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1 ***β*-cyclodextrin/chitosan-magnetic graphene oxide-surface**
2 **molecularly imprinted polymer nanocomplex coupled with**
3 **chemiluminescence biosensing bovine serum albumin**

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8 **Abstract**

9 In this report, a sensitive and selective chemiluminescence (CL) biosensor for
10 bovine serum albumin (BSA) coupled with surface molecularly imprinted polymer
11 nanocomplex using *β*-cyclodextrin/chitosan-magnetic graphene oxide as backbone
12 material (*β*-CD/Cs-MGO-SMIP) was promoted. Then, the material *β*-CD/Cs-MGO in
13 which *β*-cyclodextrin, chitosan and graphene oxide was used to provide
14 multi-imprinting sites and large surface area was characterized by SEM, XRD and
15 FTIR, and then it was found that *β*-CD/Cs-MGO-SMIP followed Langmuir isotherm
16 equation and pseudo-second order sorption kinetics when binding the template. It
17 demonstrated fast mass transfer, promoted rate of removal of the biomacromolecule
18 and excellent recognition and adsorption ability for the imprinting cavities situated at
19 the surface of the *β*-CD/Cs-MGO, which enabled easy access to BSA. Subsequently, a
20 high sensitive CL biosensor to BSA based on the strong recognition effect between
21 *β*-CD/Cs-MGO-SMIP and BSA which decided the high selectivity has been proposed
22 and the proposed biosensor could be assay in the range of 5.0×10^{-7} - 1.0×10^{-4}

23 mg/mL with a detection limit of 1.1×10^{-7} mg/mL. The obtained recoveries were
24 between 94% and 106% when determining samples.

25 **Keywords:** chemiluminescence biosensor; bovine serum albumin; magnetic graphene oxide;
26 β -cyclodextrin; chitosan; surface molecularly imprinted polymer

27 **1 Introduction**

28 Bovine serum albumin (BSA), implicated to be a potential autoimmune trigger of
29 insulin-dependent diabetes mellitus (IDDM) though the causal association remained a
30 controversial topic [1], was a component of the whey protein system in cows' milk,
31 bovine milk or milk-based paediatric formula during infancy [2]. The level of BSA in
32 bovine milk has been used as a marker of the health of the mammary gland and of
33 milk quality [3]. Analytical approaches for the determination of bovine serum albumin
34 were proposed to be chemometrics [2], optical biosensor [3] and so on. A cheap,
35 convenient and sensitive chemiluminescence (CL) [4] biosensor for selective
36 determination of BSA was intentionally developed, but specific molecular recognition
37 ability was required. Thus, novel receptor-like techniques for biological recognition
38 were emerged rapidly to specificity recognize BSA.

39 For this purpose, surface molecular imprinting technique was considered as a
40 promising way to design a synthetic receptor in which the space structure of
41 mimicking biomolecules was recorded and the specific recognition was achieved
42 definitely [5]. Certainly, the synthesis of surface molecular imprinting supporting
43 materials that could improve the selectivity and adsorbing capacity to target
44 biomacromolecule was particularly important [6].

45 Recently, chitosan (Cs) has attracted considerable attention [7] as one of the most
46 promising materials due to its biodegradability, biocompatibility and non-toxicity [8].
47 With a natural mucopolysaccharide with similar structural characteristics to cellulose,
48 Cs has been applied in preparation of molecularly imprinted resin [9],
49 integrated-optical sensors [10] and porous membrane [11]. On account of the
50 abundant hydroxyl and amino group, when preparing surface molecular imprinting
51 polymer (SMIP), Cs was full of the advantages of multiple imprinting sites which
52 would accelerate the imprinting process, improve the selectivity and adsorbing
53 capacity [12].

54 β -cyclodextrin (β -CD), with a lipophilic inner cavity with hydrophilic outer
55 surfaces which was able to interact with a large variety of guest molecules forming
56 non-covalent inclusion complexes [13], had already demonstrated its potential in
57 separation and analytical application since it could bind angstrom-sized guests
58 through apolar interaction in protic media [14]. As a supramolecular host compound,
59 β -CD was willing to be chosen as functional monomer to prepare MIP to achieve high
60 selectivity and great adsorption capacity [15].

