of 0.036 [22, 24]. However, the average size of nanoparticles as determined by TEM
225 was approximately 17 nm as reported in our previous work. The reason for the difference in
226 size in DLS and TEM is attributed to sample preparation which is different in each of them. In
227 TEM, the chitosan-coated MNPs were spread out in a thin film and dried prior to

228 measurement, while DLS measured particle size in solution. Thus, TEM was capable of
229 distinguishing individually coated MNPs, while DLS measured the aggregation of MNPs in
230 solution.

231 The cationic character of the elaborated particles was pointed out via electrokinetic
232 study by measuring the zeta potential as a function of pH. It is noted that the particles are
233 positively charged at acidic pH with a surface potential greater than +40 mV. This confirms
234 the presence of amino groups on the particle surface in their protonated form, which is
235 attributed to the presence of chitosan on the particle surface. Because chitosan has multiple
236 amino groups, it is sensitive to the pH of the solution. The pKa of chitosan is 6.2, indicating
237 that at or near biological pH half of the amino groups are deprotonated, promoting
238 intramolecular hydrogen bonding and leading to precipitation. Chitosan modified particles
239 were found to produce a net positive charge at lower pH. The reason for positive charge is
240 because of the protonation of free amino group present on surface of chitosan modified
241 nanoparticles. At higher pH, that is towards basic the value of zeta potential changes from
242 positive to negative. The data implied that the nanoparticles could electrostatically bind
243 negatively charged DNA [25].



244

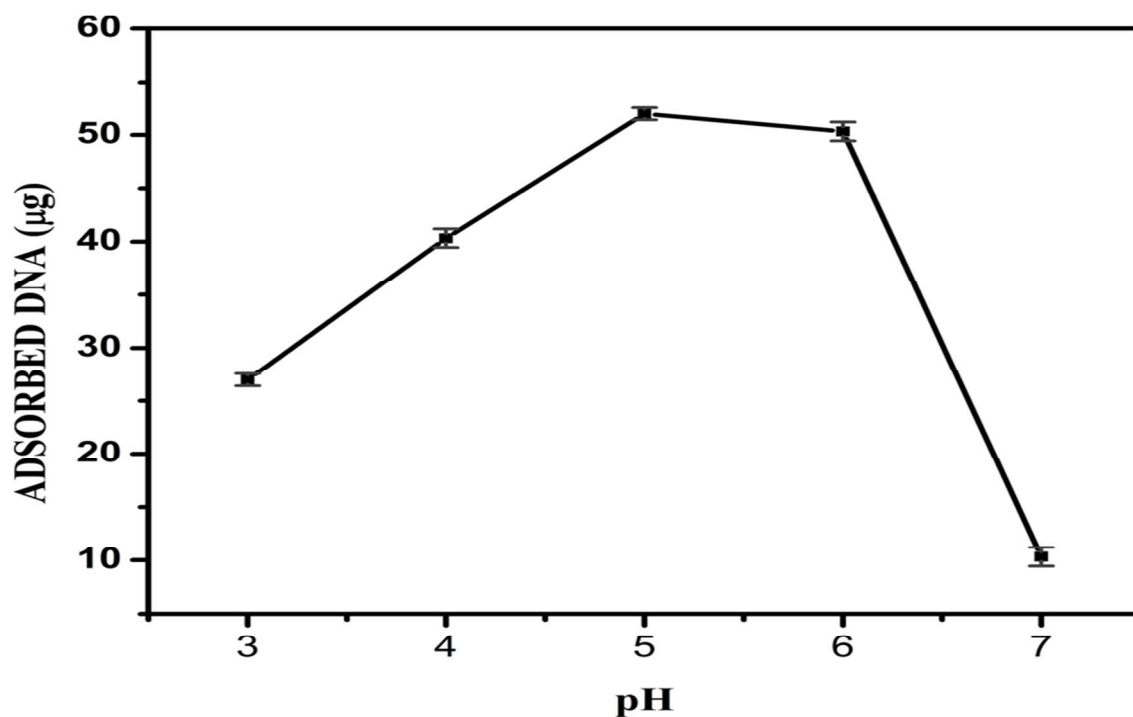
245 **Fig 1a. SEM of bare Fe₃O₄ nanoparticles, b. SEM of Fe₃O₄@silica@chitosan**
246 **Nanoparticles and c. Size distribution of chitosan functionalized Fe₃O₄.silica**
247 **superparamagnetic nanoparticles**

