



**Chitosan reduces vitamin D bioaccessibility in food emulsions by binding to mixed micelles**

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## 21 **Abstract**

22 Consumption of sufficiently high quantities of dietary fibers has been linked to a range of  
23 health benefits. Recent research, however, has shown that some dietary fibers interfere with lipid  
24 digestion, which may reduce the bioavailability of oil-soluble vitamins and nutraceuticals. For  
25 this reason, we examined the impact of a cationic polysaccharide (chitosan) on the  
26 bioaccessibility of vitamin D using the standardized INFOGEST *in vitro* digestion model. The  
27 vitamin D was encapsulated within an emulsion-based delivery system that contained whey  
28 protein-coated corn oil droplets. Our results showed that chitosan promoted severe droplet  
29 flocculation in the small intestine and reduced the amount of free fatty acids detected using a pH-  
30 stat method. However, a back-titration of the digested sample showed that the lipids were fully  
31 digested at all chitosan levels used (0.1-0.5%), suggesting that chitosan may have bound some of  
32 the free fatty acids released during lipid digestion. The presence of the chitosan decreased the  
33 bioaccessibility of vitamin D by about 37%, but this effect did not depend strongly on chitosan  
34 concentration (0.1-0.5%). It was hypothesized that chitosan bound to the vitamin-loaded mixed  
35 micelles and promoted their precipitation. The knowledge gained in this study might provide  
36 useful insights in designing emulsion-based delivery systems with high vitamin bioaccessibility.

37

38 **Keywords:** chitosan; emulsion; nanoemulsion; vitamin D; bioaccessibility; *in vitro* digestion

39

## 40 **1. Introduction**

41       There has been considerable interest in the food industry in the design of functional foods  
42 and beverages that not only taste good, but also have specific health benefits <sup>1</sup>. A number of  
43 approaches are being utilized to create these healthier versions of processed foods. One approach  
44 is to decrease the levels, or at least reduce the negative effects, of food ingredients that have been  
45 linked to increased health risks, such as fat, sugar, and salt <sup>1</sup>. Another approach is to control the  
46 structural organization of the constituents within foods so as to alter their behavior inside the  
47 gastrointestinal tract (GIT). An example of this approach is to create foods in which the  
48 macronutrients are digested more slowly, thereby inhibiting glucose or lipid spikes in the blood  
49 that may lead to diabetes or heart disease <sup>2,3</sup>. Yet another approach is to fortify foods with  
50 bioactive ingredients that have been linked to beneficial health effects, such as vitamins,  
51 minerals, and nutraceuticals <sup>4,5</sup>. For example, vitamin D is vital for bone health and other critical  
52 physiological functions <sup>6</sup>, but in many countries, some segments of the population are deficient  
53 in this essential micronutrient <sup>7</sup>. Nevertheless, the amount of fortification must be carefully  
54 controlled because excessive vitamin D intake can have adverse health outcomes, such as  
55 gastrointestinal disorders and kidney dysfunction <sup>8,9</sup>. For this reason, the design of food matrices  
56 that can regulate the release and absorption of micronutrients like vitamin D is of great interest to  
57 the modern food industry <sup>10</sup>.

58       The purpose of the current study was to examine the impact of a dietary fiber (chitosan) on  
59 the bioavailability of vitamin D encapsulated within emulsion-based delivery systems. In  
60 general, dietary fibers are claimed to have a number of potentially beneficial health effects <sup>11-16</sup>.  
61 For instance, they can inhibit glucose absorption, promote satiety, and thereby reduce overall  
62 calorie consumption <sup>17</sup>. Dietary fibers have also been shown to modulate the gut microflora <sup>18</sup>,

63 which is claimed to promote a healthy immune system and reduce the susceptibility to certain  
64 chronic diseases<sup>19</sup>. Dietary fibers have also been shown to modulate the rate and extent of lipid  
65 digestion in emulsion-based delivery systems<sup>20,21</sup>, which may impact the bioavailability of  
66 encapsulated oil-soluble vitamins. Several possible mechanisms have been proposed to account  
67 for the ability of dietary fibers to interfere with lipid digestion: (1) formation of coatings around  
68 oil droplets<sup>22,23</sup>; (2) promotion of droplet flocculation<sup>24</sup>; (3) thickening or gelling of  
69 gastrointestinal fluids<sup>25-27</sup>; (4) binding to critical components in the lipid digestion process, such  
70 as bile salts, free fatty acids<sup>24,28</sup>, digestive enzymes<sup>29</sup>, and, calcium ions<sup>30</sup>; (5) binding to mixed  
71 micelles<sup>31</sup>.

72 The tendency for specific dietary fibers to be involved in these different mechanisms  
73 depends on their molecular and physicochemical characteristics (such as molecular weight,  
74 charge, conformation, and solubility), as well as food matrix properties (such as composition and  
75 structure). We hypothesized that chitosan could impact the bioaccessibility of vitamin D by  
76 interfering with the lipid digestion process by one or more of the above mechanisms.

77 Food-grade chitosan is commonly produced by deacetylation of the chitin found in the  
78 shells of crustaceans, such as crabs and shrimps<sup>32,33</sup>. It is one of the few positively charged  
79 polysaccharides available and so has been widely used as a functional ingredient in foods and  
80 other commercial products for its binding, structure building, film forming, and other functional  
81 attributes<sup>34</sup>. Chitosan is widely used in research studies but does not currently have GRAS  
82 approval for use as a food additive in the US<sup>35</sup>, although it is used in some other countries<sup>36</sup>. The  
83 positive charge on chitosan molecules is due to aliphatic amino groups that are protonated (-  
84 NH<sub>3</sub><sup>+</sup>) under acidic conditions: pK<sub>a</sub> ~ 6-7<sup>37</sup>. The cationic nature of chitosan is believed to be  
85 responsible for many of its physiological effects in the human gut after digestion. Several studies

86 have shown that chitosan can inhibit lipid digestion and reduce the bioaccessibility of  
87 hydrophobic bioactives (such as curcumin)<sup>38,39</sup>. These effects have been attributed to some of  
88 the physicochemical mechanisms listed earlier. For instance, cationic chitosan can form a  
89 protective coating around anionic oil droplets, or promote their flocculation, which inhibits lipid  
90 digestion by reducing the ability of lipase to reach the lipid phase<sup>40</sup>. Besides, chitosan can bind  
91 to anionic free fatty acids and bile salts<sup>31</sup>, which might alter the number of nutraceutical-loaded  
92 mixed micelles available for adsorption in the upper gastrointestinal tract (GIT).

93 The main objective of the current study was therefore to examine the impact of chitosan on  
94 the gastrointestinal fate of vitamin D-loaded oil droplets in emulsion-based delivery systems. In  
95 particular, we used the standardized INFOGEST simulated GIT model to examine the impact of  
96 chitosan on lipid digestion and vitamin bioaccessibility<sup>41</sup>. The results obtained from this study  
97 may facilitate the design of more effective emulsion-based delivery systems for oil-soluble  
98 vitamins and other non-polar bioactive agents.

## 99 **2. Materials and Methods**

### 100 **2.1. Materials**

101 Corn oil (Mazola, ACH Food Companies, Memphis, TN, USA) was obtained from a  
102 supermarket. Whey protein isolate (WPI) was provided by Agropur Inc (Eden Prairie, MN).  
103 Chitosan (Chitoclear cg 800, degree of deacetylation >75%, viscosity 600-1200 mPa·s) was  
104 provided by Primex ehf. (Siglufjordur, Iceland). Vitamin D<sub>3</sub> (1,0 Mill. I.U./g) was supplied by  
105 BASF (Ludwigshafen, Germany). Porcine gastric mucin, pepsin from porcine gastric mucosa  
106 (250 units/mg), pancreatin from porcine pancreas, porcine lipase (100-400 units/mg), porcine  
107 bile extract, and bile acid assay kit were purchased from the Sigma-Aldrich Company (St. Louis,  
108 MO, USA). Ethyl alcohol (ACS/USP grade) was purchased from Pharmco Products, Inc.

