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Graphical Abstract:



**Biobased thermoplastic elastomer** 

1	
2	Novel biobased thermoplastic elastomer consisting of synthetic polyester
3	elastomer and polylactide by in situ dynamical crosslinking method
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15	

1 **ABSTRACT:** Owing to the sustainability and environmental friendliness of biobased 2 polymers, we adopted synthesized biobased polyester elastomer (BPE) and polylactide (PLA) as the 3 two components to produce a new biobased thermoplastic vulcanizate (TPV) by an in situ 4 dynamical crosslinking and mixing method. The effects of blending ratio on the dynamic 5 crosslinking and micromorphology of TPV were investigated by mixing torque measurements, degree of crosslinking measurements, TEM, DSC, and rheological properties. A large amount of 6 crosslinked BPE particles were dispersed in the PLA continuous phase, with the particle sizes 7 8 ranging from 1 to 4  $\mu$ m, indicating the occurrence of phase inversion during the dynamical 9 crosslinking and mixing process. The tensile strength and elongation at break of the biobased TPVs 10 ranged from 11.4 MPa to 17.8 MPa and 154% to 184%, respectively. Reprocessing did not significantly reduce the mechanical properties, as an indication that biobased TPVs, like 11 12 thermoplastics, have good reprocessability. In vitro cytotoxicity tests showed that our TPVs were 13 nontoxic, at least towards mouse fibroblasts. Thus, these novel biobased TPVs with excellent 14 mechanical properties and low cytotoxicity are reported for the first time in the flied of 15 thermoplastic elastomers for engineering and biomedical applications.

16

17 KEYWORDS: Biobased thermoplastic vulcanizate; Morphology; Reprocessability;
18 Biocompatibility

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# 1 **INTRODUCTION**

Thermoplastic elastomers (TPEs) behave like conventional elastomers, but they are thermoplastic and can be reshaped and recycled. TPEs represent a great technological advance since they pose less threat to the environment.[1] Compared with traditional rubbers, TPEs do not require further crosslinking, can be processed in simple machines, and consume less energy. Besides, the scraps generated during production can be reground and recycled, which could save the petroleum resources and reduce environmental pollution. TPEs have proven themselves in meeting a wide range of demanding engineering requirements in automotive applications.[2]

9 TPEs are classified into two categories according to the method of preparation: (i) chemically 10 synthesized TPEs, including styrenic block copolymers, thermoplastic copolyesters, thermoplastic 11 polyurethanes, and thermoplastic polyamides; (ii) blends and elastomeric alloys, containing 12 elastomer-plastic simple blends, thermoplastic vulcanizates (TPVs), and melt-processable 13 rubbers.[3] TPVs are a very special class of TPEs, consisting of a thermoplastic matrix and a 14 crosslinked elastomer as the dispersed phase.[3-5] TPVs are produced by dynamic crosslinking, 15 which consist of the selective crosslinking of the vast elastomer and its fine dispersion in the 16 thermoplastic under intensive mixing. The elastomer is the majority component, and its weight 17 fraction is greater than 50%. The increasing viscosity and elasticity of the elastomer through 18 vulcanization affects the phase continuity and promotes the phase inversion, i.e. the majority phase 19 becomes the dispersed phase.[6] TPVs have several advantages over the traditional thermoset 20 elastomer. Functional properties of TPVs similar to those of thermoset elastomers can be obtained 21 by using the classical processing tools for polymer melts, but, at the same time, TPVs are recyclable

as thermoplastics. TPVs have been widely applied to various fields such as the automobile, building,
and electronic industries. Nowadays, TPV is produced worldwide at a rate of 450,000 tons per
annum. Nevertheless, the current TPVs are blends of petroleum-dependent polymers such as
ethylene–propylene–diene rubber (EPDM)/polypropylene (PP) blend, acrylonitrile–butadiene
rubber (NBR)/PP blend, NBR/polyethylene (PE) blend, EPDM/PE blend, EPDM/nylon-6 blend,
acrylate rubber (ACM)/nylon-6 blend, and butyl rubber (IIR)/polyamide blend.[7-13]