61 In current century, as a fascinating new carbon materials with honeycomb and
62 one-atom-thick structure, graphene oxide (GO) has attracted worldwide attention
63 [16]. Due to its large specific surface area, good biocompatibility and chemical
64 stability, GO was used as supporting material to prepare SMIP [17]. Moreover, for the
65 abundant of hydroxyl and carboxyl, integration of GO with other materials, such as
66 organic functional material, was always highly desirable [18-19]. In this case, a

67 method to improve the properties of GO was that coprecipitating Fe_3O_4 nanoparticles
68 onto GO sheets surface to obtain magnetic graphene oxide (MGO) which possessed
69 the merits of GO of high adsorption capacity and Fe_3O_4 nanoparticles of easy
70 separation [20-21].

71 In particular, the combination of β -CD, Cs and MGO (β -CD/Cs-MGO) serving
72 as supporting material in the preparing process of SMIP made the recognition of
73 nanocomplex (β -CD/Cs-MGO- SMIP) to BSA selectively and efficiently for its
74 exhaustless binding sites. Accordingly, fast mass transfer, promoted rate of removal of
75 the biomolecule and excellent recognition and adsorption ability for the imprinting
76 cavities in the proximity of the surface of the β -CD/Cs-MGO was achieved, which
77 enabled easy access to BSA. When the synthesized β -CD/Cs-MGO-SMIP, as potential
78 optical receptor, was introduced in CL analytical method for the detection of
79 biomacromolecular BSA, nice analytical performance characteristics such as
80 selectivity and sensitivity were obtained. Finally, the proposed
81 β -CD/Cs-MGO-SMIP-CL biosensor was applied to detect BSA in samples.

82 **2 Experiment**

83 **2.1 Materials**

84 BSA (96%), N-N methylene double acrylamide (MBA, A.R),
85 N,N,N',N'-tetramethyl ethylenediamine (TEMED, A.R) and Diethyl amino ethyl
86 methacrylate (DMAEMA, 99%) were purchased from Aladdin Industrial Co. (China);
87 β -CD, Cs, Ferrous sulfate(A.R) and Ammonium persulphate (APS, AR) were
88 supplied by Sinopharm Chemical Reagent Co. Ltd (China); The ethanol, acetic acid,
89 luminol and all the other chemicals unless specified were of analytical reagent grade

90 and used without further purification.

91 Redistilled water was used throughout the work. Phosphate buffer (PBS,
92 pH=7.4, 0.01 mol/L) solution was used to prepare all BSA solutions which were
93 stored in refrigerator (4°C).

94 **2.3 Apparatus**

95 The IFFM-E flow injection CL analyser (Xi'an Remex Electronic instrument
96 High-Tech Ltd., China) was equipped with an automatic injection system and a
97 detection system. PTFE tubes (0.8 mm i.d.) were used to connect all of the
98 components in the flow system. 50 mg β -CD/Cs-MGO-SMIP and non-imprinted
99 polymer (β -CD/Cs-MGO-SNIP) was filled in capillary, and was collected between
100 pump and CL analyser with PTFE tubes as recognition elements. A magnet was
101 placed by the side to fix the β -CD/Cs-MGO-SMIP (β -CD/Cs-MGO-SNIP) on the
102 capillary to preventing its run off with solutions. When BSA solution ran through the
103 capillary, BSA molecule could be absorbed by β -CD/Cs-MGO-SMIP selectivity, a CL
104 signal I_1 was obtained, while β -CD/Cs-MGO-SNIP could not absorb BSA molecule,
105 another CL signal I_2 was obtained. Then the difference $\Delta I = I_2 - I_1$ was the
106 concentration of BSA in the linear relationship. In this way, the specific recognition
107 and measuring system was obtained. XRD measurement was made on a D8 focus
108 spectrometer (Brooke AXS, Germany). A FEI QUANTA FEG250 field emission
109 scanning electron microscopy (SEM, USA) was employed to observe the morphology
110 of the nanoparticles. A vibrating-sample magnetometer (VSM) (MAG-3110, Freescale)
111 was used at 300 K to characterize the magnetic properties of β -CD/Cs-MGO-SMIP.

112 **2.3 Preparation of MGO**

113 MGO was prepared by modified Hummers method [22] and our group. Firstly,
114 120 mL of H₂SO₄ was added into 5.0 g nature graphite powder and 2.5 g of NaNO₃
115 subsequently. Then, 6.0 g of KMnO₄ was added gradually under stirring and the

116 diluted suspension was stirred at 98°C. Subsequently, 50 mL of 30% H₂O₂ was
117 added drop by drop. Finally, the mixture was filtered and washed till the pH = 7.0.
118 MGO was synthesized according to a modified procedure described in our group
119 [23]. While suspending 0.5 g GO in 200 mL of solution containing 5.1 g
120 (NH₄)₂Fe(SO₄)₂·6H₂O and 7.5 g NH₄Fe(SO₄)₂·12H₂O under N₂ atmosphere, the
121 solution was sonicated. Then, 10 mL of 8 mol/L NH₄OH aqueous solutions was
122 added drop wise to precipitate the iron oxides till the pH = 11.5. The reaction was
123 maintained at 80°C for 30 min. The obtained black precipitation was separated,
124 washed and then dried under vacuum at 60°C.

