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## ARTICLE

## Freestanding HRP–GOx redox buckypaper as oxygen-reducing biocathode for biofuel cell applications

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Horseradish peroxidase (HRP) was immobilized on redox buckypapers followed by electropolymerization of pyrrole-modified concanavalin A enabling the subsequent additional immobilization of the glycoprotein glucose oxidase (GOx). Biocatalytic buckypapers were formed using pyrene-modified 2,2'-Azino-bis(3-ethylbenzothiazoline-6-sulfonic acid) or Bis-Pyr-ABTS, a redox mediator, as a cross linker. ABTS-functionalized buckypaper enhances electron transfer of the bioelectrocatalytic reduction of hydrogen peroxide by HRP. Since H<sub>2</sub>O<sub>2</sub> is produced during glucose oxidation by GOx in the presence of oxygen, the bienzymatic GOx-HRP biocathode achieves the complete reduction of oxygen into water. Clearly improved performance of the biocathode was obtained by using an improved biocompatible immobilization strategy, enabling the prevention of enzyme loss while, ensuring both diffusion of glucose and O<sub>2</sub> and the local production of H<sub>2</sub>O<sub>2</sub>. These freestanding flexible oxygen-reducing biocathodes can operate in physiological conditions and show a high onset potentials at 0.60(± 0.01) V. In the presence of glucose (5 mM), such biocathodes exhibit a stable current density output of 1.1(± 0.1) mA cm<sup>-2</sup> at 0.1 V under continuous one-hour discharge. Furthermore, a marked increase in lifetime was observed, the biocathode displaying 64 % of its initial electrocatalytic activity after 15 days.

### Introduction:

Glucose biofuel cells are promising candidates for powering implantable biomedical devices by generating electricity out of body fluids<sup>1</sup>. Several studies have reported different examples of implanted biofuel cells operating in vivo in various animals such as insects<sup>2</sup>, snails<sup>3</sup>, clams<sup>4</sup>, lobsters<sup>5</sup>, rats<sup>6-10</sup> and rabbits<sup>11</sup>.

High-potential bioelectrocatalytic reduction of substrates such as oxygen or hydrogen peroxide by redox enzymes is an important challenge for the development of powerful biocathodes in enzymatic biofuel cell setups. Multicopper enzymes such as laccases<sup>12, 13</sup> or bilirubin oxidases<sup>14-16</sup> are generally used in biofuel cell design. However, they are known to not only lose activity in the presence of inhibitors such as chloride or urate ions, but they also do not demonstrate optimal

efficiency under physiological conditions, i.e. 5 mM glucose and 0.14 mM NaCl<sup>9, 17-19</sup>. Therefore, there is great interest to develop alternative biocathodes<sup>20</sup>. In particular the combination of GOx and HRP<sup>21</sup> has demonstrated the complete reduction of oxygen into water in the presence of glucose. This bienzymatic alternative is very interesting for the fabrication of biocathodes because these enzymes are both operational under physiological conditions and resistant towards inhibitors<sup>18</sup>. The process principle is based on the initial enzymatic reduction of oxygen to H<sub>2</sub>O<sub>2</sub> by GOx during glucose oxidation, while H<sub>2</sub>O<sub>2</sub> is then further electro-enzymatically reduced to water by adjacent HRP. The involved electrons are provided by the electrode and transferred to the HRP's heme center. This bienzymatic biocathode showed increased performance due to the synergy between the high

surface area of carbon nanotubes (CNT)-modified graphite electrode and the high turnover of these enzymes immobilized thereupon. Furthermore, this technique has to rely on the efficient wiring of HRP in order to ensure a high overpotential for the hydrogen peroxide reduction reaction.

However, the aforementioned electrode designs lack sufficient stability and their performance still lags behind existing multicopper enzyme biocathodes. A major challenge in the development of biofuel cells using such bienzymatic cathodes is to eliminate parasitic side reactions caused by  $\text{H}_2\text{O}_2$  which can reduce the performance of the said biocathode<sup>22</sup> or provoke unwanted toxicity issues<sup>23</sup>.

Recent strategies have been attempted to optimize the synergistic effect between these two enzymes in order to increase their performance in terms of current density and onset potential. Co-adsorption of GOx and HRP on double-walled carbon nanotube (DWCNT)-based electrodes<sup>23</sup> or their non-covalent immobilization on CNT using boronic acid<sup>18</sup> was attempted. To date, all bienzyme modified electrode studies were performed on systems where enzymes were directly wired to the electrode.