248

249 **3.2 DNA adsorption on Fe₃O₄@silica@chitosan Nanoparticles.**

250 The effect of the pH of buffer on the adsorption of DNA onto the surface of Fe₃O₄
251 @silica@chitosan nanoparticles was studied at different pH values ranging from 3.0 to 7.0
252 .The initial concentrations of DNA and nanoparticles were set at 20.0 mg/L and 20 mg,
253 respectively. Fig. 2 reveals that the maximum adsorption of DNA occurs at pH 5.0. As shown
254 in Fig. 4, the maximum amount of captured DNA (52 μg) occurred at pH 5. The DNA binding
255 efficiency at pH 5 was calculated to be 88%, as per Equation 1. The binding mechanism of
256 DNA on the surface of Fe₃O₄@silica@chitosan nanoparticles is most likely to be electrostatic

257 interactions between positively charged surface of the nanoparticle and negatively charged
258 phosphate backbone of DNA. DNA is the molecule with a backbone of phosphodiester
259 linkages. Phosphate groups are present in phosphodiester bond, and these are responsible for
260 imparting negative charge to DNA. At neutral pH DNA molecule is negatively charged. It is a
261 strong acid with pK_a value less than 1.0 Chitosan; a polycationic molecule has free amino
262 groups at low pH which gives positive charge to molecule. The pK_a of protonated amino
263 groups of chitosan is 6.2. Hence chitosan can hold positive charge below 6.2 and provide a
264 DNA capture state below 6.2. According to the data shown in figure maximal binding of DNA
265 occurs at pH 5.0. Above this pH the concentration of adsorbed DNA remains almost constant
266 to about pH 6.0. At pH above 6.0 there is a drastic decrease in amount of DNA adsorbed
267 owing to the pK_a of chitosan at which chitosan is deprotonated [26].



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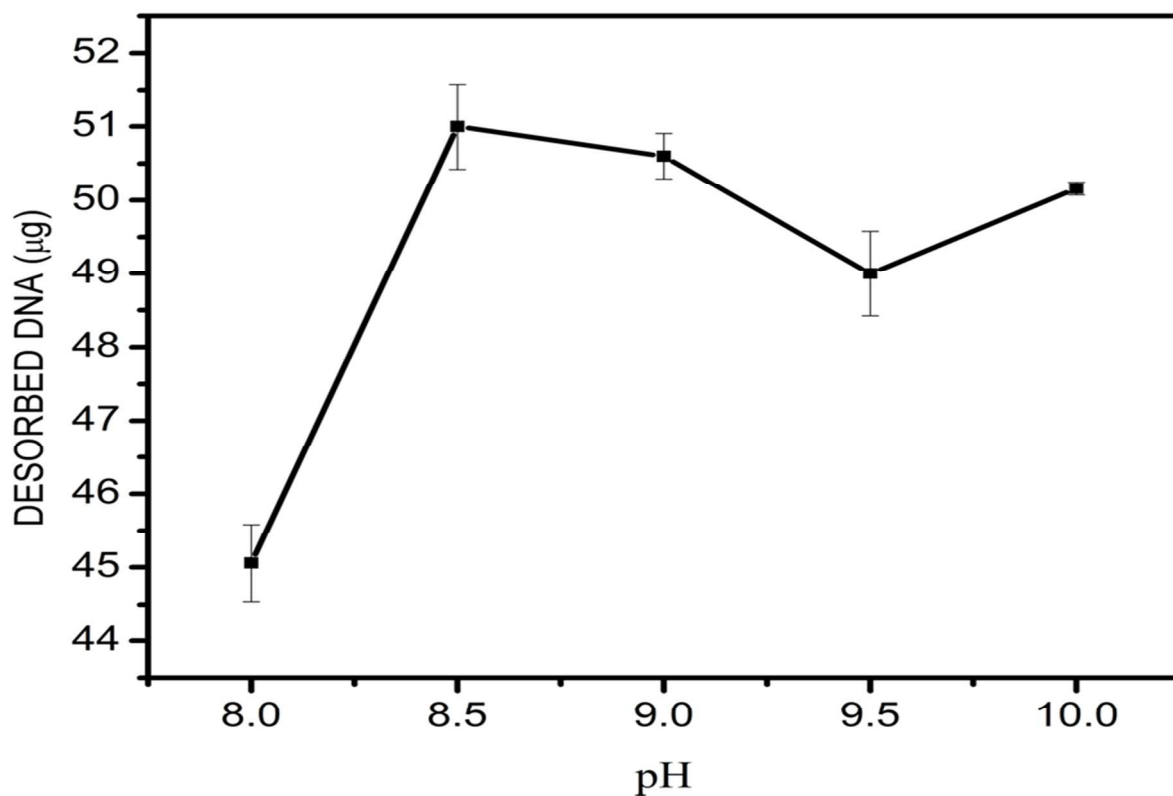
269