7 Biobased polymers have attracted much attention in the past decades owing to environmental 8 concerns, climate change, and the depletion of fossil fuels. Biobased polymers are currently 9 sustainable alternatives to conventional petroleum-based polymers, and these polymers derived 10 from renewable resources mainly include starch-based polymers, polylactide (PLA), 11 polyhydroxyalkanoates (PHAs), cellulosic-based polymers and soy-based polymers.[14-18] One of 12 the most promising polymers in this regard is PLA, whose monomer has been produced by the 13 microbial fermentation of agricultural by-products on a commercial scale.[19] PLA is not only 14 renewable but also biodegradable; therefore, it has been used in medical materials, disposable 15 plastics, and fibers. Although many biobased elastomers have been reported, such as poly(glycerol 16 sebacate)[20], poly(polyol sebacate)[21], and poly(diol citrate)[22], these elastomers were designed 17 for biomedical materials with fast degradation. Recently, our group has focused on the use of 18 large-scaled biobased monomers to synthesize biobased elastomers with excellent mechanical 19 properties and environment stability for engineering applications.[23-25]

The synthesis of TPEs based on renewable resources has also gained extensive academic interests.
For example, biobased TPUs were synthesized from diphenylmethane diisocyanate, 1,4-butanediol,

# **RSC Advances Accepted Manuscript**

# **RSC** Advances

Page 6 of 37

1	and a polyol based on a di-functional dimer fatty acid.[26] Kobayashi et al. prepared novel biobased
2	TPEs by the enzymatic copolymerization of macrolide as the hard segments and 12-hydroxystearate
3	as the soft segments.[27] Wanamaker et al. developed a series of biobased TPEs with polylactide as
4	the hard segments and polymenthide as the soft segments.[28] However, up to now, there is few
5	report on using a blending method to prepare TPVs from biobased polymers. Consequently, the
6	development of totally biobased TPVs is of great importance and highly desired in both academia
7	and industry, providing an alternative to traditional petroleum-based TPVs.
8	Biobased polyester elastomer (BPE) synthesized from biobased diols and diacids have been
9	developed in our laboratory.[23] These elastomers exhibit satisfactory elasticity, excellent
10	mechanical properties after reinforcement and good biocompatibility. In the present work, biobased
11	plastic (PLA) and biobased polyester elastomer (BPE) are chosen as the two components to prepare
12	a new TPV derived exclusively from renewable resources by the dynamic in situ crosslinking
13	method. The important reason for choosing PLA as the plastic matrix and BPE as the rubber matrix
14	was the potential compatibility between PLA and BPE.[29] The effects of composition on the
15	properties of the biobased TPVs, such as morphology, rheological properties, mechanical properties,
16	reprocessability, and biocompatibility were studied. Biobased TPVs with both reprocessability and
17	thermoplasticity were first reported by in situ dynamic crosslinking and mixing.
10	

# 1 MATERIALS AND METHODS

2 **Raw Materials.** The polylactide (PLA) was purchased from Natureworks (USA) as grade 2002D. It has a density of 1.24 g/cm<sup>3</sup>, a number-average molecular weight of ~133,000 g/mol, a 3 4 polydispersity index of 1.50, a glass transition temperature of 60 °C, and a melting point of 152 °C. 5 Our biobased polyester elastomer (BPE), which was synthesized according to a procedure described 6 previously, [23, 29] had a number-average molecular weight of ~35,000 g/mol, a polydispersity index of 3.69, and a Tg of -56 °C. The dicumyl peroxide (DCP) used was commercial product. The 7 8 BPE chemical structures are shown in Scheme 1. BPE, with the presence of itaconate, can be 9 readily crosslinked by dicumyl peroxide (DCP) into a network.

10 Preparation of Biobased TPVs. BPE and PLA were dried in a vacuum oven at 60 °C for at least 12 11 h before processing. The dynamically crosslinked BPE/PLA blends were fabricated by the 12 following steps: (i) a BPE/PLA premix was prepared by melt-mixing with a given blending ratio 13 BPE/PLA (60/40, 70/30, or 80/20) for 5 min by using a Haake internal mixer (HAAKE Rheomix 14 600 OS, Thermal Fisher Scientific, USA) at 170 °C at a rotational speed of 80 rpm; (ii) the 15 BPE/PLA premix and DCP were mixed on a 6-inch two-roll mill at room temperature to produce a 16 BPE/PLA blend; (iii) the BPE/PLA blend from step-(ii) was dynamically crosslinked for 8 min at 170 °C at a rotational speed of 80 rpm in the Haake internal mixer. The dynamically crosslinked 17 sample was hot-pressed at 180 °C to form 1 mm thick sheets, which were then cold-pressed. 18

19 **Characterization.** The morphology was determined by an H-800-1 transmission electron 20 microscope (Hitachi Co., Japan) at 200 kV. The samples were cryomicrotomed at -100 °C to 21 produce sections with 60 nm thickness, which were then vapor-stained with  $OsO_4$  for 20 min.