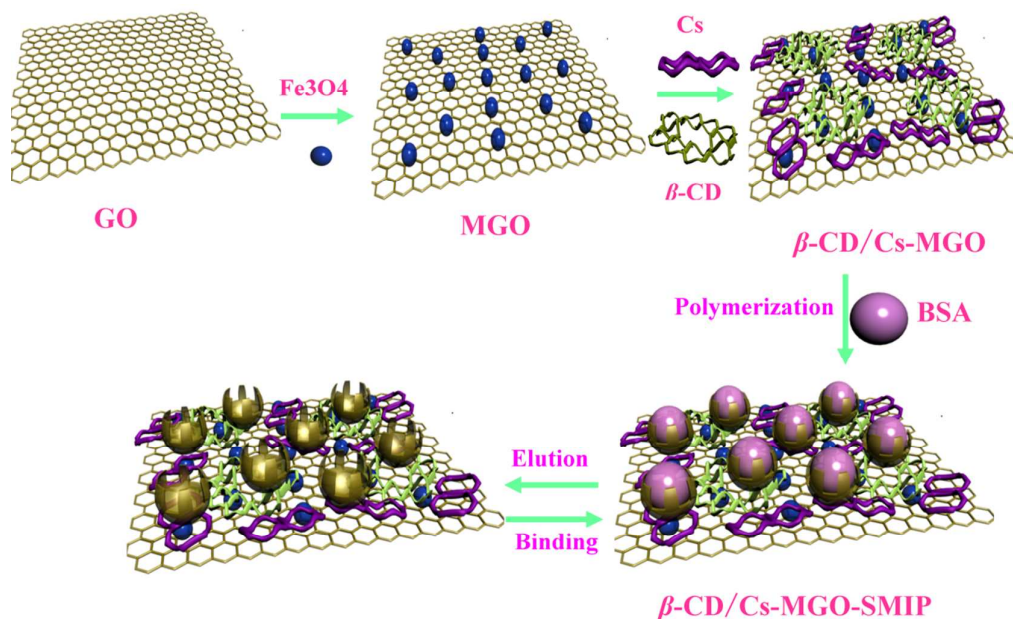
125 **2.4 Preparation of β -CD/Cs-MGO**

126 In a typical procedure, 0.1 g newly obtained MGO was added to the molten Cs
127 colloidal acetic acid solution and the pH of the solution was adjusted to be 5.5. Then,
128 80 mg β -CD was added to the mixture with vigorous stirring. After that, 3 mL
129 glutaraldehyde was added. The reaction was carried out at 70°C for 60 min under
130 constant mechanical stirring. The precipitate was isolated in the magnetic field and
131 washed with double-distilled water. The obtained composites β -CD/Cs-MGO was
132 then dried under vacuum.

133 **2.5 Preparation of β -CD/Cs-MGO-SMIP**

134 A modified procedure described in our work and previous literature was used to
135 synthesize β -CD/Cs-MGO-SMIP [23]. The preparing process was shown in Fig. 1.
136 MBA (64 mg) were dissolved in 35 mL PBS solution by ultrasonication.
137 Subsequently, 32 mg of BSA was dissolved to the solution. Then, 15 mL of
138 β -CD/Cs-MGO (150 mg) dispersed in 10 mL ethanol and 5 mL PBS solution by
139 ultrasonication was added into above solution. The mixture was degassed for 10 min
140 and purged with nitrogen stream for 10 min. Then, the solution was shaken for 0.5 h

141 to preassemble. By adding 30 mg of APS and 0.2 mL TEMED to the mixture,
 142 polymerization was initiated and continued under shaking at 25°C for 10 min. The
 143 particles were collected by magnetic separation and washed with NaCl solution until
 144 no BSA in the supernatant. Finally, they were washed with PBS solution and dried.
 145 The β -CD/Cs-MGO-SNIP was in exactly the same, yet without addition of BSA.



