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## PAPER

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### 1. Introduction

One of the most prevalent factors affecting human health is air pollution according to the World Health Organization (WHO).<sup>1</sup> Due to NO<sub>2</sub>, NH<sub>3</sub>, H<sub>2</sub>S, CO<sub>2</sub>, *etc.*, which are considered the most hazardous pollutants, the ambient environment becomes contaminated, which can lead to fatal conditions such as lung cancer, heart attack, strokes, skin allergies, asthma and neurological disorders.<sup>2–6</sup> Moreover, an upsurge in automobilization and industrialization has led to an enormous rise in the emissions of NO<sub>2</sub> gas, which is one of the most common hazardous gases. NO<sub>2</sub> released by industrial processes, vehicle exhaust and combustion endanger human health. The thinning of the ozone layer and the development of acid rain are some of the causes of NO<sub>2</sub>, which affects aquatic, terrestrial and human lives.<sup>7–9</sup> Thus, NO<sub>2</sub> gas sensing equipment is in high demand.

<sup>b</sup> Department of Materials Science and Engineering, University of Illinois at Urbana-Champaign, Urbana, IL, 61801, USA

## Fabrication of a room-temperature NO<sub>2</sub> gas sensor with high performance at the ppb level using an rGO/BiOCl heterostructure†

Neeraj Dhariwal,<sup>a</sup> Preety Yadav,<sup>a</sup> Amit Sanger,<sup>a</sup> Sung Bum Kang, <sup>b</sup> M. S. Goyat, <sup>c</sup> Yogendra Kumar Mishra<sup>d</sup> and Vinod Kumar \*

In recent years, the continuous and accurate detection of human hazardous gases, such as NO<sub>2</sub>, using a low-cost gas sensing device is quite important. For a new generation of gas sensors, rGO or 2-D materials have gained considerable attention. This work presents a low-temperature rGO/BiOCl heterojunction fabricated NO<sub>2</sub> gas sensor that exhibits an excellent response ( $R_g/R_a = 3.78$ ) for NO<sub>2</sub> at 100 ppb compared to pristine BiOCl. The selected synthesis pathway results in the generation of a perforated floral morphology. Moreover, the sensor showed outperforming selectivity with a quick response/recovery of ~9 s/21 s at ambient temperature (25 °C). Additionally, it has an ultralow LOD (~0.06 ppb). Besides, the mechanism of gas sensing was initially elucidated through finite-difference time-domain (FDTD) simulation. This analysis confirms that rGO in BiOCl serves as a bridge, enhancing the transfer of electrons from BiOCl to NO<sub>2</sub> and resulting in a substantial increase in the depletion region and a heightened sensor response. Our fabricated NO<sub>2</sub> gas sensor offers a low gas detection limit with high accuracy and fast response at even lower temperatures.

Two-dimensional layered materials, such as graphene and MXenes, have been thoroughly studied owing to their high mechanical strength, excellent carrier mobility and high surface-to-volume ratio.<sup>10–13</sup> Numerous promising materials, including graphene and its derivatives, which have a larger surface area, are theoretically viable and can be used to detect gases. Additionally, their 2-D planar structure facilitates charge transport with brief diffusion paths. rGO has been widely used for gas sensor fabrication, which facilitates surface enhancement and functionalisation.<sup>14–16</sup> In contrast to graphene, rGO can increase adsorption energy and promote the adsorption of gases, which remains unaffected by orientation/sites. Consequently, rGO flakes have attracted attention as a potential component of gas-sensing materials.

Bismuth oxychloride, or BiOCl, is believed to be the most significant component of two-dimensional materials. It builds the [X–Bi–O–Bi–X] structure layer by layer and is joined by interlayered van der Waals forces and intra-layer bonding.<sup>17</sup> Because of its amazing structural, optical, and physiochemical qualities, this material has been used in various applications, including water filtration and catalysis.<sup>18,19</sup> However, this material has not been studied much in the realm of gas detection, especially NO<sub>2</sub>. Semiconductor materials supported by rGO have been considered the most appropriate composite material for gas sensing devices because of the substantial amount of physisorption sites.<sup>20,21</sup> When combined with rGO, several common metal oxides, including ZnO, SnO<sub>2</sub>, WO<sub>3</sub> and

<sup>&</sup>lt;sup>a</sup> Department of Physics, NSUT, Dwarka sec-3, New Delhi-110078, India. E-mail: vinod@nsut.ac.in

<sup>&</sup>lt;sup>c</sup> Department of Applied Science, School of Engineering, University of Petroleum and Energy Studies, Dehradun, 248007, Uttarakhand, India

<sup>&</sup>lt;sup>d</sup> Mads Clausen Institute, SDU NanoSYD, University of Southern Denmark, Alsion 2, DK-6400, Sønderborg, Denmark

