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# A remarkable sensitivity enhancement in a gold nanoparticle-based lateral flow immunoassay for the detection of *Escherichia coli* O157:H7†

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Because of the distinctive features of ease-of-use, low cost and portable detection, a gold nanoparticle (AuNP) based lateral flow immunoassay (LFA) is an effective and currently used method for the detection of *Escherichia coli* O157:H7; however, its low sensitivity limits its practical use. In the present study, the size and uniformity of AuNPs have been systematically optimized to maximally amplify both the visual inspection signals (the color of test line) and the quantitative data (light intensity) recorded using a bioassay reader. The remarkable enhancement of detection sensitivity can be increased to  $10^2$  colony forming units per mL by taking advantage of the optimized AuNPs and the separated incubation of the AuNPs/antibody/*E. coli* O157:H7 complex. Quantitative detection of *E. coli* O157:H7 was partially obtained in a wide concentration range with good repeatability. The new, optimized AuNPs-based LFA is well suited to fast quantitative and qualitative food analysis.

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## 1. Introduction

Since its discovery in 1982, *Escherichia coli* O157:H7 has become a public health concern worldwide because of its capability of contaminating food and water, causing severe intestinal infection in humans such as gastrointestinal illness, hemolytic uremic syndrome, and occasionally kidney failure. The great demand for a rapid, accurate sensor that can be used widely is an urgent and challenging task for food safety. In the past few decades, numerous efforts have been devoted to various methods for the detection of *E. coli* O157:H7, including a molecular biological method (polymerase chain reaction-based analysis),<sup>1</sup> DNA and RNA probes,<sup>2</sup> surface plasmon resonance,<sup>3</sup> immunomagnetic separation analysis,<sup>4</sup> electrochemical biosensor,<sup>5</sup> and quartz crystal microbalance techniques.<sup>6</sup> Although each approach has its own advantages, most reports are usually of a time consuming method, and/or one that requires expensive equipment and skilled workers.

From the standpoint of ease/broadness of use, low cost and portable detection, lateral flow immunoassay (LFA), particularly, gold nanoparticle (AuNPs) based LFA, is an effective and

currently used method,<sup>7,8</sup> which is ideally suitable for on-site testing. Wang *et al.*<sup>9</sup> have reported a visually inspected LFA using AuNPs for simultaneous detection of three pesticides. Parolo *et al.*<sup>10</sup> have reported an enhanced LFA using AuNPs loaded with enzymes capable of detecting human immunoglobulin G (IgG). This paper was the inspiration establishing a special AuNP-based LFA to detect *E. coli* O157:H7,<sup>8</sup> but the sensitivity ( $10^4$  colony forming units (CFU) mL<sup>-1</sup>) was not very high and limits its practical use as a commercial product. The objective of the present study was to develop a high performance AuNP-based LFA for *E. coli* O157:H7 detection that would achieve high sensitivity and stability.

Generally, there are three ways to improve the detection sensitivity of an AuNP-based LFA such as designing a sensitive bioassay reader, optimizing the test procedure and improving the properties of the probe materials.<sup>11</sup> Compared with the other two ways, exploring the optimized label probes for LFA is a simple and effective means to improve the detection sensitivity. It is well known that AuNPs play a critical role in LFA, because both visual inspection signals (the color of the test line) and quantitative data (light intensity) recorded by the 'Assay Reader' originate from AuNPs, which are mainly dependent on their size, shapes, uniformity and aggregation behaviours,<sup>12–27</sup> as well as the wavelength coupling between the light source and AuNPs.

In this present study, the size and uniformity of AuNPs were systematically optimized to maximally amplify the detection signals to improve the sensitivity. In addition, the separated incubation of AuNPs/antibody/*E. coli* O157:H7 complex was used to modify the conventional AuNP-based LFA to improve the stability. The new optimized AuNPs-based LFA allowed us to

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detect *E. coli* O157:H7 with an estimated detection limit of  $10^2$  CFU mL<sup>-1</sup>, which is much lower (two orders in concentration) than that of a conventional AuNP-based LFA.

