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1 **Molecular characteristics of collagen extracted from the starry**
2 **triggerfish skin and its potential in development of biodegradable**
3 **packaging film**

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Abstract

Collagen from alternative sources is being considered for various industrial applications. This study presents the extraction of collagen, a product of high value, from the skin of starry triggerfish (*Abalistes stellatus*). The feasibility of utilising the extracted collagens for fabrication of biodegradable food packaging film via casting method has also been investigated. The extracted acid solubilised collagen (ASC) and pepsin solubilised collagen (PSC) with the yield of 7.1 ± 0.2 % and 12.6 ± 0.1 % (wet weight basis), respectively, were identified as type I collagen. ATR-FTIR spectra displayed that both ASC and PSC molecules had intact triple helical structure stabilised mainly by the hydrogen bonds. Net charge of ASC and PSC became zero at pHs of 5.6 and 5.4, respectively as determined by zeta potential titration. Furthermore, ASC based packaging film showed the highest tensile strength (TS), elastic modulus (E) and contact angle (θ), but lowest elongation at break (EAB) and water vapour permeability (WVP) ($P < 0.05$), compared with PSC film. Increased glass-transition temperature (T_g) and endothermic melting temperature (T_m) accompanied with higher enthalpy (ΔH) were detected in ASC film, indicating a strong protein-protein interaction in film network. Based on thermal analysis, ASC film contained higher heat-stable mass residues (30.9 %, w/w) as compared to PSC film (14.3 %, w/w) in the temperature range of 50-600 °C. Microstructure of ASC film had finer and smoother surface without layering or cracking phenomenon; however, coarser surface was observed in PSC film. Therefore, the skin of starry triggerfish could serve as a potential source of collagen for food packaging film applications.

Keywords: Starry triggerfish skin, Collagen, Molecular properties, Film formation, Mechanical properties

1 **1. Introduction**

2 Collagen is an extracellular matrix component that is frequently used as
3 biomaterial.¹ Type I collagen, the most common type of collagen is the predominant
4 component of connective tissues such as skins, bones, tendons, dentin, cornea,
5 vascular systems or fibrous capsule of internal organs.^{2,3} Type I collagen is known as
6 fibrillar collagen and play a structural role by contributing to the molecular
7 architecture, shape and mechanical properties of skin tissues.^{4,5} The traditional
8 sources of collagen and collagen-derived products are bovine and porcine skins and
9 bones. Nevertheless, porcine collagen is unacceptable for some religions, while those
10 from bovine sources are at risk of contamination with foot-and-mouth disease and
11 bovine spongiform encephalopathy (BSE).⁶ As a consequence, marine collagen and
12 its products are in very high demand due to the lack of disease transmission and
13 dietary restriction. From the fish processing operations, a large amount of collagen-
14 rich by-products (60-70 %) including skins, bones, scales, fins, head, guts and frame
15 are discarded, which causes pollution and emit offensive odours.^{2,7} It is imperative to
16 develop a procedure for utilising these by-products to provide a practically feasible
17 and economically viable solution that could lead to an increased revenue, energy-
18 conserving, profitability for fish-processors and green approach in terms
19 environmental protective aspect and waste management benefits. Therefore, these
20 underutilised resources have attracted the increasing attention as the raw material for
21 marketable value-added product such as collagen, gelatine, hydrolysate, etc. Among
22 the fish processing waste, fish skin is promising raw material for collagen extraction
23 as about 70-80 % of its dry matter is collagen, and thus could be used as a
24 replacement for mammalian sources.² Nevertheless, a low yield of collagen is
25 obtained with the traditional process using acetic acid as the extraction solvent.² The
26 appropriate concentration of pepsin has been reported to cleave peptides in the
27 telopeptide region, thereby increasing the collagen yield and decreasing the time of
28 extraction process without any detrimental effect on the integrity of collagen
29 structure.¹ Due to the enormous amount of fish viscera, especially stomach, pepsin of
30 fish origin could be recovered and used to maximise the yield of collagen from fish
31 skin.¹

32 Collagen has a wide range of applications in various branches of industries
33 due to its excellent film-forming ability, low-antigenicity, low-allergenicity, non-
34 toxicity, biocompatibility and biodegradability. Due to the strong mechanical

1 properties, collagen films could be used in food packaging industry. Collagen films
2 could become an integral/edible part of meat products, thus they can function to
3 provide safety benefits, control undesirable changes, reduce the shrink loss of meat
4 and meat based products during storage, thereby extending the shelf life and retains
5 their visual appeal for longer period.⁸ Collagen has been used for producing edible
6 casings for meat processing industries (sausages/salami/snack sticks) and drug
7 delivery carriers or wound dressings in the medical fields.⁹ Fibrillar collagens are very
8 well suited for the production of edible sausage casings and films, since they form
9 readily stable networks that are able to shrink and stretch to accommodate contraction
10 and expansion of meat batter during continuous processing.¹⁰ Apart from that collagen
11 with high market value can be used for medical and tissue engineering as well as
12 bioengineered teeth, skin tissue, etc

13 Starry triggerfish (*Abalistes stellatus*) belongs to the order Tetraodontiformes
14 and is a member of the Balistidae family. This species is used for surimi and fillet
15 production, in which a large amount of skin is produced as by-product. Due to its
16 thick skin, it could be potential source of collagen, especially when fish pepsin is
17 employed as the extraction aid. The collagen extraction from fish skin would not only
18 increase the added value to these by-products, but also accelerate the development of
19 fish processing industries and reduce environmental pollution. However, no
20 information regarding the molecular characteristics and film-forming ability of
21 collagen from the skin of this species has been reported. Therefore, the objective of
22 present study was to extract and comparatively characterise the acid solubilised
23 collagen (ASC) and pepsin solubilised collagen (PSC) from the skin of starry
24 triggerfish. Moreover, the extracted collagen from triggerfish skin was used for the
25 development of biodegradable food packaging film in order to replace the
26 conventional petroleum based plastic packaging films. The mechanical and thermal
27 properties of collagen based films were determined with a view to facilitate their
28 application in food packaging industry.

29

30 **2. Materials and methods**

31 *2.1. Chemicals*

32 Bovine haemoglobin, β -mercaptoethanol (β -ME), L-tyrosine and bovine
33 serum albumin were purchased from Sigma Chemical Co. (St. Louis, MO, USA).
34 High molecular weight marker was purchased from GE Healthcare UK (BKM, UK).

1 Trichloroacetic acid, Folin-Ciocalteu's phenol reagent, glacial acetic acid, glycerol,
2 sodium hydroxide (NaOH) and tris(hydroxymethyl) aminomethane were obtained
3 from Merck (Darmstadt, Germany). Sodium dodecyl sulphate (SDS), *N,N,N',N'*-
4 tetramethyl ethylene diamine (TEMED) and Coomassie blue R-250 were procured
5 from Bio-Rad Laboratories (Hercules, CA, USA). All the chemicals used in this study
6 were of analytical grade.

7 *2.2. Fish skin and stomach preparation*

8 The skin of starry triggerfish (*A. stellatus*) and stomach of albacore tuna
9 (*Thunnus alalunga*) was obtained from local surimi processing plant, Perak, Malaysia.
10 The samples were packed in polythene bags and kept in ice using a skin/ice ratio of
11 1:2 (w/w) and transported within 3 h to the School of Industrial Technology,
12 Universiti Sains Malaysia, Penang, Malaysia. The skin was denuded manually and the
13 cleaned skin was washed with iced tap water (0-2 °C). The prepared skin was then cut
14 into small pieces (0.25×0.25 cm²) to increase its surface area. Both prepared skin and
15 stomach were placed in polyethylene bags and stored at -20 °C until use. The storage
16 time was less than 2 months.

17 *2.3. Preparation of stomach extract.*

18 The frozen stomach of albacore tuna was thawed using running water (26-28
19 °C) until the core temperature reached -2 to 0 °C. The sample was cut into pieces (1×1
20 cm²) and finely ground in liquid nitrogen using a National blender (Model MX-
21 T2GN, Taipei, Taiwan) to a powder form according to the method of Ahmad and
22 Benjakul.¹ Stomach powder was suspended in 50 mM sodium phosphate buffer (pH
23 7.2) at a ratio of 1:10 (w/v). The mixture was stirred continuously at 4 °C for 30 min.
24 The suspension was centrifuged at 7,700 × g for 30 min at 4 °C using a Beckman
25 Coulter centrifuge (Model Avanti J-E, CA, USA) to remove the tissue debris. The
26 supernatant was collected and referred to as 'stomach extract'. The protein content in
27 the stomach extract was measured as per the Lowry method using bovine serum
28 albumin as a standard.¹¹

29 *2.4. Assay of proteolytic activity*

30 Prior to assay, the stomach extract from albacore tuna was adjusted to pH 2
31 with 1 M HCl and the mixture was allowed to stand at 4 °C for 10 min as described
32 by Nalinanon et al.¹² The treated stomach extract was centrifuged at 5,000 × g for 10
33 min at 4 °C using a refrigerated centrifuge. The acidified supernatant was collected
34 and used as the sources of activated pepsin.