1	The dumbbell-shaped specimens were measured according to ASTM D412 by using a CMT 4104
2	electrical tensile instrument (Shenzhen SANS Test Machine Co., Ltd., China) at a crosshead speed
3	of 500 mm/min. For each BPE/PLA ratio, five specimens were tested and the average was taken. To
4	evaluate the reprocessability of the biobased TPVs, we reprocessed each biobased TPV for five
5	times by mixing the TPV in a Haake internal mixer for 8 min and compression molding at 180 °C to
6	form 1 mm thick sheets, and the tensile properties of the reprocessed biobased TPVs were measured.
7	Rheological measurements were performed on an RPA 2000 rheometer (Alpha Technologies, Akron,
8	Ohio). The strain scanning conditions were 180 °C, 1 Hz, and a strain range of 0.2-470%. For a
9	detailed study on the performance of the reprocessed biobased TPVs, we reset the RPA strain
10	scanning conditions to track the changes in rheological properties. Each sample underwent the
11	following test sequences: (i) to simulate the mixing process, the following conditions were used: a
12	temperature of 180 °C, a frequency of 1 Hz, and a strain range of 0.2-470%; (ii) to simulate the
13	molding process, a temperature of 180 °C was maintained for 5 min. Each scanning process was
14	repeated 5 times.

In vitro cytotoxicity testing was carried out on mouse fibroblasts (L-929) by MTT assays. All samples were sterilized with 75% ethanol and then rinsed twice with PBS solution. The samples were exposed to  $Co^{60}$  for 15 min and incubated in Dulbecco's modified Eagle's medium (DMEM) at a proportion of 3 cm<sup>2</sup>/ml for 24 h at 37 °C. The extract solution was then filtered (0.22 µm pore size) to eliminate any solid particles in the sample. L929 cells were grown in DMEM supplemented with 10% fetal bovine serum (FBS) at a density of  $5.0 \times 10^4$  cells/well and incubated in 5% CO<sub>2</sub> under humidified conditions at 37 °C. After the incubation, the medium was replaced by the

1	prepared extract dilution which was used as the new culture medium, while the initial medium was
2	used as a negative control. The cells were allowed to proliferate for 3 days, and the number of
3	viable cells was determined by adding 5 mg/mL of MTT in the culture medium. After a further
4	incubation of 4 h, the medium was aspirated, the formed blue formazan crystals were dissolved in
5	isopropanol (BDH, Poole, England), and the absorbance at 570 nm was determined. All sample
6	extracts were tested at least three times to obtain consistent results. The relative viability was
7	calculated by
8	Relative cell viability = $(A_{test} - A_0)/(A_{control} - A_0)$ (1)
9	where $A_{test}$ is the absorbance of the sample, $A_{control}$ is the absorbance of the controlled well
10	containing cells with DMEM, and $A_0$ is the absorbance of the solution containing only DMEM. The
11	morphology of the sample incubated for 3 days was observed by an inverted phase contrast

12 microscope before MTT testing.

## 1 **RESULT AND DISCUSSION**

2 *Mixing Torque and Temperature.* Figure 1 shows the mixing torque and temperature as a function 3 of time during the dynamic crosslinking of the BPE/PLA blends with different blending ratios of 4 BPE/PLA prepared by step-(ii) in section 2.2. Initially, the mixing torque increases with the increase 5 in mixing time because of the introduction of the cold BPE/PLA blend into the mixer, and then 6 decreases owing to the melting of the blend. The subsequent dramatic increase in mixing torque is 7 related to the dramatic changes in the viscosity and elasticity of the BPE phase due to the 8 crosslinking of BPE. After that, the torque slowly declines until the end of the dynamic crosslinking 9 process, indicating the full homogenization of the biobased TPV. The temperature curve with 10 different DCP contents exhibits a decrease with the introduction of the cold BPE/PLA blends into 11 the hot mixer and the melting of the blends. Then the temperature increases continuously, 12 surpassing the set temperature due to viscous energy dissipation and crosslinking. The stable torque 13 and temperature of the biobased TPVs decrease as the BPE content increases because the high BPE 14 content results in a lower viscosity of the whole system. Both the torque and temperature curves are 15 similar to those reported for other dynamically crosslinked systems, such as EPDM/PP TPV[30, 31], 16 NBR/PP TPV[9].