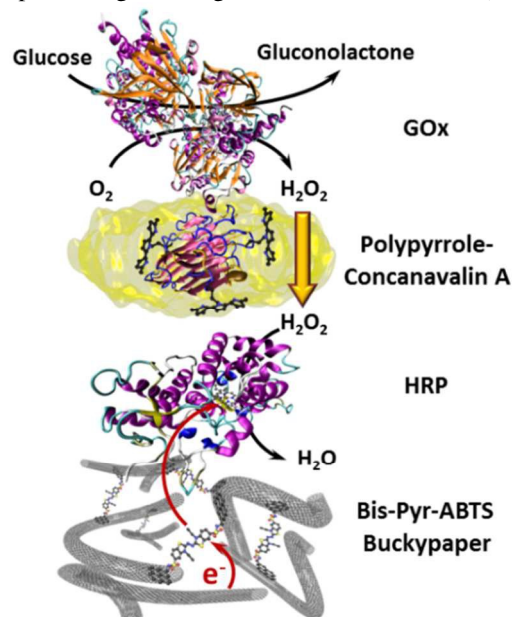
In fact, even though direct electron transfer can provide optimal output voltages, mediated electron transfer can drastically increase the energy conversion yields leading to clearly improved current densities<sup>24</sup>. Confining enzymes together with their corresponding redox mediator in a highly conducting, porous matrix could considerably enhance the electron transfer and optimize the mass transport of the related substrates. Furthermore, this problem remains one of the key issues in the development of biocathodes in terms of their operational ability under physiological conditions.

In this context, the main strategy herein, focused on the enzyme immobilization technique for the bienzymatic HRP-GOx system in order to maximize the current density and minimize overpotential via mediated electron transfer.

We have proposed to electrogenerate controlled films using pyrrole while combining them with the recognition properties of concanavalin A towards glycosylated proteins like GOx. The electropolymerization of pyrrole groups enables to form a conductive polymer at the surface of the electrode. Polypyrrole favors entrapment of biomolecules such as HRP, while concanavalin A provides an anchor for glycosylated biomolecule immobilization by bioaffinity interactions. Another key advantage of this design is that immobilizing a glycoenzyme through its carbohydrate moiety has no effect on its catalytic properties. The recognition site is generally located in areas that are not involved in enzymatic activity, and hence the enzymes can retain their activity even when their carbohydrate regions are functionalized.

A freestanding redox-buckypaper (BP), reinforced by a cross linking redox mediator pyrene-modified 2,2'-Azino-bis(3-ethylbenzothiazoline-6-sulfonic acid) (Bis-Pyr-ABTS)<sup>25</sup>, was used as the conductive platform for the immobilization of HRP and GOx. While ABTS enables the mediated electronic communication between HRP and the flexible BP. HRP is further immobilized by electro-polymerization of a pyrrole-

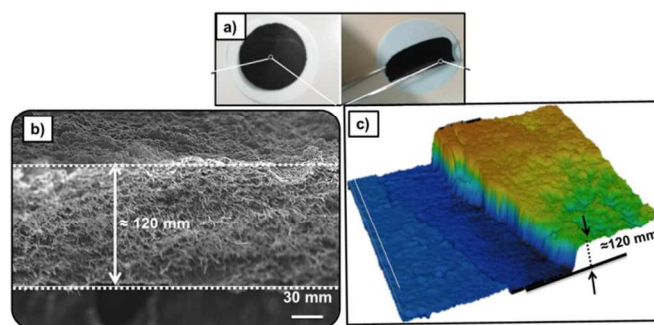
modified concanavalin A layer which then allows the biocompatible high loading immobilization of GOx (scheme 1).



Scheme 1: Sketch of the biocathode functioning based on bis-pyrrole-ABTS BP after adsorption of HRP and subsequent electropolymerization of pyrrole-concanavalin A for the immobilization of GOx.

## Results and discussions:

The morphology of the BPs was investigated by SEM and 3D confocal microscopy. Typical images are displayed in Figure 1. The BP cross section shows a porous structure with a specific volume equal to  $5 \text{ cm}^3 \text{ g}^{-1}$ . The fabricated BP shows thicknesses about  $120 \mu\text{m}$  for a BP weight of  $25 \text{ g m}^{-2}$ . Moreover, the BP electrodes exhibit excellent long-term mechanical stability in aqueous solution.