109 (Shelbyville, KY, USA). All other chemicals and reagents (analytical grade or higher) were  
110 purchased from either Sigma-Aldrich or Fisher Scientific (Pittsburgh, PA, USA). Double  
111 distilled water was produced by a laboratory water-purification system (Nanopure Infinity,  
112 Barnstaeas International, Dubuque, IA, USA) and was used to prepare all solutions in this study.

## 113 **2.2. Emulsion Preparation**

114 Oil-in-water emulsions were prepared according to a method reported previously <sup>42</sup>. An  
115 aqueous phase was prepared by dispersing powdered WPI into buffer solution (5 mM phosphate,  
116 pH 7.0) and then stirring for at least 3 hours at ambient temperature. The resulting solution was  
117 then stored at 4 °C overnight to completely hydrate the protein. The aqueous phase was filtered  
118 through Whatman qualitative filter paper (Fisher Scientific) before being used to remove any  
119 insoluble matter. The mixture of oil and aqueous phases was first subject to 2-min blending by a  
120 high-speed mixer (M133/1281-0, Biospec Products, Inc., ESGC, Switzerland) at 10,000 rpm, and  
121 then homogenized by passing through a microfluidizer (M110Y, Microfluidics, Newton, MA) at  
122 an operation pressure of 12,000 psi for five times. The final composition of the emulsion was 10  
123 wt% oil phase (2 wt% vitamin D in corn oil) and 90 wt% aqueous phase (1.11 wt% WPI in buffer  
124 solution). This led to a WPI concentration of 1 wt% in the final emulsion.

## 125 **2.3. Chitosan Solution Preparation**

126 A chitosan stock solution was prepared by dissolving 1 wt% chitosan in 0.5% (v/v) acetic  
127 acid solution and then storing at 4 °C overnight to ensure complete hydration. Any insoluble matter  
128 was then removed from this solution by centrifugation (Sorvall Lynx 4000 centrifuge, Thermo  
129 Scientific, Waltham, MA, USA) at 15,000 rpm for 30 min at room temperature.

## 130 **2.4 Emulsion and Chitosan Mixing Method**

131 The chitosan stock solution was diluted with different amounts of 0.5% (v/v) acetic acid  
132 solution to obtain a series of solutions containing different chitosan levels (0%, 0.2%, 0.4%, 0.6%,  
133 0.8% and 1%). These solutions were then mixed with the emulsions at a 1:1 (v/v) ratio by adding  
134 the emulsions dropwise into beakers containing the chitosan solutions. The resulting mixtures were  
135 then stirred for 5 min to ensure they were homogenous and then placed at room temperature  
136 overnight before *in vitro* digestion.

## 137 **2.5. Particle Size Measurements**

138 The particle size distribution of the emulsions was determined using laser diffraction  
139 (Mastersizer 2000, Malvern Instruments Ltd., Malvern, Worcestershire, UK). Samples were  
140 diluted in aqueous solutions and stirred in the dispersion unit at a speed of 1200 rpm to ensure  
141 homogeneity. A 1:1 (v/v) mixture of 0.5% (v/v) acetic acid and phosphate buffer (5 mM, pH 7.0)  
142 was used to dilute the initial samples. Double distilled water with pH adjustment was used for the  
143 mouth (pH 4.8) and stomach (pH 3) samples. Phosphate buffer (5 mM, pH 7.0) was used to dilute  
144 the small intestine samples. The refractive index of the corn oil used in the calculations was 1.472.  
145 Average particle sizes are reported as the surface-weighted mean diameter ( $D_{3,2}$ ). The particle size  
146 of the mixed micelle samples was measured by dynamic light scattering (Zetasizer, Nano ZS series,  
147 Malvern Instruments Ltd.). Phosphate buffer (5 mM, pH 7.0) was used to dilute the samples prior  
148 to analysis to avoid multiple scattering effects.

## 149 **2.6. Particle Surface Potential Measurements**

150 The surface potential ( $\zeta$ -potential) of the particles in the emulsions was measured using  
151 electrophoresis (Zetasizer Nano ZS series, Malvern Instruments Ltd.). Prior to analysis, the  
152 emulsions were diluted with the same solutions used for the laser diffraction measurements.



## 153 **2.7. Confocal Microscopy**

154 Confocal microscopy images were acquired according to a method described previously<sup>43</sup>.  
155 Prior to measurement, the oil phase was dyed with Nile red solution (1 mg Nile red in 1 ml  
156 ethanol) at a ratio of 1:20 (v/v) of dye to oil phase. An aliquot (5  $\mu$ L) of sample was put onto a  
157 microscope slide and then a coverslip was placed on top. The excitation and emission  
158 wavelengths used for Nile red fluorescence analysis were 543 and 605 nm, respectively. The  
159 microscopy images were acquired using a confocal scanning laser microscope (Nikon D-Eclipse  
160 C1 80i, Nikon, Melville, NY, USA) with a 60 $\times$  oil immersion objective lens. The images  
161 obtained were stored and analyzed using the instrument software (NIS-Elements, Nikon,  
162 Melville, NY).

## 163 **2.8. *In vitro* Digestion**

164 The chitosan-emulsion mixtures were passed through a simulated GIT model based on the  
165 standardized INFOGEST method<sup>41</sup>. All solutions were preheated to 37  $^{\circ}$ C prior to use and the  
166 whole GIT procedure was performed at this temperature.

167 *Mouth Phase:* Preheated simulated saliva fluid containing 0.003 g/ml mucin was mixed 1:1  
168 (v/v) with the test samples. The sample was then agitated using a thermally-incubated shaker  
169 (Model 4080, New Brunswick Scientific, New Brunswick, NJ, USA) for 2 min at a shaking  
170 speed of 100 rpm.

171 *Stomach Phase:* The sample from the mouth phase was mixed 1:1 (v/v) with simulated  
172 gastric fluids containing pepsin (2000 U/ml in the final digestion mixture). After adjusting to pH  
173 3.0, the sample was then agitated using the same incubated shaker for 2 h at 100 rpm.

174 *Small Intestine Phase:* The sample from the stomach phase was mixed 1:1 (v/v) with  
175 simulated intestinal fluids containing bile salts (10 mM in the final mixture) and pancreatic

176 enzymes (trypsin activity of 100 U/ml and lipase activity of 2000 U/ml in the final mixture).  
177 After adjusting to pH 7.0, the sample was incubated in a water bath for 2 h with continuous  
178 stirring. During this time, an automatic titration unit (Metrohm, USA, Inc.) was used to maintain  
179 the sample at pH 7.0 by adding alkaline solution (0.25 M NaOH) to titrate the free fatty acids  
180 (FFAs) released. The volume of alkaline solution required to achieve neutralization was recorded  
181 and used to calculate the % of FFAs generated. A back titration to pH 9.0 was also carried out to  
182 determine the total level of free fatty acids released (since some of them may be protonated at  
183 neutral pH). A blank test was carried out using the same composition as the sample being tested  
184 but without the oil to determine the contribution of any non-lipid components to the titration  
185 curves. After 2 h of digestion under small intestine conditions, an aliquot of intestine sample was  
186 centrifuged (Sorvall Lynx 4000 centrifuge, Thermo Scientific, Waltham, MA, USA) at 30,970  
187  $\times g$  (18,000 rpm) for 50 min at 4 °C to separate the micelle phase.