*Morphology.* TPV morphology, which is one of the most crucial characteristics, results from the complex relationship between the composition, viscosity, and elasticity ratios of the individual components, the processing conditions, and the crosslinking reaction. We firstly investigated the effect of crosslinking agent content on the morphology of the biobased TPVs. The TEM micrographs of the biobased TPVs with different DCP contents are depicted in Figure 2. In the

1	TEM micrographs, PLA appears as the light domains and BPE as the dark domains owing to the
2	staining effect of the double bonds of BPE. PLA is dispersed in the BPE matrix and exhibits
3	elongated structures for the BPE/PLA blend without DCP (Figure 2(a)), because BPE, in a larger
4	amount than PLA, tends to form the continuous phase. With the addition of the curing agent DCP,
5	BPE is dispersed in the PLA matrix; that is, phase inversion has occurred after the in situ dynamic
6	crosslinking accompanied by mechanical mixing. The increase of DCP content increases the degree
7	of crosslinking of BPE, which can be validated by the dynamic crosslinking curves (Figure S1) and
8	extracting experiments (Figure S2) in the supporting information. For the biobased TPVs with a
9	lower DCP content (0.02 phr) (Figure 2(b)), the crosslinked BPE in the shape of thin strips exhibits
10	a larger particle size and heterogeneous distribution. A lower degree of crosslinking results in a
11	smaller difference in viscosity between BPE and PLA and thus produces lower shear during the
12	dynamical crosslinking process to separate the BPE particles. Besides, BPE flows and deforms
13	more easily at a lower degree of crosslinking and is thus prone to aggregate, leading to its
14	nonuniform dispersion in PLA matrix. The viscosity of the BPE phase increases with the increase of
15	DCP content, resulting in an increase in the difference between the viscosities of BPE and PLA and
16	an increase in the effective shear stress. The crosslinked BPE particles can be easily broken up into
17	smaller particles during shear and dispersed homogeneously in the PLA matrix, as shown in
18	Figure2(c). The higher the DCP content, the faster the crosslinking of the BPE phase and the earlier
19	the occurrence of phase inversion. In a relatively short time, the curing rate becomes far greater than
20	the shear rate, and it becomes too difficult for the PLA matrix, with a relatively low viscosity, to
21	break up the highly crosslinked and very viscous BPE into small particles. Thus, a high degree of

crosslinking results in the aggregation of large particles, and the morphology is shown in Figures 2 (d), 2(e). The particle size of BPE shown in Figure 2(c) is the smallest, demonstrating that the 3 optimal DCP content is 0.06 phr. Therefore, in the latter investigations we adopted a DCP content of 4 0.06 phr to prepare biobased TPVs. The diagrams of phase inversion for biobased TPVs with 5 different degree of crosslinking are shown in Scheme 2 to better illustrate the in situ dynamical 6 crosslinking process.

7 The performance of TPV is also related to the blending ratio of elastomer to plastic. If the TPV 8 contains high elastomer content, the performance of the TPV is close to that of traditional rubbers 9 and TPV exhibits better elasticity than TPE. However, a higher elastomer content will lead to a 10 higher difficulty in phase inversion and a larger size of the dispersion phase, thus resulting in a 11 reduction in mechanical properties and a poor thermoplastic process ability. Thus, the effect of 12 blending ratio on the morphology of biobased TPVs was investigated, and the TEM micrographs of 13 biobased TPVs with different blending ratio are depicted in Figure 3. The morphology of TPV 14 consists of vast BPE particles dispersed in the PLA continuous phase, indicating that the crosslinked 15 BPE particles are broken up into small particles and the phase inversion takes place during the 16 dynamic crosslinking process. The BPE particles have an irregular, oval or elongated shape. The 17 particles size ranges from 1 to 4  $\mu$ m, and some neighboring BPE particles are interconnected. At a 18 high BPE content (Figure 3(c)), there is obvious aggregation in the BPE phase, resulting in a larger 19 particle size and wide particle distribution. The high the BPE content, the higher the particle 20 aggregation and the more difficult the breakup of crosslinked BPE particles. In other words, a 21 higher BPE content makes phase inversion more difficult and results in larger BPE particles. These

1 results indicate that the blending ratio of elastomer to plastic has a great impact on the breakup of

2 the crosslinked elastomer phase during dynamic crosslinking.