**Figure 1.** a) Photographs of a as formed BP on a membrane filter and bent with a tweezers. b) SEM image of Bis-Pyr-ABTS BP's cross section. c) Confocal image of Bis-Pyr-ABTS BP.

The electrochemical behavior of Bis-Pyr-ABTS BP/HRP based cathodes was investigated in presence of increasing concentration of  $\text{H}_2\text{O}_2$  to examine the catalytic  $\text{H}_2\text{O}_2$  reduction

via mediated electron transfer (MET) and to verify their chloride-tolerance in the presence of 140 mM NaCl.

The Bis-Pyr-ABTS BPs were incubated in a phosphate buffer saline solution (PBS) (0.1 mM) containing HRP (5 mg mL<sup>-1</sup>) and kept at 4 °C overnight to insure efficient adsorption thereof.

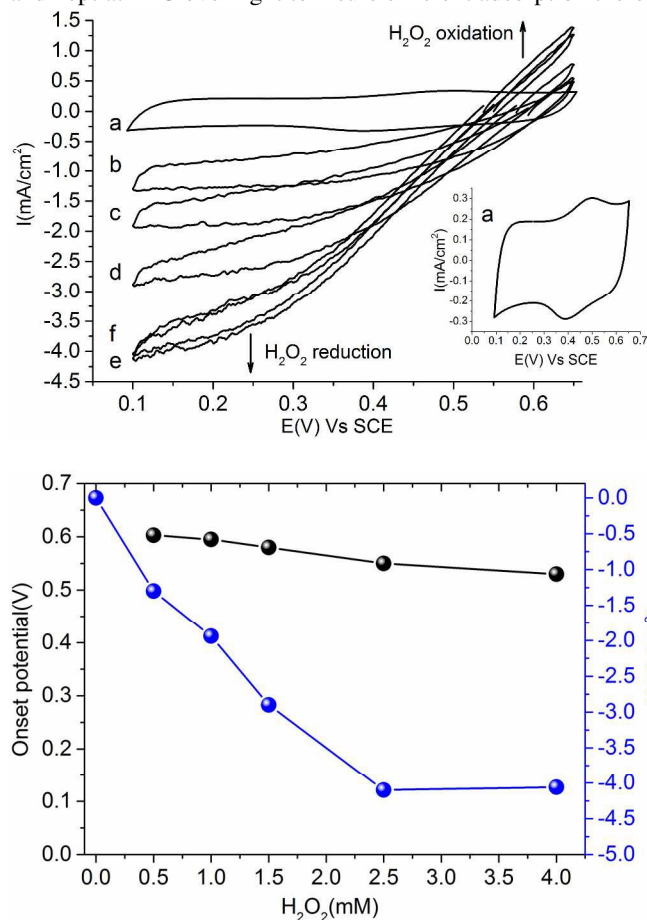


Figure 2. A) Electrode responses of Bis-Pyr-ABTS BP/HRP in the presence of (a) 0, (b) 0.50, (c) 1.0, (d), (e) 2.50 and (f) 4.0 mM H<sub>2</sub>O<sub>2</sub> and (inset) electrode responses of Bis-Pyr-ABTS BP/HRP in the presence of 0 mM H<sub>2</sub>O<sub>2</sub>. (Measurements were performed in 0.1 M PBS (pH 7.4) solution under a nitrogen atmosphere. Potentials are reported versus SCE. Scan rate: 2 mV.s<sup>-1</sup>. B) Plot of the onset potential (black axis) and evolution of the catalytic current (blue axis) recorded at the Bis-Pyr-ABTS BP/HRP electrodes towards H<sub>2</sub>O<sub>2</sub> concentration.