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#### Paper

CuO, demonstrated improved gas sensing capabilities compared to base metal oxides.<sup>22–25</sup> Despite this, the non-uniform hybridization between rGO and metal oxides leads to a ring-like deposition because particles are concentrated on droplet edges as a result of the coffee ring effect.<sup>26,27</sup> Consequently, the sensitivity and repeatability of the manufactured sensors are severely reduced.<sup>28–32</sup> Therefore, it was necessary to fabricate a novel and effective composite to detect NO<sub>2</sub> gas with high sensitivity along with the small size and ultrathin morphology of the rGO/BiOCl nanocomposite. The obtained structure can enhance the number of available active sites and electrical conductivity, which can further increase gas sensing performance. Thus, it is fascinating to investigate nanocomposites that exhibit strong selectivity towards NO<sub>2</sub> gas.<sup>33</sup>

In this regard, we fabricated heterogeneously assembled rGO flakes on semiconductor material, i.e. bismuth oxychloride. The rGO/BiOCl nanocomposites are synthesized using a one-step hydrothermal technique without any precipitating agent. The manufactured gas sensor has a high level of NO<sub>2</sub> gas selectivity and has minimal effect on humidity with remarkable sensitivity and excellent response/recovery time at room temperature (25 °C). The outstanding catalytic function of rGO and the charge transmission occurring between rGo flakes and BiOCl nanoflower account for this remarkable performance. Because rGO with a two-dimensional structure defines a large surface-tovolume ratio, more active sites are available. The accessible active sites are responsible for the catalytic activity of rGO, which improves sensor performance. Furthermore, rGO's electrical structure has a significant catalytic process conductive nature. In rGO, electron transport during catalytic processes is facilitated by  $sp^2$  hybridised carbon atoms with delocalized pi-electrons. The kinetics of the catalytic process taking place on the rGO surface are improved by this electron mobility, which also strengthens the charge transfer mechanism. Simulation of rGO/BiOCl by finite difference time-domain confirms the improved build-in potential, leading to efficient gas detection sites when used as a gas sensor. The methodology proposed in

this work could result in the development of a 2-D material/ semiconductor hybrid  $NO_2$  gas sensor with higher sensitivity.

### 2. Experimental section

#### 2.1. Synthesis

A one-step hydrothermal process was used to yield BiOCl and rGO/BiOCl (see Fig. 1). To synthesize mesoporous floral, such as BiOCl, 6.58 g of Bismuth Nitrate (Bi(NO<sub>3</sub>)<sub>3</sub>·5H<sub>2</sub>O) (purity 98%, Merck) was dissolved in 19 mL of ethylene glycol, and 0.78 g sodium chloride (NaCl) (purity 99%, Sigma Aldrich) was dissolved in 3 mL de-ionized (DI) water and allowed to stir at 500 rpm for 30 min at 50 °C to form a homogeneous mixture. After that, both solutions were mixed thoroughly at 500 rpm for 1 h at 70 °C. Simultaneously, rGO along with DI water at different amounts (0-4 wt %) was allowed to ultrasonicate for 2 h. Afterwards, the rGO solution was mixed with a BiOCl solution for 1 h to attain a homogeneous mixture. Then, both the suspensions (i.e. containing rGO and BiOCl salt solution) were transferred into the autoclave and allowed to remain at 150 °C for 15 h. After obtaining precipitates, contaminants were removed by centrifuging them at 8000 rpm and rinsing them several times with DI. Prior to drying in a vacuum oven at 100 °C for 24 h to obtain floral, such as BiOCl and rGO/BiOCl.

#### 2.2. Gas sensing setup

A well-defined experimental setup contributes valuable insights into the gas sensing field. Fig. 2 illustrates the sensing setup used for this study. The setup includes a robust design for valuable and accurate measurements. The experimental setup includes a gas sensing chamber of 3 mL volume in which a controlled amount of  $NO_2$  is purged with precise measurement and standard instruments to monitor the gas level.  $NO_2$  gas (Sigma Aldrich, 1 ppm, with dry air used for balancing gas concentration) was combined with dry air using two Mass Flow Controllers (MFCs, MF-3000), which were further inserted into

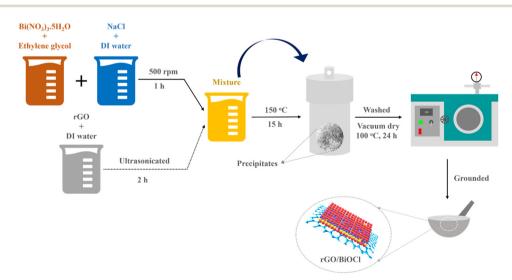


Fig. 1 Synthesis route for rGO/BiOCl heterostructure.

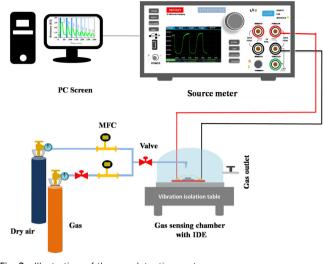


Fig. 2 Illustration of the gas detection system.

the gas sensing chamber with the desired gas concentration. Further, the gas flow rate was set at 100 SCCM. Additionally, an IDE comprising advanced sensing material was placed within the chamber to keep track of and evaluate the gas interactions. Gas sensing setup includes a Keithley 2450 source meter for real-time detection of sensor response towards varying NO<sub>2</sub>. All these measurements are performed under a controlled environment and a room temperature of 25 °C.