270

271 **Fig.2. Effect of pH on adsorption of DNA on Fe_3O_4 @silica@chitosan nanoparticles.**

272 **3.3 DNA desorption from Fe_3O_4 @silica@chitosan Nanoparticles.**

273 Fig. 3 represents the amount of DNA desorbed from the Fe₃O₄ @silica@chitosan
274 nanoparticles at basic pH. The amount of eluted DNA is maximum at pH 8.5. The desorbed
275 amount increases with the increase in pH of Tris buffer from 7.5 to 8.5. At pH 8.5 the desorbed
276 amount was found to be ~ 51.0 µg. The elution efficiency was calculated to be nearly 98%
277 which was expressed as per equation 2. Above pH 8.5, the desorbed DNA amount reached a
278 plateau. At pH 9.0, the amino groups in the chitosan modified MNPs are expected to be
279 deprotonated and the captured DNA can be eluted from the electrically neutral surface of the
280 MNPs with gentle agitation at room temperature. The elution of DNA occurs due to separation
281 of negatively charged DNA from positively charged nanoparticles. The positive charge of
282 particles is due to the amino group which deprotonates and becomes neutral above pH 6.2.
283 Hence negative charge separates from the surface of neutral nanoparticles [18].

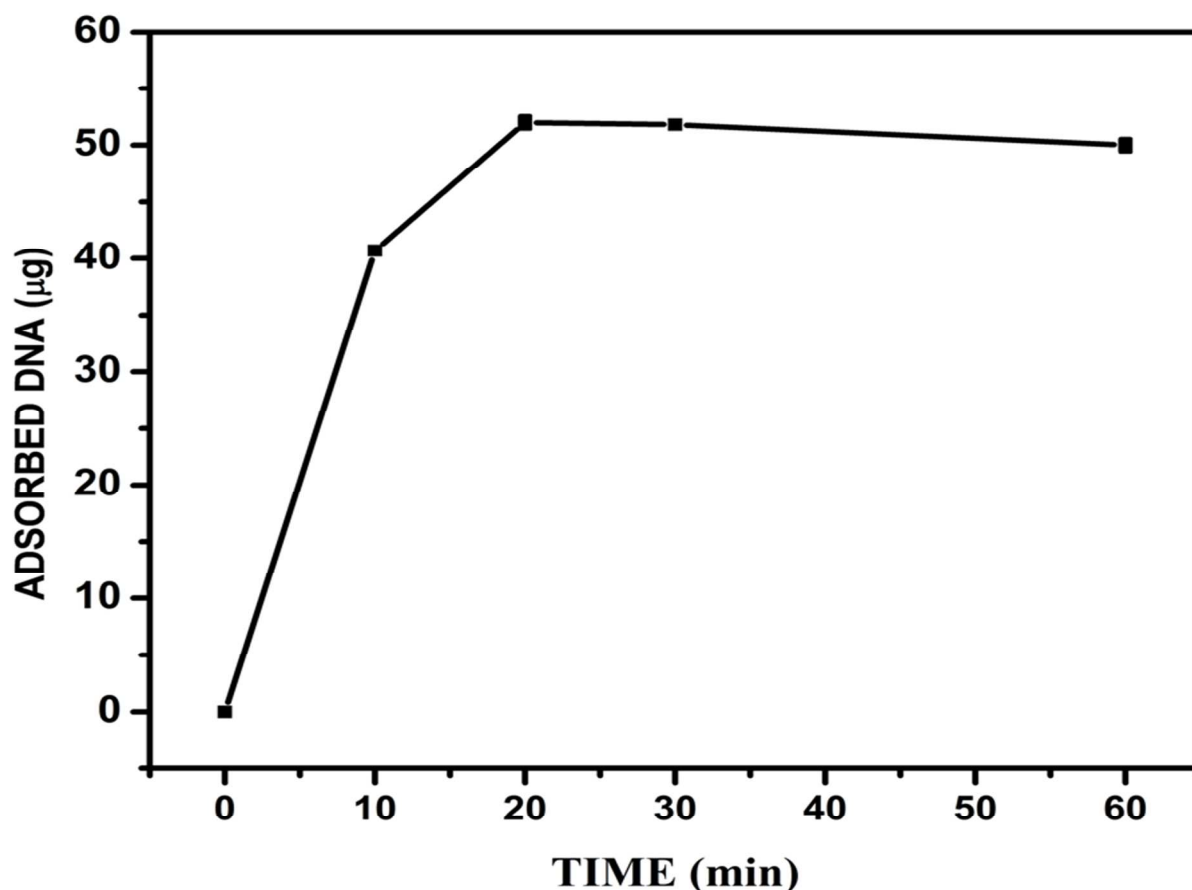


284
285 **Fig.3. Effect of pH on desorption of DNA from Fe₃O₄ @silica@chitosan nanoparticles.**

286 3.4 Effect of contact time

287 The effect of contact time on the amount of DNA adsorbed on Fe₃O₄
288 @silica@chitosan nanoparticles surface was assessed. The amount of nanoparticles was kept

289 20.0 mg and optimum pH of 5.0 was selected for this study. The result indicated maximum