146

147

Fig. 1 The preparing process of β -CD/Cs-MGO-SMIP

148 2.6 Adsorbing properties of β -CD/Cs-MGO-SMIP and β -CD/Cs-MGO-SNIP

149 Adsorption isotherm: 100 mg β -CD/Cs-MGO-SMIP and β -CD/Cs-MGO-SNIP
 150 nanoparticles were placed into 10 mL centrifuge tubes respectively. Then, 8.0 mL of
 151 different concentration solution of BSA was added into the tube and shaken at 25°C
 152 for 1 h. After magnetic separation, the concentration of the supernatant in the tube was
 153 determined by CL instrument and the adsorbing capacities were calculated.

154 Rebinding dynamics: 100 mg β -CD/Cs-MGO-SMIP and β -CD/Cs-MGO-SNIP
 155 nanoparticles were dispersed in 8.0 mL 2.0 mg/mL BSA solution. Immediately, the
 156 solution was shaken at 25°C for 2.5 min, 5 min, 7.5 min, 10 min, 20 min, 40 min and
 157 60 min respectively. After magnetic separation, the concentration of the supernatant in

158 the tube was determined by CL instrument and the adsorbing capacities were
159 calculated. The adsorbing capacity was calculated from the following formula:

$$Q_e = (c_0 - c_e)V/m$$

160 Where Q_e (mg/g) was the mass of protein adsorbed by unit mass of dry particles,
161 c_0 (mg/mL) and c_e (mg/mL) were the concentrations of the initial and balance solution,
162 respectively, V (mL) was the total volume of the adsorption mixture, and m (g) was
163 the mass of the β -CD/Cs-MGO-SMIP (β -CD/Cs-MGO-SMIP) added.

164 2.7 Selectivity studies of β -CD/Cs-MGO-SMIP and β -CD/Cs-MGO-SNIP

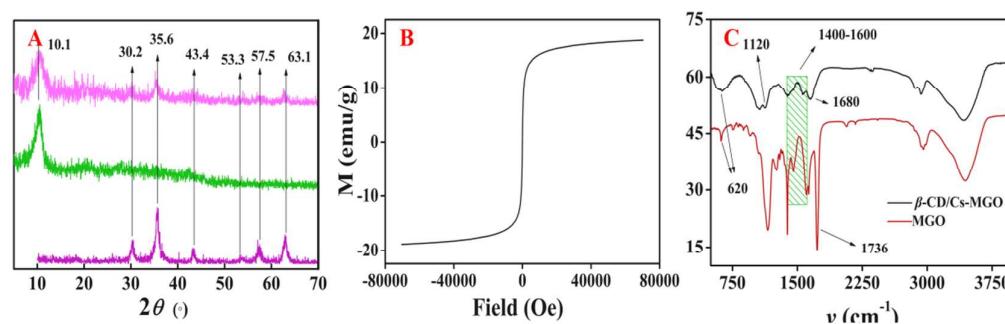
165 100 mg β -CD/Cs-MGO-SMIP and β -CD/Cs-MGO-SNIP nanoparticles were
166 placed into 10 mL centrifuge tubes respectively. Then, 8.0 mL 2.0 mg/mL BSA
167 solution, Bovine hemoglobin (Bhb) solution, Lysozyme (Lys) solution, Cytochrome
168 C (CyC) solution and Ribonuclease A (RNase A) solution were added into the tube
169 respectively. The solution was shaken at 25°C for 30 min. After magnetic separation,
170 the concentration of the supernatant in the tube was determined and the adsorbing
171 capacity of β -CD/Cs-MGO-SMIP and β -CD/Cs-MGO-SNIP nanoparticles to BSA,
172 Bhb, Lys, CyC and RNase A were determined.

173 3 Results and discussion

174 3.1 Characterization of GO, MGO and β -CD/Cs-MGO

175 Fig. 2 (A) illustrated the XRD patterns of obtained GO and MGO particles.
176 Obviously, MGO displayed several diffraction rings at $2\theta = 30.2^\circ$, 35.6° , 43.4° , 53.3° ,
177 57.5° and 63.1° which were corresponded to (220), (311), (400), (422), (511), and
178 (440) the six indices of the Fe_3O_4 inverse spinel structure and the characteristic peak
179 of GO at $2\theta = 10.1^\circ$. The satisfying result provided a remarkable support that MGO
180 was successful prepared. As indicated in Fig. 2 B, the magnetization measurement
181 performed that the saturation magnetization of β -CD/Cs-MGO-SMIP was 18.9 emu/g,