## 188 **2.9. Direct Mixing of Micelle and Chitosan**

189 In one series of experiments, we aimed to determine the impact of adding chitosan to the  
190 mixed micelles formed during digestion. To achieve this, a corn oil-in-water emulsion (5% oil)  
191 was subjected to the above *in vitro* digestion procedure, and then the resulting mixed micelle  
192 phase was collected after centrifugation. Different amounts of chitosan stock solution (1 wt.%)  
193 was then mixed with the mixed micelle samples to reach 0%, 0.0125%, 0.025%, 0.03%,  
194 0.0375%, 0.05% and 0.0625% of chitosan, which is similar to the chitosan levels present in the  
195 chitosan-emulsion mixtures after *in vitro* digestion. The mixed micelle-chitosan mixtures were  
196 then placed in the incubated shaker at 37 °C at 100 rpm for 2 h. Afterwards, the micelle-chitosan  
197 mixtures were centrifuged (Sorvall Lynx 4000 centrifuge) at 30,970  $\times g$  (18,000 rpm) for 30 min  
198 at 4 °C to precipitate the sediment. The vitamin D concentration in the micelle-chitosan mixtures

199 and the supernatants formed after centrifugation were measured using the method described in  
200 the following section. The mass of the sediment was weighed after oven-drying at 37 °C  
201 overnight. The percentage of sediment formed was then calculated using the following  
202 expression:

$$203 \quad \text{Sediment percentage} = 100 \times \frac{m_{\text{sediment}}}{m_{\text{mixture}}}$$

204 Here,  $m_{\text{mixture}}$  and  $m_{\text{sediment}}$  are the mass of the micelle-chitosan mixture and the sediment,  
205 respectively.

## 206 **2.10 Vitamin D Measurement**

207 The extraction and analysis of the vitamin D concentration was carried out using a protocol  
208 based on a previous study<sup>44</sup>. The vitamin D was extracted using an organic solvent consisting of  
209 a 1:1 (v/v) mixture of hexane and ethanol for three times. After being treated using a saturated  
210 sodium chloride solution, the combined extracts were dried under a nitrogen atmosphere and  
211 then re-dissolved in HPLC-grade methanol. After being passed through a 0.45 µm filter to  
212 remove any particles (VWR International, Philadelphia, PA, USA), the samples were analyzed  
213 by HPLC.

214 A reverse phase-HPLC system (Agilent 1100 series, Agilent Technologies, Santa Clara,  
215 CA, USA) with a Zorbax SB-C18 column (4.6×250 mm, 5 µm, Agilent Technologies, Santa  
216 Clara, CA, USA) was used to carry out the separation and analysis. The mobile phase consisted  
217 of a methanol and water mixture (95:5, v/v), and a flow rate of 1 ml/min was used. After  
218 injection of 20 µL of sample, the absorbance of the eluent was monitored at 265 nm.

219 The vitamin bioaccessibility (%) was calculated from measurements of the vitamin D  
220 concentrations in the total digest and in the mixed micelles:

221 
$$\text{Bioaccessibility} = 100 \times \frac{C_{\text{micelle}}}{C_{\text{digest}}}$$

222 Here,  $C_{\text{micelle}}$  and  $C_{\text{digest}}$  are the concentrations of vitamin D in the mixed micelle phase and  
223 in the total digest collected after the simulated small intestine phase, respectively.

## 224 **2.11. Statistical Analysis**

225 The digestion process and all measurements were carried out in triplicate, while the  
226 emulsion preparation was carried out in duplicate. The means and standard deviations were  
227 calculated by combining the data from these different measurements. Depending on the  
228 homogeneity of the variances, either a Duncan test (homogenous) or Dunnett's T3 test  
229 (inhomogeneous) was used in the analysis of variance (ANOVA) at a confidence level of 95% to  
230 determine the statistical differences among treatments. Statistical calculations were carried out  
231 using commercial software (SPSS, IBM Corp., Armonk, NY, USA).

## 232 **3. Results and Discussion**

### 233 **3.1. Physical and Structural Properties During *In vitro* Gastrointestinal Digestion**

234 Initially, corn oil-in-water emulsions containing different chitosan concentrations were  
235 prepared. These mixtures were then passed through the *in vitro* digestion model to obtain a better  
236 understanding of their potential gastrointestinal fate, especially the impact of the chitosan on  
237 lipid digestion and vitamin bioaccessibility. The particle size, surface charge, and microstructure  
238 of the emulsion-chitosan mixtures were measured in each stage of the GIT model.

239 *Initial:* The emulsion-chitosan mixtures were prepared by adding the corn oil emulsion (in  
240 phosphate buffer, pH 7) drop-by-drop into the chitosan solution (in acetic acid solution, pH 3.7).  
241 The resulting solutions had pH values ranging from 3.9 to 4.6, increasing with decreasing  
242 chitosan concentration. The surface charge of the particles in all of the emulsions was highly

243 positive. The pure emulsion (no chitosan) had a surface charge of +48.8 mV (Fig. 3), because the  
244 final pH was below the isoelectric point of the adsorbed proteins ( $pI \approx 5$ ). The pure emulsion had  
245 a monomodal distribution and a mean particle diameter of 148 nm, which is fairly similar to that  
246 of the original emulsion *i.e.*, 139 nm (Figs. 1 and 2a). The confocal microscopy images showed  
247 that these emulsions contained fine oil droplets that were evenly distributed throughout the  
248 samples (Fig. 4). These results indicate that the pure emulsion was stable under these pH  
249 conditions, which is probably due to the strong electrostatic repulsion between the highly  
250 cationic droplets.

251 In the presence of chitosan, the positive surface potential of the emulsions remained  
252 relatively high and positive (+41.7 to +47.3 mV) with increasing chitosan concentration (0.1-  
253 0.5 %) (Fig. 3). This effect may have been because the chitosan did not bind strongly to the  
254 droplet surfaces under these acidic conditions because both the chitosan and lipid droplets had  
255 strong positive charges, leading to an electrostatic repulsion. In addition, as the pH increased  
256 from 4.1 to 4.6, and therefore moved closer to the isoelectric point of the adsorbed whey  
257 proteins, some of the cationic chitosan molecules could have bound to anionic patches formed on  
258 the protein-coated droplet surfaces<sup>45</sup>. As a result, the net positive charge remained relatively  
259 high. The confocal microscopy images suggest that appreciable droplet flocculation occurred in  
260 the emulsions at all chitosan levels used, which is most likely a result of bridging or depletion  
261 flocculation<sup>45,46</sup>. The extent and nature of flocculation depended on the chitosan concentration.  
262 At low chitosan levels (0.1%), severe droplet flocculation occurred (Fig. 4) and the emulsions  
263 visually separated into a cream layer on top and a serum layer at the bottom (Fig. 5).  
264 Surprisingly, the measured mean particle diameter only increased slightly to 156 nm in the  
265 presence of 0.1% chitosan (Fig. 1), which suggests that either the flocculated droplets were only

266 held together by relatively weak reversible attractive interactions, or that only a small fraction of  
267 the droplets were flocculated.

268 When the chitosan concentration was increased to 0.3%, the flocculated oil droplets  
269 appeared to be more evenly spread (less clumping) and the emulsions showed less phase  
270 separation (Figs 4 and 5). In this case, the mean particle diameter increased significantly ( $p <$   
271 0.05) to 286 nm (Fig. 1) and the particle size distribution became bimodal. These results suggest  
272 that the oil droplets were more strongly aggregated to each other and formed a 3D-network that  
273 was more resistant to gravitational separation. At 0.4 and 0.5% chitosan, there was some  
274 evidence of clumping of the flocculated droplets, a steep increase in mean particle diameter, and  
275 a shift in the particle size distribution to higher values (Figs. 1 to 3). These effects may have been  
276 due to increasing bridging and/or depletion flocculation as the chitosan level was increased <sup>46,47</sup>.