1 Proteolytic activity of acidified stomach extract from albacore tuna was
2 determined using haemoglobin as a substrate as per the method of Nalinanon et al.¹²
3 To initiate the reaction, 200 μL of stomach extract were added into the assay mixture
4 containing 200 μL of 2 % (w/v) haemoglobin, 200 μL of distilled water and 625 μL
5 of McIlvaine's buffer [0.2 M Na-phosphate and 0.1 M Na-citrate, pH 2.0].
6 Appropriate dilution was made to ensure that the amount of enzyme was not excessive
7 for available substrate in the assay system. The reaction was conducted at 50 °C for
8 20 min. To terminate enzymatic reaction, 200 μL of 50 % (w/v) trichloroacetic acid
9 (TCA) were added. Unhydrolysed protein substrate was allowed to precipitate for 15
10 min at 4 °C, followed by centrifuging at $4,725 \times g$ for 10 min at room temperature
11 (26-28 °C) using a MIKRO 20 centrifuge (Hettich Zentrifugen, Tuttlingen, Germany).
12 The oligopeptide content in the supernatant was measured by the Lowry method using
13 tyrosine as a standard.¹¹ One unit of activity was defined as the amount releasing
14 $1 \mu\text{mol}$ of tyrosine per min ($\mu\text{mol Tyr/min}$). A blank was performed in the same
15 manner, except that the acidified stomach extract was added into the reaction mixture
16 after the addition of 50 % (w/v) TCA.

17 2.5. Extraction of collagen

18 All procedures were carried out at 4 °C with a gentle stirring. The collagen
19 from the skin of starry triggerfish was extracted following the method of Ahmad and
20 Benjakul¹ with a slight modification. Skin was soaked in 0.1 M NaOH with a
21 skin/solution ratio of 1:20 (w/v) with the continuous stirring to remove non-
22 collagenous proteins for 6 h. The alkaline solution was changed every 2 h. The
23 alkaline treated skin was then washed with cold water until the pH of the wash water
24 became neutral or faintly basic. Residual fat in the skin was removed using 10 % (v/v)
25 butyl alcohol with a skin/solution ratio of 1:10 (w/v) for 18 h with a change of
26 solution every 6 h. Defatted skin was thoroughly washed with 15 volumes of cold
27 water (4-5 °C). The defatted skin was soaked in 0.5 M acetic acid with a skin/solution
28 ratio of 1:15 (w/v) for 48 h in the absence and presence of acidified stomach extract at
29 a level of 25 units/g of defatted skin. The mixture was filtered with two layers of
30 cheesecloth to remove undissolved debris. The filtrate was added with NaCl to obtain
31 the final concentration of 2.6 M in the presence of 0.05 M tris(hydroxymethyl)
32 aminomethane (pH 7.0). The resultant precipitate was collected by centrifuging at
33 $20,000 \times g$ for 60 min at 4 °C. The pellets were dissolved in 10 volumes of 0.5 M
34 acetic acid and dialysed against 9 volumes of 0.1 M acetic acid and distilled water,

1 respectively. The dialysate was finally freeze-dried using a Model Coolsafe 55,
2 Scanvac, (Coolsafe, Lyngø, Denmark). The dried powder extracted in the absence and
3 presence of stomach extract was referred to as ASC and PSC, respectively. The yield
4 of ASC and PSC was calculated and expressed as dry matter/wet weight of skin. ASC
5 and PSC were then subjected to following analysis.

6 *2.6. Amino acid analysis*

7 ASC and PSC samples were hydrolysed under reduced pressure in 4 M
8 methane sulfonic acid containing 0.2 % (v/v) 3-(2-aminoethyl) indole at 115 °C for
9 24 h. For tryptophan determination, the samples were hydrolysed by 3 N
10 mercaptoethanesulphonic acid to avoid the decomposition of tryptophan. The
11 hydrolysates were neutralised with 3.5 M NaOH and diluted with 0.2 M citrate buffer
12 (pH 2.2). An aliquot of 0.4 mL was applied to an amino acid analyser (MLC-703;
13 Atto Co., Tokyo, Japan). The degree of hydroxylation of proline was calculated as the
14 percentage of hydroxyproline from total imino acids.

15 *2.7. SDS-polyacrylamide gel electrophoresis (SDS-PAGE)*

16 SDS-PAGE was performed by the method of Laemmli.¹³ The ASC and PSC
17 samples were dissolved in 5 % (w/v) SDS and the mixtures were incubated at 85 °C
18 for 1 h. The mixture was centrifuged at 4,000 × g for 5 min at room temperature to
19 remove undissolved debris. Solubilised samples were mixed at 1:1 (v/v) ratio with the
20 sample buffer [0.5 M Tris HCl, pH 6.8, containing 4 % (w/v) SDS, 20 % (v/v)
21 glycerol and 0.1 % (w/v) bromophenol blue] in the presence or absence of 10 % (v/v)
22 β-ME. The mixtures were boiled in boiling water for 2 min. Samples (15 µg protein)
23 were loaded onto polyacrylamide gels comprising of 7.5 % running gel and 4 %
24 stacking gel and subjected to electrophoresis at a constant current of 15 mA/gel using
25 a Mini Protein II unit (Bio-Rad Laboratories, Inc., Richmond, CA, USA). After
26 electrophoresis, gel was stained with 0.05 % (w/v) Coomassie blue R-250 in 15 %
27 (v/v) methanol and 5 % (v/v) acetic acid and destained with 30 % (v/v) methanol and
28 10 % (v/v) acetic acid. High molecular weight marker (GE Healthcare, Aylesbury,
29 UK) was used to estimate the molecular weight of proteins. Type I fish skin collagen
30 was used as a standard.

31 *2.8. ATR-FTIR analysis*

32 ASC and PSC samples were subjected to attenuate total reflectance-Fourier
33 transform infrared spectroscopy (ATR-FTIR). FTIR spectrometer (Model Equinox 55,
34 Bruker, Ettlingen, Germany) equipped with a horizontal ATR Trough plate crystal

1 cell (45° ZnSe; 80 mm long, 10 mm wide and 4 mm thick) (PIKE Technology Inc.,
2 Madison, WI, USA) was used. For spectra analysis, the collagen samples were placed
3 onto the crystal cell and the cell was clamped into the mount of FTIR spectrometer.
4 The spectra in the range of 600-4000 cm^{-1} with automatic signal gain were collected
5 in 32 scans at a resolution of 4 cm^{-1} and were rationed against a background spectrum
6 recorded from the clean empty cell at 25 °C. Analysis of spectral data was carried out
7 using the OPUS 3.0 data collection software programme (Bruker, Ettlingen,
8 Germany). Prior to data analysis, the spectra of ASC and PSC were first normalised to
9 the band at amide III, and a linear baseline correction was then applied on all the
10 spectra.

11 *2.9. UV-Vis absorption*

12 UV-Vis absorption spectra of ASC and PSC samples were recorded using UV-
13 Vis spectrophotometer (Model UV-1800 Shimadzu, Kyoto, Japan). ASC and PSC
14 solutions were prepared by dissolving the desired quantity (5 mg/mL) of collagen in
15 0.5 M acetic acid. Prior to the measurement, the base line was set with 0.5 M acetic
16 acid. The spectra was obtained by scanning the wavelength of ASC and PSC solution
17 in the range of 190-500 nm with a scan speed of 50 nm/min at room temperature.

18 *2.10. Differential scanning calorimetry*

19 Differential scanning calorimetry (DSC) of ASC and PSC samples was run
20 following the method of Rochdi et al.¹⁴ with a slight modification. The samples were
21 rehydrated by adding deionised water or 0.05 M acetic acid to dried samples at a
22 sample/solution ratio of 1:40 (w/v). The mixtures were allowed to stand for 2 days at
23 4 °C. DSC was performed using a differential scanning calorimeter (Perkin Elmer,
24 Model DSC7, Norwalk, CA, USA). Temperature calibration was run using the indium
25 thermogram. The accurate weight of samples was placed in aluminium pans and then
26 pans were hermetically sealed. The samples were scanned at 1 °C/min over the range
27 of 20-50 °C using iced water as the cooling medium. An empty pan was used as the
28 reference. Total denaturation enthalpy (ΔH) was estimated by measuring the area
29 under the endothermic peak in the DSC thermogram. The denaturation temperature
30 (T_m) was estimated from the endothermic peak of DSC thermogram.

31 *2.11. Measurement of ζ -potential*

32 ASC and PSC samples were dissolved in 0.5 M acetic acid at a concentration
33 of 0.5 mg/mL. The mixture was stirred at 4 °C for 12 h. The ζ -potential of each
34 sample (20 mL) was measured using a zeta potential analyzer (ZetaPALS,

1 Brookhaven Instruments Co., Holtsville, NY, USA). The ζ -potential of samples
2 adjusted to different pHs with 1 M nitric acid or 1 M KOH using an autotitrator (BI-
3 ZTU, Brookhaven Instruments Co., Holtsville, NY, USA) was determined. The pH
4 rendering zero ζ -potential was obtained from the titration curve.