Figure 2A displays the cyclic voltammograms of these biocathodes in the presence and absence of H<sub>2</sub>O<sub>2</sub>. In absence of H<sub>2</sub>O<sub>2</sub>, the resulting cyclic voltammograms reveal a reversible peak system characteristic of the one-electron oxidation of ABTS at  $\Delta E_{1/2} = +0.46$  V vs. SCE (Fig. 2A inset). It clearly appears that the presence of H<sub>2</sub>O<sub>2</sub> induces the appearance of a cathodic current reflecting the H<sub>2</sub>O<sub>2</sub> reduction by MET. As expected, upon addition of increasing amounts of H<sub>2</sub>O<sub>2</sub>, the catalytic cathodic current increases continuously reaching a maximum current density of  $-4.1 (\pm 0.2)$  mA cm<sup>-2</sup> at 2.5 mM of H<sub>2</sub>O<sub>2</sub>. At H<sub>2</sub>O<sub>2</sub> concentration higher than 2.5 mM, we observed

the appearance of an oxidative current at a potential higher than 0.5 V. The latter is attributed to the direct oxidation of H<sub>2</sub>O<sub>2</sub> at the CNT electrode.

Figure 2B shows the current response of the Bis-Pyr-ABTS BP/HRP cathode as a function of H<sub>2</sub>O<sub>2</sub> concentration. The shape of the calibration curve with a linear part and a pseudo plateau at saturating substrate conditions indicates a typical enzymatic dependence.

The onset potential of  $0.6 (\pm 0.01)$  V for the reduction of H<sub>2</sub>O<sub>2</sub> with Bis-Pyr-ABTS BP/HRP is relatively stable and even more positive compared to oxygen reduction by high-potential BOD<sub>26</sub>,<sup>27</sup> and laccases<sup>28, 29</sup>. The observed high-potential H<sub>2</sub>O<sub>2</sub> reduction current density is slightly reduced at higher H<sub>2</sub>O<sub>2</sub> concentration, which is likely due to the concomitant H<sub>2</sub>O<sub>2</sub> oxidation at the CNT electrode surface.

As far as we know, this value of onset potential for the electrocatalytic reduction of H<sub>2</sub>O<sub>2</sub> is one of the highest, in comparison to those of other reported studies using HRP for H<sub>2</sub>O<sub>2</sub> reduction<sup>16, 27, 29</sup>. As can be seen in Figure 2B, the biocathode shows high onset potential values of  $0.60 (\pm 0.01)$  V vs. SCE. Table 1 summarizes the current density and onset potential of this work in comparison with the values described in other reports using HRP as biocathode catalyst.

Table 1: Comparison of the performance of HRP biocathodes for H<sub>2</sub>O<sub>2</sub> reduction via DET conditions with the presented Bis-Pyr-ABTS BP/HRP electrode

Ref.	conditions	Electron Transfer	Onset <sub>max</sub>	I <sub>max</sub> saturation
181818 181818 171615 141312 111098	0.1 M PBS at pH 7.4	DET	+0.43 V	196 $\mu$ A cm <sup>-2</sup> at 0.8 mM
23	0.1 M PBS at pH 7.4	DET	+0.38 V	120 $\mu$ A cm <sup>-2</sup> at 1 mM
22	67 mM PB at pH 7.0	DET	+0.47 V	800 $\mu$ A at 1 mM
30	0.1 M PB at pH 6.0	DET	+0.62 V	1.2 mA cm <sup>-2</sup> at 5 mM
This work	0.1 M PBS at pH 7.4	MET	+0.60 V	4.1 mA cm <sup>-2</sup> at 2.5 mM

The observed high efficiency of electrocatalytic reduction of the Bis-Pyr-ABTS BP/HRP cathodes compared to similar setups with DET is attributed to the presence of ABTS, which might enhance the electron transfer between the electrode surface and the active center of the redox enzyme. This effect may considerably minimize the parasitic oxidation of H<sub>2</sub>O<sub>2</sub> on the electrode, which is the major limitation of the use of this system.

A very important drawback in the use of enzymatic cathodes, such as those based on laccases as biocatalysts in biofuel cells, comes from their poor performance at neutral pH and the

inhibition effect of anions such as chloride. Hence, we investigated the catalytic performance of Bis-Pyr-ABTS BP/HRP for  $\text{H}_2\text{O}_2$  reduction under physiological conditions, namely in presence of chloride. After an initial stabilization of the catalytic cathodic current, the injection of NaCl (140 mM) after 700 s does not induce any inhibitory effect, the catalytic current remaining stable for 700 s (Figure 3). For comparison, Figure 3 shows an example of chrono-amperometric measurements under similar inhibiting conditions for a previously-reported Bis-Pyr-ABTS BP containing laccase<sup>25</sup>. In contrast to HRP based cathodes, this laccase cathode undergoes a rapid and partial decrease of the electrocatalytic current for oxygen reduction over time (a decrease of 22% after 8 min).