## 2. Experimental section

### 2.1. Reagents

Hydrogen tetrachloroaurate(III) trihydrate (HAuCl<sub>4</sub>·3H<sub>2</sub>O), sodium citrate (C<sub>6</sub>H<sub>5</sub>Na<sub>3</sub>O<sub>7</sub>·2H<sub>2</sub>O), and bovine serum albumin (BSA) were purchased from Sigma-Aldrich Chemical Co. (St. Louis, MO, USA). The sample pad, nitrocellulose (NC) membrane, conjugate release pad, and absorbent pad were obtained from Schleicher and Schuell GmbH (Dassel, Germany). The antibody pairs, namely, murine anti-*E. coli* O157:H7 monoclonal antibody and goat anti-*E. coli* O157:H7 polyclonal antibody and donkey anti-mouse IgG were purchased from Meridian Life Science, Inc (Memphis, TN, USA). Other reagents were of analytical grade and purchased from Sinopharm Chemical Corp. (Shanghai, China).

### 2.2. Instruments

A SkanFlexi BioAssay reader system for reading the AuNP-based LFA strip was supplied by the Skannex Biotech Co., Ltd. (Oslo, Norway). The BioDot XYZ platform combined with a motion-controller, BioJet Quanti3000k dispenser and an Air-JetQuanti3000k dispenser for solution dispensing were purchased from BioDot (Irvine, CA USA). The structures of the nanoparticles were observed using transmission electron microscopy (TEM) on a Jeol JEM-2010 electron microscope. Ultraviolet-visible (UV-Vis) absorption spectra were recorded using a TU-1810 UV-Vis spectrophotometer obtained from the Purkinje General Instrument Co. Ltd. (Beijing, China).

### 2.3. Bacterial strains and growth condition

Bacterial strains were prepared according to a method reported by Xie *et al.*<sup>8</sup> *E. coli* O157:H7 strain ATCC 43888 was cultured in Luria-Bertani medium (Oxoid, Basingstoke, UK) at 37 °C for 20 h before use. Serial dilutions of cultures in phosphate buffered saline (PBS, Sigma Chemical Company, St. Louis, MO, USA, 0.01 M, pH 7.4) were made and plated onto trypticase soy agar (Becton, Dickinson and Company, Sparks Glencoe, MD, USA) to determine the number of viable *E. coli* O157:H7 cells. The plates were then incubated at 37 °C for 24 h. The number of cells was counted when the bacterial colonies could be clearly seen on the plates.

### 2.4. Preparation of AuNPs of different sizes

AuNPs were prepared according to a method given in a previous report.<sup>26,28</sup> Briefly, 100 mL of  $2.5 \times 10^{-4}$  M HAuCl<sub>4</sub> solution was heated to 120 °C in an oil bath under vigorous stirring for 30 min. Then, a predetermined volume of 1% sodium citrate solution was added into the previous solution with continued boiling. After 20 min, the color of the boiled solution changed to ruby red, indicating the formation of AuNPs. The solution was cooled to room temperature before use in further experiments. Different predetermined volumes of sodium citrate solution would give different sized AuNPs.

### 2.5. Preparation of AuNPs with different polydispersity indices (PDIs)

AuNP solutions with different PDI were prepared by mixing two AuNP samples with the pre-widened PDI. The AuNPs with a PDI of 0.20 were prepared by the previously mentioned Frens method.<sup>24</sup> The other sample with a PDI of 0.65 was prepared as follows: 1 mL of 1% sodium citrate solution was added into 100 mL of  $2.5 \times 10^{-4}$  M boiled HAuCl<sub>4</sub> solution heated with an electric heating jacket. A series of AuNPs with the same plasmonic wavelength peak and different PDI such as 0.26, 0.39, 0.47, 0.52, and 0.61 were prepared by adjusting the ratio of the amount of the two AuNPs samples with pre-widened PDI.