5 *2.12. Fabrication of ASC and PSC based films for food packaging applications*

6 ASC and PSC based films were prepared according to the casting method
7 reported by Kozłowska et al.¹⁵ with a slight modification. The collagen samples were
8 dissolved in 0.5 M acetic acid to obtain film-forming solution (FFS) with a
9 concentration of 2 % (w/v). Glycerol as plasticiser was added to FFS at the
10 concentration of 25 % (w/w) based on the dry weight of collagen, and the air bubbles
11 in FFS were removed by a vacuum oven in ice bath. Subsequently, a volume of 8 mL
12 FFS was poured onto a rimmed silicone resin plate (5×5 cm²) and dried in an
13 environmental chamber (PSX-330H; Laifu Technology Co., Ltd., Ningbo, China) at
14 25±0.5 °C and 50±5 % relative humidity (RH). The resulting collagen based films
15 were manually peeled off and conditioned at 25±0.5 °C and 50±5 % RH for 48 h prior
16 to analyses.

17 For DSC, TGA and SEM studies, films were conditioned in a dessicator
18 containing dried silica gel for 1 week to minimise the plasticising effect of water,
19 followed by drying in a dessicator containing P₂O₅ gel for 2 weeks at room
20 temperature (28-30 °C) to obtain the most dehydrated films (≤4 % moisture content).

21 *2.13. Analyses*

22 *2.13.1. Measurement of stress-strain properties*

23 The stress-strain properties, such as tensile strength (TS), elastic modulus (E)
24 and elongation at break (EAB) of collagen based films were determined as described
25 by Iwata et al.¹⁶ using the Universal Testing Machine (Lloyd Instrument, Hampshire,
26 UK). The test was performed in the controlled room at 25-28 °C and ~50±5 % RH.
27 Ten films (2×5 cm²) with the initial grip length of 3 cm were used for testing. The
28 films were clamped and deformed under tensile loading using a 100 N load cell with
29 the cross-head speed of 30 mm/min until the samples were broken. The TS was
30 expressed in MPa and calculated by:

$$31 \quad \text{TS (MPa)} = \frac{P_{\max}}{A} \quad \text{Eq. (1)}$$

1 where P_{max} is the maximum force (N) necessary to pull the sample apart, and A is the
2 initial cross-sectional area of the sample film (m^2) determined by multiplying the film
3 width by the film thickness.

4 Percentage elongation at break is the amount of uniaxial strain at fracture and
5 was calculated by:

$$6 \quad \text{EAB (\%)} = \frac{l_b - l_o}{l_o} \times 100 \quad \text{Eq. (2)}$$

7 where l_b is the film elongation at the moment of failure and l_o is the initial grip length
8 (3 cm) of samples multiplied by 100.

9 Elastic modulus was expressed in MPa and was determined by calculating the
10 slope of the elastic (linear) region of an engineering stress-strain curve:

$$11 \quad E \text{ (MPa)} = \frac{\Delta S}{\Delta e} \quad \text{Eq. (3)}$$

12 where ΔS is the change in tensile stress and Δe is the change in tensile strain over the
13 elastic region.

14 2.13.2. Water vapour permeability (WVP)

15 WVP was measured using gravimetric modified cup method based on ASTM
16 method (American Society for Testing and Materials) as described by Shiku et al.¹⁷
17 Briefly, collagen based films were sealed on an aluminium permeation cup containing
18 dried silica gel (0 % RH) with silicone vacuum grease and rubber gasket, and held
19 with four screws around the cup's circumference. After measuring the initial weight,
20 test cups were placed in a desiccator containing the distilled water (30 °C, ~50±2 %
21 RH). Consequently, test cups were weighed to the nearest 0.0001 g with an electronic
22 balance (Model CPA225D, Sartorius Corp., Goettingen, Germany) at 1 h intervals
23 over an 8 h period. A plot of weight gained versus time was used to determine the
24 WVP and the slope of the linear portion of this plot represented the steady state
25 amount of water vapour diffusing through the film per unit of time (g/h). Five films
26 were used for analysis and WVP of the film was calculated as follows:

$$27 \quad \text{WVP (g m}^{-1} \text{ s}^{-1} \text{ Pa}^{-1}) = w l A^{-1} t^{-1} (P_2 - P_1)^{-1} \quad \text{Eq. (4)}$$

28 where w is the weight gain of the cup (g); l is the film thickness (m); A is the exposed
29 area of film (m^2); t is the time of gain (s); $(P_2 - P_1)$ is the vapour pressure difference
30 across the film (4,244.9 Pa at 30 °C).

31 2.13.3. Contact angle measurement

1 Contact angle (θ) of collagen based films was measured in a conditioned room
2 (25 °C) by the sessile drop method using contact angle meter (Model KSV CAM 101,
3 KSV Instruments, Ltd., Helsinki, Finland), equipped with image analysis software.
4 Briefly, film sample (2×2 cm²) was placed on a movable platform and levelled
5 horizontally. A droplet of ultra-pure water (30 μ L) was placed on a film surface using
6 500 μ L microsyringe (Hamilton Robotics Inc., Bonaduz, GR, Switzerland) attached
7 with a needle of 0.75 mm diameter. Image analyses were carried out using image
8 recorder CAM 200 software and the contact angles were noted.

9 *2.13.4. Differential scanning calorimetry*

10 Thermal properties of collagen based films were determined using differential
11 scanning calorimeter. Temperature calibration was performed using the indium
12 thermogram. The films (4-5 mg) were accurately weighed into aluminium pans,
13 hermetically sealed and scanned over the temperature range of -30 to 200 °C
14 (1st heating scans) and -30 to 300 °C (2nd heating scans) with a heating rate of 10
15 °C/min. The dry ice was used as a cooling medium and the system was equilibrated at
16 -50 °C for 5 min prior to the scan. The empty aluminium pan was used as a reference.
17 The glass transition temperature (T_g) was calculated as the inflexion point of the base
18 line, caused by the discontinuity of the specific heat of the sample. The melting
19 temperature (T_m) was estimated from the endothermic peak of DSC thermogram and
20 transition enthalpy (ΔH) was determined from the area under the endothermic peak.
21 All these properties were calculated with help of the DSC-7 software.

22 *2.13.5. Thermo-gravimetric analysis*

23 The dried collagen based films were scanned using a thermo-gravimetric
24 analyser (Perkin Elmer, Model TGA-7, Norwalk, CT, USA) from 40 to 600 °C at a
25 rate of 10 °C/min. Nitrogen was used as the purge gas at a flow rate of 20 mL/min.
26 The percent weight loss (%) versus temperature plots were taken for thermo-
27 gravimetric analysis (TGA) and derivative weight loss (%) against temperature was
28 taken for differential thermo-gravimetric analysis (DTG).

29 *2.13.6. Microstructure*

30 Microstructure of upper surface and cryo-fractured cross-section of the
31 collagen based films was visualised using a scanning electron microscope (Model
32 JSM-5800 LV, JEOL, Tokyo, Japan) at an accelerating voltage of 10 kV. The
33 collagen based films were cryo-fractured by immersion in liquid nitrogen. Prior to
34 visualisation, the collagen based films were mounted on brass stub and sputtered with

1 gold in order to make the sample conductive, and photographs were taken at 8000x
2 magnification for surface. For cross-section, cryo-fractured films were mounted
3 around stubs perpendicularly using double sided adhesive tape, coated with gold and
4 observed at the 5000x magnification.

5 *2.14. Statistical analyses*

6 All experiments were performed in triplicate and a completely randomised
7 design (CRD) was used. Data were presented as means± standard deviation and the
8 probability value of <0.05 was considered significant. Analysis of variance (ANOVA)
9 was performed and mean comparisons were done by Duncan's multiple range tests.
10 Analysis was performed using a SPSS package (SPSS 11.0 for windows, SPSS Inc,
11 Chicago, IL, USA).

13 **3. Results and discussion**

14 In recent years, a trial has been continuously performed to extract the collagen
15 from the marine sources for further applications in food and nutraceutical industries.
16 Although fish collagen is an alternative to the commercially available mammalian
17 collagens, but so far, there has been a gap between the scientific interest and the wide
18 industrial application of this source of collagen. In this work, we reported the
19 extraction and characterisation of acid solubilised collagen (ASC) and pepsin
20 solubilised collagen (PSC) from starry triggerfish skin. The collagen extraction from
21 fish skin trimmings will not only provide scope for the secured disposal of the solid
22 waste but also would be an option for producing a valuable product, which will bring
23 about significant returns. Due to the environmental concerns, the use of biodegradable
24 packaging material has recently attracted considerable interest as a substitute for
25 petroleum based plastic packaging. This study highlights the feasibility of utilising
26 ASC and PSC for the development of biodegradable food packaging films.