277 *Mouth:* The physical and structural properties of the samples changed appreciably after  
278 exposure to the oral phase. After mixing with the simulated salivary fluids, the solutions had pH  
279 values from 4.5 to 5.1. The pure emulsion was unstable under mouth conditions with visible  
280 phase separation, an increase in mean particle diameter ( $D_{3,2} = 9.7 \mu\text{m}$ ), and evidence of floc  
281 formation in the microscopy images (Figs. 1, 4 and 5). This effect may have been because of the  
282 relatively low surface potential ( $\zeta = -0.17 \text{ mV}$ ) of the protein-coated oil droplets near the  
283 isoelectric point of the proteins, which led to a relatively weak electrostatic repulsion between  
284 them.

285 The addition of chitosan improved the stability of the emulsions by an amount that  
286 depended on the concentration used (Fig. 5). As the chitosan level was increased, the mean  
287 particle diameter decreased reaching a value of 331 nm at 0.3% chitosan level (Fig. 1), but a  
288 broad particle size distribution was observed (Fig. 2d). This effect may have been due to the

289 ability of the chitosan molecules to adsorb to the surfaces of the protein-coated oil droplets,  
290 increase their positive charge, and strengthen the electrostatic repulsion between them. This  
291 hypothesis is supported by the observation that the  $\zeta$ -potential of the droplets became  
292 increasingly positive as the chitosan level increased (Fig. 3). Nevertheless, the confocal  
293 microscopy images showed that the protein-coated oil droplets were still highly flocculated in  
294 the presence of chitosan (Fig. 4). These results suggest that there were still some bridging and/or  
295 depletion flocculation at high polysaccharide levels, but the flocs formed were weak enough to  
296 dissociate when the samples were diluted for the particle size measurements.

297 *Stomach:* In the stomach phase, the emulsion samples were exposed to highly acidic  
298 conditions (pH 3), as well as digestive enzymes (pepsin). All the samples were highly unstable to  
299 droplet aggregation (Figs. 1, 2, and 4) and phase separation (Fig. 5). The mean particle diameter  
300 was relatively high ( $> 7 \mu\text{m}$ ) at all chitosan levels (0 to 0.5%) (Fig. 1). Droplet aggregation was  
301 probably a result of changes in electrostatic interactions, bridging flocculation, and protein  
302 digestion. After exposure to the stomach phase, the  $\zeta$ -potential of the particles was positive in all  
303 the samples, increasing from +5.3 mV in the absence of chitosan to +23.2 mV in the presence of  
304 0.5%, chitosan. One might have expected that this large increase in particle charge would have  
305 led to stronger electrostatic repulsion between the oil droplets, but there was not a major change  
306 in particle aggregation with increasing chitosan levels. This phenomenon might be explained by  
307 a number of factors: (1) the change in pH caused partial or full displacement of the chitosan from  
308 the oil droplet surfaces; (2) the dilution of the samples reduced the amount of chitosan coating  
309 the droplet surfaces, thereby promoting bridging; (3) the digestion of the adsorbed proteins by  
310 pepsin reduced the stabilizing effects of the emulsifier; and (4) the higher ionic strength of the  
311 gastric fluids screened the electrostatic repulsion<sup>48</sup>.

312 *SI-Initial:* Since pH is known to play a critical role in determining the physical and  
313 structural properties of protein-stabilized emulsions<sup>49</sup>, we measured the properties of the  
314 samples at the beginning of the small intestine phase before adding the digestive enzymes and  
315 bile salts. This was accomplished by adjusting the sample collected after the stomach phase to  
316 pH 7. The properties of all the samples changed appreciably when the pH was increased. The  
317 average mean particle diameter of the pure emulsion decreased steeply to 281 nm (Fig. 1), and  
318 populations of both small and large particles were seen in the particle size distribution (Fig. 2a).  
319 This result matched with the confocal microscopy images, which showed most of the flocs were  
320 dispersed into small oil droplets with only a few large droplets (Fig. 4). The breakdown of the  
321 flocs can mainly be attributed to an increase in the electrostatic repulsion between the droplets  
322 due to an increase in their surface potential to a high negative value (-37.5 mV) (Fig. 3). The fact  
323 that there were large individual oil droplets present suggests that some coalescence occurred  
324 within the mouth and/or stomach phases. Visual observation of the pure emulsions indicated that  
325 they were stable at the beginning of the small intestine phase (Fig 5). Overall, these results  
326 suggest that most of the oil droplets stayed intact and were evenly dispersed throughout the  
327 samples.

328 In contrast, the emulsions containing chitosan became more unstable when they were  
329 moved from the stomach phase to the initial part of the small intestine phase. Visual observations  
330 showed that all these emulsions underwent phase separation, with a white cream layer on top and  
331 a clear serum layer at the bottom (Fig. 5). The addition of chitosan significantly ( $p < 0.05$ )  
332 increased the mean particle diameter of these samples, with the effect becoming more  
333 pronounced with increasing chitosan concentration (Fig. 1). Extensive droplet flocculation was  
334 also observed in the confocal microscopy images (Fig. 4). This effect can be attributed to at least



335 two phenomena. First, chitosan is slightly positively charged at pH 7 whereas the protein-coated  
336 droplets are strongly negatively charged, thereby promoting bridging flocculation. Second,  
337 chitosan loses most of its positive charge under neutral conditions ( $pK_a$  around 6.5), which  
338 causes it to precipitate. These two mechanisms are supported by the electrophoresis  
339 measurements, which show that the negative charge on the particles decreased with increasing  
340 chitosan concentration: from -37.5 mV in the absence of chitosan to -2.5 mV in the presence of  
341 0.5% chitosan (Fig. 3). In summary, the presence of the chitosan appears to promote the  
342 aggregation of the oil droplets.

343 *SI-End:* The properties of the samples were measured again after bile salts and digestive  
344 enzymes were added and the samples were then incubated for 2 hours. At the end of the small  
345 intestinal phase, the mean particle diameter of the pure emulsions increased significantly ( $p <$   
346 0.05) to around 970 nm (Fig. 1). This change might be brought about by the digestion of the lipid  
347 droplets and the formation of large colloidal structures like vesicles and insoluble calcium soaps  
348 <sup>50</sup>. The magnitude of the surface potential in the pure emulsion sample increased slightly to -44.0  
349 mV (Fig. 3), which has been attributed to the presence of colloidal particles comprised of anionic  
350 constituents, such as free fatty acids, bile salts, and peptides <sup>50</sup>. The confocal microscopy images  
351 indicated that most of the oil droplets had been digested by the end of the small intestine phase  
352 (Fig. 4).

353 Compared to the beginning of the small intestinal phase, the mean particle diameters of the  
354 samples containing chitosan decreased greatly after the small intestine phase. Even so, the  $D_{3,2}$   
355 value still increased with increasing chitosan concentration: from 0.97  $\mu\text{m}$  in the absence of  
356 chitosan to 3.33  $\mu\text{m}$  in the presence of 0.5% chitosan (Fig. 1). The confocal microscopy images  
357 also indicated that most of the oil droplets were digested at all chitosan concentrations, but that

358 there were slightly more lipid-rich particles remaining at higher chitosan levels (Fig. 4).  
359 Interestingly, these results show that even though the emulsions containing chitosan were highly  
360 flocculated at the beginning of the small intestine phase, most of the oil droplets were still  
361 digested by the end. Unlike at the beginning of the small intestine phase, the surface potential of  
362 the samples containing chitosan was highly negative and did not change much at different  
363 chitosan levels ranging from -32.0 to -40.6 mV. This effect can be attributed to the relatively  
364 high level of anionic components in the small intestine phase, such as free fatty acids and bile  
365 salts. Presumably, these components bound to the positively charged chitosan molecules and  
366 neutralized their charge.