182 which was sufficient to meet the need of magnetic separation process. Fig. 2 C
 183 showed the Fourier Transform Infrared Spectroscopy (FTIR) of MGO and
 184 β -CD/Cs-MGO. The peaks at 1400-1600 cm^{-1} were the characteristic peaks of
 185 benzene ring. In the spectrum of MGO, the peak at 620 cm^{-1} was the characteristics of
 186 Fe_3O_4 nanoparticles. The strong intensity and shape absorption band at 1736 cm^{-1} was
 187 attributed to the stretching vibration of C=O band. In the spectrum of β -CD/Cs-MGO,
 188 the board and moderate intensity peak at 620 cm^{-1} contain the characteristic peak of
 189 Fe_3O_4 nanoparticles and the flexural vibration of N-H in acid amide. The peak at 1126
 190 cm^{-1} was on account of the stretching vibration of C-N. When reacted with $-\text{NH}_2$, the
 191 peak of C=O at 1736 cm^{-1} shifted to 1680 cm^{-1} which confirmed the reaction of MGO
 192 and β -CD/Cs.

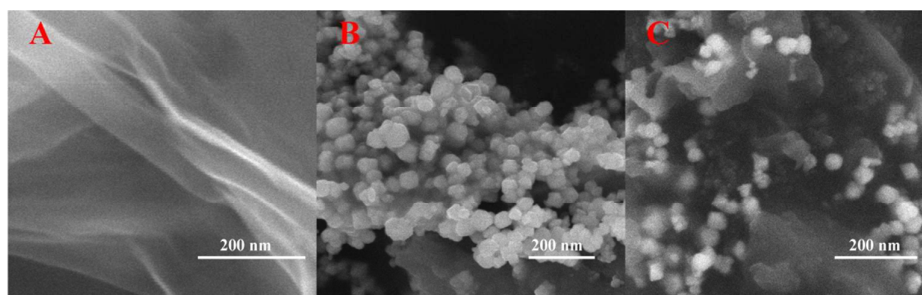


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194 **Fig. 2** XRD patterns of obtained GO and MGO (A), VSM magnetization curves of
 195 β -CD/Cs-MGO-SMIP (B) and FTIR of MGO and β -CD/Cs-MGO (C)

196 Scanning Electron Microscope (SEM) was used to characterize the surface
 197 morphology of the GO, MGO and β -CD/Cs-MGO. As shown in Fig. 3 A, a wrinkle
 198 and thin film was observed in the image of GO. A loose 3D network structure
 199 consisting of 2D GO sheets was displayed clearly. Fig. 3 B clearly revealed that Fe_3O_4
 200 nanoparticles were decorated on the GO surface which did not alter the microstructure
 201 of GO significantly and the incorporation of Fe_3O_4 on GO sheets enabled the
 202 maximum utilization of GO. Obviously, a large amount of Fe_3O_4 nanoparticles were

203 immobilized onto the GO films. As shown in Fig. 3 C, the obvious difference on the
204 surface of β -CD/Cs-MGO compared with MGO indicated interaction between GO
205 and β -CD, Cs. A higher surface area which was served as supporting interface to get
206 more binding sites in SMIP was obtained after the immobilization of β -CD and Cs
207 onto the MGO.



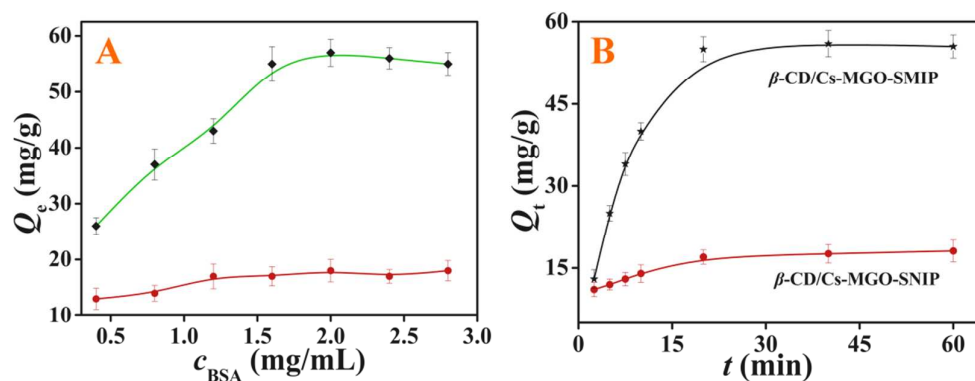
208

209 **Fig. 3** The surface morphology of GO (A), MGO (B) and β -CD/Cs-MGO (C) in SEM images

210 3.2 Batch binding properties of β -CD/Cs-MGO-SMIP

211 The adsorption results were shown in Fig. 4. The adsorption isotherm (Fig 4 A)
212 to BSA increased with the increasing of the BSA concentration before reaching
213 maximum 58 mg/g ($Q_m = 58$ mg/g). Obviously, β -CD/Cs-MGO-SMIP exhibited a
214 significant imprinting effect binding more than thrice as much BSA compared to its
215 SNIP which was prepared at the same conditions. As we could observe in Fig. 4 (B),
216 both the SMIP and SNIP particles could reach the maximum adsorption within 20 min
217 for the imprinting cavities on the surface or in the proximity of the surface of
218 β -CD/Cs-MGO-SMIP.