#### 2.3. Sensor fabrication

There are numerous effective methods for the deposition of nanoparticles, which have been employed for required monolayer and multilayer colloidal crystal processes.<sup>34</sup> Because the spin coating technique is flexible, affordable, and easy to fabricate, we chose it for the creation of single-layered colloidal-based sensors. Initially, the surface of the electrodes was cleaned with hexane and anhydrous ethanol, which were further desiccated for 1 h at 60 °C. The 10 mg synthesized BiOCl and rGO/BiOCl were initially dispersed in 1 mL ethanol, followed by spin coating over interdigitated electrodes (IDE), as shown in Fig. 3, at 4000 rpm for 1 min, then dried for 30 min at 80 °C and was further used for NO<sub>2</sub> sensing.

#### 2.4. Characterization

The formulation, phase, and generated strain of the synthesized nanoparticles were examined by X-ray diffraction within a  $2\theta$  range from 20° to 80° using Cu-k $\alpha$  radiation. The morphology and interfacial structure of the synthesized samples were envisioned using a scanning electron microscope (SEM) with elemental mapping. Raman spectroscopy was employed to understand the structural characteristics of the synthesized materials. UV-Vis spectrometry and dielectric measurements were performed to better understand the electronic and optical properties. The total surface area and pore volume of BiOCl and rGO/BiOCl were measured using BET. To investigate the manufactured sensor's reaction to NO<sub>2</sub> gas, *I–V* characterization was performed. Specific environmental conditions were maintained in the test chamber for the sensor device.

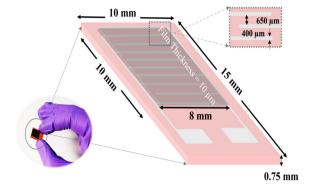


Fig. 3 Thin film-based sensor fabrication over IDE

### 3. Results and discussion

#### 3.1. Structural evaluation

Fig. 4(a) shows the XRD peaks of the synthesized BiOCl and rGO/ BiOCl nanoparticles. The peak position along with the corresponding planes matches the JCPDS number 06-0249, confirming the proper phase formation. The observed pattern demonstrates that the peaks of rGO/BiOCl shift along with the broadening of the peaks, which is due to changes in lattice parameters and the strain developed between the bonds. Analysis of the data yielded the tetragonal structure, and the crystallinity was determined using the Debye Scherer formula<sup>35</sup>:

$$D = \frac{k\lambda}{\beta\cos\theta},\tag{1}$$

where *k* represents the Scherer's constant, *i.e.* 0.9;  $\lambda$  denotes the wavelength of Cu-k $\alpha$  radiations; and  $\beta$  and  $\theta$  denote FWHM and Bragg's angle, respectively. Moreover, the lattice constant was examined by applying eqn (2):

$$d_{hkl} = \frac{1}{\sqrt{\frac{h^2 + k^2}{a^2} + \frac{l^2}{c^2}}},$$
(2)

where  $d_{hkl}$  is used to represent interplanar spacing, which can be determined with Eqn (3):<sup>36</sup>

$$d_{hkl} = \frac{\lambda}{2\sin\theta}.$$
 (3)

Further, the X-ray density ( $\rho_{XRD}$ ) for BiOCl and rGO/BiOCl is examined by employing eqn (4):<sup>37,38</sup>

$$\rho_{\rm XRD} = \frac{ZM}{Na^3},\tag{4}$$

where *Z* and *N* denote the number of molecules per unit cell and Avogadro number, respectively, and *M* and  $a^3$  represent the molecular weight and volume of the unit cell, respectively. Additionally, the mass of the sample (*m*) and its volume (*V*) were used to calculate bulk density ( $\rho_{exp}$ ), as indicated by Eqn (5):<sup>39</sup>

$$\rho_{\exp} = \frac{m}{V}.$$
 (5)

The measured values of both  $\rho_{\rm XRD}$  and  $\rho_{\rm exp}$  are demonstrated in Table 1, indicating that X-ray density increases for

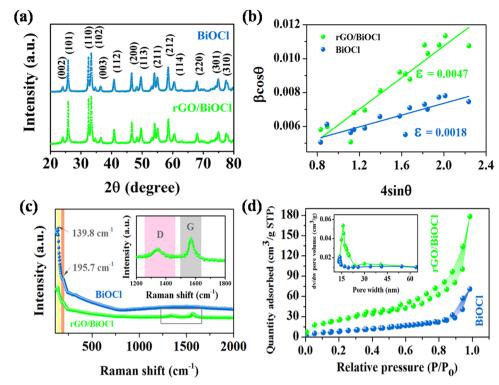


Fig. 4 (a) XRD peaks pattern, (b) Williamson–Hall plot, (c) Raman spectra and (d) N<sub>2</sub> sorption isotherm for pristine BiOCl and rGO/BiOCl along with the pore size distribution curve (inset).

rGO/BiOCl, which is the primary reason why synthesized samples have porosity, and the porosity was calculated using the following formula:  $^{40}$ 

$$P = 1 - \frac{\rho_{\exp}}{\rho_{\rm XRD}}.$$
 (6)

We can recognize the difference in both densities in Table 1. The variation in densities in the samples is related to porosity, which may explain the existence of pores in the synthesized materials.