3 Thermal Properties. The thermal behavior of pure BPE, neat PLA, and biobased TPVs was 4 investigated by DSC measurements. Figure 4 shows the DSC curves, and Table 1 summarizes the 5 relevant data. All the biobased TPVs exhibit two clear glass transitions  $(T_{\sigma})$ , demonstrating that BPE/PLA TPV is a phase-separated system during cooling. With the addition of BPE to PLA, the  $T_g$ 6 7 of PLA shifts to lower temperatures, while the  $T_g$  of BPE shifts to higher temperatures. The shifts of 8 these  $T_{es}$  towards each other indicate some compatibility between PLA and BPE. The heat of cold crystallization ( $\Delta H_{cc}$ ) and the heat of melting ( $\Delta H_m$ ) for the BPE component of the biobased TPVs 9 10 are lower than those for pure BPE because of the crosslinking of BPE. The cold crystallization 11 temperature  $(T_{cc})$  and  $\Delta H_{cc}$  of the PLA component increase with the addition of BPE, indicating an 12 increase in the degree of cold crystallization of PLA. The incorporation of flexible and branched 13 BPE chains resulted in larger free volume of PLA chains than neat PLA. Consequently, BPE 14 improved the mobility of PLA segment, and thus the cold crystalline ability of PLA was enhanced 15 **Rheological Properties.** TPVs can be processed by common plastic processing equipment, such as 16 extruders, injection and molders. Hence a thorough understanding of the flow behavior of biobased 17 TPVs under high shear is important to the determination of processing parameters. To explore the influence of the blending ratio on the rheological properties of biobased TPVs, a strain sweep test 18 19 was carried out at 180 °C. Figure 5 displays the variations of storage modulus (elastic modulus,  $G'_{1}$ ), 20 loss modulus (viscous modulus, G''), loss factor (tan  $\delta = G'/G'$ ) and complex viscosity ( $\eta^*$ ) with 21 strain amplitude for the biobased TPVs. The G' of the biobased TPVs exhibits a linear region at low

1	strains and nonlinear region at high strains. It can be clearly seen that $G'$ progressively decreases
2	with the increase of strain, similar the so-called Payne effect of filled rubber systems. Thus, the
3	rheological properties of TPVs can be analogically compared with that of the filled rubber system.
4	According to the Payne effect, the nonlinearity of $G'$ is related to the disintegration of the secondary
5	network of filler agglomerates. However, the secondary structure of TPVs corresponds to the
6	crosslinked BPE domains dispersed in the PLA matrix in the form of aggregates and/or
7	agglomerates. We can infer that this nonlinearity of TPVs is associated with the disintegration of
8	agglomerated BPE domains and the debonding of crosslinked BPE domains from the PLA matrix.
9	The $G'$ increases with the increasing BPE content because a higher content of crosslinked BPE
10	results in more elastic biobased TPVs and tend to form the strong networks of crosslinked BPE to
11	PLA.
12	The strain dependency of $G''$ of biobased TPVs is presented in Figure 5(b). $G''$ shows a maximum
13	in the transition region from the linear to nonlinear viscoelastic behavior. Generally, $G'$ is related to
14	the formation of filler networks and $G''$ to the breakdown and reformation of these structures. The
15	variation of $G''$ on strain depends on the rates of network breakdown and reformation as well as the
16	sliding of macromolecular chains at the domain surface. The value of loss maximum increases with
17	the increase of BPE content and appears at high strains. Biobased TPVs with higher BPE contents

have stronger networks, and the breakdown of larger crosslinked agglomerated BPE domains dissipates more energy. The loss factor is determined by both the loss and the storage modulus (tan  $\delta = G'/G''$ ). It can be seen from Figure 5(c) that biobased TPVs are more elastic (G' > G'') in the low strain region. With increasing strain, the G' and G'' curves intersect at tan  $\delta = 1$  (G'=G''). This

intersection denotes the transition from elastic to viscous behavior. With further increases in strain,
 the biobased TPVs become more viscous. The high elasticity at high content of crosslinked BPE is
 manifested by a substantial shift of the intersection point to higher strains.