290 adsorption at 20 minutes as shown in Fig. 4. However about 93% of DNA was adsorbed in less
291 than 10 min. The results point out the ability of nanoparticles to quickly adsorb DNA from
292 solutions in less time and hence can be utilized for fast isolation protocol.



293

294 **Fig.4. Effect of contact time on the amount of DNA adsorbed on Fe₃O₄@silica@chitosan**
295 **nanoparticles .**

296 **3.5 Effect of Temperature on binding of DNA to Fe₃O₄@silica@chitosan nanoparticles.**

297 The effect of temperature on adsorption of DNA on Fe₃O₄@silica@chitosan
298 nanoparticles was studied at optimal pH and stirring time of 10 min. Table.1 represents the
299 purity of DNA when subjected to different adsorption temperatures. The temperature has a
300 great role to play in DNA Adsorption. The double stranded DNA structure is maintained by
301 hydrogen bonds between the two strands. At temperatures above 90 ° C double stranded form

302 is separated into single strands and hence no adsorption of DNA should be expected. At low
 303 temperatures ($\leq 50\text{ }^{\circ}\text{C}$) both DNA and RNA are adsorbed on the particle. However when the
 304 temperature reached $70\text{ }^{\circ}\text{C}$ pure DNA was isolated and no RNA contamination was found and
 305 the purity remained constant to up to $90\text{ }^{\circ}\text{C}$. The A_{260}/A_{280} ratio indicates the presence of protein
 306 contamination at $30\text{ }^{\circ}\text{C}$ to $50\text{ }^{\circ}\text{C}$ adsorption temperatures and RNA contamination at
 307 temperatures above $80\text{ }^{\circ}\text{C}$ [27].

308 **Table.1** Purity of DNA when subjected to different adsorption temperatures.