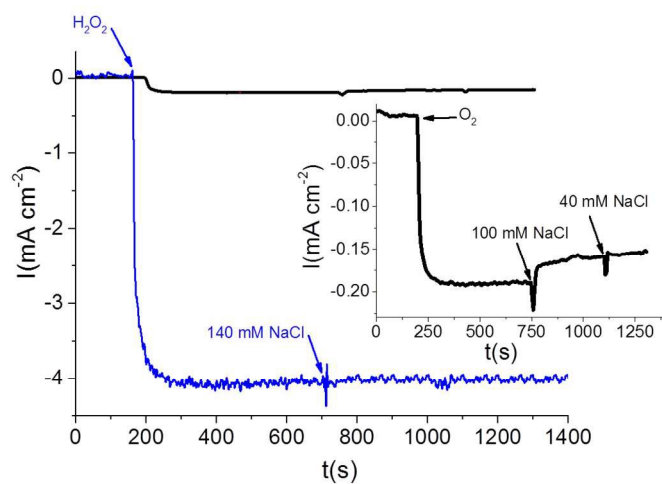


Figure 3. Evolution of the current density for reduction of  $\text{O}_2$  or  $\text{H}_2\text{O}_2$  at 0.1 V versus SCE recorded at (blue) Bis-Pyr-ABTS BP/HRP cathode and at (black and inset) a Bis-Pyr-ABTS BP/ Laccase cathode in 0.1 M PB (pH 7.4). Measurements were performed (blue) in PB with injection of  $\text{H}_2\text{O}_2$  (2.5 mM) after 170s then NaCl (140 mM) after 700 s or (black and inset) under a nitrogen atmosphere saturated with  $\text{O}_2$  after 200 s and with successive increments of NaCl concentration (100 and then 40 mM after 750 and 1120 s).

We engineered a bienzymatic biocathode for oxygen reduction via the catalytic cascade reactions using combined HRP and GOx catalysts. Multi-enzyme cascades have been widely used for biosensors or biofuel cells involving metabolons but are often faced with problems of combining different enzymatic activities or pH profiles<sup>31-33</sup>. In this bienzyme configuration, both enzymes present similar specific activities and optimum pH values. GOx catalyzes the oxidation of glucose to gluconic acid with the concomitant generation of  $\text{H}_2\text{O}_2$ . The biocatalytically-generated  $\text{H}_2\text{O}_2$  from the consumption of dissolved  $\text{O}_2$  then acts as the oxidizer for HRP. Electrons, which reduce  $\text{H}_2\text{O}_2$ , are transferred from the electrode surface to the HRP by ABTS. Our approach consists in the GOx immobilization on a Bis-Pyr-ABTS BP/HRP electrode previously modified by an electrogenerated polypyrrole concanavalin A film.

The possibility to form a polymeric proteinaceous film not only allows the entrapment of HRP but also acts as a binding bridge between BP and glycosylated enzymes like GOx.

The polypyrrole-Con A film was generated at Bis-Pyr-ABTS BP/HRP by controlled potential electrolysis ( $E_{\text{applied}} = +0.65$  V versus SCE,  $Q = 10$   $\text{mC cm}^{-2}$ ) in PBS. The resulting Bis-Pyr-ABTS BP/HRP Polypyrrole-Con A electrodes were washed with PBS and then incubated at room temperature in GOx solution (5 mg/mL in PB, pH 7.4) for 4h. Finally, unbound GOx was eliminated by washing with PB (0.1 M, pH 7.4).

In order to determine the capacity of such a bienzymatic system in its reduction of  $\text{O}_2$ , its response to glucose was studied. Figure 4A shows the cyclic voltammograms recorded at a Bis-Pyr-ABTS BP/HRP/Polypyrrole-Con A/GOx electrode in 0.1 M PBS (pH 7.4) containing various glucose concentrations under an air atmosphere. In the absence of glucose and presence of  $\text{O}_2$ , any catalytic current is observed at the Bis-Pyr-ABTS BP/HRP/Polypyrrole-Con A/GOx electrode. In contrast, in the presence of glucose and  $\text{O}_2$ , the biocathode exhibits a remarkable catalytic current peak with a current density of about  $-1.1 (\pm 0.1)$   $\text{mA cm}^{-2}$  at 0.1 V. The cyclic voltammograms exhibit an onset potential of  $+0.6 (\pm 0.01)$  V for the electrocatalytic  $\text{H}_2\text{O}_2$  reduction. The observed cathodic current density indicates the efficient conversion of the enzymatically generated  $\text{H}_2\text{O}_2$  to water, where the involved electrons are transferred from the electrode to HRP via ABTS. Such observations indicate that Bis-Pyr-ABTS BP/HRP/Polypyrrole-Con A/GOx possesses a high electrocatalytic activity toward  $\text{H}_2\text{O}_2$  reduction, and by consequence, towards  $\text{O}_2$  reduction.