The complex viscosity ( $\eta^*$ ) of biobased TPVs is shown in Figure 5(d). All biobased TPVs exhibit 4 a decrease in  $\eta^*$  with increasing strain, an indication of the shear thinning behavior of polymers. 5 6 According to the entanglement theory, the decrease in viscosity is attributed to a decrease in the entanglement deformation of the entanglement network. The  $\eta^*$  of biobased TPVs present a much 7 8 lower rate of decline with strain at low strains than at high strains. The behavior at low strains is 9 related to the strong network and molecular entanglement brought by crosslinked BPE to crosslinked BPE and crosslinked BPE to PLA. As the strain increases, the network tends to collapse 10 and deform, exhibiting higher shear thinning behavior. As shown in Figure 5(a), biobased TPVs 11 with high BPE contents have high viscosity, similarly to the highly filled rubber systems. The shear 12 13 thinning behavior of biobased TPVs with increasing strain rate is an indication of the good 14 processability of these materials.

*Mechanical Properties.* The stress-strain curves of the biobased TPVs with various blending ratios are shown in Figure 6, and the relative data are summarized in Table 2. Neat PLA shows very high tensile strength and low elongation at break, characteristic features of a brittle material, while neat BPE shows low tensile strength and high elongation at break, typical elastomeric characteristics. Compared with that of neat PLA, the stress-strain curves of biobased TPVs change from plastic (with necking and yielding) to elastic behavior (without necking and yielding). As shown in Figure 6, the tensile strength and hardness of the biobased TPVs decrease with increasing BPE content,

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range from 17.8 MPa to 7.4 MPa and 97° to 86°, respectively, implying the PLA phase is a major factor determining the tensile strength and hardness. The permanent set decreases with increasing BPE content. In addition, the elongation at break at a blending ratio of 80/20 (BPE/PLA, w/w) is relatively low, presumably because of the nonuniform distribution of the crosslinked BPE particles in the PLA matrix (as shown in Figure 3(c)). Generally, TPVs exhibit large reversibility and small residual strains. The elastomeric crosslinked BPE particles dispersed in the PLA matrix make the biobased TPVs recoverable from a highly deformed state. As a result, the higher the BPE contents, the smaller the tensile set at break and the higher the elasticity, as shown in Figure 6(b). The tensile sets at break of the biobased TPVs with a BPE content higher than 70% are smaller than 30%, indicating excellent elastic recovery. **Reprocessability of Biobased TPVs.** An advantage of TPVs over conventional thermosetting rubbers is that TPVs can be reprocessed without significantly changing their physical properties. To

13 examine the reprocessability of the biobased TPVs, the tensile properties of the TPV with a 14 blending ratio of 70/30 were measured after the TPV was reprocessed one, three, and five times, 15 and the results are shown in Figure 7. Figure 7 shows that the tensile strength and elongation at 16 break of the TPV do not change significantly after it was reprocessed one and three times. These 17 results indicate that the biobased TPVs can be reprocessed without significant reduction of 18 mechanical properties, behaving like a TPE. However, the tensile strength significantly decreases 19 after the TPV was reprocessed five times because of the breakdown of crosslinked BPE domain 20 from the strain during the process.

21 To track the changes of rheological properties of the biobased TPVs after reprocessing, we

### **RSC Advances**

adopted RPA to simulate the molding cycle. Strain scanning was used to simulate the mixing	
process and the TPV was kept in the die at 180 °C for 5 min to simulate the molding process. The	
complex modulus ( $G^*$ ) and complex viscosity ( $\eta^*$ ) as a functional of strain for the biobased TPVs	
with a blending ratio of 70/30 are shown in Figure 8. The variations of $G^*$ and $\eta^*$ at low and high	
strain amplitudes in all the five strain sweeps are shown in Table 3. The $G^*$ and $\eta^*$ decrease with	ipt
increasing strain amplitude, manifestations of the Payne effect. Both $G^*$ and $\eta^*$ slightly decrease	SCL
with the number of sweep tests at the same strain amplitude. The modulus $G^*$ at a strain of 1%	ŝnu
recovers to 90% and 70% of the initial modulus in the 2nd sweep and 5th run sweep, respectively,	Mai
while the $G^*$ at 470% strain is recovers to only 75% and 49% in the 2nd sweep and 5th run sweep,	D
respectively. The changes of $\eta^*$ are similar to those of $G^*$ . These results are attributed to the	pte
irreversible deformation of the network formed by the disintegration of crosslinked BPE aggregates	Ce
and debonding of BPE domains from the PLA matrix, as well as the rupture of chain entanglements	Ac
and chains connecting the aggregates, corresponding to the Mullins effect or stress softening effect.	<b>B</b>
However, the changes of $G^*$ and $\eta^*$ in the low strain region are readily recovered, suggesting that	Ŭ D
the BPE domains form highly elastic networks at low strains.	Va
<i>Biocompatibility.</i> The cytotoxicity of a material is evaluated to determine whether it is suitable for	Ad
biomedical applications. In vitro cytotoxicity testing by MTT colorimetry is used to evaluate the	S