367 The surface potential of the mixed micelles collected after centrifugation of the digest were  
368 also measured (Fig. 4). The  $\zeta$ -potential of the mixed micelle samples were fairly similar to those  
369 of the equivalent whole intestinal samples, suggesting that the mixed micelles dominated the  
370 overall charge characteristics.

### 371 **3.2. Release of Free Fatty Acids During Intestinal Digestion**

372 The release of free fatty acids (FFA) from the emulsions within the small intestine phase  
373 was recorded using a pH stat method by adding increasing volumes of alkaline solution to  
374 maintain a neutral pH. The FFA-time release profiles are shown in Fig. 6a and the final FFA  
375 values are shown in Fig. 6b. The measured FFA values increased rapidly during the first few  
376 minutes of digestion but then increased more steadily at longer times. In general, the level of  
377 FFAs detected in the pure emulsions was higher than that detected in the emulsions containing  
378 chitosan. For instance, the final FFA value was around 65% for the pure emulsion, whereas it  
379 was around 47% to 53% for the emulsions containing chitosan. These results appear to be  
380 inconsistent with the confocal microscopy images, which showed that most of the oil droplets

381 had been fully digested by the end of the small intestine phase (Fig. 4). This apparent  
382 inconsistency might be due to the fact that a fraction of the FFAs were not ionized at pH 7 and so  
383 could not be titrated. To test this hypothesis, a back titration to pH 9 was carried out, since this  
384 protocol has previously been shown to be capable of measuring all of the FFAs present<sup>51</sup>. After  
385 back titration, the final FFA values of all the samples (102% to 115%) suggested that full lipid  
386 digestion had occurred. This result suggests that chitosan did not inhibit lipid digestion, but  
387 instead altered the amount of FFAs that could be detected by the pH stat method at pH 7.  
388 Presumably, the cationic chitosan molecules bind to any anionic free fatty acids at neutral pH  
389 thereby reducing the number of titratable protons (H<sup>+</sup>) released.

390 In previous studies, it has been suggested that chitosan can inhibit lipid digestion through a  
391 number of mechanisms, including inducing oil droplet flocculation, forming coatings around oil  
392 droplets, or binding to digestive components (like enzymes or bile salts)<sup>52</sup>. Our current results  
393 suggest that some of these earlier observations might have been because a back-titration step was  
394 not carried out. As a result, not all of the FFAs released during lipid digestion were measured. In  
395 addition, most of the earlier studies were carried out using an *in vitro* digestion method that  
396 contained different levels of digestive enzymes, calcium, and other components to the  
397 standardized INFOGEST digestion method used in the current study<sup>41</sup>. In particular, the  
398 INFOGEST method uses higher levels of pancreatic enzymes and lower levels of calcium, which  
399 may alter the rate and extent of lipid digestion. Having said this, our results still show that  
400 chitosan does interfere with the lipid digestion process under neutral conditions.

#### 401 **3.4. Vitamin Bioaccessibility**

402 The vitamin D bioaccessibility in the emulsion-chitosan mixtures was measured after they  
403 had been passed through the entire *in vitro* simulated digestion model (Fig. 7). The pure

404 emulsion had the highest bioaccessibility (68.5%), which is quite similar to the value published  
405 previously (75.2%) for a fairly similar system<sup>44</sup>. The addition of chitosan significantly ( $p < 0.05$ )  
406 reduced the bioaccessibility of the vitamin in the emulsion (37.5% to 47.0%), but the decrease  
407 did not depend strongly on chitosan concentration. There have been few previous studies on the  
408 impact of chitosan on the bioaccessibility of lipophilic bioactives. One study showed that  
409 chitosan enhanced the bioaccessibility of curcumin<sup>24</sup>, while others showed that it reduced the  
410 bioaccessibility of EGCG and carotenoids<sup>52,53</sup>. These differences might be due to differences in  
411 the bioactive agents, food matrices, and *in vitro* digestion models used by different researchers.

412 In general, the bioaccessibility of oil-soluble vitamins in emulsion-based delivery systems is  
413 governed by two processes: (1) their release from the oil droplets due to digestion of the  
414 triglycerides; (2) their solubilization within the mixed micelles. Several previous studies have  
415 suggested that there is a relationship between the extent of lipid digestion and the bioaccessibility  
416 of hydrophobic bioactives<sup>24,38,52</sup>. As shown by Figs. 4 and 6, however, the majority of the oil  
417 phase was fully digested by the enzymes in this study, so all of the vitamin D should have been  
418 released from the oil droplets. Thus, the decrease in vitamin bioaccessibility observed in the  
419 presence of chitosan was probably not due to its impact on lipid digestion. Instead, we  
420 hypothesized that it was related to the micellization process. This process may be altered through  
421 a number of physicochemical mechanisms: (1) modification of the properties of the mixed  
422 micelles formed, such as the size of their hydrophobic domains<sup>42</sup>; (2) reduction of the total  
423 amount of mixed micelles formed during digestion<sup>54</sup>; and, (3) precipitation of some of the mixed  
424 micelles<sup>55</sup>. In this study, we believe that the cationic chitosan molecules bound to the anionic  
425 vitamin-loaded mixed micelles, which led to the formation of large insoluble aggregates. These  
426 aggregates would be removed from the digest during the centrifugation process and so would not

427 be detected as part of the mixed micelle phase. This hypothesis is supported by visual  
428 observations of the samples, which showed that an increasing amount of sediment was formed at  
429 the bottom of the tubes as the chitosan concentration was increased (Fig. 5). It should be noted,  
430 however, that these precipitated mixed micelles might be liberated when the chitosan is digested  
431 by the gut microbiota in the colon, and so the vitamin may be released and become bioaccessible  
432 again. This might be a good strategy for controlling the release of vitamin D in the human body,  
433 but further *in vivo* studies are needed to test this.

### 434 **3.5. Interaction Between Micelle and Chitosan**

435 Finally, we carried out an additional experiment to examine the potential interactions  
436 between chitosan and mixed micelles. In this case, chitosan was directly mixed with the mixed  
437 micelle phase formed by digestion of a pure emulsion sample. In the absence of chitosan, the  
438 mean particle diameter of the mixed micelle solution was 218 nm (Fig 8a), which is higher than  
439 that reported for simple micelles (< 10 nm). This was probably because a variety of other  
440 colloidal structures were formed during digestion under fed state conditions, including vesicles,  
441 calcium soaps, and protein aggregates<sup>56,57</sup>. The addition of 0% chitosan solution (just acetic acid  
442 solution), significantly ( $p < 0.05$ ) increased the mean particle size of the mixed micelles to 380  
443 nm. It is possible that the acetic acid changed the ionic equilibration of the free fatty acids  
444 thereby altering the mixed micelle structure. The addition of 0.1 to 0.5% chitosan solutions  
445 reduced the mean particle size, which was similar to that of the pure micelle samples.  
446 Interestingly, the chitosan level did not appear to alter the particle size.

447 We hypothesize that the cationic chitosan bound to some of the anionic mixed micelles and  
448 caused them to precipitate. As a result, only the properties of the mixed micelles remaining in the  
449 aqueous phase would be measured by the dynamic light scattering instrument. This hypothesis

450 was supported by measurements of the percentage of sediment formed, with the amount  
451 increasing from 0.09% at 0% chitosan to 0.4% at 0.5% chitosan (Fig. 8b). This hypothesis is also  
452 supported by the surface potential measurements, which showed that the colloidal particles in the  
453 mixed micelle phase were strongly negatively charged at all chitosan levels (Fig 8c). Any mixed  
454 micelles that bind to the chitosan are neutralized and precipitate, and are therefore not measured  
455 by the  $\zeta$ -potential instrument.