### 2.6. Preparation of AuNP-antibody complex

The anti-*E. coli* O157:H7 monoclonal antibody (300 μL) with a concentration of 166 μg mL<sup>-1</sup> was added into 3 mL of a pH adjusted AuNP solution and was stirred for 60 min. Then, 0.15 mL of 3% (w/v) BSA solution was added and the solution was stirred for another 30 min. Later, 0.15 mL of 10% (w/v) PEG20000 solution was added and the mixture was stirred for another 30 min. The mixture was centrifuged at 9000g for 30 min and the precipitate was then dissolved in 300 μL of 50 mM Tris/HCl buffer. The AuNP-labeled monoclonal antibody complex was dried for 2 h at 30 °C before further use.

### 2.7. Preparation of AuNP test strips

A sample pad was pre-treated with 50 mM of borate buffer (pH = 7.4) containing 1% BSA, 0.5% Tween 20, and 0.05% sodium azide, and further dried at 60 °C for 2 h. The goat anti-*E. coli* O157:H7 polyclonal antibody (1.0 mg mL<sup>-1</sup>) and donkey anti-mouse IgG (1.0 mg mL<sup>-1</sup>) were sprayed onto the test (T) and control (C) lines on the NC membrane, respectively, and then dried at 35 °C. The NC membrane was blocked with 5% BSA in 0.02 M PBS (pH = 7.2) to avoid the background of the strip. The absorption pad and glass fibre membrane were used without further treatment. The NC membrane, absorption pad, glass fibre membrane, and pre-treated sample pad were assembled on a poly(vinylchloride) plate to form the final test strip.

### 2.8. Detection of *E. coli* O157:H7

The *E. coli* O157:H7 culture was diluted into different concentrations from  $2.8 \times 10^7$  to  $2.8 \times 10^2$  CFU mL<sup>-1</sup> in sterile PBS, which were then mixed with the AuNP-antibody complex. Then, the mixtures were placed onto the test strip. The SkanFlexiBioAssay Reader was used to quantitatively detect the *E. coli* O157:H7 after 10 min. All the experiments were performed in triplicate.

## 3. Results and discussion

Fig. 1 shows the schematic of conventional and modified AuNP-based LFA strips. Generally, the strip contains mainly three parts such as sample pad, NC membrane, and absorbent pad (AuNP-antibody conjugate pad, T and C line with modified corresponding antibodies). In the conventional strip (Fig. 1A),

the target analyte (*E. coli* O157:H7 culture) flow laterally through the test strip. Firstly they interact with the antibody-labelled AuNPs in the conjugate pad, and aggregate subsequently at the T line because of the specific interaction between the analyte and the antibody, which leads to a darkening color of the T line which is then detected optically. The non-*E. coli* O157:H7 cannot interact with the antibody-labelled AuNPs and no red line develops at the test line. The colored antibody-labelled AuNPs should bind to the C line and form a red-colored band regardless of the presence of *E. coli* O157:H7.

Unlike the conventional strip, a separated incubation of the target analyte was proposed for the modified strip (Fig. 1B), which gives LFA three distinctive advantages. Firstly, it eliminates the AuNP-antibody conjugate pad, making the fabrication of the strip easier. Secondly, the separated incubation of *E. coli* O157:H7 allows easier control of the reaction time (about 5 min), resulting in the complete interaction with antibody labelled AuNPs, rather than the instantaneous reaction at the AuNP-antibody conjugate pad. This effective incubation of *E. coli* O157:H7 with antibody labelled AuNPs gives a high detection performance. Lastly, the amount of the separated incubation of *E. coli* O157:H7 can be randomly increased, and used many times for a large quantity of strips, which significantly improves the stability and repeatability of the test.

It is well known that the size of the AuNPs has an important effect on the performance of AuNP-based LFA.<sup>28</sup> Large sized AuNPs usually have a high steric hindrance, which affects the interaction with the labelled antibody/target analytes and impedes the fluidity in the strip, while AuNPs that are too small are not the best option for showing visual inspection signals. In addition, different labelled antibodies/target analytes favour the interaction with different size AuNPs. For the detection of *E. coli* O157:H7 on a strip, people usually randomly choose AuNPs in the range from 20 to 60 nm; there is not much reported in the literature about the precise investigation of the small window of size effect on the detection performance.