Additionally, the Williamson–Hall plot between  $\beta \cos \theta$  and  $4\sin \theta$  was used to determine the strain developed by forming a nanocomposite using eqn (7):<sup>41</sup>

$$\beta\cos\theta = \frac{k\lambda}{D_{\rm WH}} + 2\varepsilon\sin\theta,\tag{7}$$

Where  $\varepsilon$  represents the generated strain in the material and  $\frac{k\lambda}{D_{\rm WH}}$  represents the intercept of the fitted line. The W–H plot for BiOCl and rGO/BiOCl has been shown in Fig. 4(b), exhibiting a rising trend in the strain after modification by rGO, which is due to dislocation formation at the interface between rGO

Table 1         Parameters calculated using XRD							
Sample	Crystallite size (nm)	$ ho_{ m XRD} ({ m g} \ { m cm}^{-3})$	$ ho_{ m exp}$	Porosity (P)	Strain (ɛ)		
BiOCl rGO/BiOCl	28.8 25.7	21.1 27.3	4.2 2.2	0.79 0.91	0.0018 0.0047		

and BiOCl when rGO is added to BiOCl. These dislocations simultaneously cause an increase in lattice strain and serve as a focus of concentration for stress. Additionally, fluctuation in bond length and bond angle of Bi–O and Bi–Cl could generate lattice strain.<sup>42–44</sup>

#### 3.2. Raman spectroscopy

When examining the structural characteristics of carbon present materials, Raman spectroscopy is a vital tool. The Raman spectra of rGO/BiOCl and BiOCl are displayed in Fig. 4(c). Pure BiOCl is represented by the tetragonal structure of space group P4/nnm with  $A_{\rm 1g},~B_{\rm 1g},~E_{\rm g1}$  and  $E_{\rm g2}$  acting as its four active modes.45 Two prominent bands are observed in the BiOCl spectrum. The bands at 139.8 cm<sup>-1</sup> and 195.7 cm<sup>-1</sup> are assigned to A1g and Eg1 stretching modes between Bi-Cl. All Raman bands of BiOCl are observed in the rGO/BiOCl sample. The D and G bands are two separate peaks located at 1345 cm<sup>-1</sup> and 1570 cm<sup>-1</sup>, respectively, observed in rGO/BiOCl, which confirms the rGO presence.46 The D band is attributed to defects, disorders and edges. The G band is formed by graphite's well-ordered sp<sup>2</sup> carbon, which arises from the zone center E<sub>2g</sub> mode. According to the Raman spectra of rGO/BiOCl, the D and G bands are highly intense, suggesting an increment in sp<sup>2</sup> domain size and further verifying the brittleness of oxygen atoms, which is favourable for gas sensing.47,48 Moreover, the rGO/BiOCl sample showed that all the rGO Raman bands were present, as indicated, demonstrating the successful creation of rGO/BiOCl.

#### 3.3. N<sub>2</sub> sorption isotherm

Using the nitrogen-sorption isotherm, the precise surface properties and pore volume of the synthesized nanomaterials were determined, and the results are shown in Fig. 4(d). The BiOCl/ rGO nanocomposite is categorized as a type II isotherm by IUPAC with an H3-type hysteresis loop, having a wide variety of pore sizes, which suggests the presence of a mesoporous structure.49 The volume of pores present in rGO/BiOCl increases by 4 times, *i.e.* 0.148 cm<sup>3</sup> g<sup>-1</sup> in comparison to 0.037 cm<sup>3</sup> g<sup>-1</sup> (BiOCl), and the average pore size increases to 15.7 nm from 12.6 nm, resulting in the highly porous nature of synthesized rGO/BiOCl. Based on calculations, the specific area of the surface of rGO/BiOCl was found to be 68.72 m<sup>2</sup> g<sup>-1</sup>, which is approximately 5 times higher than that of BiOCl (13.19 m<sup>2</sup> g<sup>-1</sup>). More active sites that facilitate gas adsorption and reaction during sensing may be available on a larger attainable surface area, allowing for a quicker response and improved sensitivity.<sup>50,51</sup>

#### 3.4. Morphological analysis

The interfacial structure, morphology and composition of BiOCl and rGO/BiOCl nanoparticles were evaluated by SEM (scanning electron microscopy). Fig. 5(a) displays the BiOCl SEM images, which suggest that the synthesized BiOCl was composed of a perforated floral-like hierarchical structure with uniform width and thickness. According to Fig. 5(b), the assynthesized BiOCl and rGO are evenly mixed in the nanocomposite, and the crinkled rGO thin layers firmly adhere to the BiOCl's outer layer to form an intact hybrid heterojunction. Furthermore, a rGO/BiOCl nanocomposite exhibits relatively smaller and thinner flakes of the perforated flower than BiOCl. This may be due to the introduction of rGO into the precursor, which provides nucleation sites in which BiOCl can form and prevent crystal growth.<sup>52</sup>

Furthermore, rGO/BiOCl nanocomposites provide an active surface modification position for BiOCl due to the rGO's oxygen

comprising functional groups, which results in a more regular shape than pure BiOCl.<sup>53</sup> It also experiences strain, demonstrated by the W–H plot, indicating the reason behind lattice distortion, which comparatively increases porosity and the surface-to-volume ratio. Because of the additional voids created by the rGO/BiOCl nanocomposite, there are more active sites that improve  $NO_2$  gas detection. Elemental distribution is examined by elemental color mapping (see Fig. 5), which validates the successful formation of rGO/BiOCl nanocomposite.