Temperature	$30\text{ }^{\circ}\text{C}$	$50\text{ }^{\circ}\text{C}$	$70\text{ }^{\circ}\text{C}$	$80\text{ }^{\circ}\text{C}$	$90\text{ }^{\circ}\text{C}$
Purity (A_{260}/A_{280})	1.24	1.30	1.85	1.87	2.0

309

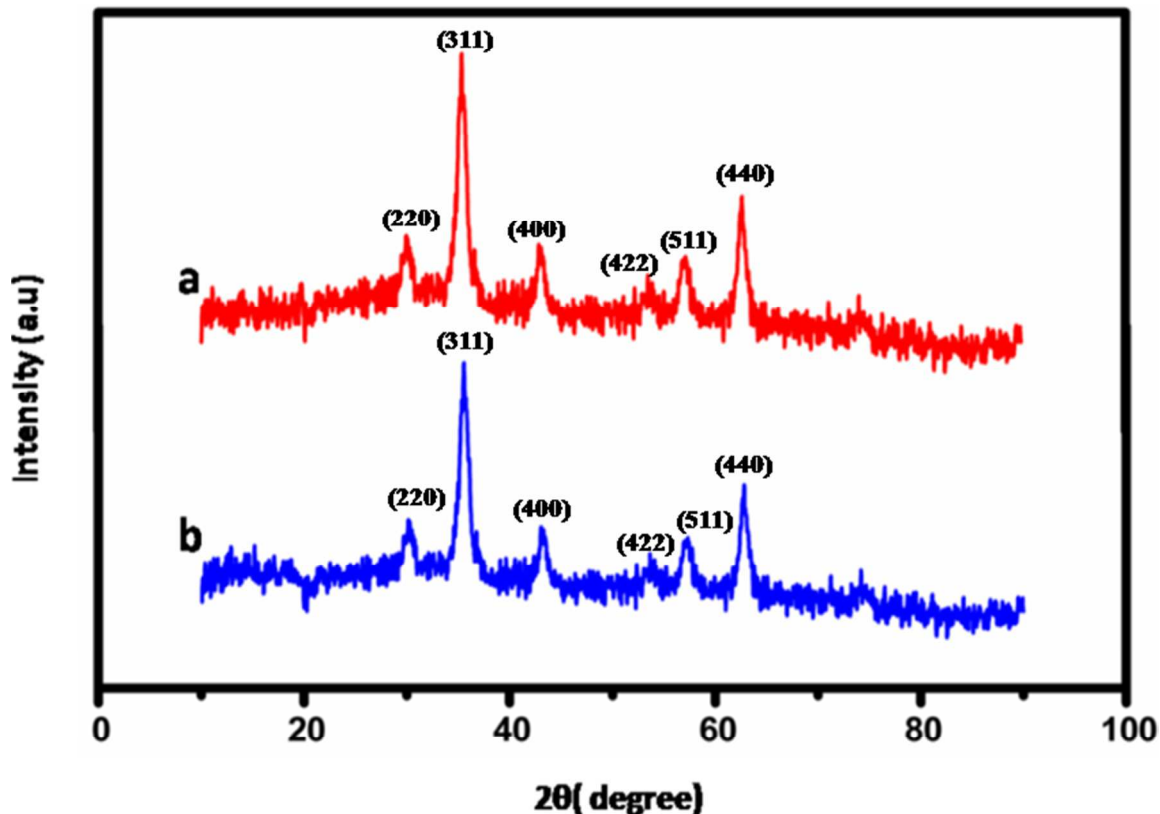
310 3.6 Reusability studies

311 Reusability studies were performed by assaying the concentration of DNA obtained
 312 from same amount of human saliva by using same set of Fe_3O_4 @silica@chitosan
 313 Nanoparticles for four subsequent experiments. The first experiment provided $52\text{ }\mu\text{g}$ DNA
 314 from 3 mL of saliva. When the same set of nanoparticles was used for second time the
 315 concentration of DNA obtained was $51\text{ }\mu\text{g}$. The obtained concentration was only 3% lower
 316 than that of the first experiment. Interestingly, even after fourth experiment high concentration
 317 of DNA was obtained. The yield after fourth experiment was $50.5\text{ }\mu\text{g}$ which are just 4% lower
 318 than the first experiment. It means even after repeated use the number of free positive groups
 319 are not decreasing significantly and hence taking part in adsorbing and eluting DNA with
 320 change in pH. This also indicates that the chitosan modified nanoparticles are highly stable.
 321 Excellent reusability of the particle makes it a suitable candidate for repeated DNA isolation.
 322 In the procedure reported in this paper, more than 96 % of DNA was desorbed in 30 min.