27 *3.1. Yield of ASC and PSC from the skin of starry triggerfish*

28 Yields of ASC and PSC extracted from the skin of starry triggerfish were
29 7.1 ± 0.2 % and 12.6 ± 0.1 % (wet weight basis), respectively. Triggerfish skin
30 contained the highly ordered type I collagen fibres at the level of 24.6 g/100 g as
31 determined by hydroxyproline content. Yields based on the initial collagen content in
32 the triggerfish skin or percent recovery (%) for ASC and PSC were 28.9 % and 51.3
33 %, respectively. During the extraction process, the skin of triggerfish was not
34 completely solubilised by 0.5 M acetic acid or pepsin, as shown by the lower yield of

1 ASC and PSC. This result was in agreement with Ahmad et al.² who reported the
2 incomplete solubilisation of unicorn leatherjacket skin in 0.5 M acetic acid. This
3 observation suggested that the collagen molecules in triggerfish skin were most likely
4 cross-linked by covalent bonds through the condensation of aldehyde groups with
5 lysine and hydroxylysine in the telopeptide region, leading to decreased solubility of
6 collagen in acid.¹⁸ From the review literature, the yields of ASC and PSC from
7 unicorn leatherjacket skin were 4.2 % and 8.5 % (wet weight basis), respectively.^{1,2}
8 The differences in extraction yields and collagen recovery between different species
9 might be governed by varying cross-linking of collagen fibrils in the raw material.
10 The higher yield of PSC as compared to ASC suggested that stomach extract (tuna
11 pepsin) facilitated the extraction of collagen from triggerfish skin. Pepsin has the
12 potential to cleave specifically at the telopeptide region of collagen molecules without
13 damaging the integrity of triple-helix.¹ Therefore, pepsin could be used as an effective
14 aid for increasing the collagen yield from the skin of starry triggerfish.

15 *3.2. Amino acid profile of ASC and PSC from the skin of starry triggerfish*

16 Amino acid profile of ASC and PSC extracted from the skin of starry
17 triggerfish is shown in Table 1. Both collagens contained glycine (319-322
18 residues/1000 residues) as the major amino acid, followed by alanine (140-144
19 residues/1000 residues), proline (107-109 residues/1000 residues) and hydroxyproline
20 (79-84 residues/1000 residues). Generally, glycine in collagen represents nearly one
21 third of the total residues and occurs as every third residue in collagen except for the
22 first 14 amino acid residues from the N-terminus and the first 10 residues from the C-
23 terminus.¹⁹ The imino acid content (proline + hydroxyproline) of ASC and PSC was
24 193 and 186/1000 residues, which was higher than those of most fish collagens such
25 as ocellate puffer collagen (170 residues/1000 residues).¹⁸ The variation in imino acid
26 content amongst different species is mostly due to different living environments of
27 habitat, particularly temperature.^{20,21} Hydroxylysine (4-5 residues/1000 residues) was
28 found in both ASC and PSC from starry triggerfish skin. It was found that the ASC
29 contained a slightly higher imino acid content than the PSC. The degree of
30 hydroxylation of proline in ASC and PSC was calculated to be 43.5 % and 42.5 %,
31 respectively. It was suggested that the teleopeptides removed by pepsin digestion
32 contained fewer imino acids. As a result, lower proportion of imino acids was found
33 in PSC. No cysteine and tryptophan were detected in either ASC or PSC. Generally,
34 type I collagen has low amounts of cysteine (~0.2%) and methionine (~1.2-1.3%).²²

1 The amino acid composition of collagens from starry triggerfish skin was found to be
2 almost similar to those of collagen from other freshwater fish including common carp,
3 channel catfish and silver carp.²³

4 *3.3. Protein pattern of ASC and PSC from the skin of starry triggerfish*

5 Protein pattern of ASC and PSC extracted from the skin of starry triggerfish
6 determined under reducing and non-reducing conditions is illustrated in Fig. 1. Both
7 ASC and PSC were composed of a heterotrimer of two α_1 -chains and one α_2 -chain
8 with the molecular weight of 119-121 and 112-117 kDa, respectively. High molecular
9 weight components, including β -chain (dimer), γ -chain (trimer) as well as the cross-
10 linked constituents were also observed in both ASC and PSC. The ratio of α_1/α_2 chain
11 was approximately 2:1 in ASC and PSC, and both collagen samples were most likely
12 classified as type I collagen.²⁰ A slight difference in the protein pattern was noticeable
13 in PSC, compared with ASC. Slight degradation of major proteins with the
14 concomitant formation of low molecular weight peptides was noticeable when pepsin
15 from albacore tuna stomach was used. It was suggested that pepsin from albacore tuna
16 stomach was able to hydrolyse tropocollagen as indicated by the decreased band
17 intensity of β - and α -chains. It was noted that molecular weights of α -chains of PSC
18 was slightly lower than that of ASC. Hence, it can be inferred that pepsin most likely
19 cleaved some peptides at telopeptide region. As a consequence, a slight decrease in
20 molecular weight of PSC was noticeable, in comparison with that of ASC. This result
21 indicated that pepsin used in this study could cleave intermolecular cross-links of α -
22 chains. It was demonstrated that two types of intermolecular bonds, side-to-side and
23 end-to-end bond, in collagen could easily be cleaved by pepsin, whereas head-to-tail
24 bond is relatively pepsin resistant.²⁴ Drake et al. reported that most of intra- and
25 intermolecular cross-links found in collagen occur through the telopeptide region.²⁵
26 No differences in the electrophoretic patterns of ASC and PSC were noticeable in the
27 presence and absence of β -ME. This indicated that there was no disulphide bond in
28 ASC and PSC. The result was in accordance with the absence of cysteine in ASC and
29 PSC (Table 1).

30 *3.4. Thermal denaturation of ASC and PSC from the skin of starry triggerfish*

31 Thermal transitions of ASC and PSC from the skin of starry triggerfish
32 dispersed in 0.05 M acetic acid or deionised water are depicted in Fig. 2. Endothermic
33 peaks with the denaturation temperatures (T_m) of 31.4 ± 0.5 and 29.2 ± 0.5 °C were
34 found in ASC and PSC dispersed in 0.05 M acetic acid, respectively. When ASC and

1 PSC were suspended in deionised water, T_m of 35.9 ± 0.5 and 33.6 ± 0.8 °C was
2 observed, respectively. It was noted that T_m shifted to a lower temperature ($P < 0.05$),
3 when ASC and PSC were dispersed in acetic acid. The results suggested that
4 intramolecular hydrogen bonds stabilising the triple helix structure of collagen might
5 be disrupted to some levels, in the presence of acetic acid, mainly due to the repulsion
6 of collagen molecules in acidic solution. This alteration resulted in the decrease in T_m .
7 Furthermore, the different T_m noticed in collagen samples was due to the different
8 medium used for suspending ASC and PSC. Nevertheless, the differences in ΔH were
9 noticeable among ASC and PSC. For collagen dispersed in acetic acid or deionised
10 water, the lowest ΔH was found in PSC, compared with ASC ($P < 0.05$). The
11 differences in T_m and ΔH among ASC and PSC samples might be governed by the
12 composition and sequence of amino acid as well as the tertiary structure of collagen.
13 T_m of ASC and PSC samples from the skin of starry triggerfish were much lower than
14 that of pig skin collagen (37 °C) and that of calf skin collagen (40.8 °C).^{26,27} This fact
15 clearly indicated that collagen from triggerfish skin was less stable than mammalian
16 collagen. Nevertheless, ASC and PSC from triggerfish skin showed the higher T_m than
17 collagen from other fish species, such as ocellate puffer fish (28.0 °C) and grass carp
18 (24.6 °C).^{18,28} In general, T_m of collagen is influenced by the imino acid content. The
19 higher imino acid content could be associated with increased T_m .¹⁸ Factors influencing
20 the thermal properties of collagen include the content of imino acid, degree of
21 hydroxylation of proline and the content of the glycine-proline-hydroxyproline
22 sequence.²⁹ The thermal transition temperature of the collagen triple helix is attributed
23 to the hydrogen bonded networks, mediated by water molecules, which connect the
24 hydroxyl group of hydroxyproline in one strand to the main chain amide or carboxyl
25 groups of another chain.³⁰ Therefore, the differences in hydroxyproline content might
26 determine the thermal transition temperatures of collagens from different fish species.

27 3.5. ATR-FTIR of ASC and PSC from the skin of starry triggerfish

28 FTIR spectra of ASC and PSC extracted from the skin of starry triggerfish are
29 depicted in Fig. 3. The major absorption bands in the spectra of both ASC and PSC
30 were described in Table 3. The spectra of both ASC and PSC had great similarity to
31 each other, which suggested that their chemical compositions were similar.³¹ For
32 amide I band, ASC had the lowest wavenumber, indicating the interaction of C=O
33 with the adjacent chains, while PSC had the highest wavenumber. Generally, the shift
34 to the lower wavenumber indicated the existence of hydrogen bonds in collagen.³²

1 The amide III band in ASC and PSC suggested the presence of triple helical structure.
2 The triple helical structure of ASC and PSC was also confirmed from IR ratio
3 between amide III and 1450 cm^{-1} which was approximately 1. The other bands,
4 arising from the stretching vibrations of N–H group and showing the existence of
5 hydrogen bonds in ASC and PSC appeared at 3293.3 and 3295.3 cm^{-1} , respectively,
6 corresponding to amide A, which occurs commonly in the range of $3280\text{--}3300\text{ cm}^{-1}$.
7 The amide B absorption bands for ASC and PSC were observed at the wavenumber of
8 $2910\text{--}5\text{--}3078.2\text{ cm}^{-1}$ and $2908.6\text{--}3081.6\text{ cm}^{-1}$, respectively. The slight differences
9 noted in peak heights and wavenumbers among ASC and PSC was correlated with the
10 differences in functional groups and intra- and intermolecular interaction. Thus, fish
11 pepsin used as extraction aid might affect the resulting PSC to some extent.