#### 3.5. Electronic and optical properties

The band structure of pristine BiOCl and rGO/BiOCl is shown in Fig. 6(a), which demonstrates the band gap energy by applying a Tauc plot using the Tauc relation:<sup>54</sup>

$$(\alpha h\nu)^2 = (h\nu - E_{\rm g}), \qquad (8)$$

Where  $\alpha$ , *h* and *v* denote absorption co-efficient, Plank's constant and frequency, respectively. Moreover,  $E_g$  denotes the material's band gap energy.

Pristine BiOCl displays a band gap value of 3.7 eV. Furthermore, rGO leads to a reduction of energy to 3.1 eV when added to BiOCl by transferring electrons to the Fermi level. In the case of rGO/BiOCl, the electronic structure is disturbed due to addition of rGO to BiOCl, which creates an additional number of energy states within the band structure, resulting in a reduced band gap. In contrast, rGO plays an important role in introducing new pathways for charge carriers, which leads to a decrease in the band gap and an increase in conductivity. Additionally, the chemical interaction between the bands of Bi-C has a significant effect on the charge transfer property. To better understand the electrical conductivity of BiOCl and rGO/BiOCl, an impedance study was conducted. As shown in Nyquist plots (see Fig. 6(b)) for BiOCl and rGO/BiOCl, heterojunction shows a small diameter of the semicircle, indicating a higher charge transfer property with lower resistance.55

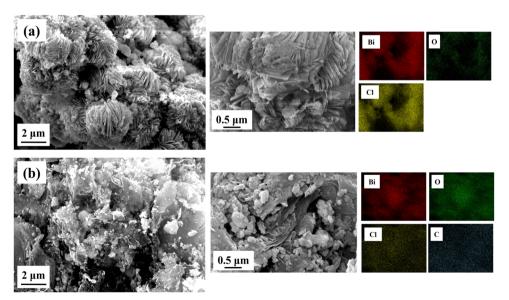
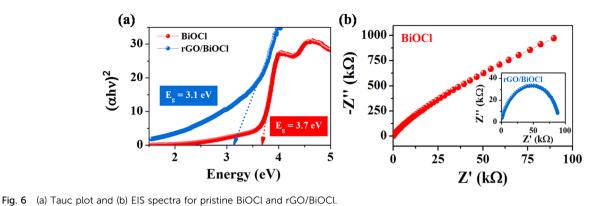


Fig. 5 Obtained morphology of (a) pristine BiOCl and (b) rGO/BiOCl along with elemental mapping using SEM.



The results revealed that the synergistic effect arising from the heterojunction of rGO/BiOCl significantly augmented the electron mobility of the system.

#### 3.6. Gas sensing performance

The sensing capability of both fabricated BiOCl and rGO/BiOCl (see Fig. 7(a)) was performed under a controlled environment at a room temperature of 25 °C. As illustrated in Fig. 7(b), when the fabricated sensor comes into contact with NO<sub>2</sub>, sensor resistance increases, indicating n-type sensor behavior. Initially, BiOCl was tested under the NO<sub>2</sub> gas exposure of 100 ppb, as shown in Fig. 7(b).

The sensor responded within  $\tau_{\rm res} = 35$  s, while  $\tau_{\rm rec} = 57$  s with a sensor response of  $\frac{R_{\rm g}}{R_{\rm a}} = 1.72$ ,<sup>56</sup> which is calculated using the following formula:

Response 
$$=\frac{R_g}{R_a}$$
, (9)

where  $R_{\rm g}$  and  $R_{\rm a}$  are the resistances of the sensor in the presence of gas and air, respectively.

Interestingly, rGO/BiOCl heterojunction shows excellent enhancement in sensor response, *i.e.*  $\frac{R_g}{R_c} = 3.78$ , with quick reaction time ( $\tau_{res}$  = 9 s) and restoration/recovery time ( $\tau_{rec}$  = 21 s) for 100 ppb at room temperature (see Fig. 7(c)); additionally, response/recovery times at different NO<sub>2</sub> concentrations are studied (see Fig. S1, ESI<sup>+</sup>). With the addition of rGO to BiOCl, the material becomes more conductive, thereby facilitating the kinetics of charge transfer while reacting with gas. The elevation in electrical conductivity yields a rapid and enhanced sensor response. Additionally, a fabricated heterojunction structure may suppress the rate of recombination of generated charge carriers while interacting with NO<sub>2</sub> gas, leading to more variation in electrical conductivity and, henceforth, higher sensor response. Furthermore, the addition of rGO enhanced the sensor's specific surface area, generating more active gas interaction sites. The sensor displays higher sensitivity and remarkable repeatability, as displayed in Fig. 7(d). The primary cause of the sensor's amazing performance is the conductive bridge formed due to rGO stacking using BiOCl with its porous nature and higher surface area. Moreover, the fabricated sensor tested up to a