323 3.7 XRD pattern

324 The XRD pattern of Fe_3O_4 @silica@chitosan nanoparticles and DNA adsorbed Fe_3O_4
 325 @silica@chitosan nanoparticles are shown in Fig.5. From the absence of (210) and (300)
 326 peaks in the XRD pattern, it can be concluded that separate maghemite ($\text{g-Fe}_2\text{O}_3$) is not

327 present in the samples [28]. The appearance of hump at $2\theta \approx 13^\circ$, which represents the
 328 presence of a DNA molecule [29]. The XRD pattern of Chitosan@Silica@Fe₃O₄ nanoparticles
 329 and DNA adsorbed Chitosan@Silica@Fe₃O₄ nanoparticles.

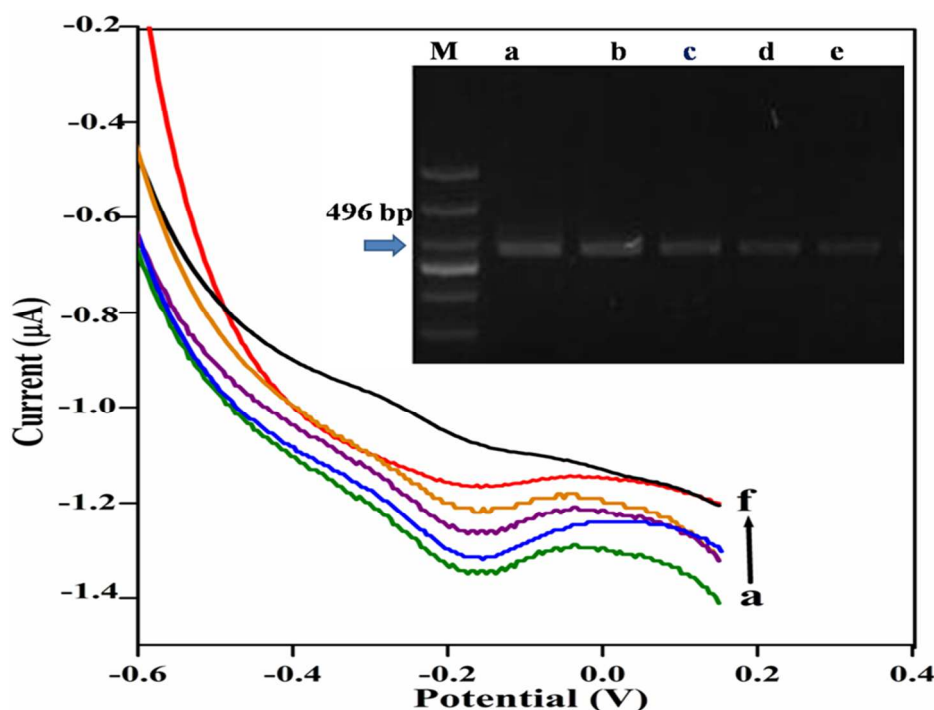


330
 331 **Fig.5** The XRD pattern of Fe₃O₄ @silica@chitosan nanoparticles and DNA adsorbed Fe₃O₄
 332 @silica@chitosan nanoparticles

333 3.8 Agarose gel electrophoresis and electrochemical analysis of the isolated DNA

334 DNA isolated by different concentration of MNP's is displayed in Agarose gel
 335 electrophoresis; the isolated DNA samples provided sharp bands with size of 496 bp (Fig. 6
 336 inset). To obtain the quantitative information about DNA fragment concentration, square
 337 wave voltammetry was used. The voltammetry is very sensitive method for DNA detection,
 338 suitable for miniaturization as well as monitoring of DNA interactions [30]. The
 339 electrochemical signals of extracted DNA are shown in Fig.6 illustrating that the extraction
 340 process is dependent on DNA concentration. The linearity of this dependence is expressed by
 341 correlation coefficient $R^2 = 0.9945$ as depicted in **Supplementary No. 1**. Fig.6. Square Wave