In order to explore the cut-off size where both visual inspection signals and quantitative data (light intensity) could be optimal, AuNPs (gold spheres) were successfully synthesized

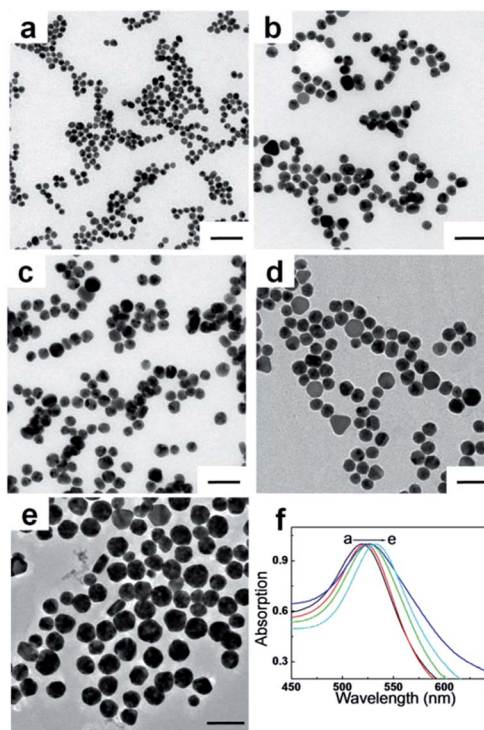


Fig. 2 Representative TEM images of AuNPs with different sizes (a): 20 nm; (b): 28 nm; (c): 35 nm; (d): 43 nm; (e): 54 nm) and their corresponding UV-Vis absorption spectra (f). The scale bar represents 100 nm.

in a finely tuned size range from 20 to 54 nm. Fig. 2 shows the TEM images of AuNPs of various sizes. It was demonstrated that the smallest AuNPs have a relatively good uniform shape, whereas larger AuNPs are mixed with non-spherical AuNPs, and have a relatively broad size distribution. The average sizes that were obtained from the TEM results were  $20 \pm 1$  nm,  $28 \pm 1$  nm,

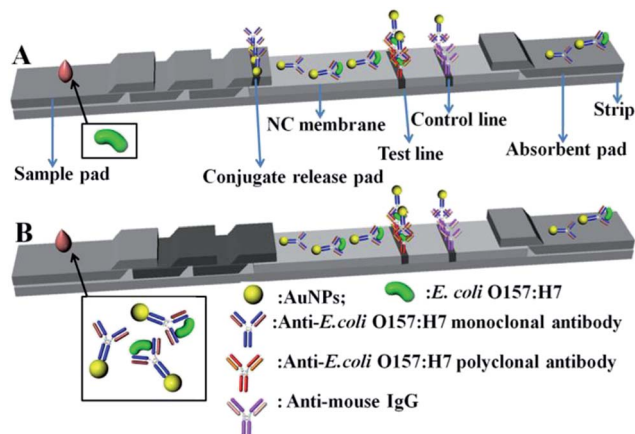


Fig. 1 Schematic of conventional (A) and modified (B) AuNP-based lateral flow immunoassay strips.



Fig. 3 Specificity of strip for the detection of *E. coli* O157:H7 (from 0 to  $10^7$  CFU mL<sup>-1</sup>) using 35 nm AuNPs.

**Table 1** The optical density on the T line in the detection of *E. coli* O157:H7 (from 0 to  $10^7$  CFU mL<sup>-1</sup>) using different sized AuNPs

Concentration (CFU mL <sup>-1</sup> )	Signal intensity of different sized AuNPs based LFA in T line									
	20 nm		28 nm		35 nm		43 nm		54 nm	
	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD
PBS	28	1	63	5	37	2	44	5	82	2
$2.8 \times 10^7$	238	10	208	2	746	32	377	21	202	19
$2.8 \times 10^6$	413	15	712	23	722	28	865	50	443	39
$2.8 \times 10^5$	284	8	287	8	872	26	782	31	392	32
$2.8 \times 10^4$	125	6	132	9	324	31	209	18	110	15
$5.6 \times 10^3$	101	6	101	5	108	12	126	15	109	12
$2.8 \times 10^3$	58	5	97	10	121	15	95	11	65	7
$5.6 \times 10^2$	7	2	90	3	100	7	8	2	32	3
$2.8 \times 10^2$	10	3	56	6	64	10	32	5	30	5