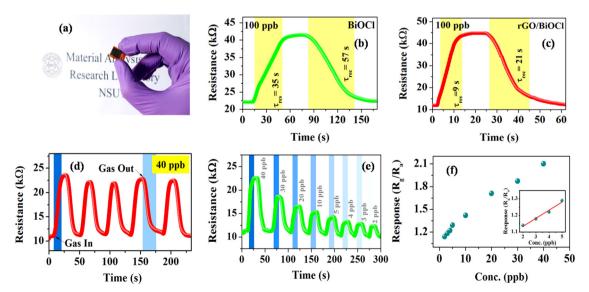


Fig. 7 (a) Thin film deposited over IDE, (b) and (c) response curve for BiOCl and rGO/BiOCl, (d) sensing repeatability curve for rGO/BiOCl, (e) variation in sensor response with different ppb levels and (f) the limit of detection for rGO/BiOCl.

low detection limit of 2 ppb (see Fig. 7(e) and Fig. S2, ESI<sup>†</sup>); theoretically, the value was obtained to be ultralow, *i.e.* 0.06 ppb (see Fig. 7(f)). The linear fit for the sensor response with ppb shows a resultant slope of 0.049 with a 0.99 value of  $R^2$ .

Variation in rGO concentration (0.5-4 wt%) in BiOCl was also tested, as shown in Fig. 8, which does not exhibit a monotonically straightforward trend. Initially, at lower concentrations of rGO, it leads to the enhancement of the sensing properties along with its electrical conductivity up to a certain threshold, and the further addition of rGO content leads to diminishing results and adverse effects on sensing parameters. This is possibly due to the agglomeration of rGO sheets and an alternating decrease in active sites, which can alter the interaction between NO<sub>2</sub> gas and material. However, the formation of a local junction enhances the depletion region; moreover, the conductivity and simultaneously lower sensor resistance. Therefore, a higher response at 2 wt% is due to the well-dispersed rGO flakes.

Selectivity is one of the salient features of any gas sensor studied by the behavior of gas with the sensor surface.57-59 Various gases, including NO, CO<sub>2</sub>, CH<sub>4</sub>, H<sub>2</sub>, H<sub>2</sub>S, NH<sub>3</sub> and NO<sub>2</sub>, were tested, while the sensor best responded to NO2 with a response of 3.78 times (see Fig. 9(a)). The electronic configuration and sensor surface characteristics of heterojunctions create preferential binding sites for NO<sub>2</sub> gas molecules, promoting the specific interaction of NO2 gas with the sensor, which leads to enhanced sensitivity compared to other gases. The impact of humidity on sensor response was investigated to learn more about the environmental effect, as shown in Fig. 9(b).<sup>60</sup> Artificial humidity was created inside the gas chamber. It is clear from the obtained results that the sensor response gradually reduced by 12% with an increased humidity of 90%. Water vapours at high humidity hinder gas molecules from reacting with the sensor surface or thwarting the process of chemisorptions.<sup>61</sup> In contrast, the sensor response was carried out at varied temperatures (near environmental temperature).<sup>62</sup> Fig. 9(c) illustrates how an increase in

temperature is linked to an increase in sensor response because of an increase in the quantity of surface electrons. The sensor also responded even at temperatures below RT although the sensor response was less at 0 °C. The diffusion rate of  $(NO_2)$  gas through the material at lower temperatures is quite slow, which reduces contact with the active sites and, correspondingly, the sensor response. Fig. 9(d) shows the stability of the rGO/BiOClbased sensor towards  $NO_2$  at 100 ppb for a long time.<sup>63</sup> Fig. 9(d) demonstrates a total decrease of 4% in the sensor response after 25 days. These studies suggest that the incorporation of superior performance and mixed dimensional gas sensors, coupled with a better understanding of underlying mechanisms, could lead to new possibilities in hybrid sensor platforms based on 2D materials.

#### 3.7. Gas sensing mechanism

Fig. 10 illustrates the rGO/BiOCl-based sensing mechanism towards NO<sub>2</sub> gas, where the rGO/BiOCl sensor works on the adsorption mechanism. Initially, ionization of oxygen molecules occurs at the sensor surface, extracting surplus electrons and simultaneously inducing alteration in both carrier concentration  $(N_d)$  and formation of a potential barrier  $(qV_{s1})$ . Temperature also plays a role in the type of adsorbed oxygen.<sup>64</sup> Elevation in the vertical position of  $qV_{s1}$ , further to  $qV_{s2}$  with NO<sub>2</sub> exposure results in the subsequent reduction in the electric current.

$$O_{2(air)} \rightarrow O_{2(ads)}$$
 (10)

$$O_{2(ads)} + e^{-} \rightarrow O_{2(ads)}^{-}$$
(11)

$$O_{2(ads)}^{-} + e^{-} \rightarrow 2O_{(ads)}^{-}$$
 (12)

$$NO_2 + 2O_{(ads)}^- \rightarrow NO_2^- + O_{2(ads)}^-$$
 (13)