219



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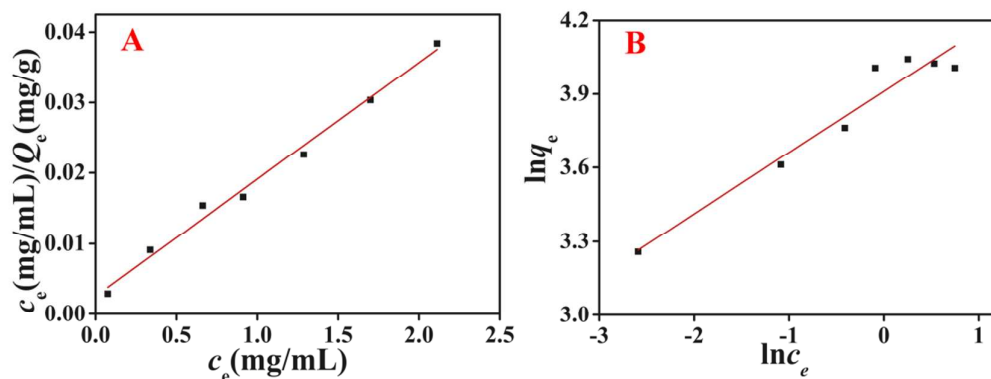
221 **Fig. 4** Binding properties of β -CD/Cs-MGO-SMIP: adsorbing capacity (A) and adsorbing time (B)222 3.2.1 Adsorption isotherms equation of β -CD/Cs-MGO-SMIP

223 Adsorption isotherms equation of β -CD/Cs-MGO-SMIP to BSA was described
 224 by Langmuir isotherm equation and Freundlich isotherm equation showed in Fig. 5 A
 225 B respectively. The Langmuir and Freundlich equations which were used for
 226 modeling adsorption isotherms were expressed in following formulas were.

227 Langmuir equations: $\frac{c_e}{Q_e} = \frac{c_e}{Q_{tm}} + \frac{1}{Q_{tm}k_L}$ Freundlich equation: $\ln Q_e = \ln k_F + \frac{\ln c_e}{n}$

228 Where c_e (mg/mL) is the equilibrium concentration of BSA, Q_e (mg/g) is the
 229 adsorption capacity, Q_{tm} (mg/g) is the theoretical saturation adsorption capacity, k_L
 230 the Langmuir constant, k_F is the binding energy constant and n is the Freundlich
 231 constant.

232 As shown in Fig. 5, the fit of a Langmuir model provided a substantially higher
 233 correlation coefficient. Accordingly, Langmuir isotherm equations ($R^2 = 0.9879$) were
 234 more appropriate than the Freundlich isotherm equations ($R^2 = 0.9302$) at present
 235 temperature. Therefore, the adsorption of β -CD/Cs-MGO-SMIP to BSA was
 236 monolayer uniform adsorption and the imprinting sites on the surface of
 237 β -CD/Cs-MGO-SMIP were homogeneous distribution. Theory adsorption capacity
 238 (Q_{tm}) of β -CD/Cs-MGO-SMIP was obtained to be 60 mg/g which was approximate to
 239 the experimental result 58 mg/g.



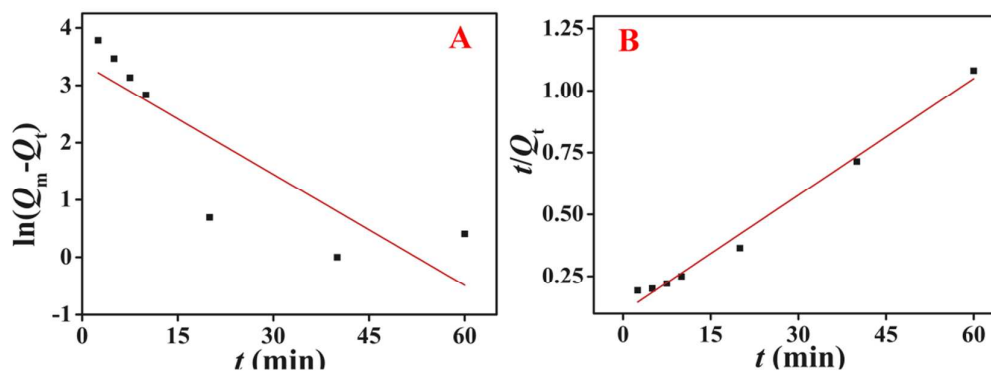
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241 **Fig. 5** Adsorption isotherms equation of β -CD/Cs-MGO-SMIP to BSA: Langmuir model (A) and