2 process and the TPV was kept in the die at 180 °C for 5 min to simulate the complex modulus ( $G^*$ ) and complex viscosity ( $\eta^*$ ) as a functional of strain 3 4 with a blending ratio of 70/30 are shown in Figure 8. The variations of G 5 strain amplitudes in all the five strain sweeps are shown in Table 3. The increasing strain amplitude, manifestations of the Payne effect. Both  $G^*$ 6 7 with the number of sweep tests at the same strain amplitude. The modul 8 recovers to 90% and 70% of the initial modulus in the 2nd sweep and 5th while the  $G^*$  at 470% strain is recovers to only 75% and 49% in the 2nd sy 9 10 respectively. The changes of  $\eta^*$  are similar to those of  $G^*$ . These resu 11 irreversible deformation of the network formed by the disintegration of cro 12 and debonding of BPE domains from the PLA matrix, as well as the rupture 13 and chains connecting the aggregates, corresponding to the Mullins effect However, the changes of  $G^*$  and  $\eta^*$  in the low strain region are readily re 14 15 the BPE domains form highly elastic networks at low strains.

16 **Biocompatibility.** The cytotoxicity of a material is evaluated to determine 17 biomedical applications. In vitro cytotoxicity testing by MTT colorimetry 18 biocompatibility of a material. L929 mouse fibroblasts were used in our cytotoxicity assays by 19 observing the number and morphology of L929 cells in extract. The values of optical density (OD) 20 correspond to the number of the live cells in the extract. Based on the cell relative growth rates 21 (RGR) calculated from the OD values, the cytotoxicity of materials can be classified into six grades, which are shown in Table 4. Grades 0 and 1 mean that the material presents very low or no cytotoxicity to L929 cells, and grades 0 and 1 are accepted as "qualified" in biomedicine. A material with Grade 2 should be further considered by combining with cell morphology. Other grades are regarded as "unqualified," indicating that the material presents very high cytotoxicity and cannot be used as a biomaterial.

6 The RGR values of the biobased TPVs are displayed in Figure 9. The RGR values of all TPVs 7 are higher than 75%, indicating that all TPVs belong to grade 1 and show low cytotoxicity to L929 8 cells. These results demonstrate that our biobased TPVs have acceptable biocompatibility. The 9 morphologies of L929 cells incubated for 3 days in the negative control and extract solutions are 10 shown in Figure 10. As shown in Figure 10(a)-(d), the L929 cells show a normal stellate 11 morphology and no negative response, implying that the cells are in good condition. Besides, the 12 cell densities of the biobased TPVs are similar to that of the negative control. In conclusion, our 13 cytotoxicity assays indicated that the biobased TPVs could be potentially used as biomedical 14 materials.

# 15 CONCLUSION

In the present work, we have developed novel biobased TPVs via the dynamic crosslinking of biobased polyester elastomer (BPE) and polylactide (PLA), in which a large amount of crosslinked BPE particles were dispersed in PLA matrix. The TEM results showed that the BPE particles had an average diameter of 1 to 4 μm in bioabased TPVs. The glass transition temperatures of BPE and PLA shifted towards each other, indicating some compatibility between BPE and PLA. The rheological studies revealed that the dispersed BPE phase formed an agglomerate network in the