456 The sedimentation of the mixed micelles in the presence of chitosan also influenced the  
457 location of the vitamin D in the system (Fig. 8d). The addition of chitosan significantly ( $p <$   
458 0.05) reduced the amount of vitamin D in the supernatant phase from 93.3% at 0% chitosan to  
459 65.9% at 0.1% chitosan (Fig 8d). Further addition of chitosan led to a further slight decrease in  
460 the percentage of vitamin D in the supernatant phase, reaching 63.3%. These results therefore  
461 support the bioaccessibility data discussed above. They suggest that chitosan binds to the  
462 vitamin-D loaded mixed micelles causing them to sediment, thereby reducing their  
463 bioaccessibility.

#### 464 **4. Conclusions**

465 In this study, the impact of chitosan addition (0-0.5%) on the gastrointestinal fate of  
466 vitamin-loaded oil-in-water emulsions was examined. In particular, the effects of chitosan on the  
467 extent of lipid digestion and the bioaccessibility of vitamin D<sub>3</sub> were investigated. The recently  
468 updated standardized INFOGEST protocol was used to simulate the conditions in the upper  
469 regions of the human gastrointestinal tract. Chitosan induced severe droplet flocculation in the  
470 small intestine phase but this did not reduce the total amount of free fatty acids released by the  
471 end of digestion. Indeed, the oil droplets in all the emulsions were fully digested, regardless of  
472 the amount of chitosan present. It is important to note that a fraction of the free fatty acids

473 released were not completely ionized under neutral pH conditions, and so a back titration was  
474 required to measure the total amount of free fatty acids released. Comparison of the results with  
475 and without the back-titration suggested that chitosan altered the ionization state of the free fatty  
476 acids. The presence of chitosan (0.1 to 0.5%) decreased the bioaccessibility of vitamin D<sub>3</sub> by  
477 about 40% when compared to the samples containing no chitosan, with the chitosan level used  
478 not having a major effect. As the triglycerides in all the samples were fully digested, we  
479 attribute the reduction in vitamin bioaccessibility to the ability of chitosan to modulate the  
480 micellization process. Cationic chitosan molecules bind to anionic vitamin-loaded mixed  
481 micelles, leading to the formation of insoluble precipitates that are removed from the mixed  
482 micelle phase. Our results therefore suggest that incorporating chitosan into foods as a functional  
483 ingredient could have a negative impact on vitamin bioaccessibility. However, *in vivo*  
484 experiments are required to determine whether the same effect occurs under more realistic  
485 gastrointestinal conditions.

486

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491

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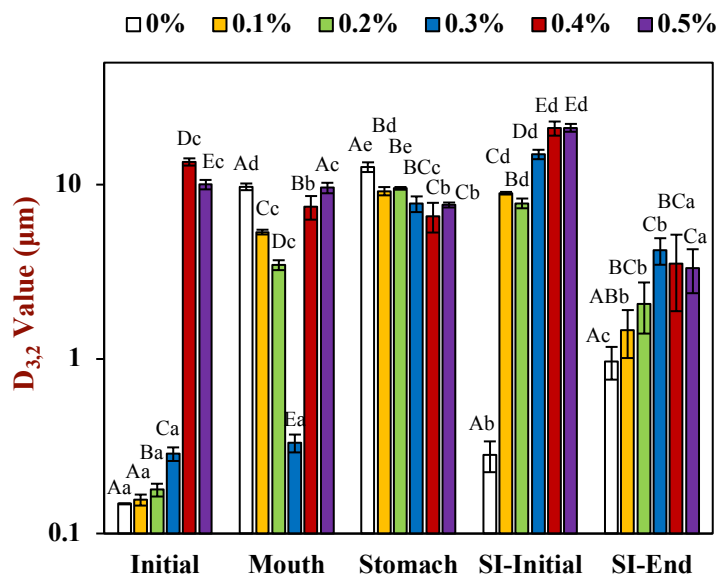


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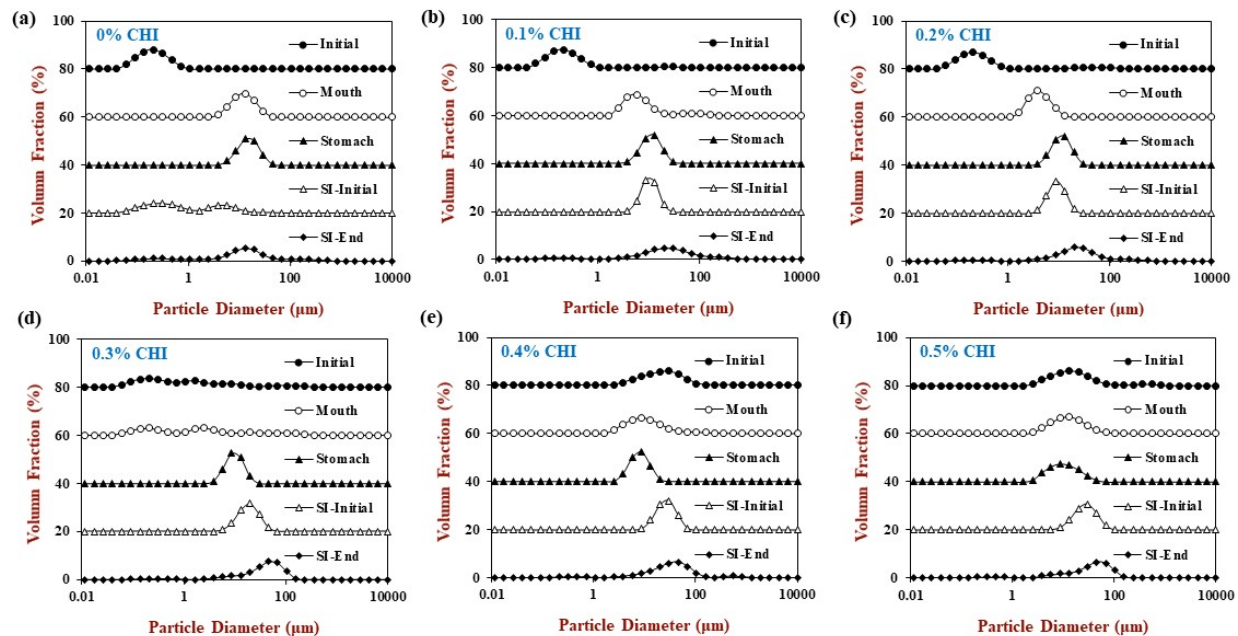


691

692 **Fig 1.** The effect of different chitosan concentrations on the surface-weighted mean particle  
 693 diameter ( $D_{3,2}$ ) of the corn oil in water emulsion during stimulated gastrointestinal tract.

694 Significant difference was labeled by different capital letters (A, B, C) for different chitosan  
 695 concentrations (same phase), whereas lower-case letters (a, b, c) for different phases (same  
 696 chitosan concentration). Abbreviation: small intestine (SI).