12 3.6. UV-Vis spectra of ASC and PSC from the skin of starry triggerfish

13 UV-Vis spectra of ASC and PSC extracted from the skin of starry triggerfish
14 are depicted in Fig. S1. ASC and PSC gave superimposed spectra which were
15 characteristic of type I collagen.³³ In UV region, a distinct absorption peaks for ASC
16 and PSC arose at 230 nm corresponding to the $n\rightarrow\pi^*$ transitions of C=O in the
17 peptide bonds of polypeptides chains.³⁴ The absorbance peak in the $230\text{--}240\text{ nm}$ was
18 considered as a suitable wavelength for detecting type I collagen. In addition, there
19 was absorbance between 200 and 220 nm , which was attributed to collagen peptide
20 bonds. The absence or weak absorbance at $250\text{--}280\text{ nm}$ showed that both ASC and
21 PSC lacked aromatic amino acids, such as tyrosine and phenylalanine, which are
22 sensitive chromophores and absorb UV light at 283 and 251 nm , respectively. The
23 absorption peaks observed were in agreement with the results from Nalinanon et al.³⁵

24 3.7. ζ -potential of ASC and PSC from the skin of starry triggerfish

25 The ζ -potential values representing the surface charge of ASC and PSC
26 measured as a function of pH are shown in Fig. 4. The surface net charge of ASC and
27 PSC decreased as the pH increased and became zero at pH of 5.6 and 5.4 ,
28 respectively. Protein molecules in an aqueous system have zero net charge at their
29 isoelectric points (pI), in which the positive charges are balanced out by the negative
30 charges.³⁶ At the pH near the isoelectric point, collagen molecules are unstable and
31 tend to coagulate or flocculate due to increased hydrophobic interaction among
32 collagen molecules. The pIs of ASC and PSC were in acidic range, possibly due to the
33 higher density of carboxyl groups. It was noted that the molecular charge of ASC and
34 PSC remained very low in the alkaline region. This might be associated with the low

1 solubility of ASC and PSC in the alkaline pH range, in which the repulsion force
2 between the molecules with the negative charge was not sufficient to cause the
3 complete solubilisation. The slight difference in the pI of ASC and PSC might be
4 caused by the differences in amino acid composition and configuration between
5 collagens.

6 *3.8. Characteristics of collagen based films*

7 The thickness and mechanical properties expressed as tensile strength (TS),
8 elastic modulus (E) and elongation at break (EAB) of ASC and PSC films are given
9 in Table 3. No significant difference in thickness was noted between ASC and PSC
10 films ($P > 0.05$). ASC film had the highest TS and E, but lowest EAB ($P < 0.05$),
11 compared with PSC film. Higher TS and E values indicating greater film strength and
12 stiffness, whilst lower EAB is an indicator of less stretch-ability prior to breakage.
13 Based on the results, ASC film was more rigid and less extensible than the PSC film
14 due to strong interaction among high molecular weight collagen chains via hydrogen
15 bonding. Consequently, the lower TS and E but higher EAB in PSC film was due to
16 the decreased structural cohesion via weaker chain-to-chain interaction or less
17 junction zones. In addition, the apparent flexibility in both ASC and PSC films was
18 coincidental with presence of glycerol in the film forming solution. Glycerol in the
19 film matrix acts as a plasticiser between the polymer chains and impeded the
20 association or interaction of protein chains, thereby yielding the weaker film
21 network.³⁷ As a consequence, the collagen matrix is more flexible and α -, β -, γ - chains
22 can slide past each other more readily during tensile deformation. In general,
23 mechanical properties of packaging films are largely associated with the nature and
24 the chemical structure of film forming materials.⁵ Therefore, these differences in
25 mechanical properties between ASC and PSC films might be governed by complex
26 interactions determined by the amino acid composition and the ratio of α/β -chains
27 present in the collagen.³⁸ Furthermore, the molecular weight distribution and imino
28 acid content of collagen play a key role in the mechanical properties of resulting
29 films.

30 Water vapour permeability values (WVP) of ASC and PSC films are shown in
31 Table 3. ASC film had the lowest WVP, compared with PSC film ($P < 0.05$). The
32 lower WVP of ASC film was coincidental with the highest TS (Table 3). In general,
33 the migration of moisture through films is governed by film network. Films with the
34 denser structure could lower the migration of moisture more effectively than those

1 with less compactness.³⁷ Furthermore, water vapour transfer normally occurs through
2 the hydrophilic portion of film network and depends on hydrophilic/hydrophobic ratio
3 of film constituents.⁵ The highest WVP in PSC was correlated with the increased
4 amino and carbonyl groups present at the teleopeptide regions, which could form the
5 hydrogen bond with water molecules. The highest free amino and carbonyl groups
6 exposed on film surface could play role in determining the hydrophilicity of film.
7 Hoque et al. stated that carbonyl and amino groups with increasing numbers could
8 form hydrogen bonds with water molecules to a higher degree, thereby increasing the
9 WVP of the resulting film.³⁹

10 Water contact angle values (θ) of ASC and PSC films are shown in Fig. S2. As
11 it is shown in Table 3, contact angle values of ASC and PSC films were $92.5^{\circ} \pm 0.1$
12 and $90.3^{\circ} \pm 0.1$, respectively. The results indicated that ASC film was slightly
13 hydrophobic than PSC film. The higher contact angle value of ASC film was
14 correlated with the lower WVP value. Generally, if the water contact angle is smaller
15 than 90° , the solid surface is considered hydrophilic and if the water contact angle is
16 larger than 90° , the solid surface is considered hydrophobic.⁴⁰

17 Thermal properties expressed as glass transition temperature (T_g), endothermic
18 melting temperature (T_m) and enthalpy (ΔH) of ASC and PSC films are shown in Fig.
19 5. T_g is associated with molecular segmental motion of disordered (amorphous)
20 structure.⁵ From the thermograms of 1st heat scanning (-30°C to 200°C) shown in
21 Fig. 5a, higher T_g was noted in ASC film (52.6°C) in comparison with PSC film (46.3
22 $^{\circ}\text{C}$) related with the plasticised collagen-rich phase. The addition of glycerol as a
23 plasticiser in both ASC and PSC films impeded protein-protein interaction in film
24 network, thereby increasing the mobility of collagen chain. A similar trend was found
25 in the T_m of these collagen films. Endothermic peaks with the T_m at 126.5 and
26 114.8°C were observed for ASC and PSC films, respectively. T_m is associated with
27 the helix-coil transition, disruption of molecular ordered structure (turn or random
28 coils) stabilised by various interactions, and changes from the native state of collagen
29 to denatured state.⁴¹ T_m is also associated with the evaporation of residual, strongly
30 hydrogen bonded water responsible for the stability of the triple helix conformation of
31 collagen macromolecules.⁵ The end result of the thermal denaturation of collagen is
32 random fragmentation of the collagen fibrils. In general, the differences in T_g and T_m
33 between ASC and PSC films were due to the differences in sequence of amino acids
34 as well as the complex interactions determined by the amino acids composition. The

1 decreased T_g and T_m of PSC film was due to the molecular weight lowering caused by
2 pepsin digestion, especially in the telopeptide region. The configuration of protein and
3 the way the inter-junction was developed to form the strong film network were crucial
4 for thermal stability. In addition, a higher enthalpy was also observed for ASC film
5 ($\Delta H = 4.2$ J/g), compared with that of PSC film ($\Delta H = 3.5$ J/g). The weaker film
6 structure had the lower thermal stability, which required a lower enthalpy for
7 destroying the intermolecular interaction. The major factors influencing the thermal
8 stability of collagen films include the content of imino acid, degree of hydroxylation
9 of proline and the content of the glycine-proline-hydroxyproline sequence. From the
10 thermograms of 2nd heat scanning (-30 °C to 300 °C) shown in Fig. 5b, ASC and PSC
11 films showed one-step like transition at the T_m of 233.2°C and 225.6 °C with an
12 enthalpy area (ΔH) of 17.1 J/g and 16.9 J/g, respectively. These endothermic peaks
13 were apparently related with the complete decomposition of triple helical collagen
14 structure caused by the irreversible breakdown of intra- and intermolecular bonds.
15 The higher values of T_m and ΔH observed in the 2nd heating scans were assigned
16 mainly to the breaking of the direct hydrogen bonds between α -chains. For the 2nd
17 heating scan of ASC and PSC film, no T_g was observed since the absorbed water
18 acting as plasticiser might be removed during the 1st heating scan. As a consequence,
19 the interaction between collagen molecules was enhanced which led to the formation
20 of more rigid film network.¹ Additionally, the higher value of ΔH (16.9-17.1 J/g)
21 required for disrupting the film network possibly explained the increase in
22 crystallinity behaviour of collagen films.