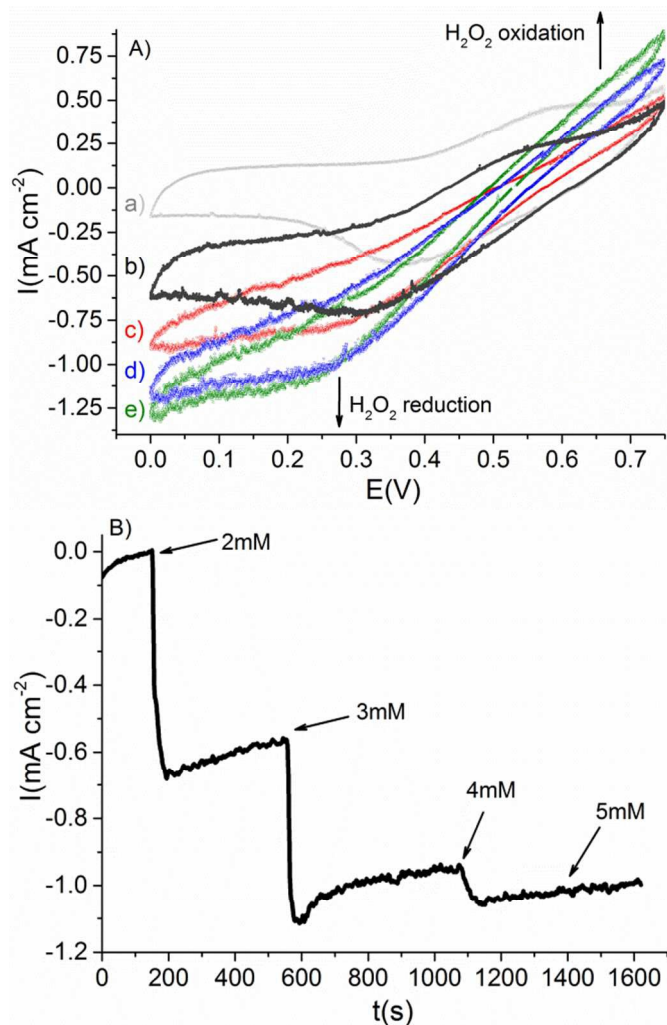


Figure 4. A) Cyclic voltammograms of Bis-Pyr-ABTS BP/HRP/Polypyrrole-Con A/GOx biocathodes in the absence (a) or presence of (b) 2, (c) 3, (d) 4 and (e) 5 mM glucose B) Evolution of the  $\text{H}_2\text{O}_2$  reduction current density upon addition of glucose recorded at this biocathode poised at 0.1 V versus SCE. Measurements were performed in 0.1 M PBS (pH 7.4) solution under an air atmosphere; scan rate:  $2 \text{ mV}\cdot\text{s}^{-1}$ .

Figure 4B shows the amperometric responses at 0.1 V after addition of defined amounts of glucose revealing an increase of the catalytic current for increased concentration of glucose from 1 to 5 mM and they then stabilize at higher concentrations. The catalytic current of the biocathode reaches saturation at 4–5 mM glucose concentration. This may be ascribed to a saturation of the peroxidase electroactivity. It should be noted that the saturation of PBS by oxygen purging does not increase the cathodic current intensity. As observed elsewhere<sup>18, 34</sup>, the resulting increase in  $\text{H}_2\text{O}_2$  production lead to localized high concentrations of hydrogen peroxide which induce an inhibition of HRP activity and/or lead to a direct electro-oxidation of  $\text{H}_2\text{O}_2$  at the BP electrode.