697

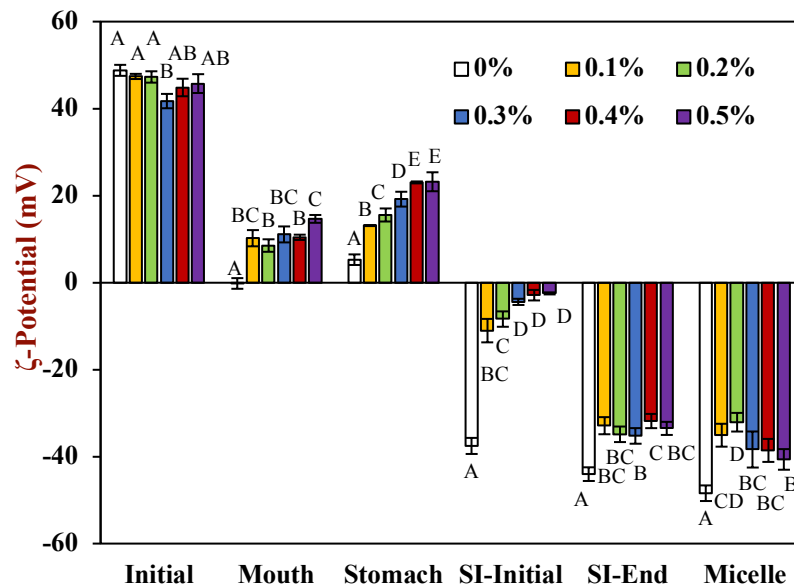


698

699 **Fig 2.** The effect of different chitosan concentrations on the particle size distribution of the corn  
 700 oil in water emulsion during stimulated gastrointestinal tract. Abbreviation: small intestine (SI).

701 Note: the volume fraction was stacked up the y-axis for comparison.

702



703

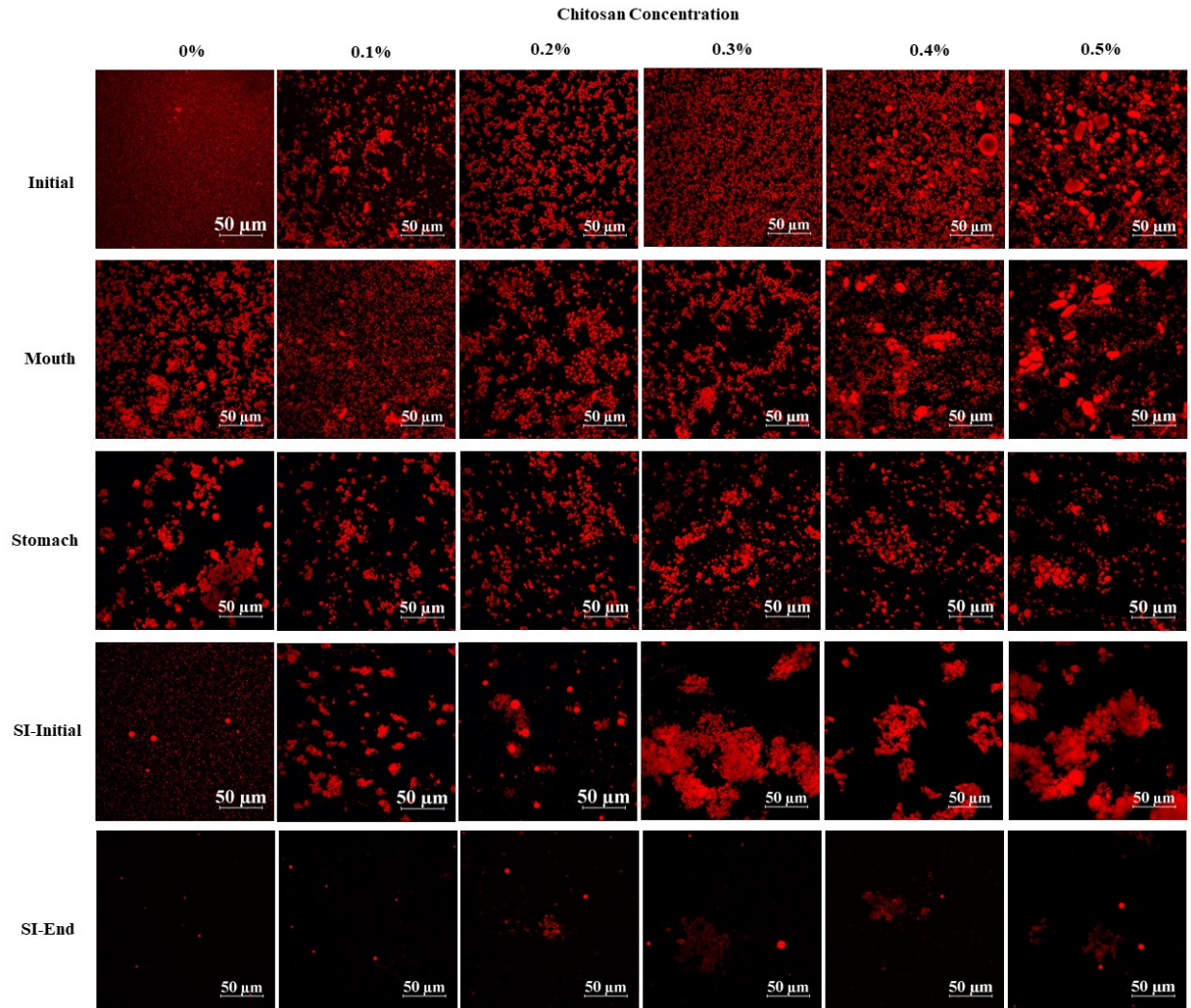
704 Fig 3. The effect of different chitosan concentrations on the  $\zeta$ -potential of the corn oil in water

705 emulsion during stimulated gastrointestinal tract. Capital letters (A, B, C) were used for

706 distinguish significant difference of samples with different chitosan concentration (same phase).

707 Abbreviation: small intestine (SI).

708



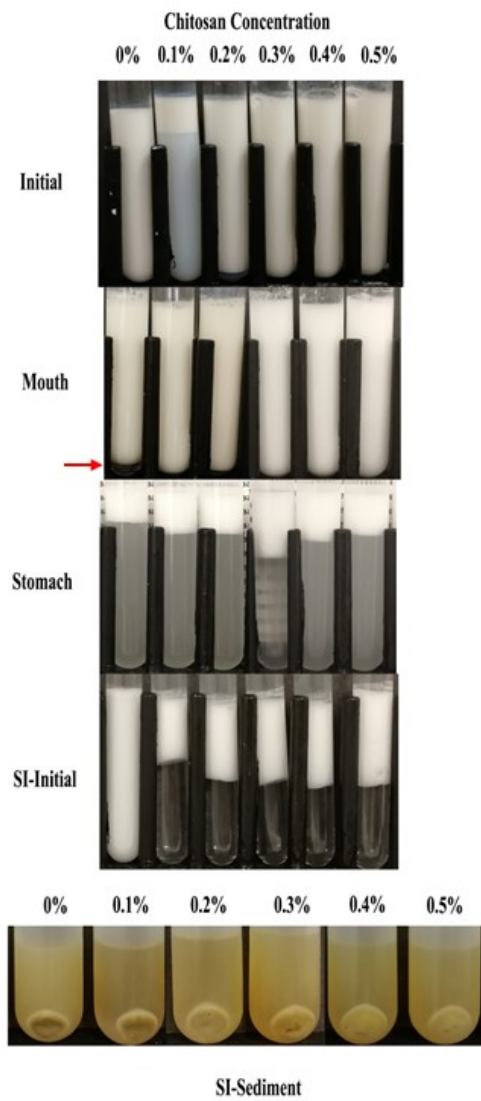
709

710 **Fig 4.** The effect of different chitosan concentrations on the confocal microscopy of the corn oil

711 in water emulsion during stimulated gastrointestinal tract. Abbreviation: small intestine (SI).