23 TGA and DTG curves revealing thermal degradation behaviour of ASC and
24 PSC films are shown in Fig. 6. Their degradation temperatures (T_d) and weight loss
25 (Δw) are presented in Table 4. Three main stages of weight loss were observed in both
26 films. The first stage weight loss of ASC film ($\Delta w_1 = 5.0$ %) and PSC film ($\Delta w_1 = 5.8$
27 %) was observed at the onset temperature (T_{d1}) of 54.3 °C and 40.6 °C, mostly
28 associated with the continuous loss of free water adsorbed in the film. The second
29 stage weight loss of ASC film ($\Delta w_2 = 27.9$ %) appeared at the onset temperature of
30 220.1 °C (T_{d2}), while PSC film showed weight loss ($\Delta w_2 = 37.0$ %) at the onset
31 temperature (T_{d2}) of 168.9 °C. This change was mostly associated with the loss of
32 glycerol compound (plasticiser) and smaller size protein fraction, as well as
33 structurally bound water. The results indicated that ASC film had higher thermal
34 stability compared to the PSC film, as evidenced by the higher T_{d2} . The third stage of

1 weight loss of ASC film ($\Delta w_3 = 36.2\%$) and PSC film ($\Delta w_3 = 42.9\%$) was observed
2 approximately at onset temperature (T_{d3}) of $355.0\text{ }^\circ\text{C}$ and $331.7\text{ }^\circ\text{C}$, respectively,
3 mostly associated with the loss of high molecular weight protein fractions. An
4 enhanced thermal stability of ASC film was attributed to the interaction between
5 collagen chains and higher imino acid content, thereby yielding the stronger film
6 network, thus leading to the higher heat resistance of the resulting film, compared
7 with PSC film. Additionally, all films had residual mass (representing char content) at
8 $600\text{ }^\circ\text{C}$ in the range of $14.3\text{--}30.9\%$. Slight variation in char content was most likely
9 due to different composition and domain or cross-links in collagen structure.

10 SEM micrographs of the surface (A) and cryo-fractured cross-section (B) of
11 ASC and PSC films are shown in Fig. 7. ASC had the compact, smooth and
12 homogeneous surface without layering and cracking phenomenon, indicating an
13 ordered film matrix. This was accompanied with the better mechanical properties of
14 ASC film. PSC film had slightly irregular and coarser surface, and micro-fibrous
15 structure (characteristics of collagen fibrils), due to entanglement of different chains
16 via covalent and non-covalent bonding, enhancing the roughness and discontinuity of
17 film surface. The reduced continuity and lack of cohesive structure integrity of PSC
18 film network therefore lowered the strength of film. These differences in
19 microstructure of ASC and PSC films were caused by the varying arrangements of
20 protein molecules during film formation.³⁷ Moreover, non-porous, smooth and
21 compact cross-section was noticeable in both ASC and PSC films, indicating good
22 structural integrity. The result suggested that both films were stabilised by protein-
23 protein interaction which might possibly led to the enhanced compactness of film
24 network in cross-section.

25 **4. Conclusion**

26 Based on the results, ASC and PSC could be successfully extracted from the
27 skin of starry triggerfish. Higher yield of PSC was extracted as compared to ASC. The
28 extracted collagens had high electrophoretic purity similar to that of type I fish skin
29 collagen containing heterotrimer of two α_1 chains and one α_2 chain without disulphide
30 bond. Both collagens retained the integrated triple helical structure during the
31 extraction process and their isoelectric point (pI) was within acidic range. In addition,
32 the distinct amino acid composition and denaturation temperature were noted in ASC
33 and PSC. ASC exhibited high thermal stability in comparison with PSC, owing to the
34 higher imino acid content. Furthermore, ASC film exhibited better mechanical and

1 thermal properties due to distinctive domains corresponding to the aggregated ordered
2 structures. Higher contact angle (θ) and lower WVP were obtained in ASC film.
3 Moreover, ASC film has smoother and homogenous surface than PSC film, and no
4 obvious signs of phase separation between film components were observed, thereby
5 confirming their potential use as food packaging material. In general, the results
6 indicated the feasibility of using the triggerfish skin as a good alternative source of
7 realistic high-quality collagen for high value applications that could enhance the
8 sustainability of fish processing industries.

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1 **Figure Legends:**

2 **Fig.1.** SDS-PAGE pattern of ASC and PSC from the skin of starry triggerfish under
3 reducing and non-reducing conditions. M: high molecular weight markers, I: type I
4 fish skin collagen, ASC: acid solubilised collagen and PSC: pepsin solubilised
5 collagen.

6 **Fig.2.** DSC thermograms of ASC and PSC from the skin of starry triggerfish
7 dispersed in 0.05 M acetic acid (a) and in deionised water (b). ASC: acid solubilised
8 collagen and PSC: pepsin solubilised collagen.

9 **Fig.3.** FTIR spectra of ASC and PSC from the skin of starry triggerfish. ASC: acid
10 solubilised collagen and PSC: pepsin solubilised collagen.

11 **Fig.4.** Zeta potential of ASC and PSC from the skin of starry triggerfish at different
12 pHs. ASC: acid solubilised collagen and PSC: pepsin solubilised collagen. Bars
13 represent the standard deviation ($n = 3$).

14 **Fig.5.** DSC thermograms of 1st heating scan (a) and 2nd heating scan (b) of ASC and
15 PSC based films prepared by casting technique. ASC: acid solubilised collagen and
16 PSC: pepsin solubilised collagen.

17 **Fig.6.** TGA and DTG curves of ASC and PSC based films prepared by casting
18 technique. ASC: acid solubilised collagen and PSC: pepsin solubilised collagen.

19 **Fig.7.** SEM micrographs of surface (a) and cryo-fractured cross-section (b) of ASC
20 and PSC based films prepared by casting technique. ASC: acid solubilised collagen
21 and PSC: pepsin solubilised collagen.

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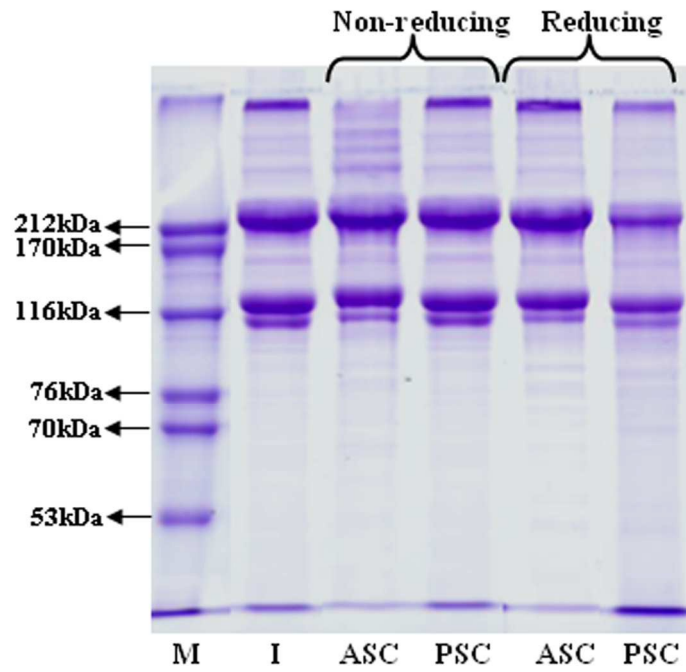