To evaluate the long-term stability of the biocathode, the current density for glucose (5 mM) was periodically recorded

by performing one-hour discharge at 0.1 V for 15 days. The biocathode still delivered  $0.7 (\pm 0.1) \text{ mA cm}^{-2}$  after 15 days (Figure 5), which represents 64 % of its initial electrocatalytic activity and constitutes the highest lifetime reported until now for a bienzymatic cathode using HRP.

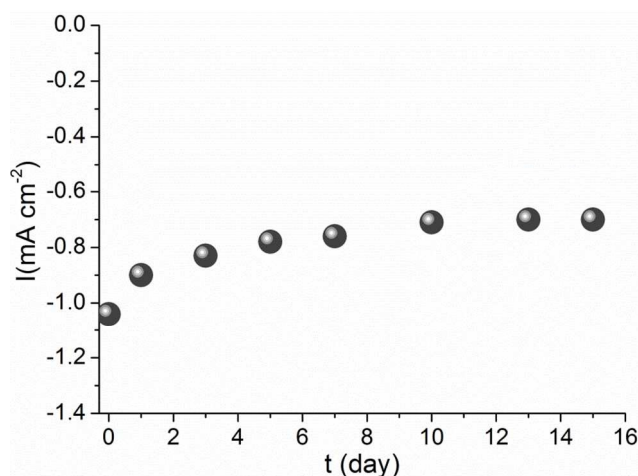


Figure 5: Long-term stability of the Bis-Pyr-ABTS-BP/HRP/Polypyrrole-Con A/GOx cathode. Measurements were performed in 0.1 M PBS (pH 7.4) solution under air atmosphere at 0.1 V vs SCE.

## Conclusions

These results demonstrate that these bienzymatic BP electrodes exhibit high current density for oxygen reduction with low overpotentials and excellent stability over weeks. This proof of concept demonstrates that redox BP/HRP/Polypyrrole-Con A/GOx can advantageously replace the conventional biocathodes based on multicopper enzymes that are employed in biofuel cells. Taking into account their possibility to operate under physiological conditions, it is expected that such bienzymatic cathodes will be useful for the development of implantable biofuel cells. The absence of inhibition by chlorides and neutral pH as well as the easy fabrication of mechanically stable enzyme buckypapers are encouraging for harvesting electrical energy from glucose and oxygen in the human body for powering implanted medical devices such as pacemakers.