242 Freundlich model (B)

243 3.2.2 Adsorption kinetics of β -CD/Cs-MGO-SMIP

244 In Fig. 6, two adsorption kinetics equations (i.e., Pseudo-first order (A) and
 245 pseudo-second order (B)) were applied to model the kinetics of BSA adsorption at
 246 β -CD/Cs-MGO-SMIP particles, providing more detailed insight on the adsorption
 247 processes. A better correlation was observed in the pseudo-second order model ($R^2 =$
 248 0.9874). It was confirmed that the obtained β -CD/Cs-MGO-SMIP follow
 249 pseudo-second order sorption kinetics when binding BSA. Theory adsorption capacity
 250 (Q_{tm}) of β -CD/Cs-MGO-SMIP was obtained to be 63 mg/g which was also
 251 approximate to the experimental result 58 mg/g.



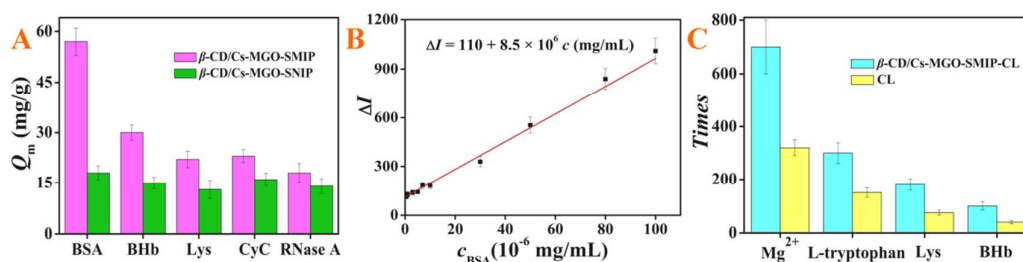
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253 **Fig. 6** Adsorption kinetics of β -CD/Cs-MGO-SMIP to BSA: Pseudo-first order (A) and

254 pseudo-second order (B)

255 3.3 Batch binding properties of β -CD/Cs-MGO-SMIP

256 Fig. 7 A showed the adsorption capacities of β -CD/Cs-MGO-SMIP and
 257 β -CD/Cs-MGO-SMIP nanoparticles to BSA, BHb, Lys, CyC and RNase A in PBS
 258 solutions with a feed concentration of 0.4 mg/mL. Evidently, all SMIP exhibited more
 259 binding capacity compared to its NIP for the macro imprinting caves which would
 260 absorb biomacromolecule more or less while no imprinting caves existed in SNIP.
 261 Certainly from the figure, BSA- β -CD/Cs-MGO-SMIP binded much more BSA
 262 compared to the other four proteins, which was of significant interest in terms of their
 263 selectivity.



264

265 **Fig. 7** Binding amounts of different proteins on the imprinted particles (A); The regression
 266 equation of the β -CD/Cs-MGO-SMIP-CL biosensor (B); Interferences study of the
 267 β -CD/Cs-MGO-SMIP-CL biosensor (C)

268 3.4 Analytical performance of β -CD/Cs-MGO-SMIP-CL biosensor

269 BSA could enhance the CL intensity of luminol in the presence of H_2O_2 and
 270 NaOH. In order to establish the optimum experiment conditions, the parameters
 271 affecting the performance of CL were then studied. Firstly, the effect of NaOH on the
 272 CL intensity was investigated and the optimal concentration of NaOH was fixed at 4.0
 273 $\times 10^{-5}$ mol/L. Subsequently, the effect of H_2O_2 on the CL intensity was studied and
 274 approached maximum intensity value was obtained 1.2×10^{-2} mol/L. Then, the
 275 concentration of luminol was employed to be 5.0×10^{-3} mol/L in subsequent
 276 experiments. Thus, under above conditions, the calibration curve of CL intensity
 277 against BSA concentration was invested to be linear in the range of 5.0×10^{-7} - $1.0 \times$

278 10^{-4} mg/mL, and the correlation coefficient was 0.9877 with a detection limit of $1.1 \times$
 279 10^{-7} mg/mL shown in Fig. 7 (B). As shown in Tab. 1, the result showed that our work
 280 was superior in both linear range and detection limit compared with other methods.