Fig. 1

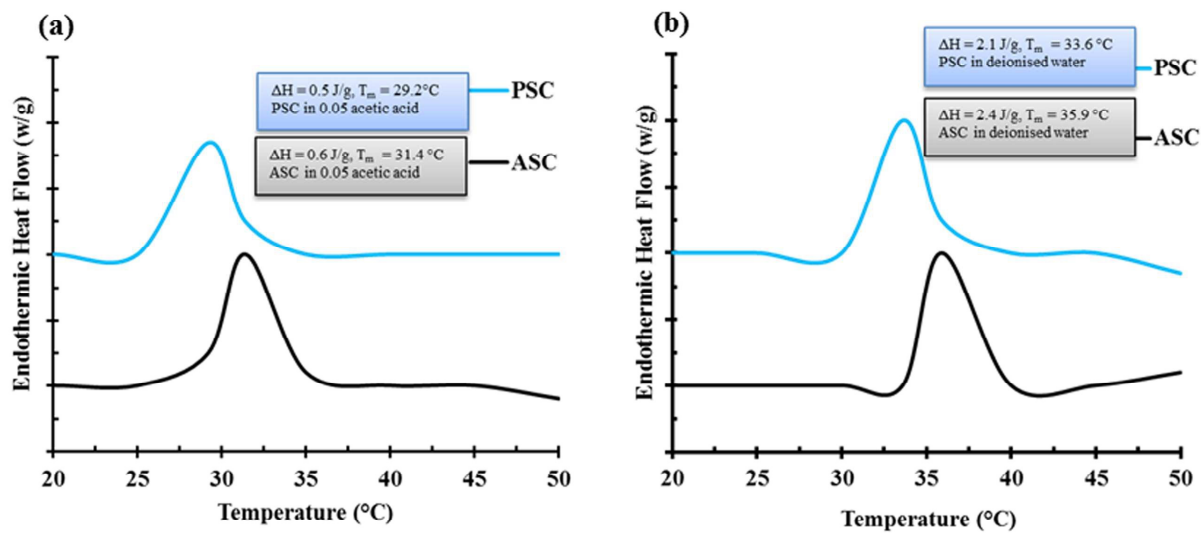


Fig.2

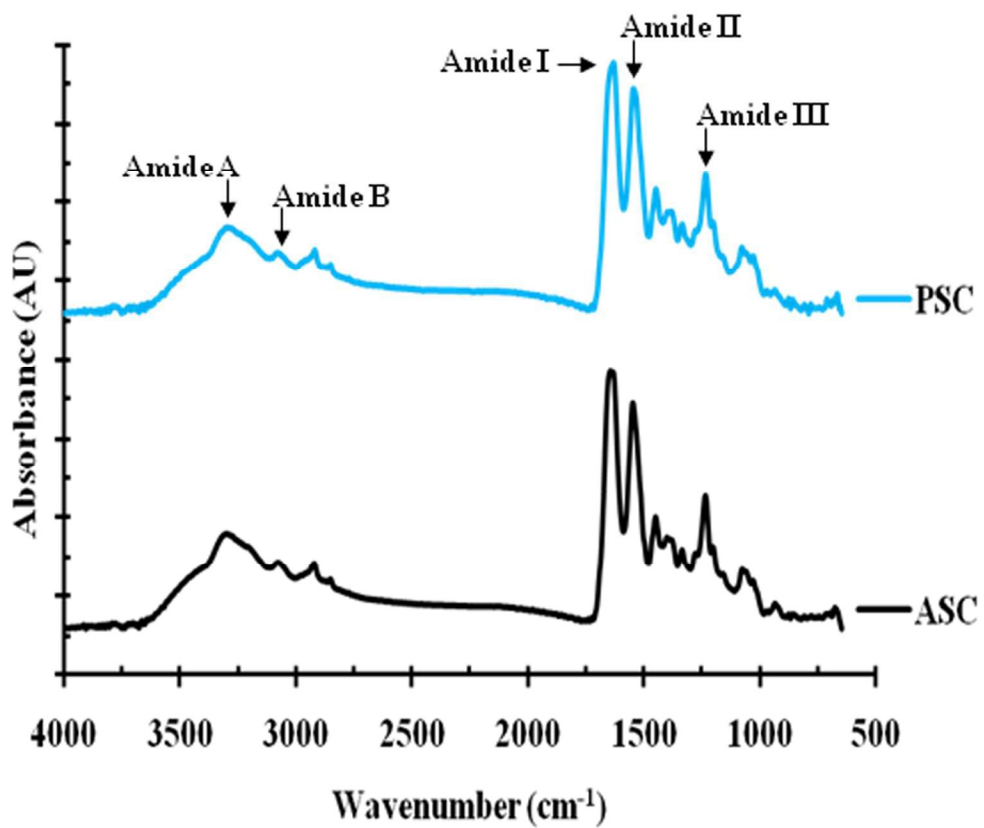


Fig. 3

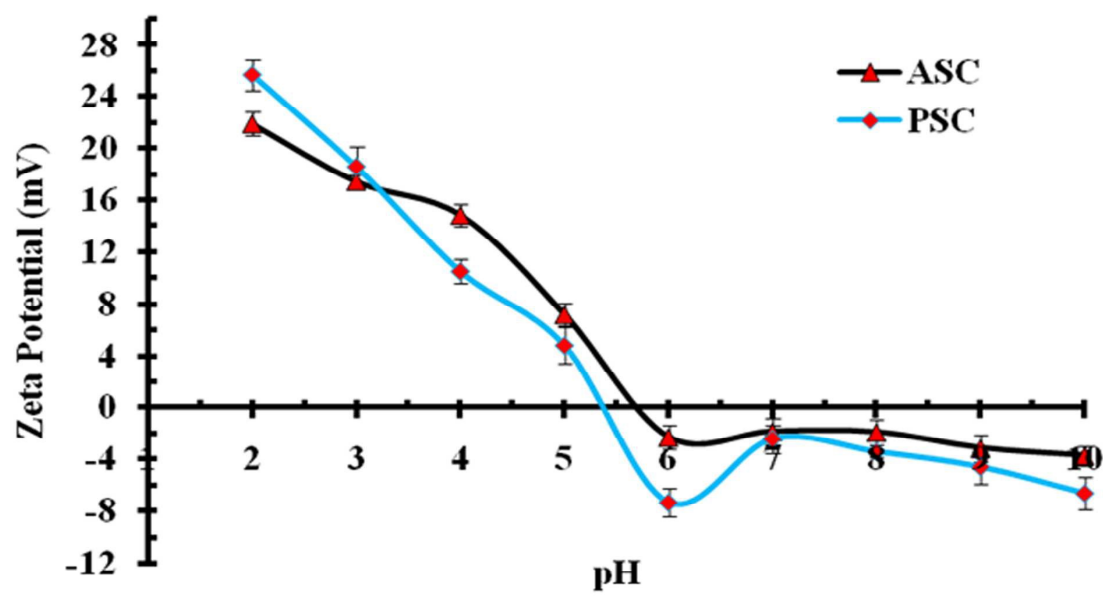


Fig. 4

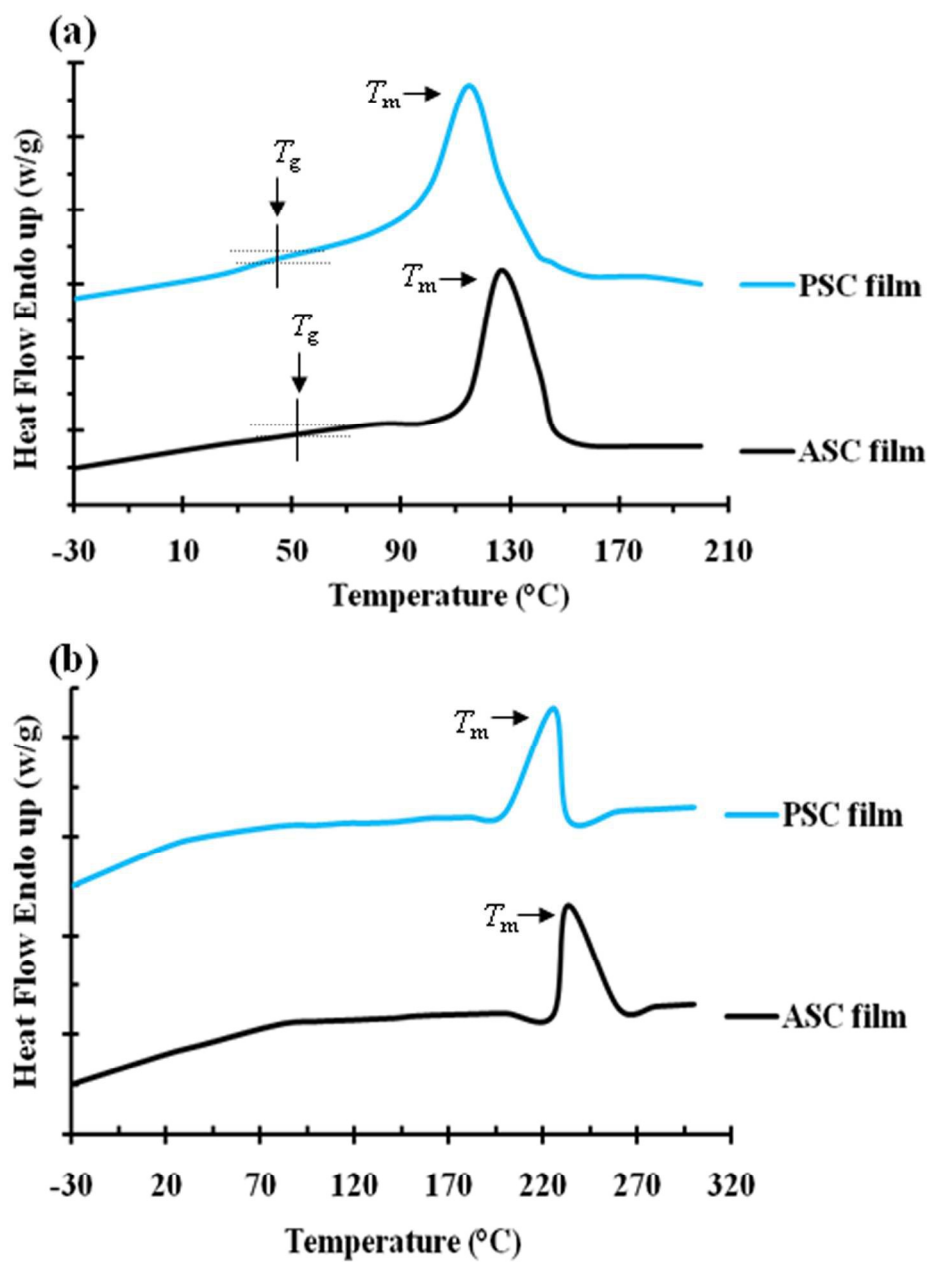


Fig. 5

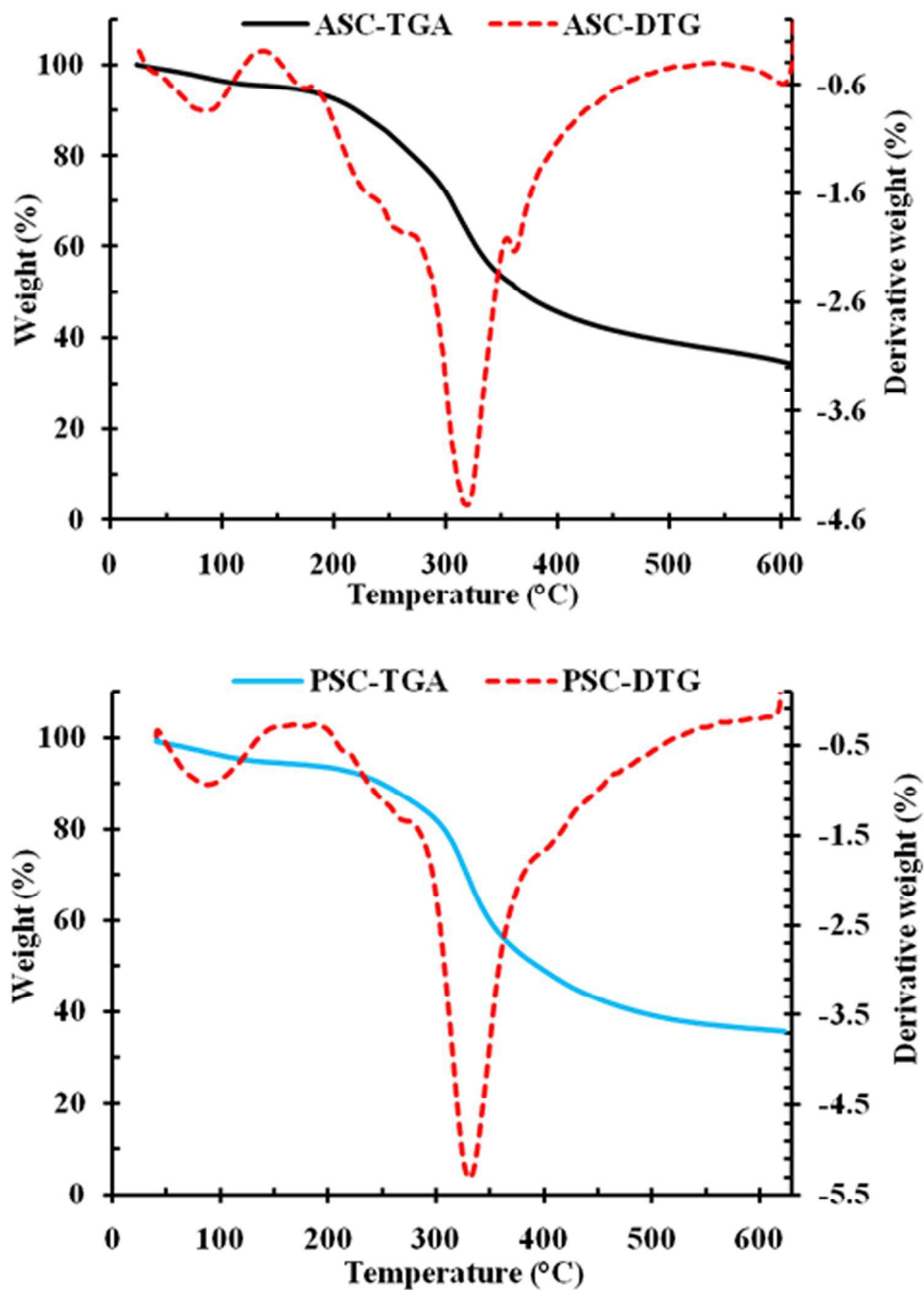


Fig.6

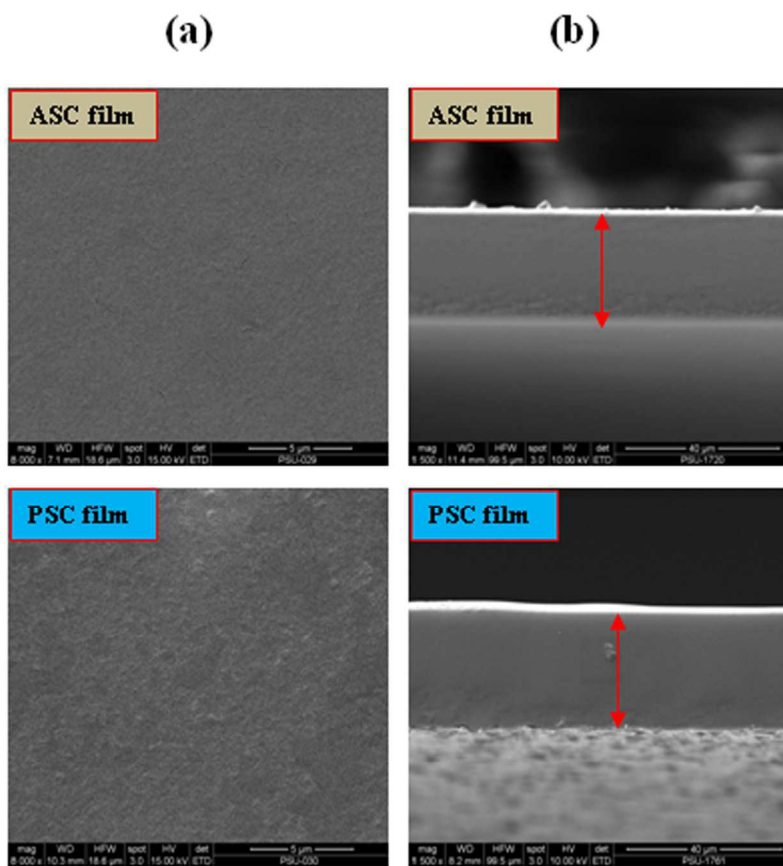


Fig.7

Table 1. Amino acid composition of ASC and PSC extracted from the skin of starry triggerfish (expressed as residues/1000 residues).

Amino acids	ASC[†]	PSC[*]
Aspartic acid/Asparagine	46	50
Threonine	25	26
Serine	35	37
Glutamic acid/Glutamine	73	75
Glycine	322	319
Alanine	144	140
Cysteine	0	0
Valine	18	20
Methionine	13	12
Isoleucine	10	8
Leucine	16	19
Tyrosine	4	3
Phenylalanine	14	12
Hydroxylysine	5	4
Lysine	26	30
Histidine	6	7
Arginine	50	52
Tryptophan	0	0
Hydroxyproline	84	79
Proline	109	107
Imino acid	193	186

[†]ASC: Acid solubilised collagen

^{*}PSC: Pepsin solubilised collagen

Table 2. General peak assignments in the FTIR spectra of ASC and PSC

Assignments	Wavenumber (cm ⁻¹)	
	ASC [†]	PSC [*]
Amide I: C=O stretching	1633.9	1636.1
Amide II: N-H bending	1545.2	1546.9
Amide III: C-H stretching	1236.8	1237.2
Amide A: N-H stretching	3415.9	3433.2
N-H stretching when involved in hydrogen bonding	3293.3	3295.3
Amide B: CH ₃ asymmetric stretching	3078.2	3081.6
Amide B: CH ₂ asymmetric stretching	2910.5	2908.6