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## Notes and references

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1. S. Cosnier, A. Le Goff and M. Holzinger, *Electrochem. Commun.*, 2014, **38**, 19–23.
2. M. Rasmussen, R. E. Ritzmann, I. Lee, A. J. Pollack and D. Scherson, *J. Am. Chem. Soc.*, 2012, **134**, 1458–1460.
3. L. Halámková, J. Halámek, V. Bocharova, A. Szczupak, L. Alfonta and E. Katz, *J. Am. Chem. Soc.*, 2012, **134**, 5040–5043.
4. A. Szczupak, J. Halámek, L. Halámková, V. Bocharova, L. Alfonta and E. Katz, *Energy Environ. Sci.*, 2012, **5**, 8891–8895.
5. K. MacVittie, J. Halamek, L. Halamkova, M. Southcott, W. D. Jamison, R. Lobel and E. Katz, *Energy Environ. Sci.*, 2013, **6**, 81–86.
6. P. Cinquin, C. Gondran, F. Giroud, S. Mazabrard, A. Pellissier, F. Boucher, J.-P. Alcaraz, K. Gorgy, F. Lenouvel, S. Mathé, P. Porcu and S. Cosnier, *PLoS ONE*, 2010, **5**, e10476.
7. F. C. P. F. Sales, R. M. Iost, M. V. A. Martins, M. C. Almeida and F. N. Crespilho, *Lab on a Chip*, 2013, **13**, 468–474.
8. H. Cheng, P. Yu, X. Lu, Y. Lin, T. Ohsaka and L. Mao, *Analyst*, 2013, **138**, 179–185.
9. A. Zebda, S. Cosnier, J.-P. Alcaraz, M. Holzinger, A. Le Goff, C. Gondran, F. Boucher, F. Giroud, K. Gorgy, H. Lamraoui and P. Cinquin, *Sci. Rep.*, 2013, **3**, 1516.
10. J. A. Castorena-Gonzalez, C. Foote, K. MacVittie, J. Halámek, L. Halámková, L. A. Martinez-Lemus and E. Katz, *Electroanalysis*, 2013, **25**, 1579–1584.
11. T. Miyake, K. Haneda, N. Nagai, Y. Yatagawa, H. Onami, S. Yoshino, T. Abe and M. Nishizawa, *Energy & Environmental Science*, 2011, **4**, 5008–5012.
12. S. Shleev, A. Jarosz-Wilkolazka, A. Khalunina, O. Morozova, A. Yaropolov, T. Ruzgas and L. Gorton, *Bioelectrochemistry*, 2005, **67**, 115–124.
13. A. Zebda, C. Gondran, A. Le Goff, M. Holzinger, P. Cinquin and S. Cosnier, *Nature Communications*, 2011, **2**, 370.
14. N. Mano, H.-H. Kim and A. Heller, *The Journal of Physical Chemistry B*, 2002, **106**, 8842–8848.
15. N. Mano and A. Heller, *J. Electrochem. Soc.*, 2003, **150**, A1136–A1138.
16. N. Mano, J. L. Fernandez, Y. Kim, W. Shin, A. J. Bard and A. Heller, *J. Am. Chem. Soc.*, 2003, **125**, 15290–15291.
17. S. C. Barton, M. Pickard, R. Vazquez-Duhalt and A. Heller, *Biosens. Bioelectron.*, 2002, **17**, 1071–1074.
18. B. Reuillard, A. Le Goff, M. Holzinger and S. Cosnier, *Journal of Materials Chemistry B*, 2014, **2**, 2228–2232.
19. E. Katz and K. MacVittie, *Energy & Environmental Science*, 2013, **6**, 2791–2803.
20. R. A. S. Luz, A. R. Pereira, J. C. P. de Souza, F. C. P. F. Sales and F. N. Crespilho, *ChemElectroChem*, 2014, **1**, 1751–1777.
21. W. Jia, C. Jin, W. Xia, M. Muhler, W. Schuhmann and L. Stoica, *Chem. Eur. J.*, 2012, **18**, 2783–2786.
22. W. Jia, S. Schwaborn, C. Jin, W. Xia, M. Muhler, W. Schuhmann and L. Stoica, *Phys. Chem. Chem. Phys.*, 2010, **12**, 10088–10092.
23. C. Agnès, B. Reuillard, A. Le Goff, M. Holzinger and S. Cosnier, *Electrochem. Commun.*, 2013, **34**, 105–108.
24. B. Reuillard, A. Le Goff, C. Agnès, M. Holzinger, A. Zebda, C. Gondran, K. Elouarzaki and S. Cosnier, *Phys. Chem. Chem. Phys.*, 2013, **15**, 4892–4896.
25. M. Bourourou, K. Elouarzaki, M. Holzinger, C. Agnes, A. Le Goff, N. Reverdy-Bruas, D. Chaussy, M. Party, A. Maaref and S. Cosnier, *Chemical Science*, 2014, **5**, 2885–2888.
26. N. Mano and L. Edembe, *Biosens. Bioelectron.*, 2013, **50**, 478–485.
27. L. Hussein, G. Urban and M. Kruger, *Phys. Chem. Chem. Phys.*, 2011, **13**, 5831–5839.
28. A. Le Goff, M. Holzinger and S. Cosnier, *Cell. Mol. Life Sci.*, 2015, **72**, 941–952.
29. L. Hussein, S. Rubenwolf, F. von Stetten, G. Urban, R. Zengerle, M. Krueger and S. Kerzenmacher, *Biosens. Bioelectron.*, 2011, **26**, 4133–4138.
30. M. Varničić, K. Bettenbrock, D. Hermsdorf, T. Vidaković-Koch and K. Sundmacher, *RSC Advances*, 2014, **4**, 36471–36479.
31. D. Sokic-Lazic and S. D. Minteer, *Electrochem. Solid-State Lett.*, 2009, **12**, F26–F28.
32. D. Sokic-Lazic and S. D. Minteer, *Biosens. Bioelectron.*, 2008, **24**, 939–944.
33. C. Mousty, S. Cosnier, D. Shan and S. Mu, *Anal. Chim. Acta*, 2001, **443**, 1–8.
34. B. Limoges, J.-M. Savéant and D. Yazidi, *J. Am. Chem. Soc.*, 2003, **125**, 9192–9203.

Horseradish peroxidase and glucose oxidase were immobilized on redox buckypapers modified by poly(pyrrole-concanavalin) for the electroreduction of oxygen into water