Thus far, charge transport through heterojunction can only be simplified using numerical, but sensing performance with charge transportation can be explained easily using Fig. 10. The same is applied to the transduction function of the heterojunction-based sensor. Using eqn (14) and (15), the effect of the heterojunction on

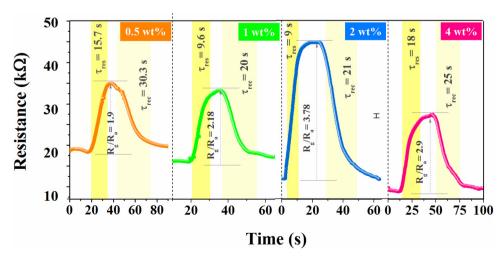


Fig. 8 Effect on NO $_2$  sensing behavior with variation in rGO concentration (0.5–4 wt%).

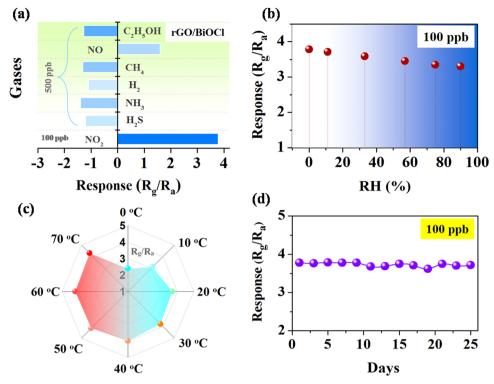


Fig. 9 (a) Sensor's selectivity using various gases, (b) the effect of humidity, (c) the effect of temperature and (d) the long-duration stability of the rGO/BiOCl-based sensor.

sensor performance with charge transport properties can be easily studied by measuring the height difference in the potential barrier.<sup>65</sup> The charge transport property between the overlapping particles is modulated by adsorbate-induced variation in the height of the potential barrier  $\Delta V_{\rm s}$  at the junction. Electron mobility within the junction region can be explained by thermo-electronic emission.<sup>66</sup> The sensing response is contingent upon the adsorbate-induced fluctuating height of the potential barrier, which can be defined as follows:

$$V_{\rm s} = \frac{2\pi Q_{\rm s}^2}{\varepsilon N_{\rm d}} = \frac{2\pi (qN_{\rm s})^2}{\varepsilon N_{\rm d}},\tag{14}$$

Response = 
$$\frac{R_g}{R_a} \approx \exp\left(\frac{e\left(\frac{V_{s2}}{V_{s1}}\right)}{kT}\right)$$
, (15)

where e, Q, k, T and  $\varepsilon$  are the elementary charge, surface charge density, Boltzman constant, operating temperature and dielectric constant, respectively. Therefore, flakes of rGO along with the associated functional group of oxygen can modulate potential barriers, which is advantageous for improving the response of gas sensing. Moreover, the enhanced point defects on the heterojunction of rGO/BiOCl provide more surface for adsorption of NO<sub>2</sub> gas and a more effective sensor response when compared to previously published NO<sub>2</sub> gas sensors (see Table 2).

The work functions of rGO ( $\Phi$  = 4.75 eV) and BiOCl ( $\Phi$  = 7.35 eV) allow for the formation of the Schottky junction, which additionally creates a bridge for the exchange of electrons from

BiOCl to rGO. Initially, the interaction of the sensor surface with the oxygen molecule forms oxygen ion species when the heterojunction composed of rGO/BiOCl is subjected to air (see Fig. 10). However, in the NO<sub>2</sub> environment, adsorption of gas molecules occurs, which preferentially interacts with the chemisorbed oxygen present. The adsorbed molecule of NO<sub>2</sub> gas entails the sequestration of electrons from O<sup>-</sup> and O<sup>2-</sup> ions present on the surface. Consequently, the greater number of electrons consumed is there to produce chemisorbed oxygen species and, henceforth, fewer electrons in rGO/BiOCl. Therefore, the region of depletion and the height of the barrier enlarge; correspondingly, sensor resistance increases (see Fig. 10).

The propensity of rGO flakes to undergo self-aggregation and self-connection is observed. The aforementioned effect continues to facilitate the development of a depletion layer over BiOCl despite the presence of local junctions. Interestingly, because of their significantly higher conductivity, the conduction pathway partially shifts towards interconnected rGO flakes, which reduces the sensor resistance. The depletion region widens when the fabricated sensor is exposed to NO<sub>2</sub> gas; however, the resistance change or resultant response is not noticeable due to well-connected rGO flakes, which allow easy charge transfer. Consequently, a boost in the sensor's response is elucidated as a result of the advantageous impact of evenly distributed rGO flakes. To better understand the sensing mechanism and to design a more sensitive gas sensor, FDTD simulation is used based on the Crowell-size model and the drift Diffusion-Poisson equation at the interface to determine the distribution of electric potential with rGO. We observed that