CH ₃ symmetric stretching	2837.2	2841.1

[†]ASC: Acid solubilised collagen

^{*}PSC: Pepsin solubilised collagen

Table 3. Mechanical properties and water vapour permeability (WVP) of ASC and PSC films prepared by casting technique

Properties	ASC film	PSC film
Thickness (μm)	28.6 \pm 2.0a	28.8 \pm 3.1a
Tensile strength (MPa)	46.7 \pm 6.5a	34.2 \pm 5.2b
Elongation at break (%)	28.5 \pm 4.4b	39.6 \pm 4.71a
Elastic modulus (MPa)	167.5 \pm 35.8a	88.3 \pm 22.1b
WVP ($\text{g m}^{-1} \text{s}^{-1} \text{Pa}^{-1}$)	4.8 \pm 0.7b	6.6 \pm 0.8a
Contact angle (θ)	92.5 \pm 0.1a	90.3 \pm 0.1b

Values are given as mean \pm SD ($n = 3$).

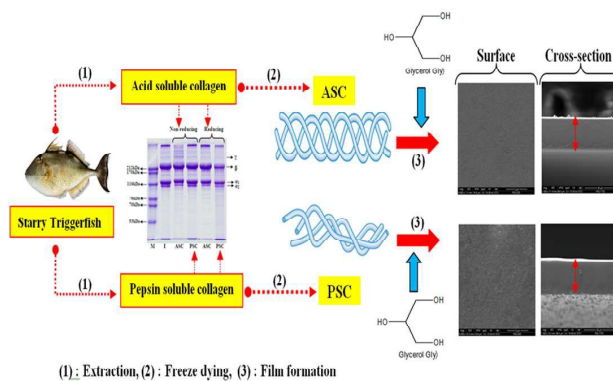
Different letters in the same row indicate significant differences ($P < 0.05$).

Table 4. Thermal degradation temperature (T_d , °C) and weight loss (Δw , %) of ASC and PSC films

Samples	Δ_1		Δ_2		Δ_3		Residues (%)
	$T_{d1\text{ onset}}$ (°C)	Δw_1 (%)	$T_{d2\text{ onset}}$ (°C)	Δw_2 (%)	$T_{d3\text{ onset}}$ (°C)	Δw_3 (%)	
ASC film	54.3	5.0	220.1	27.9	355.0	36.2	30.9
PSC film	40.6	5.8	168.9	37.0	331.7	42.9	14.3

Δ_1 , Δ_2 and Δ_3 denote the first, second and third stage weight loss, respectively, of film during TGA heating scan.

Graphical Abstract



Novel biodegradable collagen films from starry trigger skin were fabricated and characterised for food packaging applications.