712

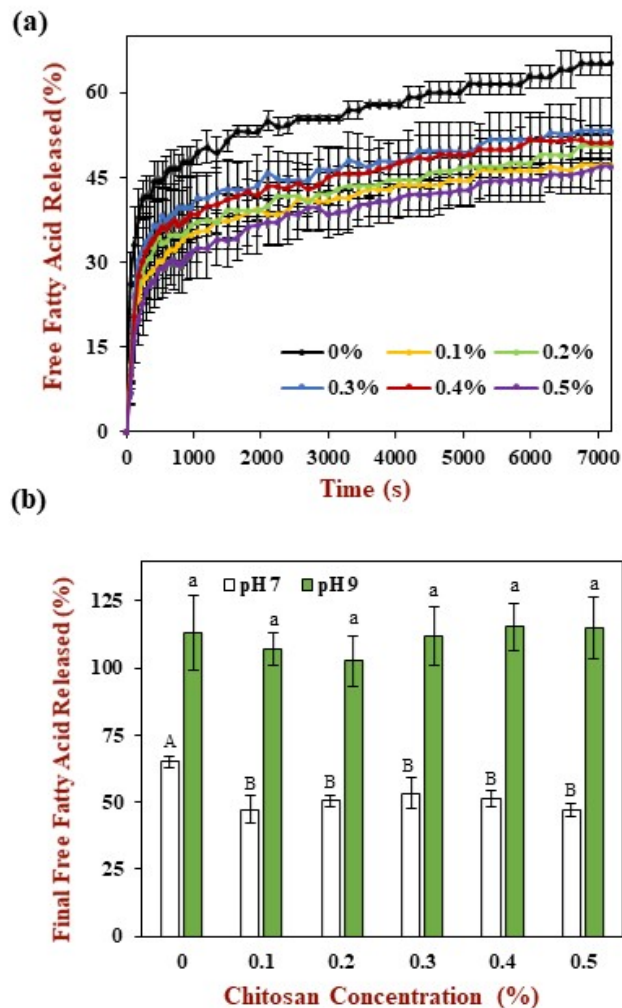




713

714 **Fig 5.** Appearance of emulsions containing different chitosan concentrations at different715 digestive stages. *Abbreviation:* SI-initial = the initial stages of the small intestine phase.

716



717

718 **Fig 6.** Impact of chitosan concentration on the release of free fatty acids (FFA) from corn oil-in-

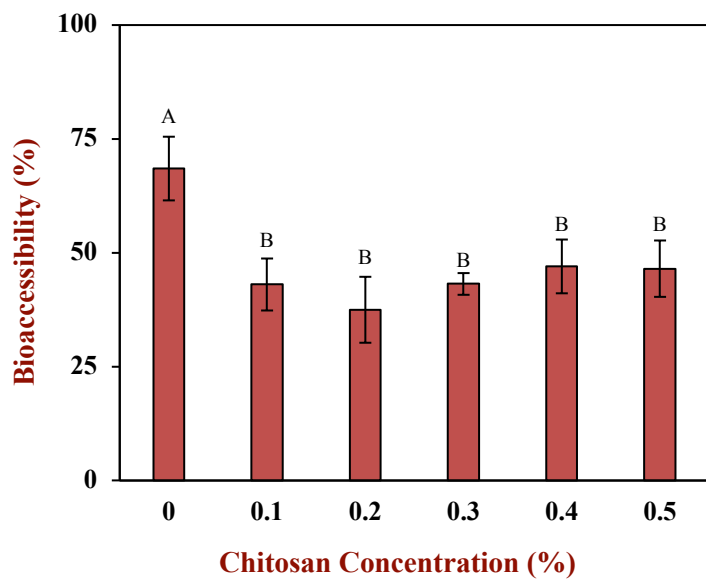
719 water emulsions during simulated digestion. (a) FFA profile at pH 7, (b) final FFA value at pH 7

720 and pH 9. Capital (A, B, C) and lower-case (a, b, c) letters were used to designate significant

721 difference among different chitosan concentrations for final FFA value at pH 7 and pH 9

722 respectively.

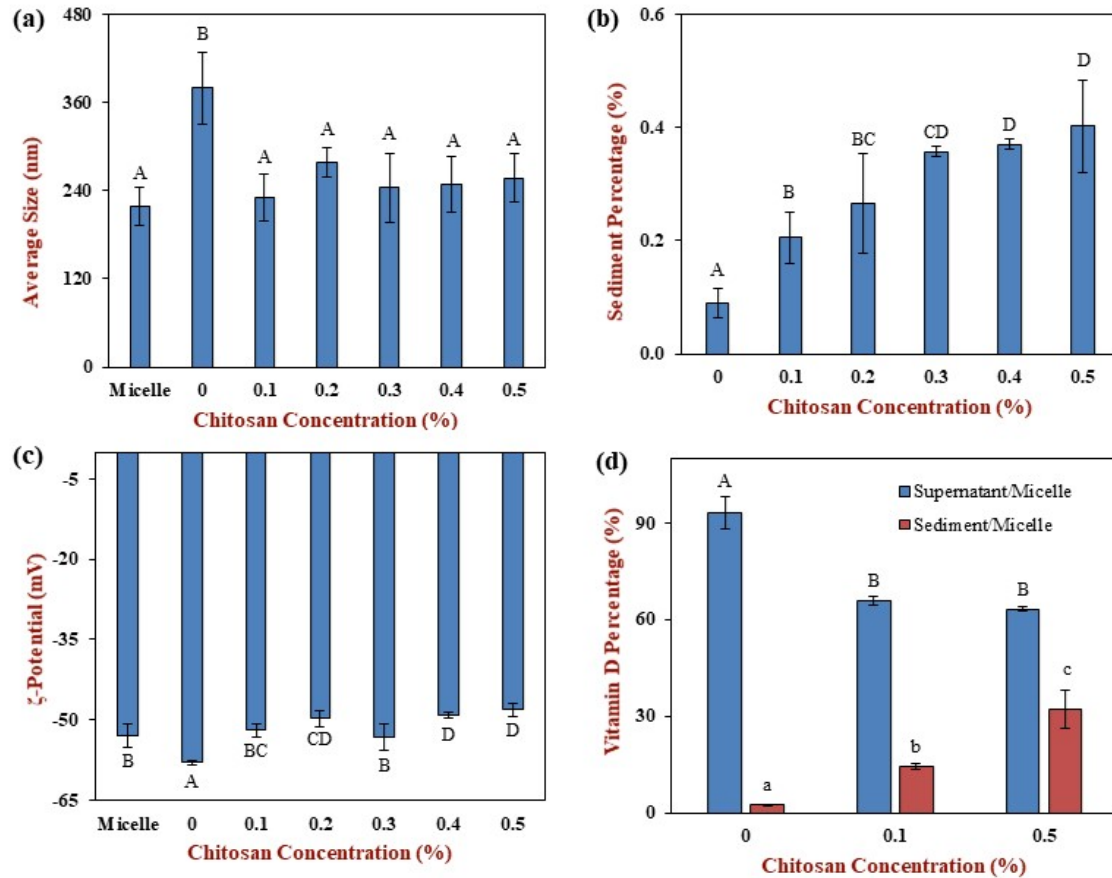
723



724

725 Fig 7. The effect of different chitosan concentrations on the vitamin D bioaccessibility of the  
726 corn oil in water emulsion during stimulated gastrointestinal tract. Samples with significant  
727 difference were labeled with different capital letters (A, B, C).

728



729

730 Fig 8. The effect of different chitosan concentrations on the physical properties and vitamin D

731 distribution of mixed micelles prepared from corn oil-in-water emulsions after exposure to the

732 simulated gastrointestinal tract: (a) mean particle diameter; (b) percentage of sediment formed;

733 (c)  $\zeta$ -potential; (d) vitamin D percentage in supernatant or sediment. Samples with significant

734 differences were labeled with different capital letters (A, B, C), whereas samples with different

735 lower-case letters (a, b, c) were used for vitamin D percentage of sediment.

736