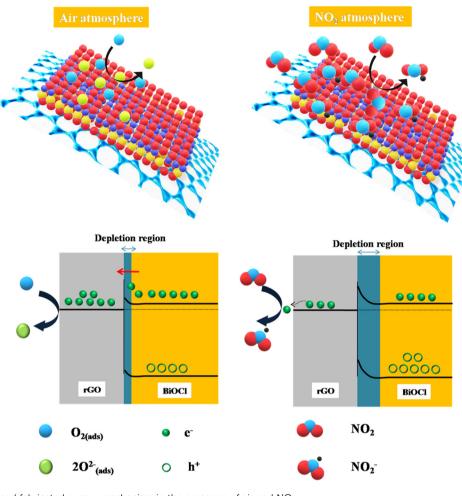


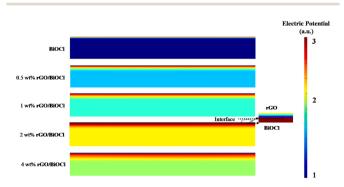
Fig. 10 rGO/BiOCI-based fabricated sensor mechanism in the presence of air and NO<sub>2</sub>.

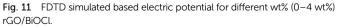
Materials	Conc. (NO <sub>2</sub> )	$\tau_{res}/\tau_{rec}$ (s)	Sensitivity/ response	Ref.
SnS <sub>2</sub>	10 ppm	170/140	36.33	67
rGO	10 ppm	71/310	21.56%	68
WSe <sub>2</sub> nanoflakes	0.05 ppm	50/1050	5.06%	69
$MoS_2$	100 ppm	71/310	21.56%	70
rGO-SnS <sub>2</sub>	5 ppm	50/48	32	71
Fe <sub>2</sub> O <sub>3</sub> @rGO	100 ppb	100/—	1.23	72
ZnO-rGO	5 ppm	165/499	25.6%	73
In2O3@rGO	500 ppb	4.2/13.3 min	15%	74
Co <sub>3</sub> O <sub>4</sub> -rGO	60 ppm	_/	80%	75
rGO-BiOCl	100 ppb	9/21	3.78	This study

Table 2 Properties of previously studied NO<sub>2</sub> gas sensors

the  $NO_2$  gas molecules became closer to the top view of the platform. The field of electric potential can be observed, which deteriorates the sensing execution of the fabricated sensor (see Fig. 11).

BiOCl has a wide band gap that limits sensor sensitivity under normal ambient light at RT. In contrast, the lower conductivity of BiOCl compared to rGO results in less efficient charge transfer and a slower sensor response. Further, when rGO/BiOCl interacts with electrophillic NO<sub>2</sub>, transfer of electrons from rGO/BiOCl to  $NO_2$  occurs, leading to a decrease in BiOCl carrier concentration, and this is why the potential barrier also increased linked with the wider depletion region. The increased sensor response has multiple causes. Firstly, in heterojunctions, such as rGO/BiOCl, specifically 2 wt% rGO, an inversion layer may form at the interface because of the different work functions and band alignments of the two materials. Secondly, electrons and holes are effectively separated in a heterojunction where the





conduction band of one material is shorter compared to the valence spectrum of the other. This separation is necessary to enhance the sensor sensitivity.<sup>76–81</sup> The pronounced build-in potential in the vicinity of the rGO/BiOCl heterojunction interface results in the formation of a significant depletion layer and a long range of coulomb interaction is generated. Interestingly, the increase in electric potential at the interface also augments the force of electrostatics within, indicating the active role of rGO in NO<sub>2</sub> sensing as a catalytic agent. However, after a certain level (>2 wt%), it shows higher conductivity, which in turn leads to a low level of modulation between the rGO and BiOCl interface, further deteriorating the sensor's sensing performance. These results match well with the experimental data.

### 4. Conclusions

In the present investigation, we delineate the conceptualization and fabrication of an ultrasensitive sensor to monitor NO2 gas in the environment. The rGO/BiOCl-dependent gas sensing material was created using a straightforward, one-step hydrothermal process, which was further coated over IDE using the spin coating technique. The heterojunction rGO/BiOCl sensor achieved an excellent response of 3.84 times with quick response/recovery time ( $\tau_{\rm res}/\tau_{\rm rec}$ = 9 s/21 s) at RT (25 °C). Moreover, this developed sensor has ultralow theoretical LOD ( $\sim 0.06$  ppb) and long-term durability. The pivotal rise in the sensor's performance is attributed to the rGO flakes providing chemisorption sites for oxygen molecules. One of the major factors is the Schottky junction formed between rGO and BiOCl, which further promotes the transport of charge carriers to the NO2 gas molecules. This phenomenon actively contributes to rising sensing dynamics, as observed in the system. The elucidation of the sensing mechanism is done initially using FDTD simulation. The outcome of the aforementioned study clarifies that the presence of rGO in rGO/ BiOCl facilitates the substantial movement of electrons from BiOCl to NO2 gas. This occurrence of this phenomenon leads to the expansion of the depletion region, which in turn causes the sensor response to increase. This study provides new insight into room temperature ultrasensitive NO2 gas sensors along with a low detection range for environmental and biomedical applications.

### Conflicts of interest

The authors declare no conflicts of interest.

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