281 **Tab.1.** Comparing results with conventional methods

Methods	Linear Range (mg/mL)	Detection Limit(mg/mL)
Our work	$5.0 \times 10^{-7} - 1.0 \times 10^{-5}$	1.1×10^{-7}
Chemometrics [2]	$3.3 \times 10^{-5} - 2.3 \times 10^{-3}$	1.4×10^{-5}
Optical biosensor [3]	$1.0 \times 10^{-5} - 1.0 \times 10^{-3}$	2.5×10^{-6}
Flow injection analysis[24]	0.0 - 28.0	0.76

282 3.4 Selectivity studies of the β -CD/Cs-MGO-SMIP-CL biosensor

283 In order to study the recognition properties of the biosensor using
 284 β -CD/Cs-MGO-SMIP nanoparticles to BSA, the CL intensity of solutions containing
 285 rich amounts of other substance such as Mg^{2+} , L-tryptophan, Lys and BHb was
 286 researched. It was evident from Fig. 7 C that 370 times Mg^{2+} (compared to the
 287 concentration of BSA) would interference the CL biosensor, while interference of 700
 288 times Mg^{2+} was observed in β -CD/Cs-MGO-SMIP-CL biosensor. As anticipated,
 289 L-tryptophan exhibited a higher interference compared with Mg^{2+} . While almost Lys
 290 interfering the detection of BSA apparently in simple CL, interference could be
 291 eliminated when employing β -CD/Cs-MGO-SMIP selectivity adsorbing BSA.
 292 Certainly, the interferences BHb were relatively more serious. Evidently, the CL
 293 method exhibited a significant interference effect more than triple concentration ratio
 294 compared to β -CD/Cs-MGO-SMIP-CL biosensor. The exhaustive study was subject to
 295 an explanation that specific structure of the MIP matrix in which biomacromolecule
 296 BSA could be fixed by the imprinting cavies appropriately.

297 3.5 Application of β -CD/Cs-MGO-SMIP-CL biosensor

298 Tab. 2 illustrated the application of β -CD/Cs-MGO-SMIP-CL biosensor in

299 samples. The results showed that the β -CD/Cs-MGO-SMIP-CL biosensor was capable
 300 of detecting BSA with a good recoveries ranging from 94% and 106%. As indicated,
 301 that the proposed β -CD/Cs-MGO-SMIP-CL biosensor was highly accurate, precise
 302 and selective, and it could be used for the analysis of samples. The application of the
 303 proposed biosensor for measuring samples demonstrated the feasibility of
 304 β -CD/Cs-MGO-SMIP in CL biosensor.

305 **Tab.2** Assay of BSA in samples by means of β -CD/Cs-MGO-SMIP-CL biosensor

Sample	c (10^{-6} mg/mL)	Added (10^{-6} mg/mL)	Found ($n=6$) (10^{-6} mg/mL)	RSD%	Recovery (%)
1 [#]	1.9	5.0	7.1	3.5	104
2 [#]	5.4	5.0	10.7	4.0	106
3 [#]	7.7	5.0	12.4	3.3	94

306 **4 Conclusion**

307 In this paper, using β -CD/Cs-MGO nanocomplex as a new supporting material in
 308 the preparing process of SMIP, a new CL biosensor to BSA based on
 309 β -CD/Cs-MGO-SMIP has been proposed. The maximum adsorption capacity of
 310 β -CD/Cs-MGO-SMIP was 58 mg/g and the obtained β -CD/Cs-MGO-SMIP followed
 311 langmuir isotherm equation and pseudo-second order sorption kinetics when binding
 312 BSA. Fast mass transfer, promoted rate of removal of the biomolecule and excellent
 313 recognition and adsorption ability for the imprinting cavities situated at the surface or
 314 in the proximity of the surface of the β -CD/Cs-MGO was achieved, which enabled
 315 easy access to the target protein molecules. The combination of high selectivity of
 316 SMIP based on the strong recognition effect between SMIP and BSA and the high
 317 sensitive CL determination method made the proposed biosensor perform excellent in

318 the determination of BSA. Based on this, the future work will focused on the
319 preparation of synthetic receptor materials as SMIP element with higher adsorption
320 capacity and selectivity for fabrication of biomimetic CL biosensors.

321

322 **Reference**

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