35 ± 1 nm, 43 ± 2 nm, and 54 ± 3 nm. The UV-Vis absorption spectra (Fig. 2f) correspond to samples shown in Fig. 2a–e. As the size of the AuNPs increases from 20 to 54 nm, the absorption peaks are noticeably red-shifted from 518 to 533 nm, showing a good agreement with results from previous reports. The different sized AuNPs obtained were used as labelled probes for testing the signal source to investigate the detection efficiency and sensitivity of *E. coli* O157:H7 in LFA.

The different sized AuNPs were first labelled with a monoclonal antibody, which interacts with *E. coli* O157:H7 and forms an AuNP/antibody/*E. coli* O157:H7 complex *via* the separated incubation. The complex flowed in the strip and was captured by the goat anti-*E. coli* O157:H7 polyclonal antibody at the T line. The visually inspected color and optical intensity at the T line can be used to evaluate the detection performances quantitatively and qualitatively, respectively.

Fig. 3 shows a typical batch of AuNP-based LFA strips used to investigate the detection performances of *E. coli* O157:H7 with 35 nm AuNP-based LFA. The detection procedure was repeated at least three times. In the present study, the visual inspection limit was defined as the minimum analyte concentration required for no obvious visual color on the T line. Following this definition, the visual qualitative inspection limit achieved with 35 nm AuNPs was around  $10^3$  CFU mL<sup>-1</sup>. The other sizes of AuNPs labelled LFA samples showed a visual qualitative inspection limit of  $10^3$ ,  $10^4$ ,  $10^5$  and  $10^6$  CFU mL<sup>-1</sup>, corresponding to AuNPs sizes of 20, 28, 43 and 54 nm, respectively.

In order to precisely and quantitatively study the detection performance of different sized AuNP probes, the test strips were further subjected to optical density analysis. The light scattering signal of the AuNP aggregates on the T line was monitored using a specific reader. The optical densities of the T line under different concentrations of *E. coli* O157:H7 from different sized AuNP labelled LFA T lines were recorded and are shown in Table 1. Generally, the optical densities decreased with the decrease of the concentration of *E. coli* O157:H7. Usually, a threshold value was set to determine the detection limits based on the optical density from the instrument, which can be roughly calculated from average signal intensity and standard deviation (SD) of the negative control (PBS) on the T line. The

threshold value was the total contribution of the average signal intensity and three times the SD (average intensity + 3SD). The corresponding concentration of *E. coli* O157:H7 can be seen as the detection limit, when the detected optical value is bigger than the threshold value. The values highlighted in red in Table 1 were used to show the detection limit from different sized AuNP labelled LFA T lines. The optical density (64 au) on the T line from a 35 nm AuNPs labelled probe was strong enough to be detected even though the concentration of *E. coli* O157:H7 was as low as  $10^2$  CFU mL<sup>-1</sup>. The same detection process was repeated three times and similar detection limits of  $10^2$  CFU mL<sup>-1</sup> were obtained, which indicated good reproducibility.

Fig. 4 shows the clear relationship between the size of the AuNPs and the detection performances of *E. coli* O157:H7 in LFA T lines. It is observed that the detection limit from the optical density at the T line firstly decreases as the size of the AuNPs becomes larger up to 35 nm, and then suddenly increases as the size of the AuNPs continues to increase. This finding implies that neither a small nor a big size of AuNPs benefits the detection limits of *E. coli* O157:H7. The cut-off size is optimized to 35 nm for the best detection performances of *E. coli* O157:H7 in AuNP-based LFA. As far as steric hindrance and the optical properties of AuNPs are concerned, smaller sized AuNPs generally have smaller steric hindrance, which



**Fig. 4** The relationship between the size of AuNPs and the detection limits of *E. coli* O157:H7. C is the concentration of *E. coli* O157:H7 at the detection limit.