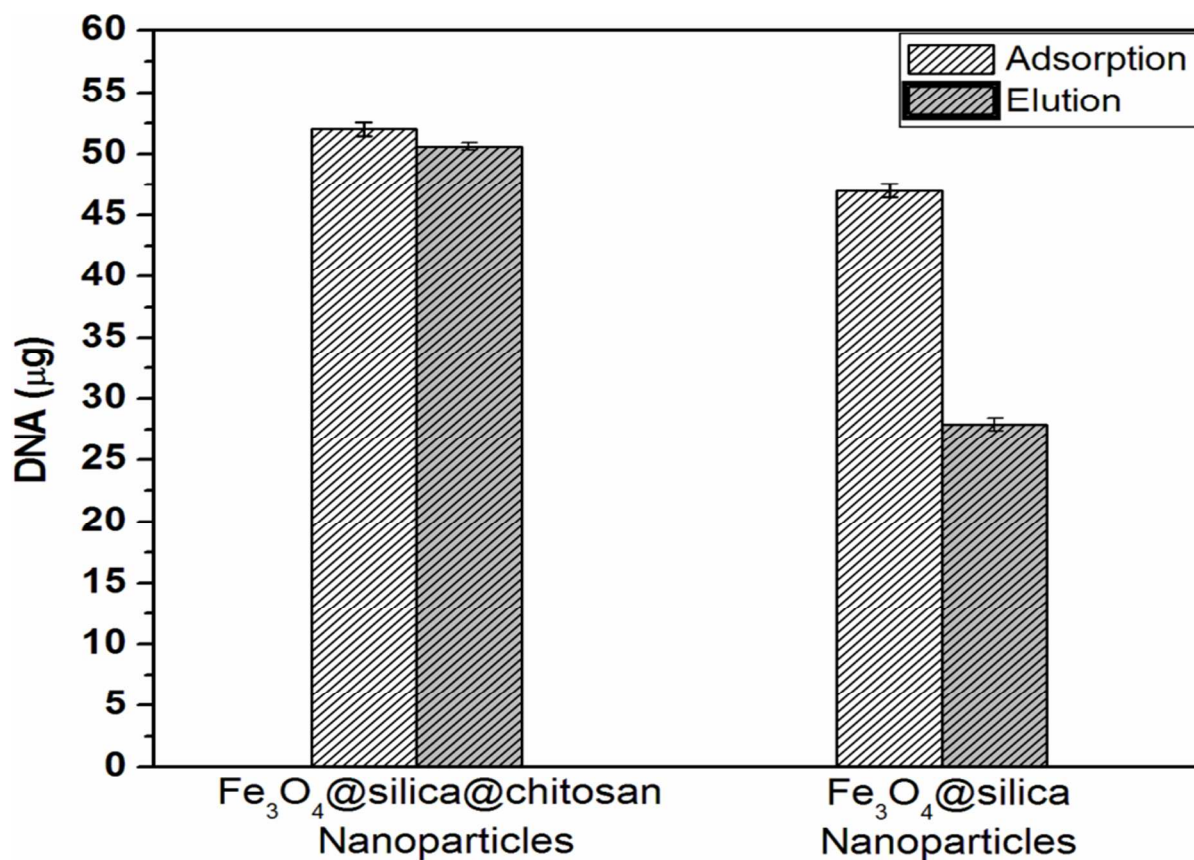
342 Voltammetry and inset: Agarose gel electrophoresis of isolated DNA with (a) 20mg, (b) 16mg
 343 (c) 12mg, (d) 8mg, (e) 4mg of Chitosan@Silica@Fe₃O₄nanoparticles and (f) electrolyte.



344
 345 **Fig.6. Square wave voltammetry and Inset: Agarose gel electrophoresis of isolated DNA**
 346 **with (a) 20mg, (b) 16mg (c) 12mg, (d) 8mg, (e) 4mg of chitosan functionalized Fe₃O₄.**
 347 **silica superparamagnetic nanoparticles and (f) electrolyte**

348 **3.9 Comparing DNA adsorption efficiency of Fe₃O₄ @silica@chitosan nanoparticles with** 349 **Fe₃O₄ @silica**

350 The study completed in this work highlights the characteristics of Fe₃O₄ @silica@chitosan
 351 nanoparticles that make it advantageous for DNA adsorption applications. The work compares
 352 DNA adsorption by chitosan coated Fe₃O₄ @silica under totally aqueous conditions with Fe₃O₄
 353 @silica under chaotropic conditions. As evident from the Fig.7, the adsorption efficiencies of
 354 Fe₃O₄ @silica@chitosan and Fe₃O₄ @silica nanoparticles was ~ 88% and ~80% respectively.
 355 Interestingly, the elution efficiency of Fe₃O₄ @silica@chitosan nanoparticles (~ 98%) was
 356 found much higher than elution efficiency of Fe₃O₄ @silica nanoparticles (60%).