1 biobased TPVs. The storage modulus and complex viscosity increase with the increasing BPE 2 content, because the elasticity and the viscosity of biobased TPVs increase with increasing degree 3 of crosslinking of BPE. The tensile strength and elongation at break of the biobased TPVs ranged from 11.4 MPa to 17.8 MPa and 154% to 184%, respectively. The tensile sets at break of the 4 5 biobased TPVs with a BPE content higher than 70% are smaller than 30%, indicating excellent 6 elastic recovery. The biobased TPVs showed no significant decrease in mechanical properties after reprocessing for up to three times. The changes of  $G^*$  and  $\eta^*$  in the low strain region after 7 8 reprocessing are readily recovered, suggesting that the BPE particles formed a strongly elastic 9 network in the low strain region. The cytotoxicity assay indicated that the biobased TPVs showed 10 no cytotoxicity to L929 cells. These biobased TPVs have proved to apply in both biomedical and 11 engineering fields.

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Page 20 of 37

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Scheme 2. Phase inversion of biobased TPVs with different degrees of crosslinking.





**Figure 2.** TEM micrographs of biobased TPVs (BPE/PLA,w/w, 70/30) with different DCP contents: (a) 0 phr; (b) 0.02 phr; (c) 0.06 phr; (d) 0.11 phr; (e) 0.22 phr.

2



2 **Figure 3.** TEM micrographs of biobased TPVs with different blending ratios of BPE/PLA: (a)

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60/40; (b) 70/30; (c) 80/20.

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3 180 °C: (a) Storage modulus (G'); (b) Loss modulus (G"); (c) Loss factor (tan  $\delta = G'/G''$ ); (d)

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4

Complex viscosity ( $\eta^*$ ).









2 Figure 7. Variations of tensile properties of biobased TPVs (BPE/PLA, 70/30) with number of

1

reprocessing.

2







Figure 9. RGR values of biobased TPVs at different incubation time.



**Figure 10.** Morphologies of L-929 cells after 3 days' incubation in the negative control and extract solutions of biobased TPVs: (a) 60/40; (b) 70/30; (c) 80/20; (d) the negative control.

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BPE/PLA			E	BPE				PLA		
	$T_g$	$T_{cc}$	$\Delta H_{cc}$	$T_m$	$\Delta H_m$	$T_g$	$T_{cc}$	$\Delta H_{cc}$	$T_m$	$\Delta H_m$
	(°C)	(°C)	(J/g)	(°C)	(J/g)	(°C)	(°C)	(J/g)	(°C)	(J/g)
0/100	-	-	-	-	-	60.0	133.0	2.1	155.1	2.4
60/40	-52.3	-20.3	4.8	-5.0	5.5	54.5	128.7	27.4	155.2	27.5
70/30	-51.5	-19.0	3.0	-4.8	4.2	54.6	113.9	26.1	155.9	27.5
80/20	-51.0	-15.7	3.0	-1.7	3.5	53.7	106.5	25.6	156.6	27.8
100/0	-54.1	-29.5	21.8	4.3	22.6	-	-	-	-	-

4 The values of  $\Delta H_{cc}$ ,  $\Delta H_m$  were normalized.

<b>BPE/PLA</b>	Tensile strength	Elongation at	Tensile set at	Shore A
	(MPa)	break (%)	break (%)	hardness (°)
0/100	54.0±3.8	7±1	-	-
60/40	17.8±1.4	184±15	92±4	97
70/30	11.4±0.4	154±8	30±2	94
80/20	7.4±0.7	120±8	12±2	86
100/0	0 8±0 1	253±7	0	56

			rur	nning.		
		First run	Second run	Third run	Fourth run	Fifth run
_	$G^{*a}$	195.5	164.3	157.3	148.7	137.1
	$\operatorname{G}^{*b}$	28.3	21.3	18.3	16.1	13.8
	$\eta^{*c}$	31108	26154	25029	23665	21818
	$\eta^{*d}$	4505	3397	2919	2563	2193

4 <sup>*a*</sup> Low strain complex modulus (modulus at 1%; kPa).

5 <sup>b</sup> High strain complex modulus (modulus at 470%; kPa).

6 <sup>c</sup> Low strain complex viscosity (viscosity at 1%; kPa).

<sup>7</sup> <sup>d</sup> High strain complex viscosity (viscosity at 470%; kPa).

8

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			e	( - ) -	iu cytotoxici	ty gra
		ma	terial.			
RGR (%)	≥100	75-99	50-74	25-49	1-24	(
Cytotoxicity grade	0	1	2	3	1	