Table 2 The optical density on the T line in the detection of *E. coli* O157:H7 (from 0 to  $10^7$  CFU mL<sup>-1</sup>) using different PDI AuNPs

Concentration (CFU mL <sup>-1</sup> )	Signal intensity of AuNPs with different PDI based LFA in T line									
	0.26		0.39		0.47		0.52		0.61	
	Mean	SD	Mean	SD	Mean	SD	Mean	SD	Mean	SD
PBS	37	2	55	3	99	2	53	1	60	2
$2.8 \times 10^7$	746	23	237	15	312	10	148	12	171	12
$2.8 \times 10^6$	722	26	645	50	566	32	413	22	351	23
$2.8 \times 10^5$	872	31	242	16	467	41	587	31	127	11
$2.8 \times 10^4$	324	27	168	20	143	15	128	8	58	10
$5.6 \times 10^3$	108	12	99	11	73	6	52	3	33	5
$2.8 \times 10^3$	121	15	69	9	42	5	50	2	34	2
$5.6 \times 10^2$	100	8	42	10	40	5	16	3	30	3
$2.8 \times 10^2$	64	9	14	2	33	6	12	3	28	3

provides a strong absorption with antibodies and *E. coli* O157:H7, and also facilitates their fluidity in the strip, while the larger sized AuNPs in a small size window would offer better optical signals for detection performances. Another possible reason is that the optimized size (35 nm) of the AuNPs has a plasmonic resonance wavelength of 525 nm, which is the same as the wavelength of the light source in the bioassay reader. This coupling effect of light wavelength<sup>29,30</sup> would maximally amplify the optical properties of AuNPs for the detection of *E. coli* O157:H7.

The size uniformity of AuNPs was further investigated to evaluate the detection performances of *E. coli* O157:H7 in AuNP-based LFA. In order to eliminate the light wavelength coupling effect, all the samples with different PDI (ESI Fig. 1f†) have the same plasmonic resonance wavelength at 525 nm, which were prepared by artificially mixing the different sized AuNP solutions together. The PDI of AuNPs (ESI Fig. 1a–e†) was tuned into 0.26, 0.39, 0.47, 0.52, and 0.61. The optical densities of T line under different concentrations of *E. coli* O157:H7 with AuNP labelled LFA with different PDIs are shown in Table 2. It is very clear to see that the higher PDIs lead to the higher detection limit (Fig. 5). It is speculated that the possible reason is follows: all samples have the same plasmonic resonance wavelength at 525 nm, which corresponds to AuNPs of 35 nm, which is the

optimized size for the best detection. A sample with a lower PDI should contain more AuNPs with 35 nm, which offer bigger contributions to the detection performance; whereas the fewer AuNPs with a size of 35 nm in samples with a higher PDI would lead to the worst detection limits. A sample with a lower PDI was of much more higher uniformity than that with a higher PDI, which provided the optimized optical signals and smaller steric hindrance for absorption with the antibody and *E. coli* O157:H7. These conditions would lead to the best detection performance.

## 4. Conclusions

In this research it has been shown that a new modified AuNP-based LFA can remarkably improve the detection performance of *E. coli* O157:H7. Firstly, the separated incubation of *E. coli* O157:H7 and the antibody labelled AuNPs significantly improve the stability of the strip and the repeatability of the experimental data. Secondly, a cut-off size of AuNPs in a small size window was found to maximally amplify both visual inspection and optical signals. The newly optimized AuNP-based LFA will provide the possibility of fast quantitative and qualitative food analysis.

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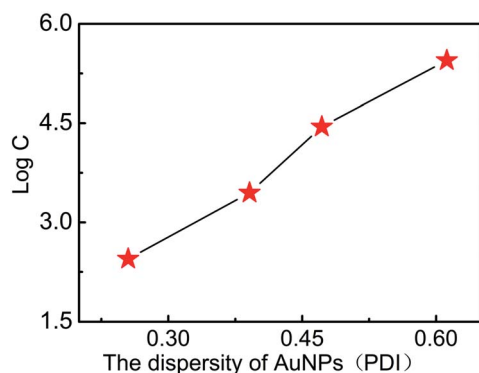


Fig. 5 The relationship between the PDI of AuNPs and the detection limits of *E. coli* O157:H7 (C is the concentration of *E. coli* O157:H7).

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