357

358 **Fig.7. Comparison of Adsorption and Elution efficiency of Fe₃O₄ @silica@chitosan**
 359 **nanoparticles with Fe₃O₄ @silica nanoparticles.**

360 The properties of Fe₃O₄ @silica@chitosan nanoparticles are compared with some recently
 361 reported materials used for DNA isolation and adsorption in Table 2.

362 **Table. 2 Comparative study of present work with some recently reported materials used**
 363 **for DNA isolation and adsorption**

Materials	Properties favorable for DNA purification	Reference
1. Fe ₃ O ₄ /SiO ₂ -GPTMSDEAE	a) Paramagnetic, pH tunable surface charge, highly stable. b) Size: 200 nm, Magnetization: 30.081 emu/g A ₂₆₀ /A ₂₈₀ : 1.79, yield: 4.75 µg from 0.2 mL Blood.	[2]
2. Haemoglobin modified	a) Superparamagnetic,	

magnetic nanocomposites	pH tunable surface charge, highly stable . b) Average crystallite size: 15.3nm [31] A_{260}/A_{280} :1.84,yield:10.5 μ gm from 1ml bacterial culture.	
3.Iron oxide nanoparticles	a) Superparamagnetic, stable, large surface area. [32] b) A_{260}/A_{280} :1.7, yield :18-20 μ g	
4.Fe ₃ O ₄ @PANI	a) High magnetization, well dispersed, [33] b) Average crystallite size: 30 nm, A_{260}/A_{280} :1.79 yield: 20.8 μ g with 10mg of Fe ₃ O ₄ @PANI from 20 μ l of crude extract.	
5.Salicylic acid coated magnetic nanoparticles.	a) Higher surface area to volume ratio, stable monodispersable. A_{260}/A_{280} :1.83, yield: 160.6 μ g/ μ L from [34] mammalian cells.	
6.Chitosan functionalized Fe ₃ O ₄ -silica superparamagnetic nanoparticles	a) Superparamagnetic, highly stable, small size, pH tunable surface charge, can be reused. Present work b) Average crystallite size: 17nm A_{260}/A_{280} : 1.85, yield: 52 μ g from 3mL Human saliva.	

364

365 It is evident that the proposed material not only has comparable properties similar to recently
366 reported materials but is better in terms of superparamagnetic nature, pH tunable surface
367 charge, and in isolation of high yields pure DNA.

368 4. Conclusion

369 Isolation and extraction of DNA from biological samples has always been of great interest and
370 challenging to scientific fraternity. Higher percentage of isolation with maintaining the good
371 quality of DNA has been concern for various known DNA isolating systems. We have
372 developed pH responsive magnetic nanoparticles for successful isolation of genomic DNA

373 from human saliva. This has potential to extend the usability in other biological samples too.
374 An investigation on the adsorption and desorption of DNA to the surface of magnetic
375 nanoparticles was performed. The optimized parameters of pH, temperature and concentration
376 were utilized for isolation of genomic DNA from human saliva. We could determine ~95%
377 DNA isolation ability, faster isolation with in 10 min of time frame and significant reusability,
378 with ~55% DNA isolation even after 5 cycles of use, make these particles highly potent in this
379 process. It also can be concluded that the proposed magnetic nanoparticles can very efficiently
380 bind to DNA and rapidly isolate DNA from real samples. The pH sensitive magnetic
381 nanoparticles are well suited not only for routine laboratory use, but also the simplicity of this
382 approach specifies their potential for automated DNA purification. The prepared Fe₃O₄
383 @silica@chitosan nanoparticle present promising prospects to be used as magnetic carrier in
384 medical diagnosis for non specific capture, detection and isolation of nucleic acid.

385 Acknowledgement

386 Authors are very grateful to Department of Physics, Shivaji University, Kolhapur for giving
387 U.V visible measurements. Authors are also thankful to DST for providing financial support.

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